

Using Parallel Stiffness to Achieve Improved Locomotive Efficiency with the Sandia STEPPR Robot

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Abstract—In this paper we introduce STEPPR (Sandia Transmission-Efficient Prototype Promoting Research), a bipedal robot designed to explore efficient bipedal walking. The initial iteration of this robot achieves efficient motions through powerful electromagnetic actuators and highly backdriveable synthetic rope transmissions. In this paper we show how the addition of parallel elastic elements at select joints are predicted to provide substantial energetic benefits: reducing cost of transport by 30 to 50 percent. Two joints in particular, hip roll and ankle pitch, reduce dissipated power over three very different gait types: human walking, human-like robot walking, and crouched robot walking. Joint springs based on this analysis are tested and validated experimentally. Finally, this paper concludes with the design of two unique parallel spring mechanisms to be added to the current STEPPR robot in order to provide improved locomotive efficiency.

I. INTRODUCTION

Recent disasters both natural and manmade have illustrated the need for robotic technologies to enter damaged or destroyed buildings, power-plants and other infrastructures in order to search for survivors, investigate conditions, or shut down critical systems. For many of these applications, the robots must traverse terrain originally designed for humans such as stairs, ramps, and uneven surfaces. Therefore, bipedal robotic systems have emerged as one preferred solution to this challenge. The recent DARPA Robotics Challenge (DRC) Trials demonstrated several robot designs that successfully employ bipedal walking to navigate complex environments [1].

An ongoing challenge for bipedal robots is achieving high system level efficiencies. One convenient way to quantify efficiency is to use cost of transport (CoT). Cost of transport can be calculated using the energy consumed, E , distance traveled, d , and the mass m

$$CoT = \frac{E}{mgd} \quad (1)$$

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Thus far, only passive dynamic walking concepts have provided improved efficiency over human walking ($CoT = 0.2$) [2]. More versatile fully actuated bipedal robots still can only achieve a cost of transport that is an order of magnitude larger than humans [3]. This means that the ability to perform actual missions is severely restricted by battery life and size. Achieving efficiencies comparable to human walking could potentially provide a ten-fold improvement in robot mission times. This is especially important for operations in hazardous environments where recharging the robot system very challenging.

Our group is developing a novel bipedal robot, known as STEPPR (Sandia Transmission-Efficient Prototype Promoting Research), that attempts to achieve dramatic improvements in walking efficiency. This robot, shown in Fig. 1, uses a combination of powerful DC motors and low transmission ratios to achieve highly backdriveable and efficient motions. While this is a multifaceted approach encompassing transmission design, walking control, and motor design, one key element is the use of elastic parallel elements to increase the efficiency of joint actuators.

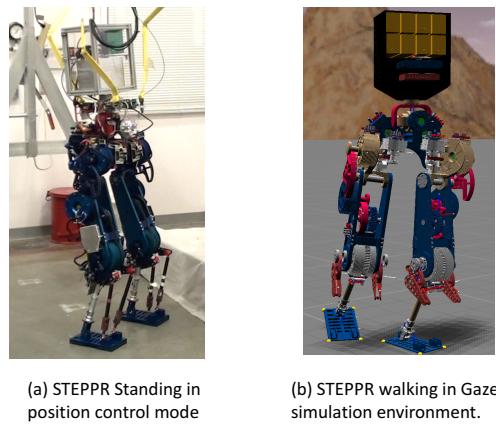


Fig. 1. STEPPR holding a standing pose (a) and walking in an SCS simulation (b).

It is well known that bipedal human like walking includes spring-like energy storage and release at several joints, most notably the ankle [4]–[10]. Parallel spring elements at certain joints can be used to substantially reduce the torque output required of the joint motor, τ_m . The mechanical power at the joint remains the same, but electrical power dissipated by the motor is substantially reduced. Since the dissipated power is proportional to τ_m^2 , reducing motor torque can play

a critical role in increasing joint efficiency. In addition, by reducing the torques on the actuator output, the actuator and drivetrain can be reduced in size. For example, gears, cables, belts, and bearings could all be reduced in size. This would enable considerable savings in weight or could be used to increase robustness and fatigue life of components.

