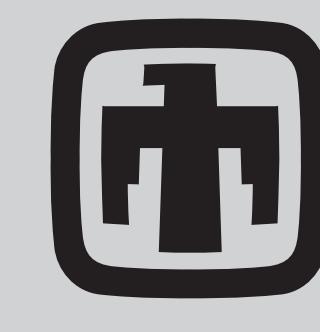


A Microfluidic Platform for High-Throughput RNAi Screening

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SANDIA2011-5075P

INTRODUCTION

High-throughput, genome-wide RNAi screens are an effective method of identifying the set of host factors that are vital to viral infection and reproduction; however, current implementations of the technology are expensive and rely on bulky equipment. We are currently developing a portable, low-cost microfluidic platform capable of rapidly and accurately performing high-throughput RNAi screens in top-level biocontainment facilities.

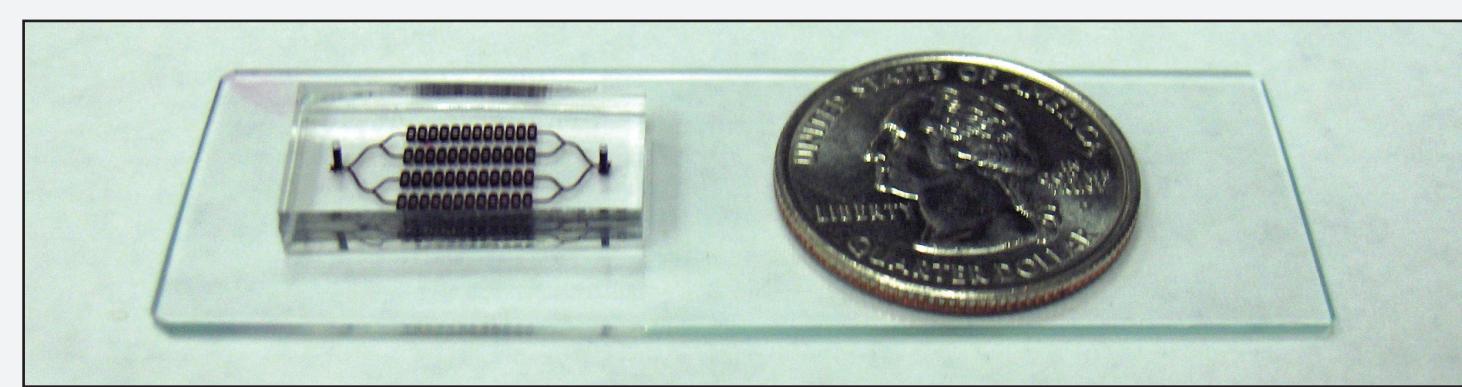


Figure 1. A 96-well diffusion-type microfluidic RNAi screening device sits on a glass slide. Cell culture, reverse transfection, viral infection and staining all take place within the device.

BACKGROUND

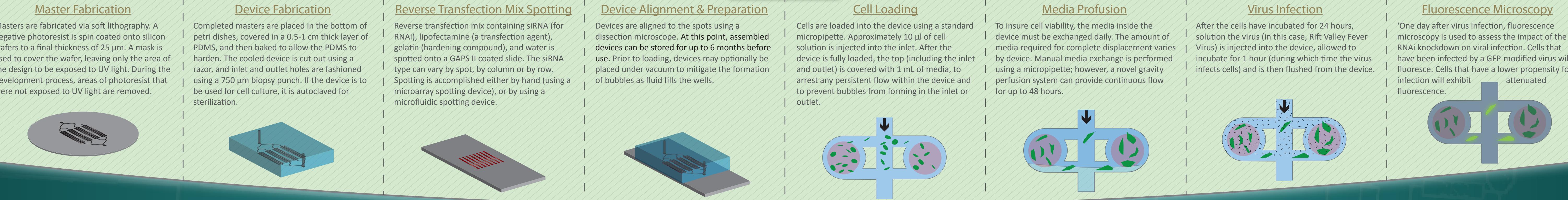
The key to mitigating the threat of viral pathogens lies in identifying the specific host proteins that a virus exploits for infection and reproduction. The subset of genes involved wanes in comparison to the tens-of-thousands of genes present in a typical host cell and is specific to each virus species/host cell pairing. Consequently, it is necessary to employ high-throughput approaches to systematically repress individual genes and determine the effect on viral pathogenesis. Current methods rely on either a microtiter or microarray platform to exploit the RNA interference (RNAi) pathway that is present in eukaryotic host cells. RNAi is a process in which cellular machinery uses small RNAs (e.g. siRNAs) to repress the expression of corresponding genes. Virologists can use RNAi to knock down a specific gene in a cell culture and then assess the effect on the ability of a virus to infect the modified cells. In a high-throughput screen (HTS), each well or spot can contain a different type of siRNA, so a multitude of genes can be screened simultaneously. Most of the current HTS RNAi technologies rely on bulky robotics to facilitate the preparation of these high-diversity samples.

