

# pH Dynamics During Concentration Polarization

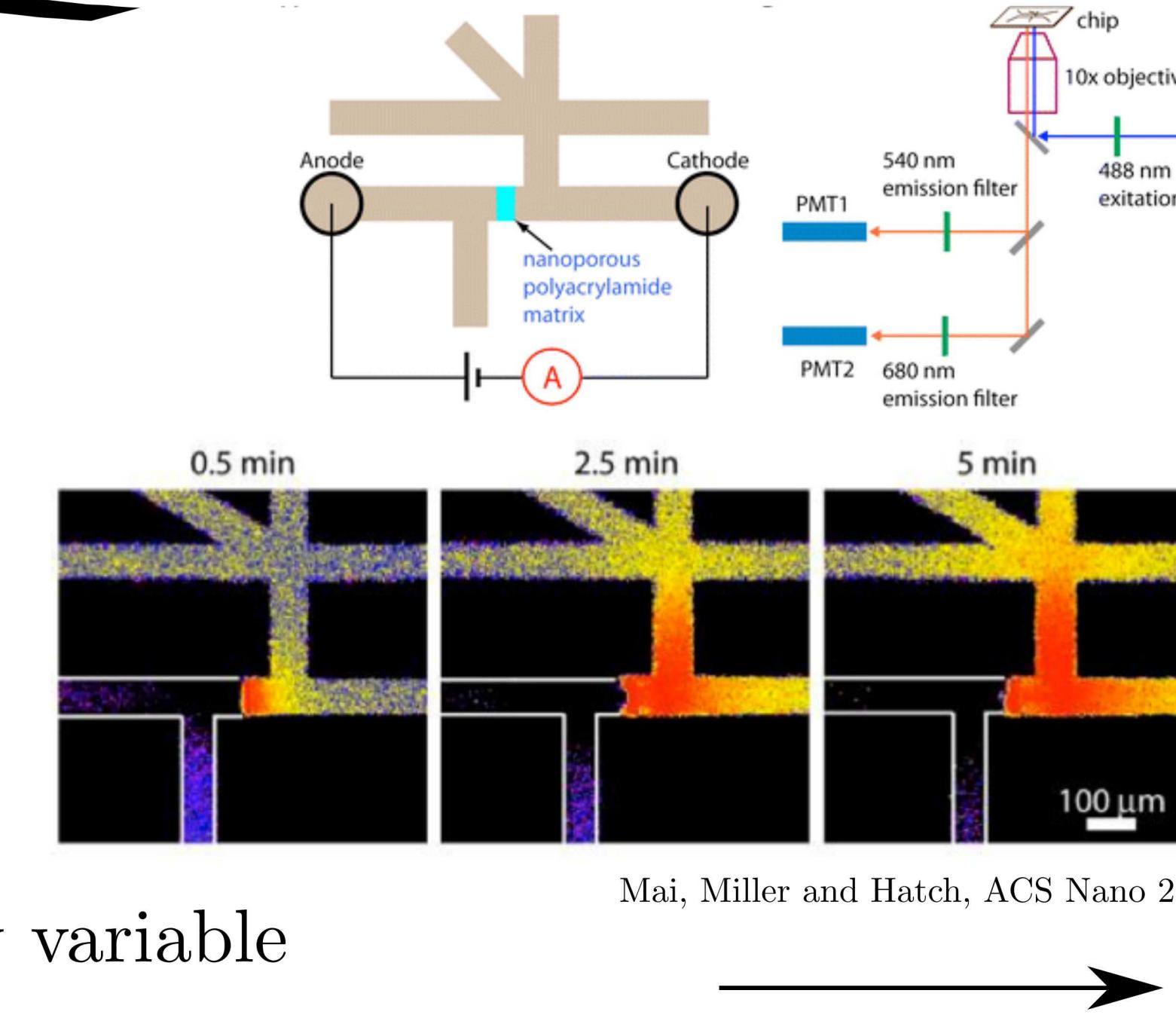
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## Motivation

