



Spatial-Temporal Modeling for Nanoscale Resolvement of Photo-Switching Fluorophores

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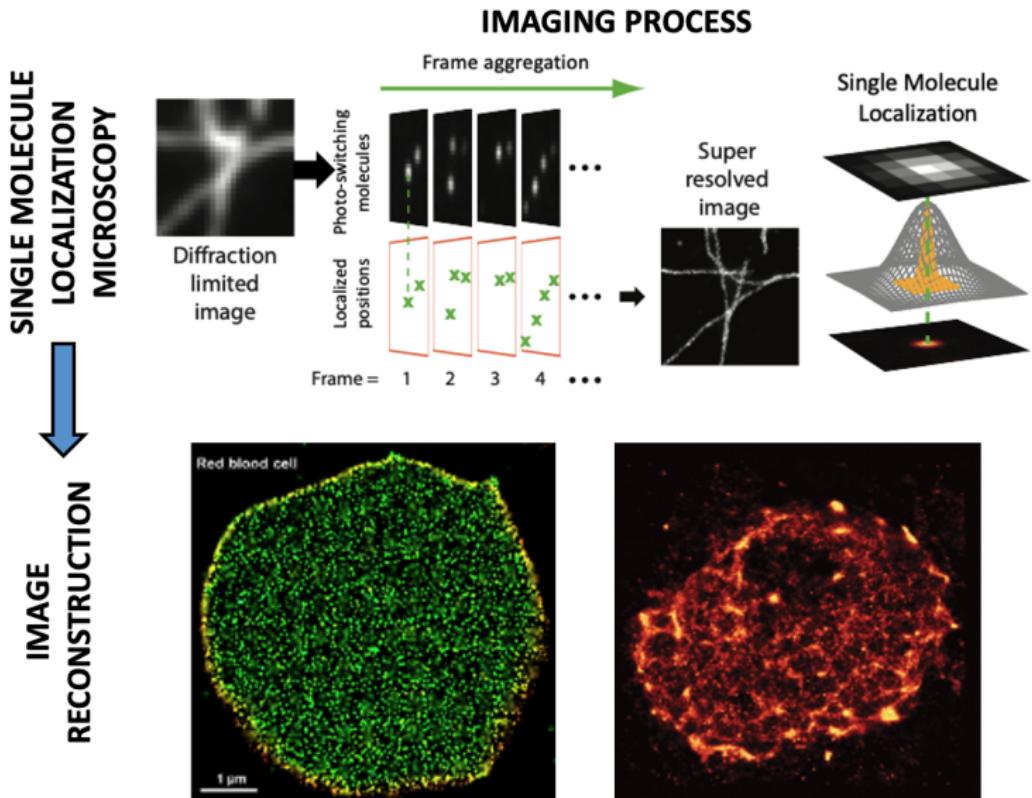
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Fluorescence Imaging I



- Imaging at high optical resolutions is frequently achieved via *stochastic* photo-switching of molecules over $\approx 10^4$ frames (Betzig et al., 2006; Heilemann et al., 2008).
- Stochastic imaging takes many different forms: DNA-PAINT, (f)PALM, (d)STORM.
- Enables sparse subsets to be detected at any one time.
- Allows us to retrieve their spatial coordinates with high precision.
- Large cellular structures/mechanisms can be imaged.

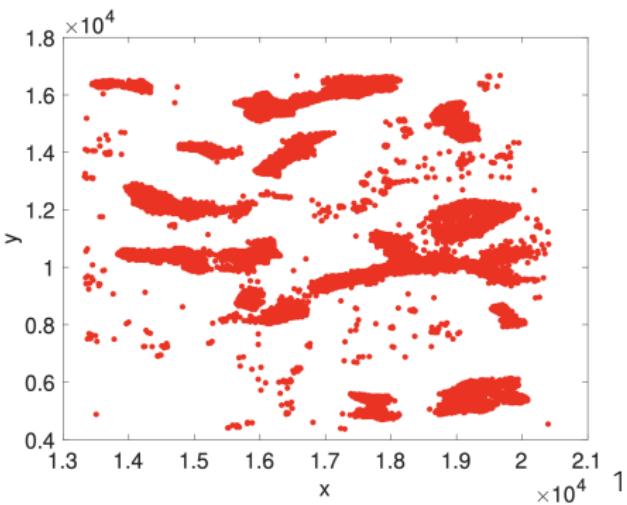
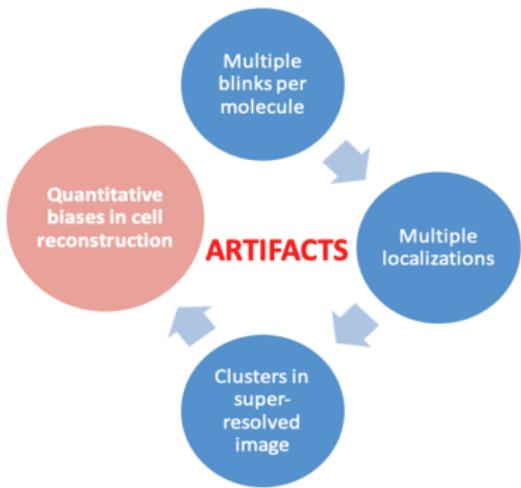
Obtaining super-resolution images I



Obtaining super-resolution images II



- Final superresolution images obtained by *superimposition* of frames.
- Final image shows dense spatial data around molecules of interest, which motivates spatial analyses.



¹Data made available courtesy of Prof. Paul French at ICL.