ADVANTAGES OF MICROFLUIDICS

Microfluidics	Microarray	Microtiter
Capital Cost	Low	High
Reagent Use	Low	Low
Cross-Contamination	Medium	High
Bench Space Requirement	Low	Medium
Difficulty of BSL-3/4 Use	Low	High

Microfluidic RNAi screening produces results that are comparable to larger screening platforms at a fraction of the cost and time. The total volume of a single microfluidic screening well is 0.2-1 nL, whereas a microtiter well requires 100-300 μ L of reagents. The microfluidic channel design mitigates cross-contamination issues associated with the microarray platforms. Unlike microarray and microtiter plate platforms, this microfluidic platform does not require bulky robotics and is capable of advanced preparation for easy and rapid transition into BSL-3/4 labs, requiring no specialized equipment beyond a fluorescence microscope and common micropipettes.

METHODS



Development of the RNAi microfluidic platform is governed by 3 underlying principles:

- 1. Simplicity:** The device must be simple to fabricate and use. It must require minimal specialized equipment to facilitate its dissemination into BSL-3/4 labs and general wet labs.
- 2. Low Cost:** The per-device and per-run costs must be minimal. Devices must be able to be prepared in advance and stored for extended periods of time prior to use.
- 3. Efficacy:** The platform must provide a level of performance comparable or superior to competing technologies while adhering to principles 1 + 2, above.

Current device iterations fulfill the design rules by adapting basic cell culture and RNAi concepts to a microfluidics workflow. The designs avoid the use of multi-layer fabrication, valve systems, and equipment like syringe pumps to minimize the complexity associated with fabrication and utilization. siRNA spotting and cell culture conditions are optimized to accommodate for simple operation while mitigating problems like cell death and siRNA cross-contamination.