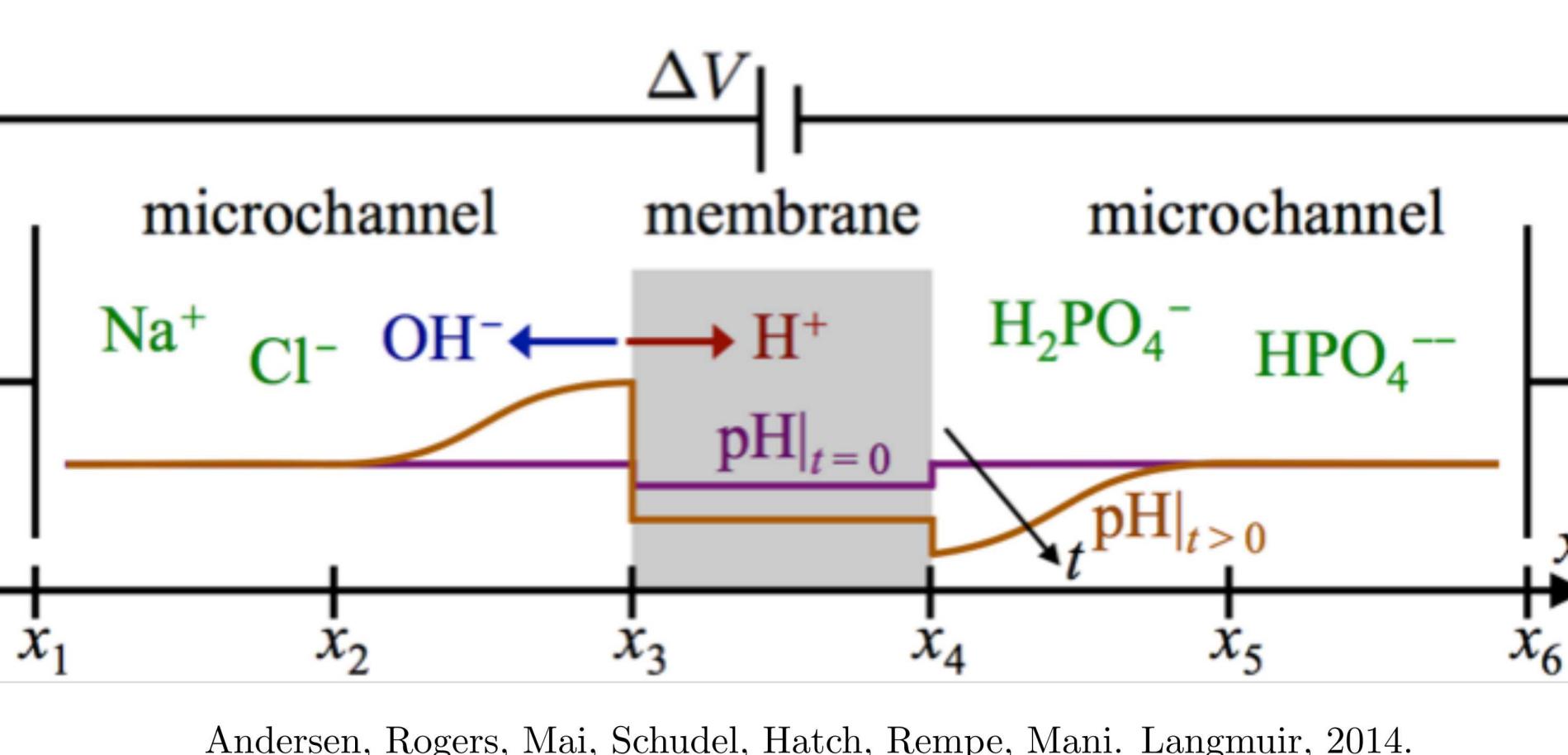
- Biological toxins are often difficult to detect because of their high activity, but low count.
- There is a real need to detect these in cases of suspected outbreaks, rather than waiting to see if symptoms occur.
- Nanofluidic electrophoretic sensing methods make ideal sensors:
  - can be mass produced and used in the field
  - can pre-concentrate samples to increase sensitivity
  - are easily integrated with other sensors
  - offer some ability for customization