Designs for passive prostheses or robots have incorporated springs, as have wearable assisting devices such as prosthetic ankles [4], or exoskeleton type suits [11], [12]. Despite the potential benefits for walking robots, to our knowledge relatively few parallel stiffness elements have been designed and tested for incorporation into fully actuated walking robots.

In this paper we use a data driven approach to examine joint level behaviors across several bipedal walking gaits. This data shows how elastic elements can provide benefits across several types of gaits. Interestingly, for a chosen joint, a fixed stiffness can be chosen and the differences across different gaits can be accounted for by adjusting the zero position of the spring. These lessons are used to design parallel elastic systems for the STEPPR ankle, hip, and knee. These concepts have been evaluated at the bench level. Full scale functional designs for the STEPPR robot have been developed and are envisioned as drop in “kits” for providing improved gait efficiency.

II. STEPPR ROBOT

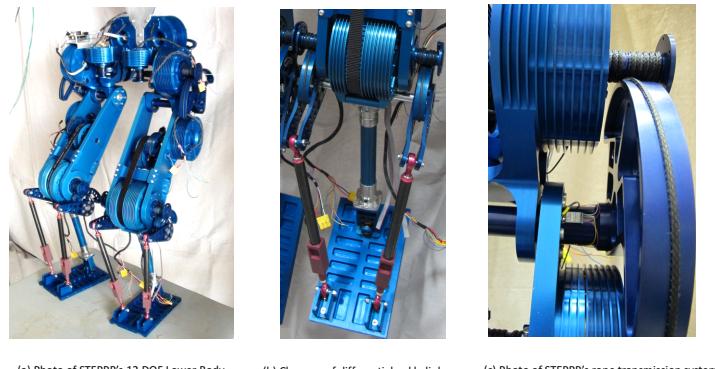
The Sandia Transmission-Efficient Prototype Promoting Research (STEPPR) robot was designed to serve as an efficient electromagnetic baseline robot testbed that supports the testing of gait-based interventions to provide even greater efficiency. STEPPR, shown in Fig. 1 and Fig. 2 includes six degrees of freedom per leg (hip adduction-abduction, flexion-extension and rotation; knee flexion-extension; and ankle dorsi-plantar flexion and inversion / eversion) as well as three rotational back joints.

All joints other than the ankles are driven with pure rotary actuators. Each ankle uses two rotary actuators that each drive a pushrod, providing a differential drive for the two ankle degrees of freedom. The pushrods form closed linkages that produce an effective gear ratio that varies by up to approximately 30 percent in the joint workspace. A close up view of the ankle linkage is provided in Fig. 2-b.

STEPPR was designed to use very high torque motors (Megaflux series from Allied Motion Technologies with highly-efficient, low-reduction transmissions. Transmission ratios from motor to joint outputs range from six to ten for different joints. These modest gear reductions are implemented at each joint using a pair of pre-tensioned synthetic ropes that wrap around an input sheave and an output pulley. A photograph of this synthetic rope transmission is shown in Fig. 2-c. This arrangement produces a drivetrain that is highly backdrivable when unpowered. Torque control is achieved through open-loop current control. Losses are dominated by joule heating in the motors.

STEPPR includes highly efficient custom joint electronics and internal communications that collectively draw less than 20 W for all 15 leg and back joints. STEPPR also allows for variable torso mass to simulate onboard batteries, computation,

and other options. In its 75 kg configuration, STEPPR requires just 100 W (1.5 A at 65 V) to stand and support its own weight using joint position control. STEPPR was designed to allow the temporary installation of support elements at certain joints to increase total locomotive efficiency. Support elements could include parallel or series compliances, mechanisms that provide pose-dependent gear reductions, switchable transmissions, or other passive or active dynamic elements. Such elements may be designed using data from simulated and tested STEPPR gaits and implemented on the robot to verify energetic benefits.



(a) Photo of STEPPR's 12 DOF Lower Body (b) Close-up of differential ankle linkage (c) Photo of STEPPR's rope transmission system

Fig. 2. Photograph of the STEPPR lower body illustrating the powerful DC motors and synthetic cable drive system.