Stochastic photo-switching I

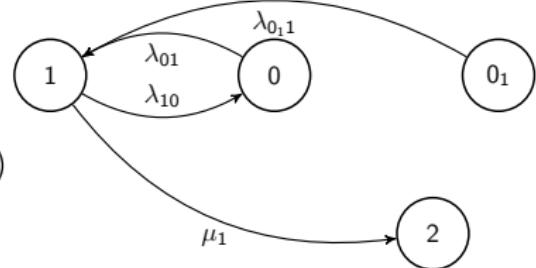
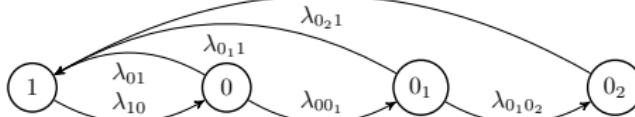
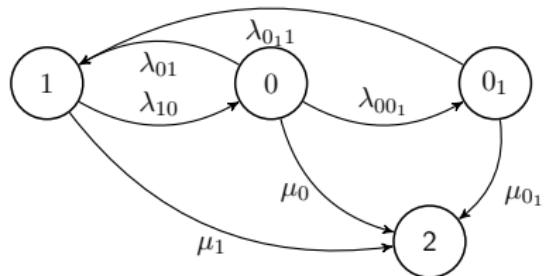
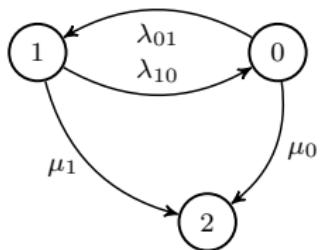


- The *photo-switching* behavior gives key information about the molecule e.g. inherent structure, pH, temperature.
- A molecule can be detected at most once in a single frame.
- Each frame gives a single representation of the mechanisms under observation.
- Utilizing the time domain in stochastic superresolution is key for analyzing underlying spatial structures.

1 We can better understand molecular structures given partially-observed localizations through time. **How do we build a spatial model that leverages temporal characteristics?**

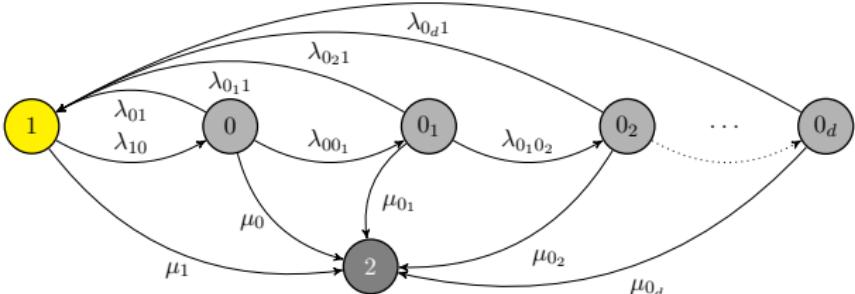
2 Can we use this to predict photo-switching rates and underlying spatial positions, including molecular count?

Characterizing photo-switching I



The photo-switching process $X(t)$

- For each molecule, let $\{X(t)\}_{t \in \mathbb{R}_{\geq 0}}$ be its underlying continuous time Markovian signal.
- Accesses a single on state (1), $d + 1$ off states ($0, 0_1, \dots, 0_d$) and an absorption state (2).
- Its state space is $\mathcal{S}_X = \{0, 0_1, \dots, 0_d, 1, 2\}$.
- $d = 0$ for DNA-PAINT, BALM.
- $d = 1$ for (f)PALM.
- $d = 2$ for (d)STORM Patel et al. (2019, 2021)



The generator G

$$G = \begin{pmatrix} -\sigma_0 & \lambda_{00_1} & 0 & 0 & 0 & \dots & \lambda_{01} & \mu_0 \\ 0 & -\sigma_{0_1} & \lambda_{0_10_2} & 0 & 0 & 0 & \dots & \lambda_{0_11} & \mu_{0_1} \\ 0 & 0 & -\sigma_{0_2} & \lambda_{0_20_3} & 0 & 0 & \dots & \lambda_{0_21} & \mu_{0_2} \\ \vdots & \vdots & \vdots & \vdots & \vdots & \vdots & \ddots & \vdots & \vdots \\ 0 & 0 & 0 & 0 & 0 & \dots & -\sigma_{0_d} & \lambda_{0_d1} & \mu_{0_d} \\ \lambda_{10} & 0 & 0 & 0 & 0 & 0 & \dots & -\sigma_1 & \mu_1 \\ 0 & 0 & 0 & 0 & 0 & 0 & \dots & 0 & 0 \end{pmatrix}$$

- The transition probability matrix $P_t = e^{Gt}$ for any $t \geq 0$ is such that $P_t(i, j) = \mathbb{P}(X_t = j | X_0 = i)$.

The non-zero transition rates λ_G in G are *unknown*.