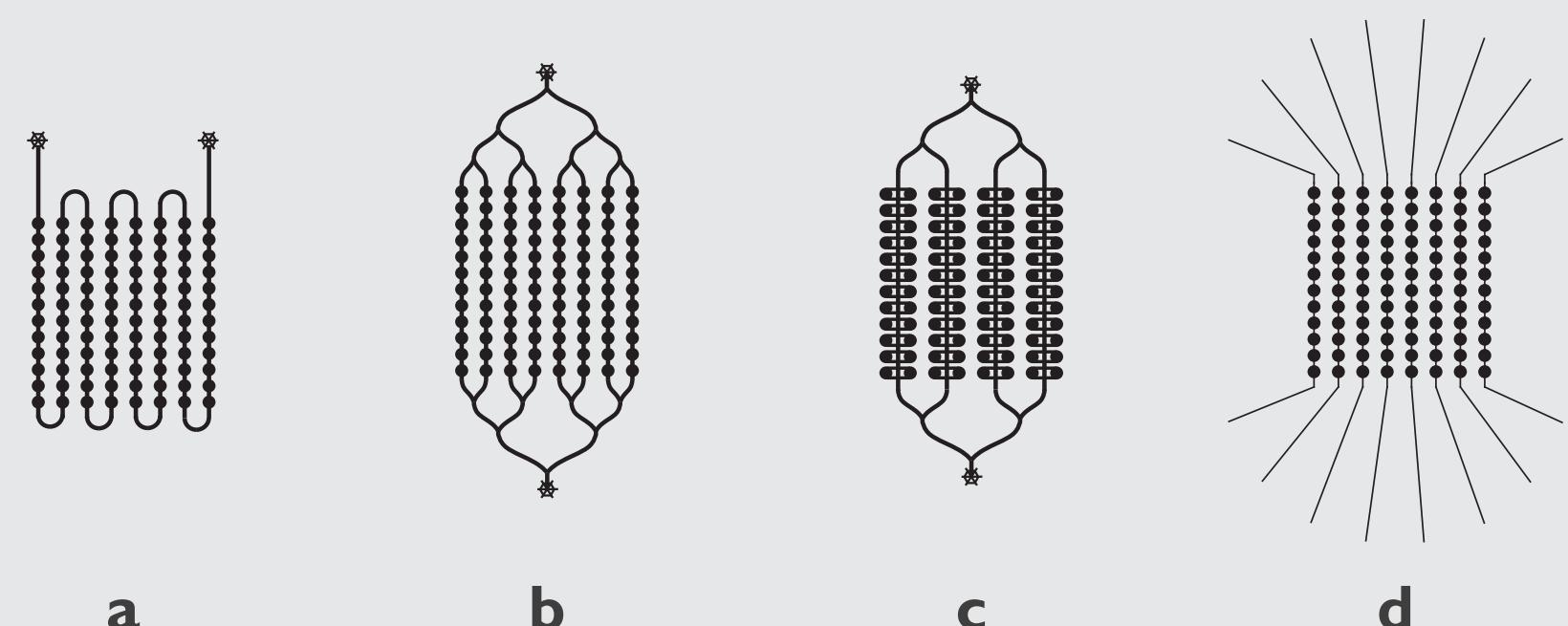


Figure 3. Current device designs: (a) inline series device, (b) split inline parallel device, (c) split diffusion device, (d) microfluidic spotting device (used to spot reverse transfection mix samples in replicate by column). All devices feature 600 μ m diameter wells and 150 μ m lines (with the exception of the spotting device, which has 75 μ m lines).