III. COORDINATE SYSTEM

We begin by outlining the coordinate system used in this paper. Since the coordinate usage in the biomechanics literature tends to differ from the robotic literature, the biomechanical data is converted to match the most common robotic coordinate system. This coordinate system is outlined in Fig. 3. The body coordinate frame is centered at the pelvis, and the coordinate frame at each joint matches this overall convention. The hip rotations (black) are measured relative to the pelvis, the knee rotations (blue) are measured relative to the hip, and the ankle rotations (red) are measured relative to the knee. Throughout the paper we refer to rotations about the x , y , and z axes as roll, pitch and yaw respectively. Note that with this sign convention, spring-like behavior appears as a negative slope on the joint torque vs. angle curve. For consistency, all joint data described in this work are from the left leg.

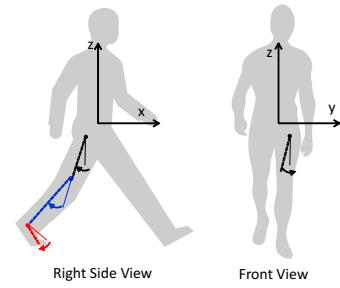


Fig. 3. An illustration of the coordinate system used throughout this work.

IV. ELASTIC ELEMENT SELECTION APPROACH

In this work we have analyzed three distinct data sets:

- 1) Human walking taken from human subjects [13].
- 2) Human-like robot walking simulations developed by the Institute for Human Machine Cognition (IHMC) for the Boston Dynamics ATLAS robot [14].
- 3) Conservative crouched gait simulations developed by IHMC for the Sandia STEPPR robot.

These three gaits provide the range of behaviors we predict for the STEPPR robot. Type 3 gaits are the motions generally associated with walking robots, slow and crouched gaits that allow the robot to maintain its balance. Type 2 gaits represent the results of advances in walking research with gaits becoming more dynamic and more similar to human gaits in speed and efficiency. This is a growing research field with several recent achievements [14]–[16]. Finally, type 1 gaits represent the “gold standard” for fully actuated bipedal walking. As gait algorithms and control strategies continue to evolve, we envision robots moving increasing towards type 1 gaits.

Our spring design approach is a sequential process. We begin by analyzing gait data joint by joint to roughly determine a parallel spring stiffness that provides benefit across all 3 gait types outlined above. Once this stiffness is determined, the gait data is again analyzed to determine the best zero location for the spring. This process must include several nuances because some gaits do not benefit from springs or do not benefit enough to influence the stiffness selection. In addition, most springs provide maximum energy benefit when unique behaviors such as selective engagement (during only a portion of the gait cycle) or unidirectional functionality are applied.

The key metric we attempt to minimize is joint motor energy consumption over the gait cycle. Since our actuators are brushless DC motors with high efficiency transmissions we use a simple DC motor model to estimate energy consumed. Specifically, we use the motor constant, K_m , the joint torque, τ_j , the joint speed ω_j , and the transmission reduction N .

$$E_m = \int \left(\frac{\tau_j(t)^2}{N^2 K_m^2} + \tau_j(t) \omega_j(t) \right) dt \quad (2)$$

The first term in the integrand represents Joule heating losses, and the second represents mechanical output energy. Other less significant loss elements are neglected for simplicity.

We choose a fixed stiffness, because as we show in this work, the stiffness for a joint can remain fixed while still providing substantial benefits. In addition, while there have been recent advancements in achieving variable stiffness, adjusting the equilibrium position can be achieved with several types of simple mechanical designs.

V. ANKLE PITCH

During human-like walking, the ankle provides most of the power input to the system, and is known to benefit from a parallel spring [4]. Interestingly, all three gait types illustrate behaviors that benefit from a parallel spring. Plots of ankle torque vs. ankle angle for each gait are shown in Fig. 4.

Consider the case of the planted left foot for the human data in Fig. 4-a. As the body center of mass moves forward and causes the ankle to dorsiflex (negative pitch), the torque required to resist the falling of the body center of mass is positive and increases as the body falls further forward. A spring located at the ankle would therefore reduce the motor torque by providing a torque that increases with dorsiflexion. The human-like robot gait shows very similar behavior (4-b). The crouched robot gait shows a different behavior, with a sharp initial drop in torque followed by a more gradual increase.

