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1 Efficient hydrogen delivery for microbial electrosynthesis via 3D-printed 2 cathodes

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13

14 Abstract

15 The efficient delivery of electrochemically *in situ* produced H₂ can be a key advantage of microbial
16 electrosynthesis over traditional gas fermentation. However, the technical details of how to supply large
17 amounts of electric current per volume in a biocompatible manner remain unresolved. Here, we explored
18 for the first time the flexibility of complex 3D-printed custom electrodes to fine tune H₂ delivery during
19 microbial electrosynthesis. Using a model system for H₂-mediated electromethanogenesis comprised of
20 3D fabricated carbon aerogel cathodes plated with nickel-molybdenum and *Methanococcus maripaludis*,
21 we showed that novel 3D-printed cathodes facilitated sustained and efficient electromethanogenesis
22 from electricity and CO₂ at an unprecedented volumetric production rate of 2.2 L_{CH₄} /L_{catholyte}/day and at a
23 coulombic efficiency of 99%. Importantly, our experiments revealed that the efficiency of this process
24 strongly depends on the current density. At identical total current supplied, larger surface area cathodes
25 enabled higher methane production and minimized escape of H₂. Specifically, low current density
26 (< 1 mA/cm²) enabled by high surface area cathodes was found to be critical for fast start-up times of the
27 microbial culture, stable *steady state* performance, and high coulombic efficiencies. Our data

28 demonstrate that 3D-printing of electrodes presents a promising design tool to mitigate effects of bubble
29 formation and local pH gradients within the boundary layer and, thus, resolve key critical limitations for
30 *in situ* electron delivery in microbial electrosynthesis.

31

32 Introduction

33 Bioelectrochemical technologies represent a key platform for recycling of CO₂ into useful fuels and
34 chemicals to enable a circular carbon economy.¹⁻³ For bioelectrochemical CO₂ conversion to operate at
35 industrial scale, two critical performance metrics need to be achieved: 1) high reaction rates, requiring
36 current densities in the range of 100-1000 mA/cm² and 2) a high selectivity for production of the target
37 compound (>90%).^{2,4} In this context, microbial electrosynthesis (MES) is particularly promising as
38 biological syntheses are highly selective, including for complex, multi-carbon compounds. Such high
39 selectivity is achieved when using strictly anaerobic microorganisms that typically utilize H₂, HCO₂⁻, or CO
40 as catabolic electron source and convert these electrons at a selectivity of >90% to specific catabolic end
41 products.⁵ So far, the volumetric electron supply in MES has been limited to current densities in the range
42 of 1 mA/cm², with rates up to 20 mA/cm² only reported for projected surface areas that widely
43 underestimate the actual active electrode surface.⁶ Therefore, a key improvement target for transferring
44 this technology from laboratory to larger scale is increasing the current density to maximize the electron
45 feed per volume.^{7,8} Hydrogen-driven MES is particularly promising as H₂ can be electrochemically
46 produced at high rates and 100% selectivity using inexpensive materials and is used by a wide variety of
47 anaerobic microorganisms.^{9,10} In traditional microbial gas fermentation, high volumetric production rates
48 are achieved but the handling and dispersion of sparingly soluble H₂ as electron carrier is a major
49 challenge.¹¹ MES is similar to H₂/CO₂-gas fermentation, with the important difference that in MES H₂ is
50 formed *in situ* at the site of microbial consumption and, therefore, circumvents the challenges of
51 introducing bulk H₂ gas via extensive purging and mixing. Further, the electrochemical production of H₂ as
52 intermediate provides a platform for electricity storage by converting electrical into chemical energy in
53 form of “green methane” (bio-power-to-gas), which can be used in the existing natural gas infrastructure.