## Experimental Setup

- In-situ polymerization creates pores.
- Experiment
  - 25-100 V/cm applied
  - 50  $\mu\text{m}$  channel passes cations
  - Concentration enriches at cathode
  - Proton transport creates pH imbalance
  - Balance of forces at membrane is highly variable
- probe mode: ratiometric pH-sensitive dye (SNARF) quantitatively measures concentration and pH dynamics near membrane



## Numerical Model



$$\text{pH} = 7.0, \text{rate} \sim 10^7 / \text{mM-s}$$

$$\text{H}_2\text{O}_{(\text{aq})} \xrightleftharpoons[k_{\text{h},\text{buf}}]{k_{\text{t},\text{buf}}} \text{OH}^-_{(\text{aq})} + \text{H}^+_{(\text{aq})}$$

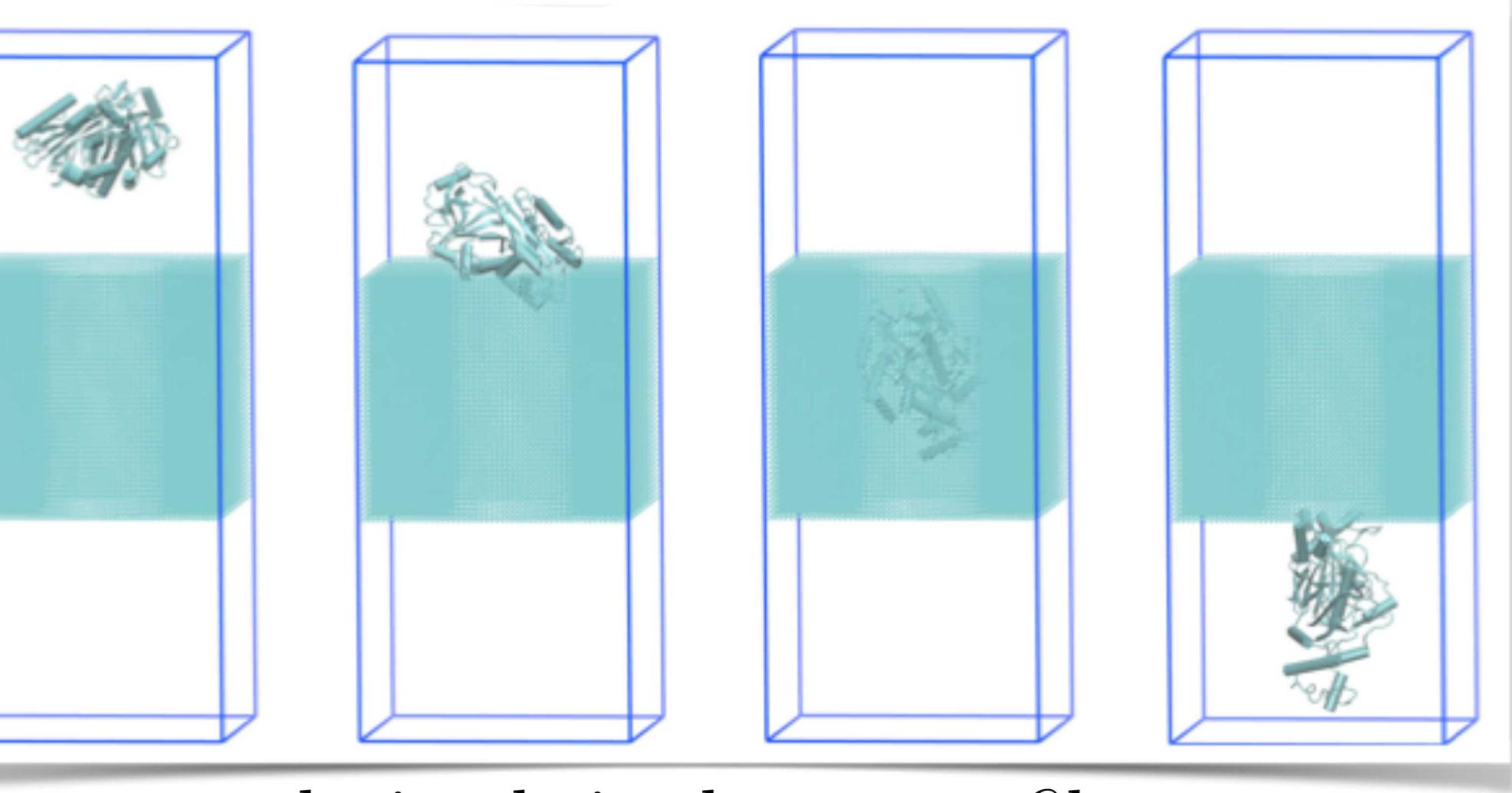
$$\frac{\partial c_i}{\partial t} + \frac{\partial}{\partial x} \left[ D_i(x) \left( -\frac{\partial c_i}{\partial x} - \frac{z_i c_i}{V_T} \frac{\partial \phi}{\partial x} \right) \right] = r_i$$