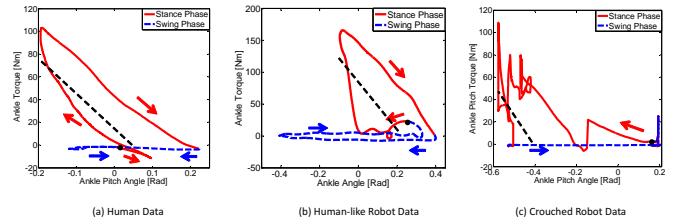


Fig. 4. Data showing the ankle torque vs. ankle position behavior for the three gait types. The black dot denotes the onset of ground contact, and the black dashed line represents the proposed $400\text{Nm}/\text{rad}$ spring.

Note that this spring-like behavior only occurs during stance and not swing. Stance only springs have been proposed in prior works [6], [7], and for ankle discussions we will assume a spring that only engages during stance. Discussion on designs that achieve this performance will be provided in later sections. With this stance-only behavior considered, Fig. 4 shows that a spring with stiffness of roughly $400\text{Nm}/\text{rad}$ shows promise for all three gait types.

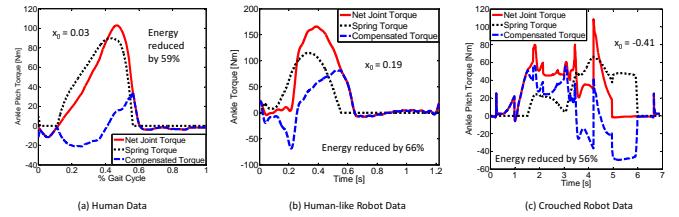


Fig. 5. Data showing the benefits of the $400\text{Nm}/\text{rad}$ parallel spring for the three gait types.

Using the stiffness of $400\text{Nm}/\text{rad}$, the optimal zero location, x_0 , was determined for each gait type. As Fig. 5 shows, this spring stiffness provides substantial energy reductions ranging from 56 to 66 percent.

VI. HIP ROLL

Hip roll behavior also benefits from a parallel spring for all three gait types. The data in Fig. 6 shows that a one-way spring with stiffness $500\text{Nm}/\text{rad}$ provides clear benefits for all three gait types. In this case, the spring does not need the stance-only behavior of the ankle, making the overall design much simpler.

The torque reductions provided by the $500\text{Nm}/\text{rad}$ parallel spring are illustrated in Fig. 7. This simple spring provides substantial energetic benefits, reducing the energy over a gait cycle by 40-90 percent.

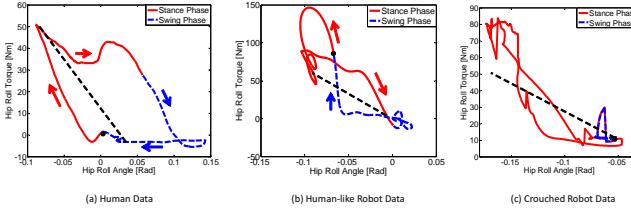


Fig. 6. Data showing the hip roll torque vs. hip roll position behavior for the three gait types. The black dot denotes the onset of ground contact, and the black dashed line represents the proposed $500\text{Nm}/\text{rad}$ spring.

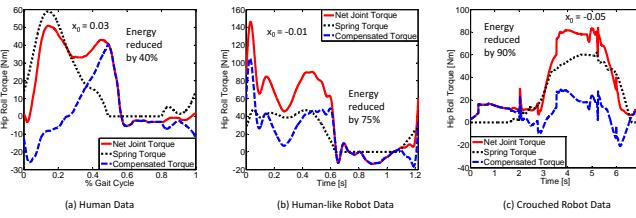


Fig. 7. Data showing the benefits of the $500\text{Nm}/\text{rad}$ parallel spring for the three gait types.

VII. HIP PITCH AND KNEE PITCH

While ankle pitch and hip roll are the joints where parallel springs provide clear gains for all three gait types, hip and knee motions benefit from more tailored designs. For example, as shown in Fig. 8, a spring with stiffness $72\text{Nm}/\text{rad}$ and zero position of -0.16rad reduces the energy per cycle by 87 percent for the human gait. However, these benefits are not seen for gait types 2 or 3.