54 Over the past decade diverse cathodes have been purposely build or modified to enhance MES processes
55 by improved properties such as increasing hydrogen formation.^{10,12,13} Cathodes with intrinsically high
56 surface area, such as carbon granules, cloth, fiber, or reticulated vitreous carbon, have emerged as
57 particularly useful to improve the process performance by retention of high bacteria loadings on

58 electrodes.^{10,12,13} However, a systematic variation of surface area and the relationship between surface
59 and current densities has not been explored so far. Additive manufacturing, commonly known as 3D-
60 printing, has been a major driver of innovation in industrial manufacturing and could prove to be
61 revolutionary for the field of MES by offering flexibility in complex and custom design of electrochemically
62 active materials.^{14,15} The technology enables the rapid development and testing of customized electrode
63 and reactor prototypes and has recently been successfully applied for improved electrochemical carbon
64 dioxide reduction.¹⁶ 3D-printing is particularly interesting for the production of next generation electrodes
65 as the technology enables the design of high surface area materials with possible structuring up to
66 nanometer-scale via post-treatment methods.¹⁴ Complex custom designs can be realized, such as
67 incorporation of flow channels to make high surface area per volume accessible, while high conductivity
68 over large electrodes is provided via incorporation of a metallic core. Metal powder printing is one option
69 to manufacture conductive metal substrates.¹⁷ In addition, the direct electrochemical 3D-printing of
70 metallic materials through electrochemical reduction of metal ions from solutions onto 3D-printed
71 conductive substrates is in development.¹⁸

72 Here, we demonstrate, to our knowledge, the first use of cathodes fabricated via 3D-printing for microbial
73 electrosynthesis. We manufactured 3D-electrodes with varying ratios of surface area to volume and used
74 these to study the effect of *in situ* H₂ supply as a function of current density on electromethanogenesis
75 using the methanogen *Methanococcus maripaludis* as model system.

76

77 Materials and Methods

78 Cathode fabrication

79 Carbon aerogel (CA) cathodes coated with a NiMo-alloy were used to enable the fabrication of highly
80 conductive, hydrogen evolving cathodes via additive manufacturing.^{10,19} The base CAs were prepared from
81 resorcinol and formaldehyde gels, which were poured into custom 3D-printed acrylonitrile-butadiene-
82 styrene (ABS) molds formed as the inverse of our desired final shape (see Figure 1A). After thermal curing
83 of the gel, the mold was removed by dissolving in acetone, leaving the complex shaped raw organic
84 aerogel, which was carbonized at high temperature in inert atmosphere to yield the CA cathodes. To
85 obtain complex shape casts, acrylonitrile-butadiene-styrene (ABS) molds were printed on a Lulzbot Taz 6
86 fused filament 3-D printer. Cylindrical lattice electrodes were constructed with 3 mm strut thickness,
87 where the geometric surface area of the electrode was controlled by the density of struts (and thus, the

88 specific surface area) within the lattice. For lattice cylinder electrodes with 55, 89, and 111 cm² geometric
89 surface area, simple cubic lattices with specific surface area 0.10, 0.12, and 0.15 cm²/cm³ were used,
90 respectively. Electrodes were designed to occupy a cylinder with dimensions 4 cm height by 2.4 cm
91 diameter. Molds based on the electrodes were created by inverting the design; the molds were printed
92 at 135% of the designed size, to account for shrinkage of the material during carbonization of the organic
93 aerogel to form the carbon aerogel.

94 Carbon aerogels were prepared from resorcinol and formaldehyde (RF) gels. In a typical synthesis,
95 resorcinol (1.23 g) and a 37% formaldehyde solution (1.7 g) in water (1.5 ml) were mixed together,
96 followed by addition of 2N nitric acid (44 μl). The mixture was poured into a custom 3D-printed ABS-mold,
97 which was placed in a sealed glass jar and allowed to cure in an oven at 80°C for 24 h to form wet organic
98 aerogels. After curing, the ABS mold was completely dissolved in a bath of acetone. The acetone bath also
99 served to solvent exchange the organic aerogels. Typically, the acetone was refreshed 2 or 3 times to fully
100 remove the ABS mold. The organic aerogels were then allowed to dry in the fume hood for 24 h. The dried
101 aerogels were carbonized in a tube furnace under nitrogen atmosphere at 1050°C for 3h with a heating
102 and cooling rate of 2°C/min to obtain carbon aerogels (CA). The CA electrodes were attached to a copper
103 wire as a current collector using conductive Ag epoxy, which was then sealed with a non-conductive
104 epoxy. The copper wire was insulated to ensure the electrochemical activity would occur only at the
105 electrode.