The observation process I

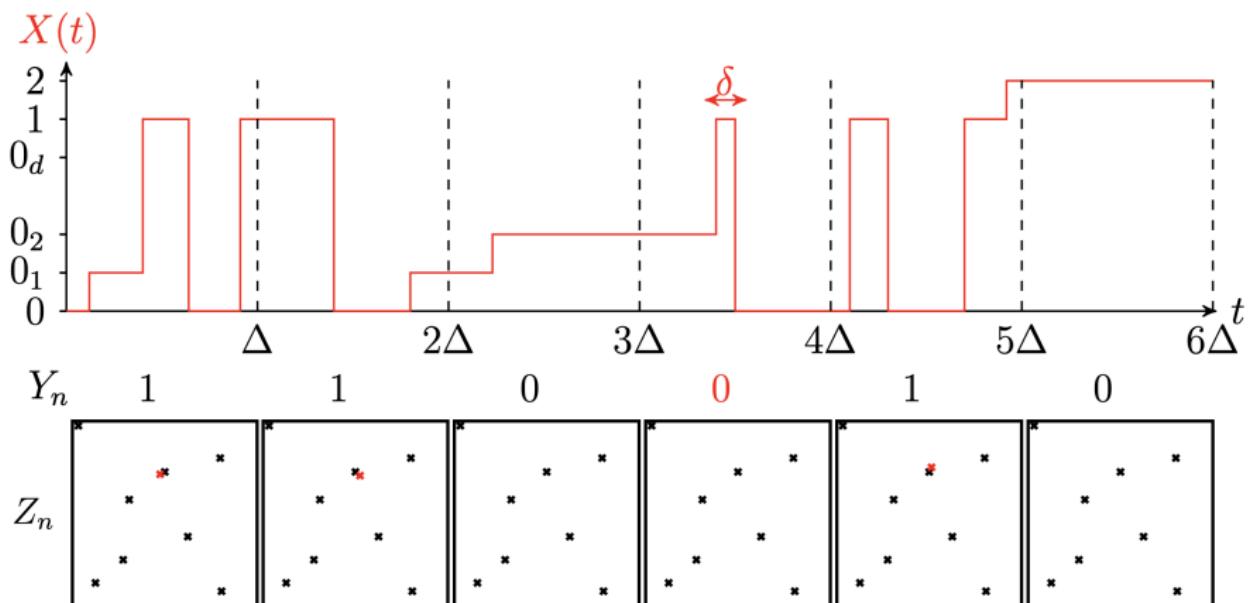
- Consider K (known for now) molecules filmed over N_F frames.
- Frame length Δ , minimum localization time is $\delta \in [0, \Delta)$.
- Let $\{Y_{n,k} \in \{0, 1\}, n = 1, \dots, N_F\}$ be the discrete-time binary process indicating whether emitter k is localized in frame n .
- $\{Z_{n,k} \in W \subset \mathbb{R}^m, n = 1, \dots, N_F\}$ is the *spatial localization process*. If $Y_{n,k} = 0$, no observation is made. Otherwise, an observation about its true spatial position $\mathbf{c}_k \in W$ is made.

$$T_{n,k} = \int_{(n-1)\Delta}^{n\Delta} \mathbb{1}_{\{1\}}(X_k(t)) \, dt, \quad Y_{n,k} = \mathbb{1}_{[\delta, \Delta)}(T_{n,k}).$$

$$Z_{n,k} = \begin{cases} \emptyset & \text{if } Y_{n,k} = 0 \\ \mathbf{z} \sim \mathcal{N} \left(\mathbf{c}, \frac{\Delta}{N_p T_{n,k}} I_2 \right) & \text{if } Y_{n,k} = 1, \end{cases}$$

N_p is the expected number of continuously emitted photons on Δ .

The observation process II



Ideal data tensor

Ideal data tensor \mathcal{Z} uses \mathcal{Y} to give *exact* fluorescent/binding spatial localizations for *each* molecule:

$$\mathcal{Z} = \begin{array}{c|ccccccc} & & & & \text{No. molecules} & & & \\ & & & & \hline & 1 & 2 & 3 & \dots & K-1 & K & \\ \hline \text{No. frames} & 1 & \left(\begin{array}{cccccc} \mathbf{z}_{1,1} & \mathbf{z}_{1,2} & \mathbf{z}_{1,3} & \dots & \mathbf{z}_{1,K-1} & \emptyset \\ \mathbf{z}_{2,1} & \emptyset & \emptyset & \dots & \mathbf{z}_{2,K-1} & \emptyset \\ \mathbf{z}_{3,1} & \mathbf{z}_{3,2} & \emptyset & \dots & \mathbf{z}_{3,K-1} & \mathbf{z}_{3,K} \\ \emptyset & \emptyset & \emptyset & \dots & \emptyset & \emptyset \\ \emptyset & \emptyset & \mathbf{z}_{5,2} & \emptyset & \dots & \emptyset & \emptyset \\ \vdots & \vdots & \vdots & \vdots & \ddots & \vdots & \vdots \\ N_F - 1 & \emptyset & \emptyset & \emptyset & \dots & \emptyset & \mathbf{z}_{N_F-1,K} \\ \hline N_F & \emptyset & \mathbf{z}_{N_F,2} & \emptyset & \dots & \emptyset & \emptyset \end{array} \right) \end{array}$$

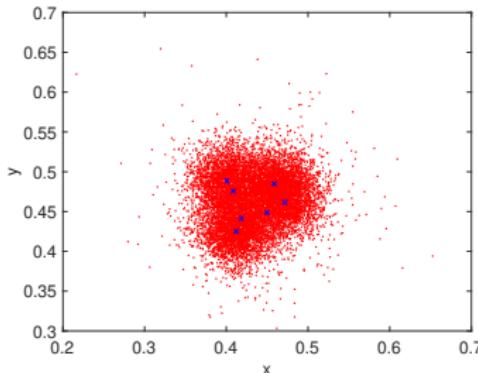
Why is the ideal case ideal?

The format of data gives us:

- The exact **number of imaged molecules**.
- The frame in which each molecule is localized.
- The **spatial localization** of each molecule.