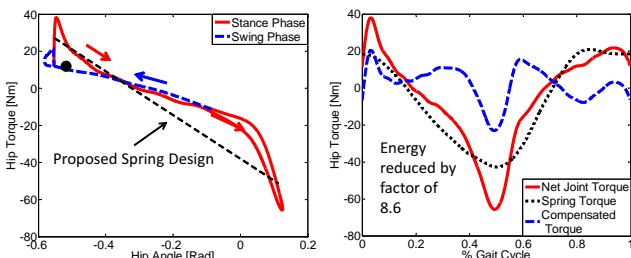


Fig. 8. Simulation showing hip pitch torque vs. hip pitch position (a) and the torque reduction when a $72\text{Nm}/\text{rad}$ parallel spring is used (b).

Similarly, a spring that acts to keep the knee out of hyperextension provides some benefit at the knee during the human-like robot gait. A spring with stiffness $200\text{Nm}/\text{rad}$ and zero position 0.2rad reduces the motor torques and allows the motor to harvest energy during the gait. The parallel spring behavior is shown in Fig. 9. The spring reduces dissipated energy by $42\text{J}/\text{cycle}$ per leg, going from $+12\text{J}/\text{cycle}$ to $-30\text{J}/\text{cycle}$ at each leg. This amount of energy savings is comparable to that achieved at the ankle for the same gait ($59.5\text{J}/\text{cycle}$ per leg).

While these two joints do not provide clear benefits across gaits, there may be cases where either or both parallel spring designs may provide energetic benefit. The hip pitch spring is

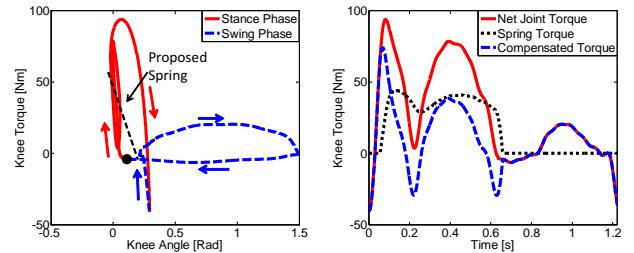


Fig. 9. Simulations based on human-like robot gait data illustrating the knee motion-torque profile (a) and the torque savings when a $200\text{Nm}/\text{rad}$ parallel spring is used (b).

especially promising because we hope to achieve more human-like gait characteristics in the future.

VIII. ENERGETIC BENEFIT SUMMARY

The net energetic savings for each gait was calculated by combining the electrical energy at each joint (hip pitch, hip yaw, hip roll, knee pitch, ankle pitch). Each joint actuator model was determined using the STEPPR motor constants for that joint and the STEPPR gear reduction for the joint. A summary of the joint spring designs is provided in Table I. The energy per cycle and predicted cost of transport for each of

TABLE I
SUMMARY OF JOINT SPRING PARAMETERS

| Joint | K All Gaits (Nm/rad) | x_0 Type 1 (Rad) | x_0 Type 2 (Rad) | x_0 Type 3 (Rad) |
|------------|------------------------------|--------------------------|--------------------------|--------------------------|
| Ankle | 400 | 0.03 | 0.19 | -0.41 |
| Hip Roll | 500 | 0.03 | -0.01 | -0.05 |
| Knee Pitch | 200 | N/A | 0.2 | 0.2 |
| Hip Pitch | 73 | -0.15 | N/A | N/A |

the three gait types is shown in Fig. 10. Note how the addition of elastic elements provides substantial reductions across all three gait types. Most importantly, this analysis predicts that the initial COT for STEPPR will be reduced from 2.76 to 1.88. Since we are optimistic more human-like gaits can be achieved, it is possible that STEPPR combined with parallel elastic elements could eventually achieve a COT of ~ 0.75 .

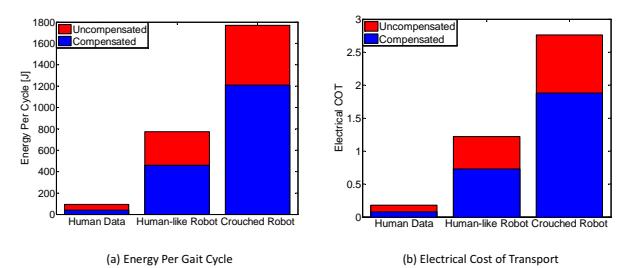


Fig. 10. Simulations illustrating the total energy per cycle (a) and predicted electrical cost of transport (b).