106 The CA electrodes were electroplated with a catalyst-layer of nickel-molybdenum for enhanced hydrogen
107 evolution properties under biological conditions. For this, each cathode was placed in NiMo-plating
108 solution at ~1 cm distance to a surrounding anode (Platinum mesh, PT008720 -350-210-23, Goodfellow),
109 which was separated from the cathode using nylon filter bags (180 micron mesh, SLSO, Amazon.com).
110 NiMo-plating solution contained per liter: 40 g NiCl₂·6H₂O, 25 g Na₂MoO₄·2H₂O, 45 g sodium citrate. The
111 pH was adjusted to 10 with NH₄OH. Under constant magnetic stirring at 900 rpm, a constant current of
112 50 mA/cm² was applied to obtain a deposition of 60 Coulombs/cm². The cathodes were soaked in
113 deionized water to remove residues from the NiMo-plating before use in the bio-electrochemical system.

114 **Microbial strain, growth medium, and culture conditions**

115 The archaeon *Methanococcus maripaludis* was chosen due to its salinity tolerance and its exceptional
116 performance in previous studies.²⁰ *M. maripaludis* was cultured using chemically defined medium-JD
117 specifically modified for use in bio-electrochemical reactors as reported previously.²⁰ In brief, medium-JD
118 contained per liter: 30 g Na₂SO₄, 4 g MgSO₄ x 7 H₂O, 0.2 g KH₂PO₄, 0.4 g NH₄HCO₃, 0.6 g KHCO₃, 0.04 g

119 CaCl₂, 7.2 g morpholinepropanesulfonic (MOPS) acid, 3.4 g MOPS Na-salt, 1 ml selenite-tungstate
120 solution, 1 ml trace element solution SL-10, 1 g NaS₂O₃, 0.4 g Cysteine-HCl and 30 mL of 1 M NaHCO₃
121 solution. The final medium-JD was prepared from autoclaved anoxic stock solutions under continuous
122 gassing with CO₂/N₂ (20/80% v/v). The final pH was 6.8.

123 *M. maripaludis* was routinely grown in batch cultures in medium-JD under H₂/CO₂ (80/20 %v/v) gas
124 atmosphere at 30°C and 250 rpm. Each reactor was inoculated from an exponentially growing culture.

125 Reactor set up and operation

126 The bioelectrochemical set up was described in detail previously.¹⁰ In brief, two-chamber glass H-cells
127 were separated by a Nafion 117 proton-exchange membrane (Fuel Cell Store Inc., College Station, TX,
128 USA, surface area 4.9 cm²). The cathode chamber volume was 100 mL. In each reactor, one three-
129 dimensional cathode, fabricated as reported above, was inserted into the cathode compartments and
130 connected by threading the copper wire through a gastight rubber stopper. The anode was a platinized
131 titanium mesh (1" × 4", TWL, Amazon) and the reference electrode Ag/AgCl (NaCl saturated; BASI). The
132 electrochemical reactors were controlled by applying a constant current using a multichannel potentiostat
133 (VMP3; Bio-Logic Science Instruments, France). For experiment 1 and 2 the current was set to 50 mA per
134 reactor and for experiment 3 the current was increased stepwise in increments of 10 mA as described in
135 the main text. The pH in the catholyte was monitored and remained constant (pH7) at all times.

136 CO₂ was supplied continuously at a flowrate of 0.15 mL min⁻¹ (CO₂ 100%) controlled via mass flow
137 controllers (EL-Flow F-100D, Bronkhorst) to ensure non CO₂-limiting conditions throughout the
138 experiments. The microbial growth medium-JD was continuously supplied via peristaltic pump at a
139 constant feed rate of 0.0676 ± 0.0025 mL min⁻¹. Each chamber was magnetically stirred at 700 rpm. All
140 reactors were operated at ambient pressure in a temperature-controlled room at 30°C. Prior to
141 inoculation the system was operated for 72 hours to reach stable pH conditions in the cathode chambers
142 (see detailed description elsewhere²⁰).