DESIGN RULES

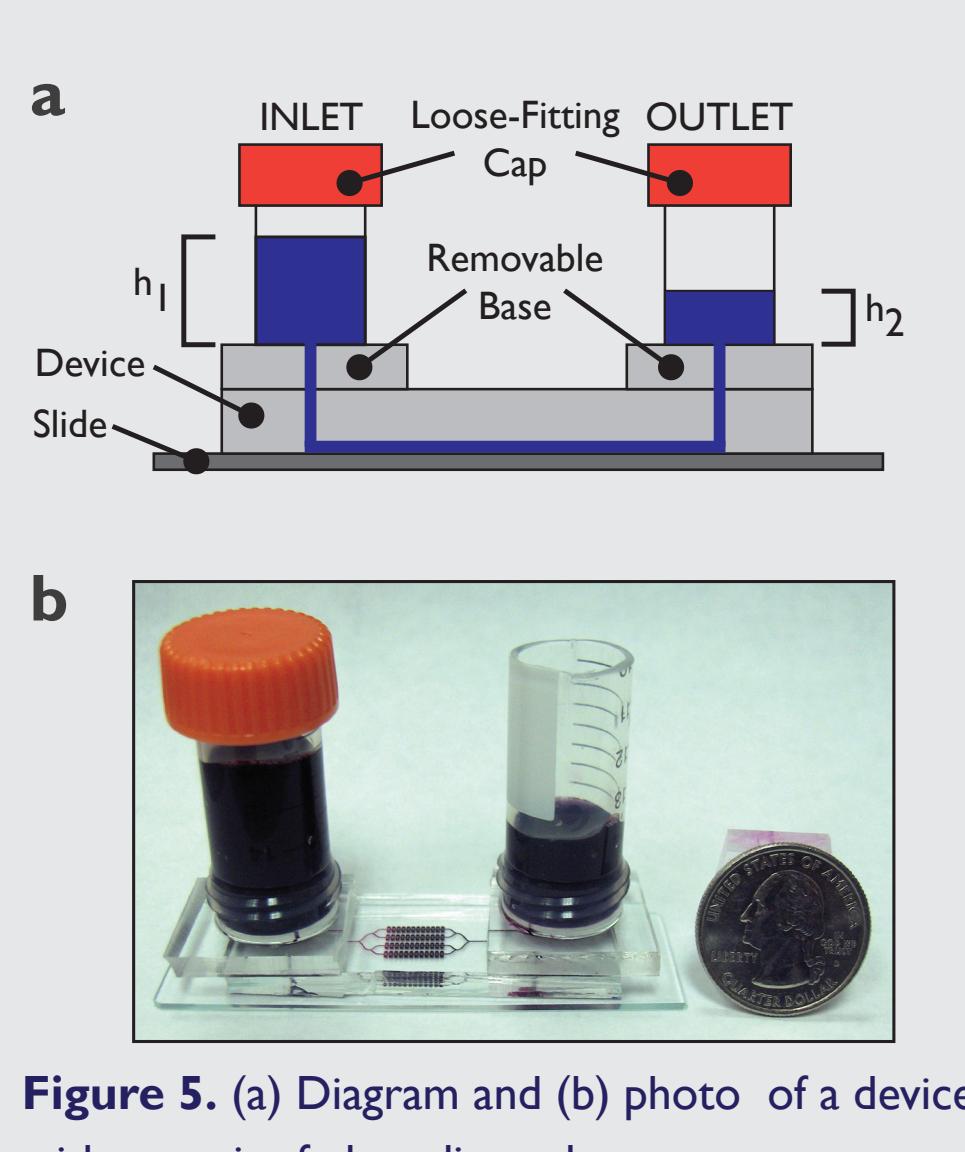
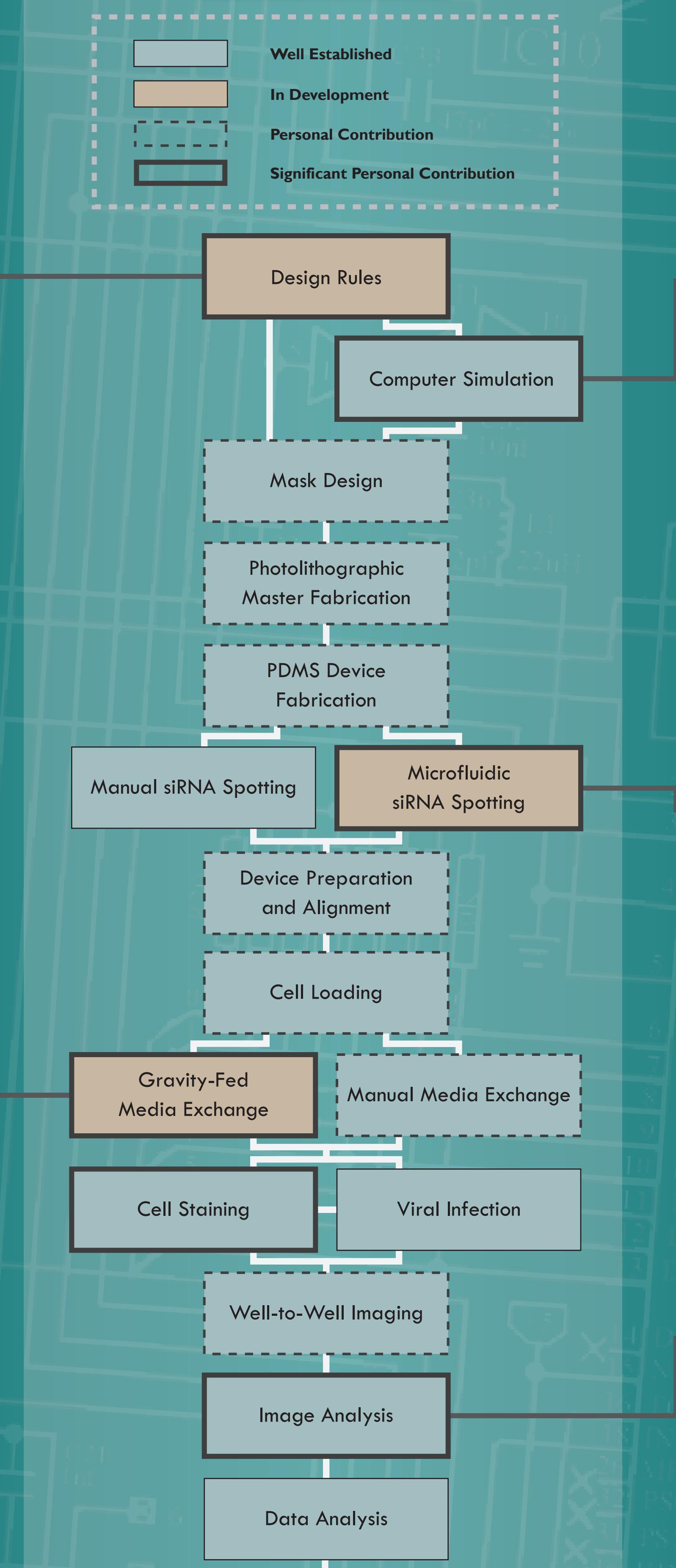