Spatial reconstruction of true molecular positions, or *cluster positions* $\mathcal{C} = (\mathbf{c}_1, \mathbf{c}_2, \dots, \mathbf{c}_K)$ can be computed via Gaussian MLE:

$$\hat{\mathbf{c}}_k = \frac{1}{\sum_{n: \mathcal{Z}_{n,k} \neq \emptyset} 1} \sum_{n: \mathcal{Z}_{n,k} \neq \emptyset} \mathbf{z}_{n,k}.$$



Why is the ideal case ideal?

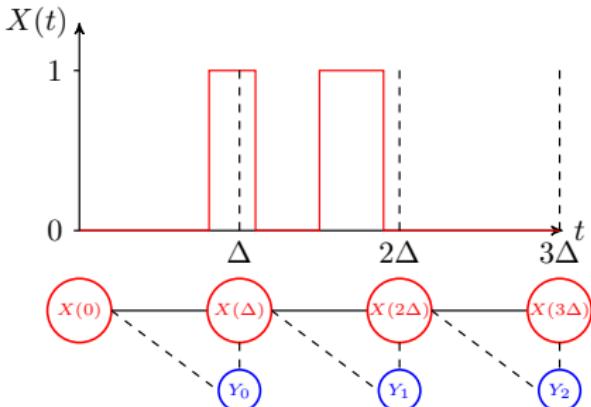


The format of data gives us:

- The exact **number of imaged molecules**.
- The **frame in which each molecule is localized**.
- The spatial localization of each molecule.

Fluorescence/binding rates in G can be estimated using \mathcal{Y} with the photo-switching Hidden Markov Model (PSHMM) (Patel et al., 2019), characterized with:

- **Initial probability vector**
 $\nu_X := \nu_i = \mathbb{P}(X(0) = i)$.
- **Transmission matrices**
 $B_{\Delta}^{(l)} := B_{\Delta}^{(l)}(i, j) = \mathbb{P}(Y_n = l, X(\Delta) = j | X(0) = i)$.





Biological imaging data

- If molecules are sufficiently well-separated in space, post-processing image recognition algorithms can be used to accurately obtain data as \mathcal{Y} and \mathcal{Z} (Lin et al., 2015).
- In dense spatial structures of interest, obtaining sufficiently good spatial separation between molecules is highly challenging, if not impossible, to engineer.
- In this case, obtaining \mathcal{Y} , \mathcal{Z} and K (number of molecules) is more difficult to obtain from imaging data alone.
- In each frame, localization algorithms fitting point-spread function to high-photon intensity regions will obtain spatial localizations; *including false positive localizations*.
- In each frame, a set of spatial localizations is obtained, without specific molecular labels.

Spatial localization set time series



No. frames	Aggregate (set union) localizations over K					
	1	2	3	...	$K - 1$	K
$Z_1 = \{z_{1,1}, z_{1,2}, z_{1,3}\}$	$z_{1,1}$	$z_{1,2}$	$z_{1,3}$...	\emptyset	\emptyset
$Z_2 = \{z_{2,1}, z_{2,K-1}\}$	$z_{2,1}$	\emptyset	\emptyset	...	$z_{2,K-1}$	\emptyset
$Z_3 = \{z_{3,2}, z_{3,K-1}\}$	\emptyset	$z_{3,2}$	\emptyset	...	$z_{3,K-1}$	\emptyset
$Z_4 = \emptyset$	\emptyset	\emptyset	\emptyset	...	\emptyset	\emptyset
:	:	:	..	:	:	:
$Z_{N_F-1} = \{z_{N_F-1,K}\}$	\emptyset	\emptyset	\emptyset	...	\emptyset	$z_{N_F-1,K}$
$Z_{N_F} = \{z_{N_F,2}\}$	\emptyset	$z_{N_F,2}$	\emptyset	...	\emptyset	\emptyset

Instead of the ideal data tensor, we have the **spatial localization set time series** $\{Z_n : n = 1, \dots, N_F\}$ of localizations in each frame by molecular and false-positive aggregation (set union):

$$Z_n = A_n \cup \left\{ \bigcup_{k=1}^K \mathcal{Z}_{n,k} \right\}.$$



Inference problem

Using the spatial localization sets $\{Z_n\}_{n=1}^{N_F}$, we want to estimate:

- The number of molecules K .
- Their spatial positions $\mathcal{C} = \{\mathbf{c}_1, \mathbf{c}_2, \dots, \mathbf{c}_K\}$.
- Fluorescence/binding rates.

Spatial point process

A (simple, finite) spatial point process $\mathcal{C} = \{\mathbf{c}_1, \mathbf{c}_2, \dots, \mathbf{c}_K\}$ contains **random spatial points** with density $f(\mathbf{c})$ over W with **cardinality distribution** $p_K(k)$ on $\mathbb{Z}_{\geq 0}$. Its density function is

$$f(\mathcal{C}) := k! p_K(k) \prod_{\mathbf{c} \in \mathcal{C}} f(\mathbf{c}).$$

Since observations sets Z_n are related to \mathcal{C} , we aim to infer:

$$f(\mathcal{C} | \{Z_n\}_{n=1}^{N_F}) \propto f(\{Z_n\}_{n=1}^{N_F} | \mathcal{C}) \pi(\mathcal{C}).$$



A pure spatial birth process I

- Before a molecule first fluoresces/binds, it ceases to be part of the underlying molecular configuration.
- We introduce a *hidden spatial point process* $\{C_n : n = 1, \dots, N_F\}$ which gives the number and positions of molecules that have already been activated before or in frame n .
- Each C_n can be probabilistically compared with Z_n at each frame.
- C_n has the property that $C_n \xrightarrow{P} \mathcal{C}$.