143 Liquid samples were taken through rubber side ports at regular intervals. Samples for gas analysis were
144 taken from the respective reactor headspace with a gas syringe. Volumetric gas flow rates of the reactor
145 off gas were measured via Milligas counter (KG MGC-1, Ritter Apparatebau GmbH & Co. Germany) at
146 regular intervals.

147 Analytical methods

148 Methane and hydrogen were measured using a gas chromatograph (equipped with a thermal conductivity
149 detector and a flame ionization detection detector, Agilent) as described previously.²¹ Cell densities were
150 measured via Spectroscopy at 600 nm (Ultrospec 2100 pro, Amersham BioSciences, Little Chalfont, United
151 Kingdom).

152 Calculations

153 Coulombic efficiencies were calculated by dividing the electrons recovered in methane by the electrons
154 supplied as current at a certain time point according to equation 1 below. With $\eta_{(CH_4,t)}$ = mol CH₄ at time
155 point t; $f_{(e,CH_4)}$ = molar conversion factor (8 electrons per mol CH₄); F = Faraday constant (96,485 C mol⁻¹
156 of electron) and I = electric current.

$$157 \quad CE [\%] = \frac{\eta_{CH_4,t} \times f_{e,CH_4} \times F}{\int_{t_0}^t I dt} \times 100 \quad (1)$$

158 The estimation of the current density at which bubble formation occurs was done using Fick's law
159 (equation 2) and the following assumptions. The diffusion coefficient (D) for hydrogen in water is 5.5*10⁻
160 ⁵ cm²/s (atmospheric pressure, 30°C).²² The solubility limit for hydrogen at 30°C in water is 0.75 mM.²²
161 Assuming complete utilization of H₂ by hydrogenotrophic microbes in the bulk liquid ($\partial\varphi = 0.75$ mM) and
162 a diffusive boundary layer of thickness $\partial x = 100$ μm.¹⁰

$$163 \quad J = -D \frac{\partial\varphi}{\partial x} = 4.5 \cdot 10^{-5} \frac{0.76}{0.01} \left[\frac{cm^2}{s} \cdot \frac{mmol}{1000 cm^3 cm} \right] = -4.125 \cdot 10^{-6} \left[\frac{mmol}{s cm^2} \right] \quad (2)$$

164 Therefore, in good approximation 4.1 nmol s⁻¹ H₂ will diffuse away from the electrode per cm². This
165 corresponds to a maximum current density of around 0.8 mA/cm² before bubble formation occurs in this
166 system.

167

168 Results

169 3D-printing for fabrication of electrode prototypes for *in situ* H₂ delivery at variable 170 current densities

171 To test how the cathodic current density influences process parameters in hydrogen-driven microbial
172 electrosynthesis, we used additive manufacturing to design and fabricate hydrogen-evolving cathode
173 prototypes with identical catalytic properties and overall volume but varying surface areas.

174 The base material was comprised of carbon aerogel, which exhibits a high electrical conductivity, and good
175 structural stability.¹⁹ After the final synthesis step of carbonization at high temperature in inert
176 atmosphere, the cathodes were electroplated with NiMo-alloy to enhance the hydrogen evolution
177 properties, as described previously (see Figure 1A).¹⁰ Sets of electrodes that share identical overall
178 cylindrical volume of 18 cm³ were fabricated with varying geometric surface areas 55 cm², 86 cm² and
179 111 cm² by controlling the density of lattice struts contained within the cylinder (Fig. 1B and C). A filled
180 cylinder cathode with the geometric surface area of 39 cm² was prepared via NiMo-plating of a
181 commercial graphite rod with the same overall cylinder dimensions, as the bulk cylinder CA fabrication
182 did not result in uniform shapes due to uneven shrinkage and cracking during drying and carbonization.