Figure 5. (a) Diagram and (b) photo of a device with a gravity-fed media exchange system.

One of the inherent problems with microfluidic cell culture systems is the buildup of waste and rapid depletion of nutrients within the wells. Continuous media profusion is the ideal approach to mitigating the problem of media stagnation. We have developed a gravity-driven system that allows for continuous media profusion for up to 48 hours without user intervention. The flow rate of media profusion can be precisely controlled by varying the difference in initial volume of the two reservoirs. Staining solution and virus particles can be injected through the reservoir holes or by removing the reversibly sealed bases.

DEVELOPMENT



The analysis of new designs and device features is accomplished through the use of an open-source workflow combining FreeCAD modeling and Elmer multi-physics simulation. A directional loading/profusion system was designed for the diffusion-type device using Elmer to optimize the fluidics (Fig. 2). The in-channel element allows for differential cell loading and media profusion (one direction increases flow into the wells for cell loading, whereas the other decreases flow to prevent cells from being rinsed from the wells).

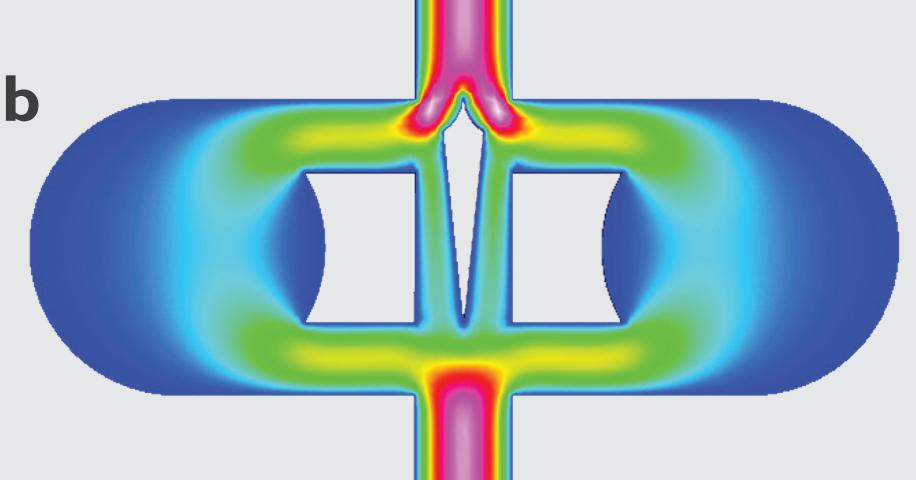


Figure 2. (a) Elmer mesh and (b) velocity profile from the directional diffusion well simulation.