Under any ν_X we define for $n \geq 1$

$$C_n = C_{n-1} \cup B_n$$

$$C_0 = \emptyset$$

$$Z_n = \Phi(C_n) \cup A_n$$



A pure spatial birth process II

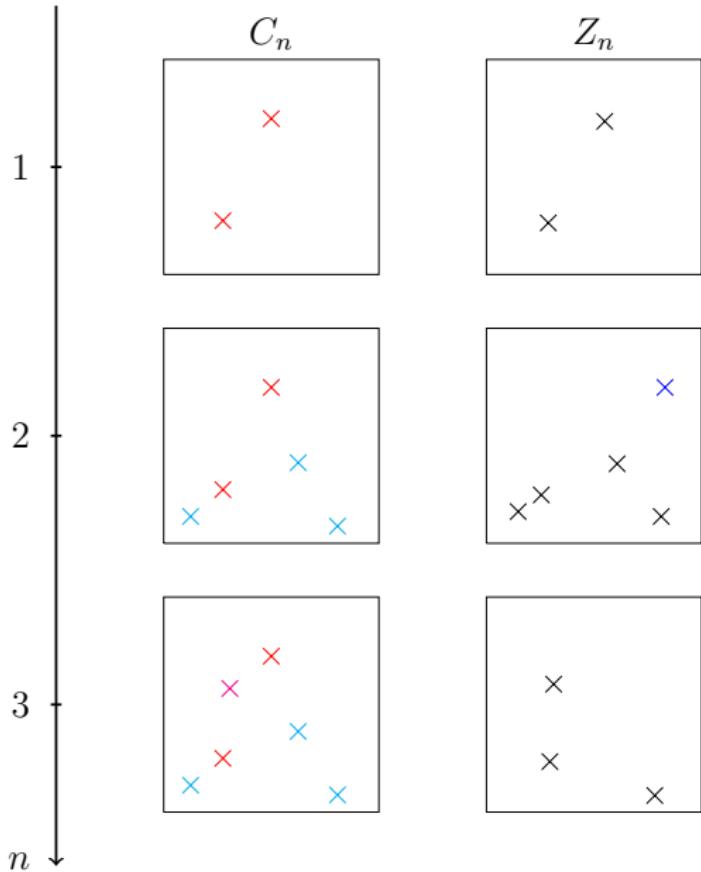
- B_n denotes the point process of molecules that are first activated in frame n .
- A_n denotes the point process of false positive observations, with rate α , in frame n .
- Each $\mathbf{c} \in C_n$ generates an offspring $\mathbf{z} \in \Phi(C_n)$, where \mathbf{z} is a variate from the density

$$f(\mathbf{z}^* | \mathbf{c}) = \mathcal{N} \left(\mathbf{c}, \frac{\Delta}{N_p T_n} I_2 \right),$$

with probability $p_{D,n}$ and is empty with probability $1 - p_{D,n}$.

$$\mathbf{z} = \begin{cases} \emptyset & \text{with probability } 1 - p_{D,n} \\ \{\mathbf{z}^*\} & \text{with probability } p_{D,n} f(\mathbf{z}^* | \mathbf{c}). \end{cases}$$

An illustration



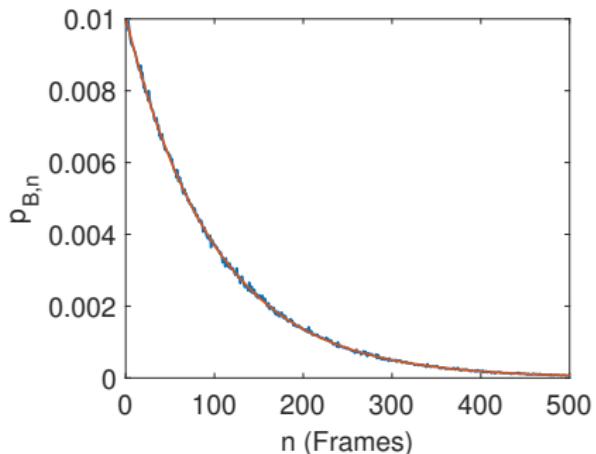
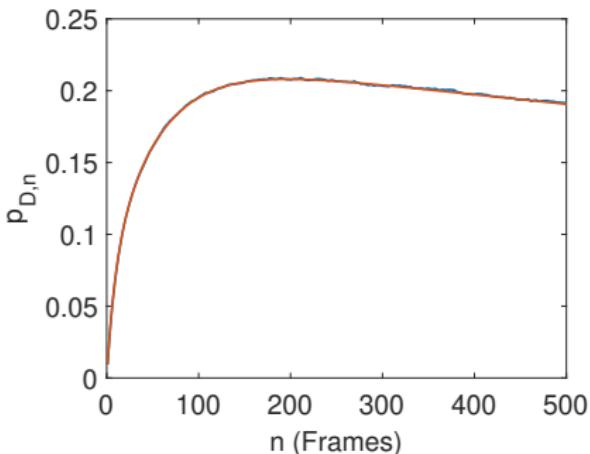
Characterizations I



For $n \geq 1$, let $p_{B,n}(\boldsymbol{\theta})$ to be the probability a molecule first appears, and $p_{D,n}(\boldsymbol{\theta})$ to be the probability of detecting a single molecule in frame n , dependent on $\boldsymbol{\theta} = \{\boldsymbol{\lambda}_G, \delta, \alpha\}$.