183 (Figure 1)

184

185 Electromethanogenesis from *in situ* produced H₂ supplied at varying current 186 densities

187 The novel 3D cathodes were employed in an integrated bioelectrochemical reactor as described
188 previously.²⁰ In brief, four identical H-cell reactors were operated in *chemostat-mode* under continuous
189 supply of gaseous CO₂ and fresh, sterile growth medium. The supply of catabolic electrons was controlled
190 by applying a constant current of 50 mA per reactor. Cathodes evolved H₂ at 100% selectivity¹⁰ and,
191 therefore, supplied equal amounts of H₂ to each reactor. The current density varied based on the available
192 cathode geometric surface area; the tested specific current densities were 0.5, 0.6, 0.9, and 1.3 mA/cm².
193 After an abiotic equilibration period of 72 hours, each reactor was inoculated with the anaerobic archaeon
194 *Methanococcus maripaludis* to an initial optical density of OD_{600, start} = 0.02.

195 The methane production profiles of the different reactors during this first experiment indicated that
196 efficient electromethanogenesis in this system strongly depended on the current density of the cathode
197 (see Fig. 2, Exp1, left column). At the lowest current density of 0.5 mA/cm^2 (high surface area), stable
198 electromethanogenesis was observed within 24 hours reaching an average coulombic efficiency of
199 $98 \pm 0.2\%$. With increasing current density, *steady state* operation was delayed and H_2 concentration in
200 the reactor off-gas increased. At 0.6 mA/cm^2 highly efficient methane production was established only
201 after 145 hrs ($\text{CE} = 97 \pm 0.4\%$), while the reactor operating at 0.9 mA/cm^2 did not reach stable methane
202 production rate within the monitored timeframe of 1 week. At the highest current density of 1.3 mA/cm^2
203 tested, substantial underutilization of H_2 was observed, which resulted in an overall low coulombic
204 efficiency of $20 \pm 4\%$ for methane (averaged between 50-190 hours). These data demonstrate that the
205 cathodes fabricated with 3D-printing technology are suitable for direct integration with microbial
206 electrosynthesis; however, the overall start-up time and coulombic efficiency strongly depended on the
207 cathodic current density.

208 (Figure 2)

209

210 Effect of initial cell concentration on reactor performance

211 To investigate whether the observed effect of current density on start-up times during experiment 1 was
212 dependent on the initial cell density, we repeated the experiment (identical set-up, unused set of
213 cathodes) and increased the initial cell density by a factor of 5 to an $\text{OD}_{600, \text{start}} = 0.1$ (Exp2). At a higher
214 initial cell density, start-up times were significantly shortened but lower current densities still resulted in
215 improved overall process performance (see Fig. 2, Exp2, right column). For current densities of 0.5 and
216 0.6 mA/cm^2 , highly efficient methane production was achieved within less than 7 hours (for coulombic
217 efficiencies see Fig. 3). At a current density of 0.9 mA/cm^2 , *steady state* methane production was reached
218 after 55 hours, while the low-inoculum culture of Exp1 did not reach stable production rates within 7 days
219 at this current density. Apparently, electromethanogenesis at the highest current density of 1.3 mA/cm^2
220 tested did not significantly benefit from a high initial cell density. Again, significant amounts of H_2 were
221 lost in the reactor off gas and the average coulombic efficiency for methane was only $12 \pm 2\%$ (cf. Fig. 3).

222 While increasing cell density significantly shortened start-up times, the achieved coulombic efficiency in
223 *steady state* conditions was dependent on the cathodic current density.

224 (Figure 3)