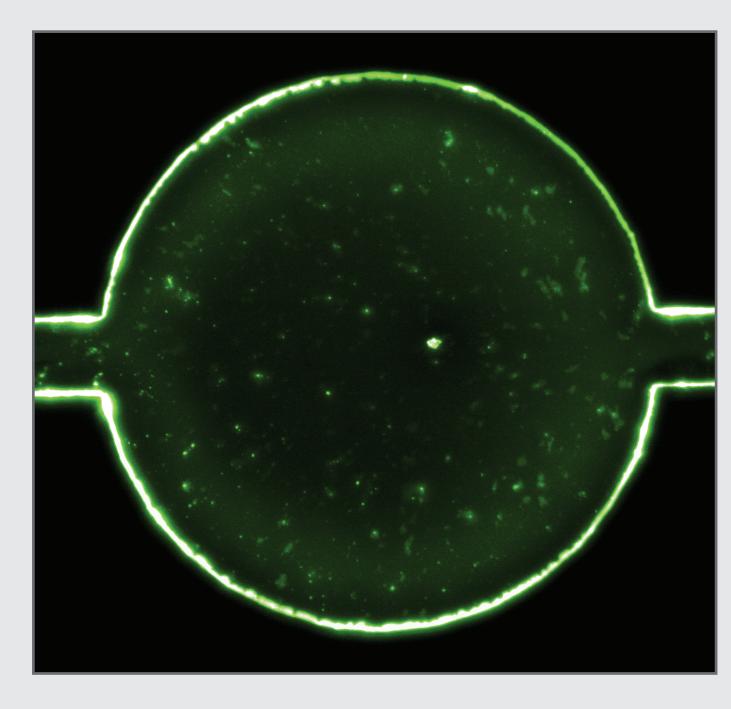


Figure 4. A 600 μ m wide spot of reverse transfection mix (gelatin, lipofectamine, water, and green fluorescing siRNA) on a GAPS II coated glass slide after drying and removal of spotting device.

During the development process, it is important to rapidly and effectively determine the number of living and dead cells within each well. While automated cell counting methods exist, they are often inaccurate, especially when analyzing images of confluent cells. As such, a hybrid macro was developed for ImageJ, allowing user intervention to correct exposure, check the automated count, and manually compensate for any errors. The macro then overlays the count information over the top-left corner of the image and saves the file as a compressed JPEG, with the count also recorded in the filename. Previous counting methods required about 8 hours per device, whereas the macro accomplishes equally accurate counts in 30 minutes.

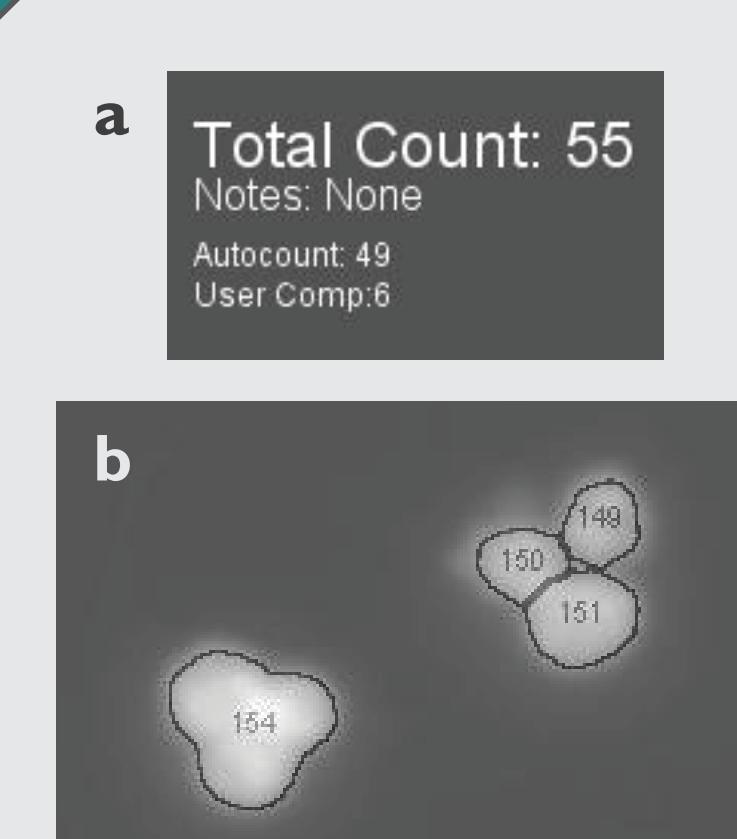


Figure 6. (a) Count detail overlay from a processed image. (b) A clump of cells (left) missed by the watershed function.