$$\frac{\partial}{\partial x} \left( -\varepsilon(x) \frac{\partial \phi}{\partial x} \right) = e \sum z_i c_i$$

$E = 25 \text{ V/cm}$
$I = 160 \text{ mM (6 mM buffer)}$
Diffusivity ( $10^{-5} \text{ cm/s}$ )
$\text{Na}^+$ 1.3
$\text{Cl}^-$ 2.0
$\text{H}_2\text{PO}_4^-$ 0.96
$\text{HPO}_4^{2-}$ 0.76
$\text{OH}^-$ 5.3
$\text{H}^+$ 9.3

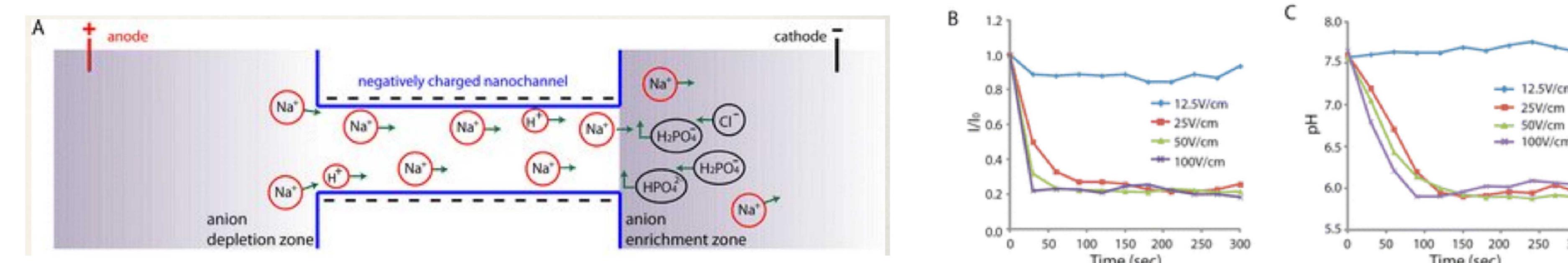
Dimensions (mm)	
Membrane Length	0.05
Resolved Simulation Length	1.55
Total Microchannel Length	41.55