225

226 **Current density as a critical determinant for biocompatibility**

227 Based on the above experiments, we hypothesized that the specific current density on the cathodes is
228 crucial for efficiently delivering H₂ *in situ* into the microbial metabolism. To test this hypothesis, we
229 increased the total current per reactor and, therefore, the current density in three consecutive steps in
230 the following experiment 3 (Fig. 4). With increasing current densities, the efficiency of bioelectrochemical
231 methane production decreased as the H₂ concentration in the off-gas increased (Fig. 5). At 60 mA total
232 current, the reactors with the three highest surface area cathodes enable methane production at almost
233 100% coulombic efficiency. Increasing the current to 70 mA led to an increase in methane production rate,
234 except in the reactor with the second smallest surface area of 55 cm², where the methane production rate
235 dropped slightly instead (*cf.*, Fig 4). A further increase in total current to 80 mA resulted in a similar effect
236 for the next larger cathode at 89 cm². Under these conditions only the cathode with the largest surface
237 area (111 cm²) resulted in a further increase in methane production rate, corresponding to a volumetric
238 methane production rate of 2.2 L_{CH₄} /L_{catholyte}/day at a coulombic efficiency of 99%. These observations
239 suggest that after exceeding a critical current density the performance ceases to increase further and,
240 more significantly, drops as highly efficient electromethanogenesis is no longer observed (see Fig. 5). For
241 the here tested system using NiMo cathodes, magnetic stirring (700 rpm) and *Methanococcus maripaludis*
242 as microbial catalyst and at the cell densities tested, this critical current density was found to be around
243 ~1.0-1.5 mA/cm² (*cf.* Fig. 5). Large surface area cathodes that enabled current densities to remain below
244 this critical threshold were successful to facilitate continuous electromethanogenesis via *in situ* H₂
245 production at record volumetric production rate. The underlying mechanism for this observed behaviour
246 is likely a combination of increased loss of gaseous H₂ due to increased bubble formation and decreased
247 biocompatibility due to locally high pH at the cathode surface at higher current densities and is discussed
248 in detail in the following section.

249

(Figure 4)

250

(Figure5)

251

252 Discussion

253 Mechanism of efficient H₂ delivery in MES

254 Similar observations of optimum performance in MES at relatively low current densities have been
255 reported for other systems.^{9,23} In an electromethanogenesis system, Geppert et al. increased the current
256 density from 0.5 to 3.5 mA/cm² and found optimum conditions at around 2.5 mA/cm², while at higher
257 current densities the fraction of electrons lost as unused hydrogen in the off-gas increased.²⁴ This was
258 interpreted by others as a “metabolic limitation of the biocatalyst”.⁸ However, microbial production of
259 methane as well as acetate from H₂/CO₂ is possible at rates exceeding the rates achieved in
260 bioelectrochemical systems today by about one order of magnitude.²⁵⁻²⁷ This demonstrates that the
261 metabolic capacity of the microorganism is not limiting. Instead, our data show that the mode of H₂
262 delivery ultimately determines the fraction of electrons available for microbial metabolism, which,
263 therefore, determines the maximum achievable production rate under the given conditions. For gas
264 fermentation, it is well known that efficient delivery of dissolved H₂ is a key limiting factor for maximizing
265 production rates, and, therefore in some cases, requires expensive pressurization to increase H₂
266 dissolution.^{25,28,29} Thus, the electrochemical production of H₂ *in situ* can provide substantial advantage
267 over introducing and dispersing bulk H₂ gas if engineered well (*cf.* Fig. 6).

268 Hydrogen-driven electrosynthesis is mainly performed by cells in suspension in the reactor bulk liquid,
269 where turbulent mixing enhances mass transfer of cathode-derived H₂ while p_(H₂) is effectively drawn close
270 to zero by microbial metabolism.³⁰⁻³² The electrode surface presents a liquid-solid interface, around which
271 a diffusive boundary layer exists. In a magnetically-stirred (200 rpm) electromethanogenesis reactor, we
272 previously determined the boundary layer around a graphite rod cathode to be ~50-100 μm.¹⁰ Therefore,
273 electrocatalytically produced H₂ needs to pass through this diffusion-limited boundary layer before it is
274 available to the microbial culture in bulk liquid (see Fig. 6). At low current density, the rate of formation
275 of dissolved H₂ is slower than microbial consumption in and diffusion out of the boundary layer, and
276 therefore no H₂ gas bubbles form (Fig. 6A). When the current density increases and the rate of hydrogen
277 formation exceeds H₂ consumption and diffusion out of the boundary layer, the solubility limit of H₂ is
278 reached and gas bubbles start to form (Fig. 6B). Such bubble formation in electrosynthesis processes is
279 generally undesirable as they can (i) passivate the active sites of the electrocatalyst reducing the electric
280 efficiency and (ii) escape the reactor unused and, therefore, reduce coulombic efficiencies and lower the
281 purity of output gas products (Fig. 6B).³³ While H₂ present in bubbles can still be available for metabolic
282 conversion in the reactor’s bulk liquid depending on the geometry and operation, as previously noted for