$$p_{B,n}(\boldsymbol{\theta}) = \boldsymbol{\nu}_X^{*\top} (B_{T^*, \delta=0}^{(0)} (B_{\Delta, \delta=0}^{(0)})^{n-1} B_{\Delta, \delta=0}^{(1)} \mathbf{1}_{d+3}$$

$$p_{D,n}(\boldsymbol{\theta}) = \boldsymbol{\nu}_X^{\top} e^{G(n-1)\Delta} B_{\Delta}^{(1)} \mathbf{1}_{d+3}.$$



Characterizations II



- $K \sim \text{Poi}(\lambda_K)$. $N_{B,n} \sim \text{Poi}(\lambda_K p_{B,n}(\boldsymbol{\theta}))$:
- $f_{B_n}(C') = e^{-\lambda_K p_{B_n}(\boldsymbol{\theta})} \prod_{\mathbf{c} \in C'} \lambda_K p_{B_n}(\boldsymbol{\theta}) b(\mathbf{c})$
- $f_{A_n}(C') = e^{-\alpha} \prod_{\mathbf{c} \in C'} \alpha a(\mathbf{c})$.
- Spatial prior over W , e.g. $a(\mathbf{c}) = b(\mathbf{c}) = 1/|W|$ (CSR).

We can then determine $f(C_{N_F} | \{Z_n\}_{n=1}^{N_F})$ by iteratively computing:

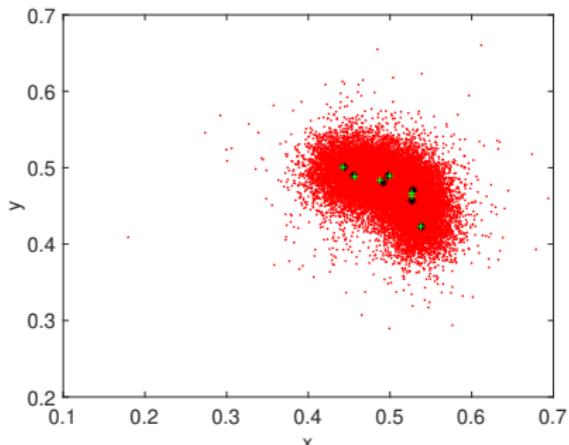
$$f(C_n | \{Z_{n'}\}_{n'=1}^n \boldsymbol{\theta}) \propto f(C_n | \{Z_{n'}\}_{n'=1}^{n-1}, \boldsymbol{\theta}) f(Z_n | C_n, \boldsymbol{\theta}).$$

- First term requires finding all smaller subsets of C_n that give rise to different birth sets in each frame.
- Second term requires finding all subsets of Z_n that could come from false positive observations and C_n . Computed offline: sets of size k yield observations of size $\leq k$, rest are false-positives.

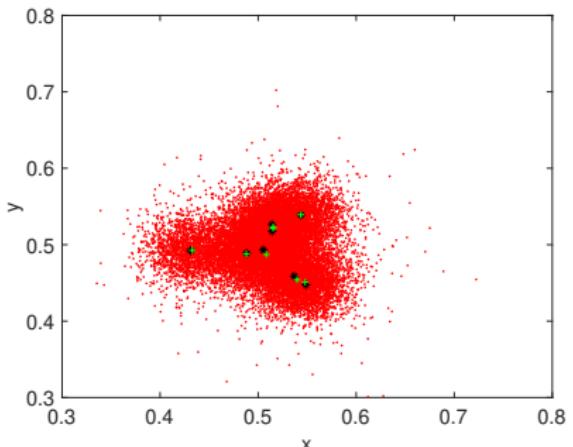


- The computation of $f(C_n | \{Z_{n'}\}_{n'=1}^{n-1}, \theta)$ can become computationally intractable for large sets C_n .
- For molecules that are already activated before imaging, e.g. in dSTORM, $p_{B,n} = 0$ for $n > 1$, which allows for fast computation.
- We use a birth-death-shift MCMC sampler to sample C_{N_F} from $\{Z_n\}_{n=1}^{N_F}$ (i.e. underlying spatial positions and its cardinality).
- $\theta = \{\lambda_G, \delta, \alpha\}$ can also be estimated within the algorithm through its contribution in $p_{D,n}$.
- In real applications the localization standard deviation is determined through the localization algorithm, and is therefore known.