## Protein Sensing



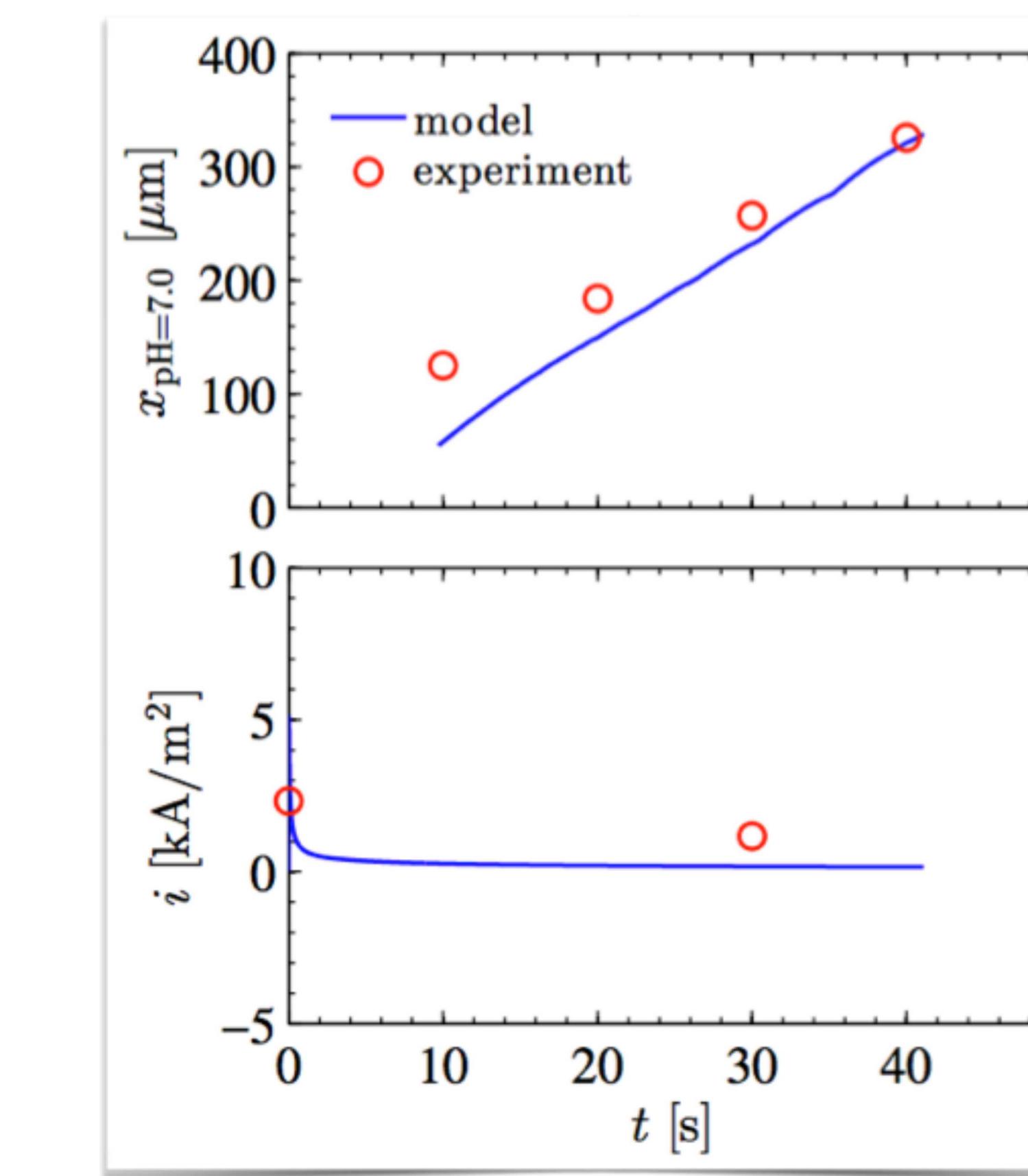
- Based on their sequence, proteins vary greatly in their charge profile, and ability to unfold.
- A membrane with well-defined, nanometer size pores requires partial unfolding for large proteins to pass.
- Voltage and solution makeup at both interfaces can be tuned to detect protein toxins or cellular distress signals.