283 gas fermentation, the size and number of bubbles increases with current density. A video documentation
284 of this process demonstrates the difference in hydrogen bubble formation under constant current
285 conditions on the here tested cathodes with varying surface areas (see supplementary information to this
286 article). It can be seen that at identical overall H₂ production rate (identical current), the cathodes with
287 lower surface areas lead to significantly increased bubble formation compared to higher surface area
288 cathodes. Based on our calculation using Fick's law and the constraints of our system (see methods section
289 for details), formation of H₂ bubbles is predicted to start at currents densities exceeding 0.8 mA/cm². This
290 can explain the observation of significant H₂ loss at current densities above 1.0 mA/cm² in the here tested
291 system (*cf.* Fig. 5).

292 (Figure 6)

293 A second, often underexplored aspect of the boundary layer in bioelectrochemical systems is the
294 formation of a pH gradient across the boundary layer and its effect on microbial metabolism. In
295 circumneutral microbial growth medium the concentration of H⁺ and OH⁻ ions is low at 0.1 μM (pH = 7).
296 Therefore, electrochemical proton reduction to H₂ at even moderate current density can lead to high local
297 pH in the diffusive boundary layer.³⁴ While the presence of a buffer in mM concentration can significantly
298 mitigate this effect,^{35,36} the rate of diffusion of the protonated buffer into the boundary layer from the
299 bulk liquid becomes limiting for a sustained formation of dissolved, bubble-free H₂ at medium or high
300 current densities (Fig. 6B). An alkaline pH in the boundary layer in combination with bubble formation
301 presumably precludes the formation of biofilms at high current densities.⁹ Although the largest fraction
302 of microbial activity during H₂-driven MES is in the bulk liquid, metabolically active microbes do come in
303 contact with the high pH environment in the cathodic boundary layer. Exposure to alkaline pH
304 environments can compromise microbial organisms like *M. maripaludis*.³⁷ In fact, in a previous study we
305 found slightly increased cell lysis of *M. maripaludis* cells grown with *in situ* electrochemically evolved
306 hydrogen (at 1 mA/cm²) compared to cultures supplied with a gaseous mix of H₂/CO₂.²⁰

307 In combination, the increased H₂ loss through bubble formation and decreased biocompatibility due to
308 high local pH can explain the here observed decline in biomass and methane formation rates after
309 exceeding a critical current density. The drop in methane formation rate seems to slightly precede the
310 decrease in biomass concentration (*cf.* Fig. 5), indicating that in the here investigated system, H₂-loss via
311 bubble formation is the dominating effect before bio-incompatible pH conditions are reached at further
312 increased current densities. The specific value of this current density threshold depends for each MES
313 system on its specific properties, including reactor configurations, operating conditions, boundary layer

314 and mixing, and microorganisms chosen. Thus, for designing advanced MES systems, it is of critical
315 importance to consider the above discussed molecular basis of bubble formation and local pH gradients.
316 Because these gradient effects increase with the thickness of the diffusive boundary layer³⁸, reducing the
317 size of this layer will mitigate these limitations and maximize the supply of electrons per reactor volume
318 while maintaining biocompatibility. 3D-printing is a particularly promising platform to effectively decrease
319 the boundary layer via advanced electrode and reactor designs that combine high surface areas with
320 improved fluid dynamic properties¹⁴ and, therefore, presents a critical opportunity to further improve the
321 performance of MES.

322

323 Conclusion

324 We demonstrated here for the first time electrocatalytically active cathodes fabricated via 3D-printing as
325 a new platform for efficient *in situ* delivery of H₂ in an integrated microbial electrosynthesis system. With
326 this tool, we identified the specific current density on the cathode surface as being critical for (i) fast start-
327 up times of the microbial culture, (ii) stable steady-state performance, and (iii) high coulombic efficiencies
328 via minimizing H₂ escape, favouring efficient microbial H₂ utilization, and maintaining biocompatible pH
329 conditions near the electrode surface. Moreover, we showed that it is not the metabolic capacity of a
330 microorganism *per se* that limits product formation rate in a MES, but the physical/chemical conditions in
331 the boundary layer.