RESULTS

Microfluidic spotting is effective for RNAi

Spots resulting from microfluidic spotting are more consistent in form and concentration across replicates than comparable spots spotted by hand (Fig. 7c) or printing by machine (data not shown). Microfluidic spotting is a viable and superior alternative to these methods when efficiency and consistency across replicates is a high priority.

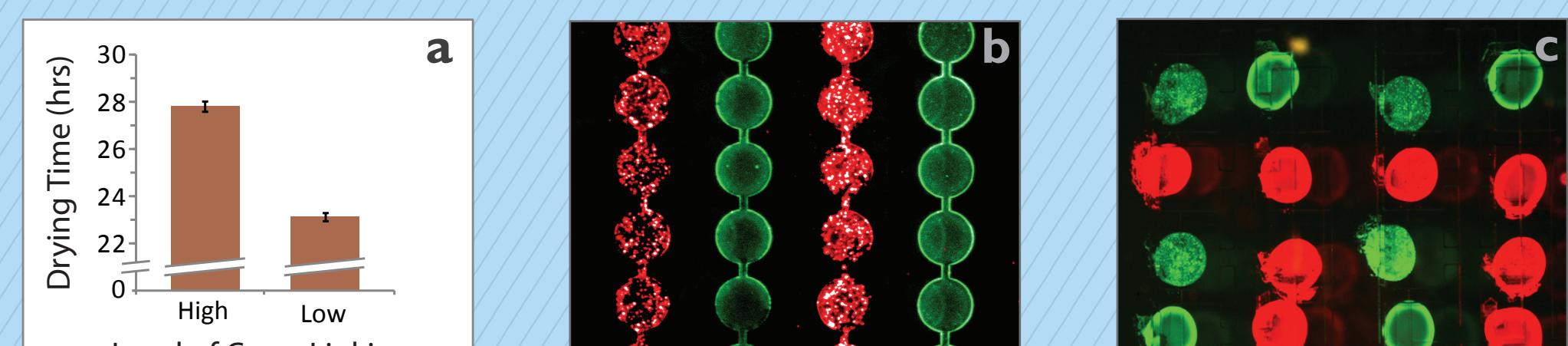


Figure 7. (a) Lower levels of cross-linking increase drying time (n=3, error bars=SE). (b) Alternating red and green fluorescent siRNA spotted with a microfluidic device (Fig. 3d). (c) A pattern of red and green fluorescent siRNA spotted by hand.

Viable cell densities are consistent across wells

Simple cell loading results in highly consistent cell counts across the wells of a microfluidic device (Fig. 8). The ability to individual count the cells within each well is a vast improvement over microtiter screening, which typically only quantifies well fluorescence, requiring additional controls to quantify the cells.