Simulations I



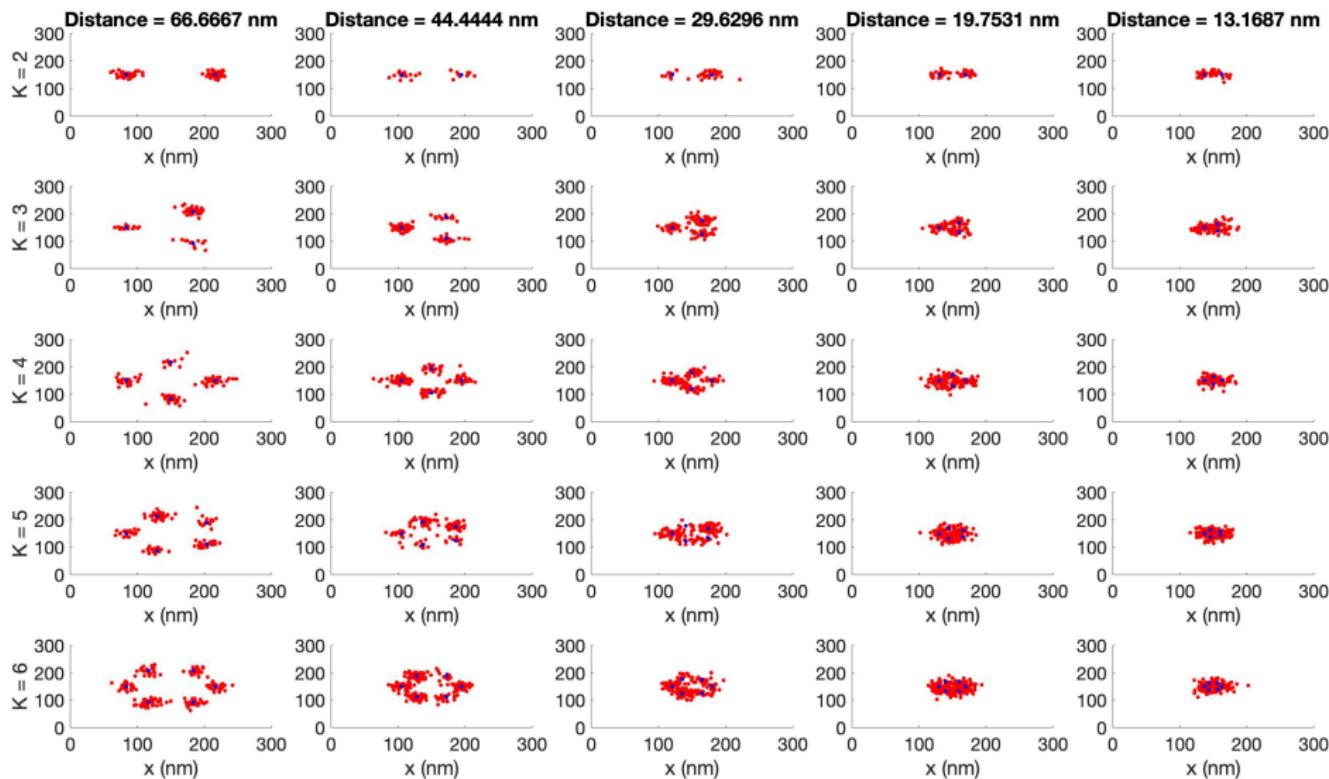
Simulation 1.



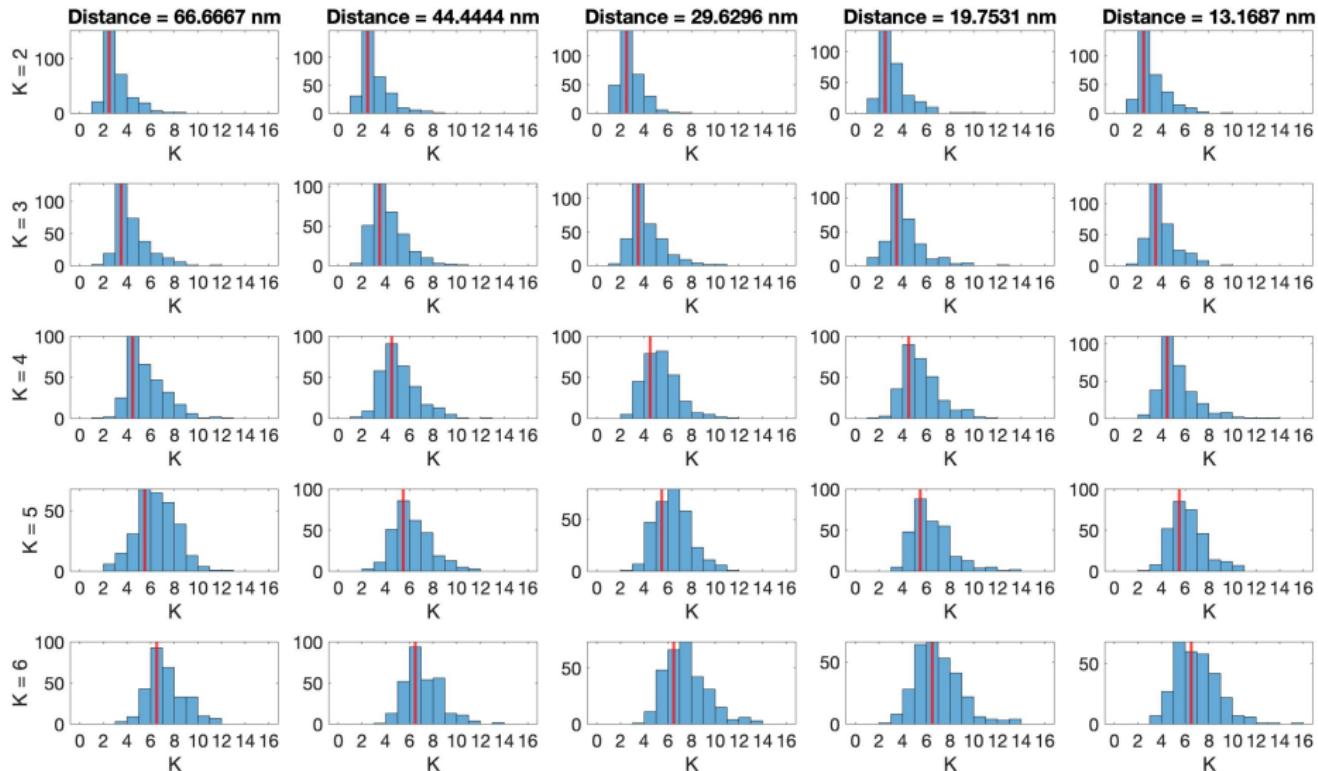
Simulation 2.

Spatial estimates of 2 simulation studies under the $d = 2$ model.