332 This proof-of concept demonstrates that advanced manufacturing of cathodes is a suitable tool for
333 bioelectrochemical technologies, which provides major advances for the rapid development of electrode-
334 prototypes and enables advanced custom design of innovative bio-electrochemical reactors. Even in our
335 non-optimized H-cell reactor the cathodes with highest surface area enabled highly efficient
336 electromethanogenesis at record volumetric rate of 2.2 L_{CH₄} /L_{catholyte}/day (111 cm², - 80 mA, CE = 99%).

337 Data availability

338 The authors declare that all the data supporting the findings of this study are available within the article
339 and its supplementary information files. Additional request should be made to the corresponding author.

340

341 Conflict of Interest

342 The authors declare that the research was conducted in the absence of any commercial or financial
343 relationships that could be construed as a potential conflict of interest.

344

345 Author Contributions

346 F.K. designed and performed the experiments in the integrated bio-electrochemical system, analyzed the
347 data, and drafted the manuscript. B.S.J and S.C. fabricated the electrodes. S.H.P. designed the electrodes
348 and molds. F.K., J.S.D., B.S.J., S.H.P., S.C., S.E.B. and A.M.S. conceived and designed the study and
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351

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481

482 Figure captions

483 **Figure 1:** Additive manufacturing process of the NiMo-plated carbon aerogel cathodes (A). Visualization
484 of computational models of inversed ABS molds for 3D-printing (B) and photograph of one set of finished

485 NiMo-plated carbon aerogel cathodes of varying surface areas (C). The geometric surface areas of the
486 different cathodes are from left to right 39 cm², 55 cm², 86 cm² and 111 cm².

487 **Figure 2:** Methane production rate, unused hydrogen in the reactor off gas and microbial growth during
488 Exp1 (initial OD = 0.02, left column) and Exp2 (initial OD = 0.1, right column).

489 **Figure 3:** Coulombic efficiencies achieved with the 3D printed cathodes of different surface areas under
490 low cell density (Exp1, left) and high cell density conditions (Exp2, right). The given values are averages of
491 4-12 individual measurements taken after reaching *steady state*, with error bars displaying the standard
492 deviation between individual measurements.

493 **Figure 4:** Effect of increasing current density on electromethanogenesis performance in reactors with
494 different cathodic surface areas. Methane production rate and unused hydrogen in the reactor off gas
495 during Exp3. The total supplied current was increased stepwise as indicated per dashed vertical lines.
496 Initial OD = 0.1.

497 **Figure 5:** Coulombic efficiencies for methane and *steady state* biomass concentrations in dependency of
498 the applied cathodic current density. Eight individual electrodes of four different surface areas 39 cm², 55
499 cm², 86 cm² and 111 cm² were tested under constant current conditions of 50 mA, 60 mA, 70 mA and 80
500 mA. The given values are averages of 4-12 individual measurements under *steady state* conditions with
501 error bars displaying the standard deviation between individual measurements.

502 **Figure 6:** Conceptual representation of the fate of H₂ in a (A) single-phase system at low current density
503 and (B) gas-evolving system at high current density on a hydrogen producing cathode during
504 electrosynthesis. The concentration of dissolved H₂ in the bulk aqueous phase is lower than in the
505 boundary layer because of microbial consumption. If the cathodic current density produces dissolved H₂
506 at a rate that exceeds its diffusion out of the boundary layer and microbial consumption, bubble formation
507 will occur (B). Hydrogen gas bubbles can passivate the active catalytic surface area of the cathode and,
508 thus, reduce electric efficiencies. If mass transfer from gaseous H₂ in bubbles to dissolved H₂ in the bulk
509 electrolyte is limited, there is a net loss of H₂ from the reaction space which reduces coulombic efficiency
510 as well as volumetric production rates. When the electrocatalytic H₂ production exceeds the rate at which
511 protons diffuse into the boundary layer, the local pH will rise to alkaline levels (indicated red, see B)
512 potentially toxic to the microorganisms. With increasing current density, number and size of bubbles will
513 increase and with that the intensity of all associated effects.

514