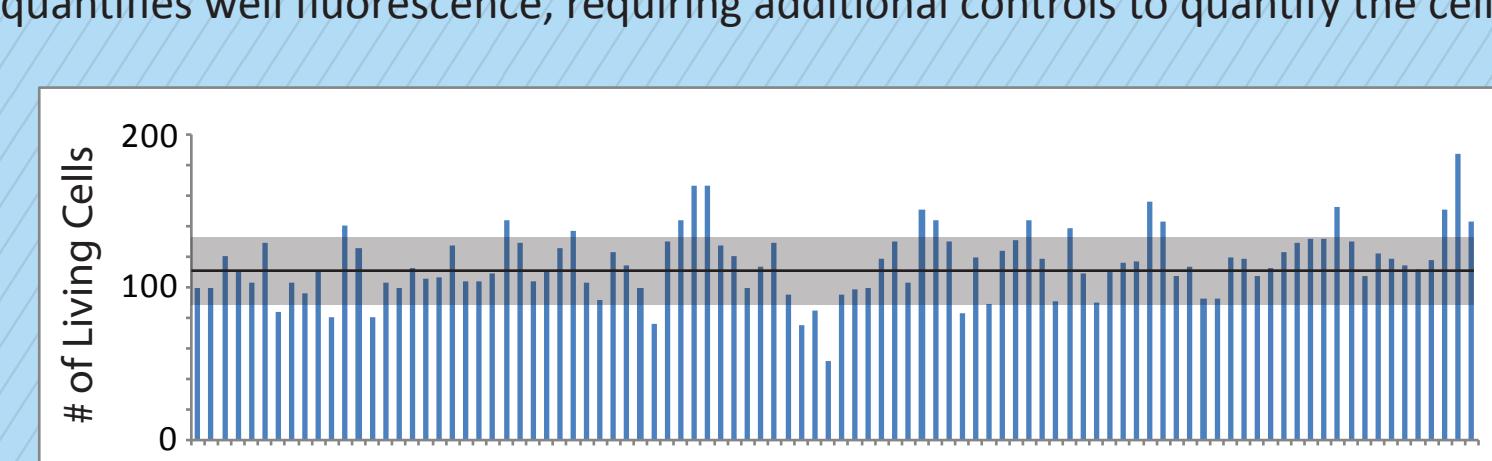


Figure 8. Per-well cell counts for an inline parallel control device (no siRNA spotting prior to loading) after 48 hrs of incubation. Grey area is one standard deviation (+/- 22.4) and the black line is the average (15.9).

Lipofectamine 2000 exhibits cytotoxicity

Spotting concentrations of Lipofectamine 2000 used for microarrays are too high for microfluidic applications, resulting in high levels of transfection mix cytotoxicity. In the experiment below, siRNAs known to be toxic do not appear to induce higher levels of toxicity than Lipofectamine spotted without siRNA (Fig. 9). Scrambled siRNA (CNT) and no spotting (Empty) have lower cell death.

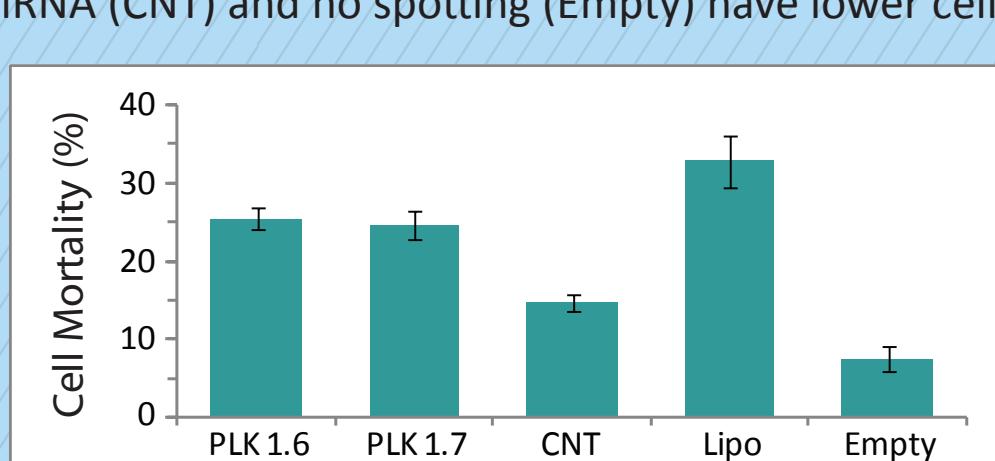


Figure 9. HeLa cell mortality as a function of reverse transfection in a microfluidic device (n=12, error bars=SE). PLK1.6/PLK1.7, known to be toxic, permeate cells at the same rate as Lipofectamine alone (Lipo). CNT mix contains scrambled siRNAs that should not interact with any genes in HeLa cells.

CONCLUSIONS AND CONTINUED DEVELOPMENT

- We have developed a 96-well microfluidics system capable of 72-hour cell culture and high-throughput RNAi
- Our tube-based gravity-fed profusion system is a simple substitute for manual media exchange or complex, multi-layer reservoirs
- Our novel microfluidic spotting system is a promising alternative to manual spotting
- A new device design will introduce direction-specific loading and profusion, improving loading density and minimizing cross-contamination
- The concentration of transfection agent in the spotting solution will be refined to minimize cytotoxicity

LOCKHEED MARTIN

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