Simulations II



Simulations III

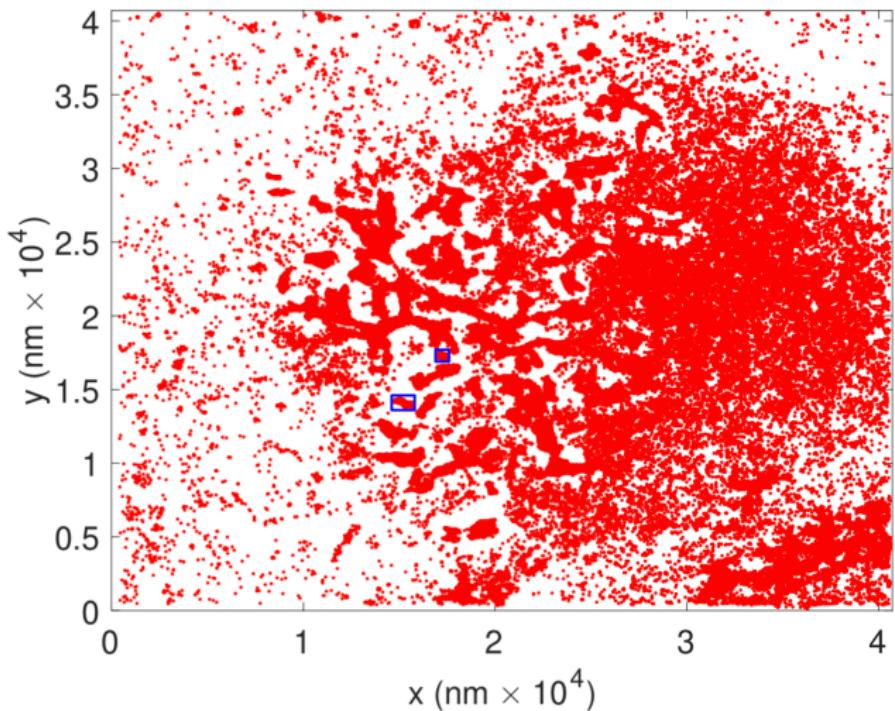


Application to Real Data I

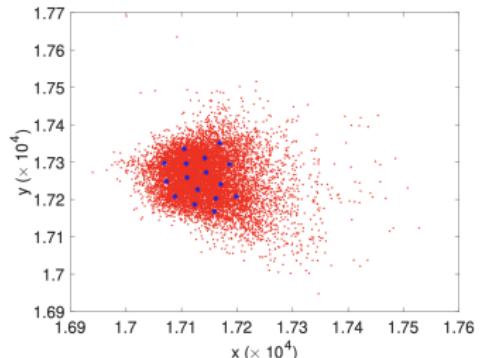
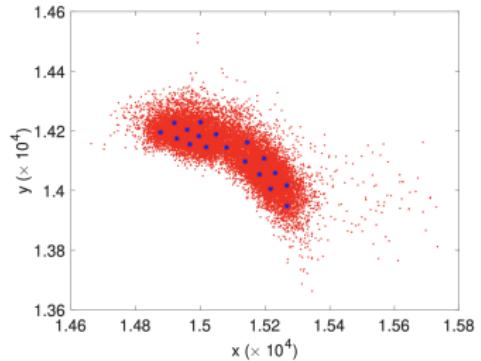
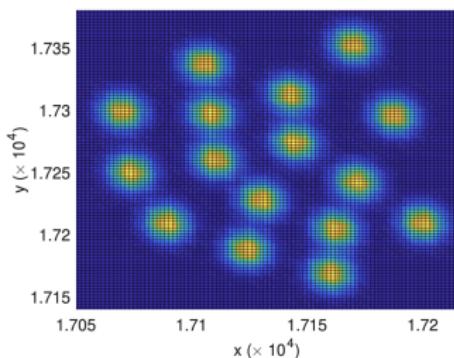
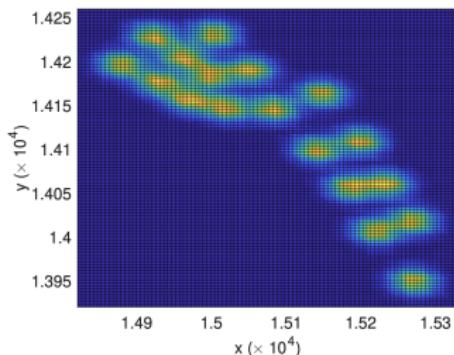


- Chromosomes labeled with Alexa Fluor 488 fluorophores embedded in Polyvinyl Alcohol (PVA) resin considered.²
- Imaged over 10^4 frames, at a frame rate of $\Delta = 0.03$ seconds, with dSTORM.
- Investigated 2 clusters of molecules using subsets of raw image.
- The algorithm of Ovesný et al. (2014) applied to find high photon intensity spots, and localizations determined via Gaussian PSFs.
- Under all experiments, the $d = 2$ model was picked, with $\mu_0 = \mu_{01} = \mu_{02} = 0$.

Application to Real Data II



Application to Real Data III



Spatial estimates (with cardinality) of two clusters of image. Spatial regularity of about between fluorophores, with structure, is observed.

²Dataset was made available by Professor Paul French, Imperial College London.



Model summary

- Leveraging temporal characteristics of molecules imaged in stochastic superresolution is key for understanding underlying spatial structures.
- Data of imaging observations has been described - both ideal and real cases.
- In the ideal case, spatial analysis is straight-forward.
- In the real case, a spatial-temporal joint point process can be formulated that utilizes photo-switching/binding temporal characteristics.
- This model is used to describe a pure birth *hidden* process of molecular positions and count as they become activated.
- Hidden process related to observation point process which includes false positive measurements.
- Inference via MCMC can be utilized to recover hidden process.
- Robust method shown on simulations and real data.

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