## Concentration Polarization



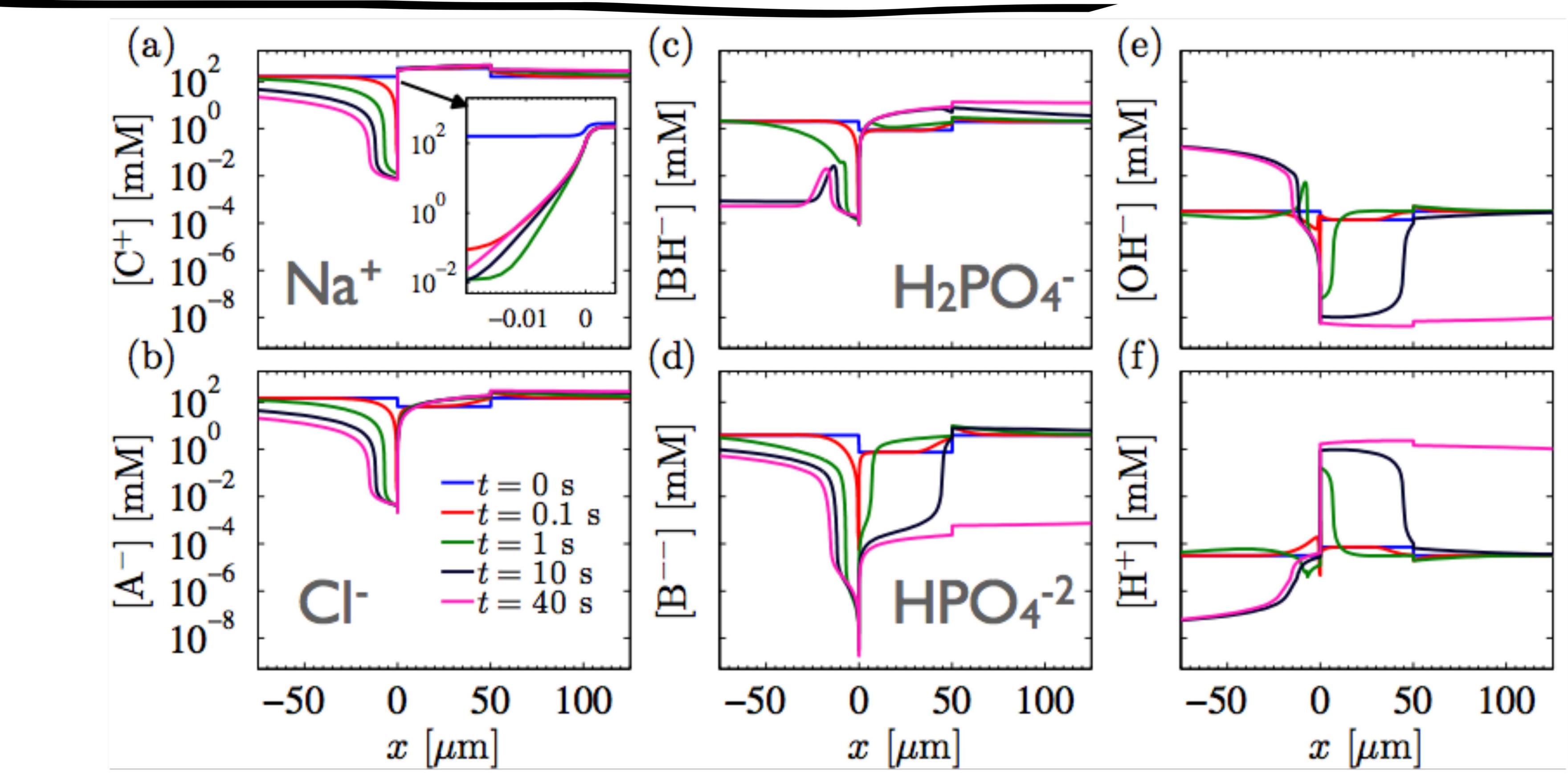
- Cations flow toward the cathode, but are rejected by the membrane.
- Those remaining form the enrichment zone, where concentrations can soar to  $O(100\times)$ .
- The amount of CP is described by the Dukhin number (the ratio of bulk to surface ion mobility) and the bulk diffusion of the co-ion.

## Key Comparison (pH Dynamics)

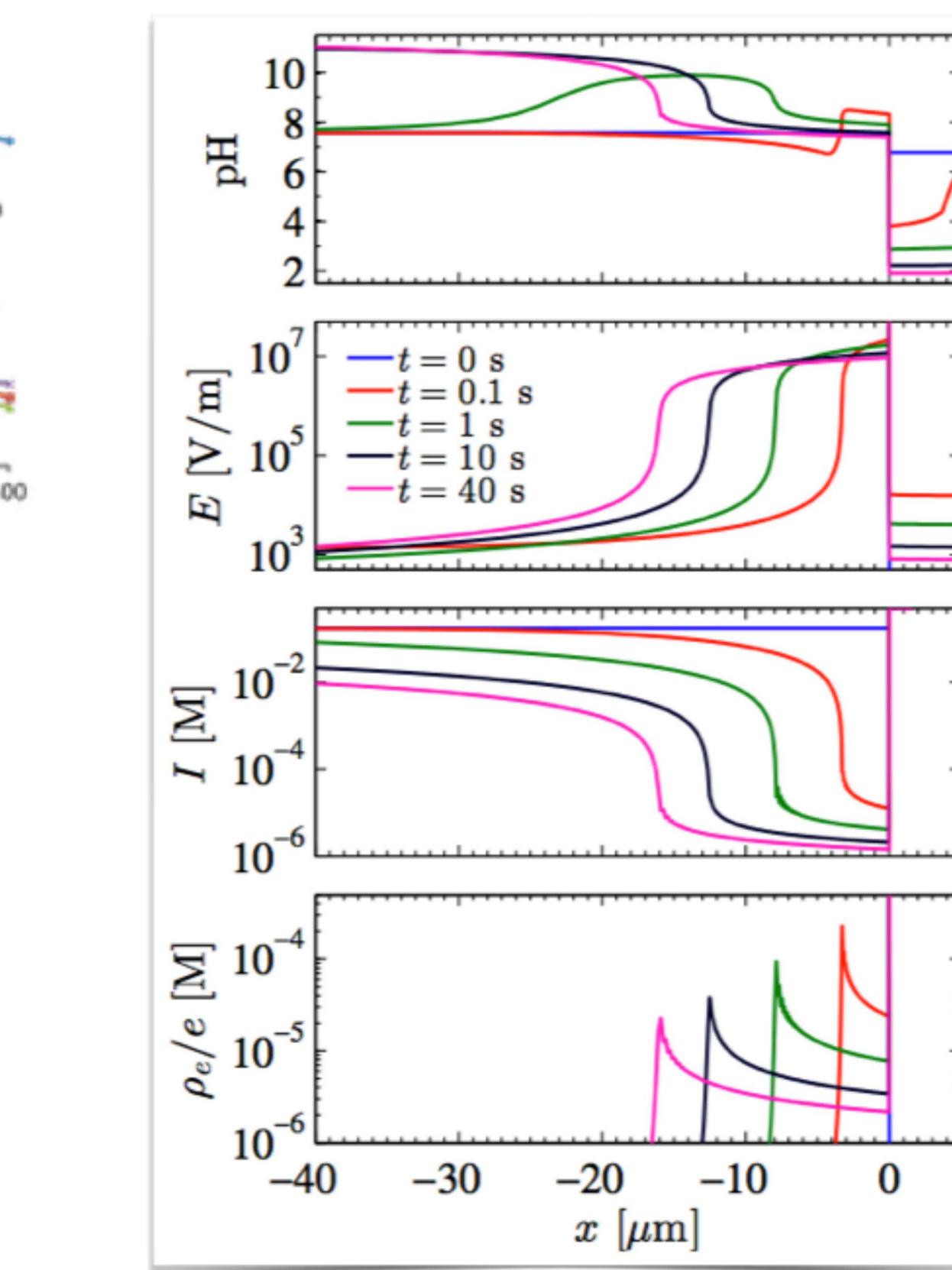


- pH dye is most sensitive at pH 7 – so we check the progression of the front
- Near-perfect fit requires adjusting only the water splitting rate.
- The strong ionic environment of the membrane catalyzes this process 10 $\times$ .
- Total current agrees qualitatively, but few experimental data points.

## At the Interface



## Time and Parameter Dependence



- Total device length affects voltage at the membrane.
- Net space-charge builds up on the  $\mu\text{m}$  scale away from the channel (conduction faster than reaction)
- The 10 $^5$  V/cm field moves with the charge front.
- violates electroneutrality, local equilibrium, and EDL theory ( $\lambda_D \sim 1\text{nm}$ )

## Conclusions

- CP allows very nonlinear tuning of the electric field and buffer concentration near an interface.
- Numerical modeling is required to capture these complex driving forces.
- $\text{H}^+$  and  $\text{OH}^-$  directly contribute  $\sim 3\%$  to net charge transport.
- Electrostatics is still the dominant driving force for protein unfolding at the interface, but varies greatly with membrane charge and hydrolysis properties.
- These provide boundary conditions for molecular simulations.