IX. SPRING DESIGN

The spring choices are summarized in table I. Since the required springs must provide large torques and high torsional stiffness, we chose to use spiral torsion springs. The spiral torsion springs were designed using well known equations [17]. We assume the springs are made of spring steel ($E = 193\text{GPa}$, $\sigma_{yield} = 1200\text{MPa}$). The maximum moment, M , and travel, θ_s , can be computed from the gait data. The spring width, w , and thickness, t , (shown in Fig. 11-a) were selected to be 38mm and 4mm respectively in order to ease fabrication.

The active length, L , and the peak stress, σ_p can be computed using formulas based on bending [17].

$$L = \frac{Ewt^3\theta_s}{12M} \quad (3)$$

$$\sigma_p = \frac{6M}{wt^2} \quad (4)$$

Based on this analysis, springs for each joint were manufactured by Associated Spring. Photographs of the springs are shown in Fig. 11-b. Note that two springs in parallel are used to achieve the desired ankle performance.

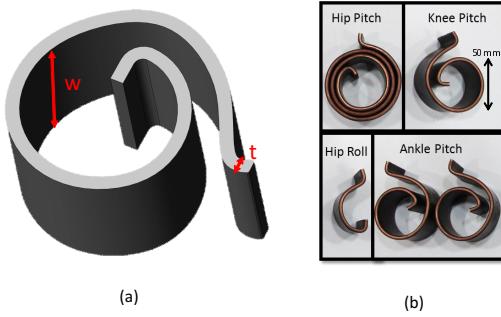


Fig. 11. Schematic diagram showing spiral spring dimensions (a) and photographs of the spring samples.

X. BENCH LEVEL VALIDATION

In order to evaluate the spring designs and their underlying analysis, several characteristic trajectories were evaluated on a custom-built dynamometer. The system, shown in Fig. 12, consists of a large geared “trajectory motor” capable of rapid motions under large torques. The trajectory motor is connected through a torque sensor to the output of a synthetic rope transmission (6:1 ratio). The input of the rope transmission is connected to an Allied Motion Megaflux motor, identical to the hip pitch motor on STEPPR. We refer to this motor as the “torque motor.” The trajectory motor operates in position control while the torque motor operates in current control. The rope transmission is highly efficient and output torque roughly scales with current command to the torque motor. With this setup we can run joint trajectories from our simulated gaits and measure the ability of the torque motor to provide the desired torque while moving as it would during a gait. The phase currents into the torque motor are measured and are used to determine motor power dissipation. We use power dissipation

rather than net motor power due to ease of measurement (motor voltages are noisy due to PWM switching). The reductions in power shown below differ from the predictions due to both the use of dissipated power rather than total power, and due to the fact that the torque motor and transmission ratio do not perfectly match either the hip roll or the ankle pitch joint on STEPPR.

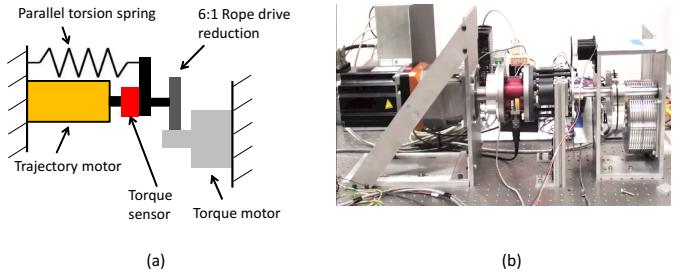


Fig. 12. Schematic diagram (a) and photograph (b) of the dynamometer setup.

A parallel torsion spring can be added in order to evaluate the energy savings. The torque trajectory is adjusted to account for the behavior of the spring. The net joint torque is assumed to remain constant, but the electrical power into the torque motor should reduce. We experimentally evaluated two characteristic trajectories with their specific springs: crouched robot hip roll, and human-like robot ankle pitch. These two were chosen because they were two of the most significant in terms of energy savings.

A. Crouched Robot Gait: Hip Roll

The results for the hip roll trajectory are shown in Fig. 13. This trajectory was evaluated at full load and full speed. As Fig. 13-a shows, the torque matches up well. As predicted, the presence of the hip roll spring saves considerable power, reducing the dissipated power by 93 percent.

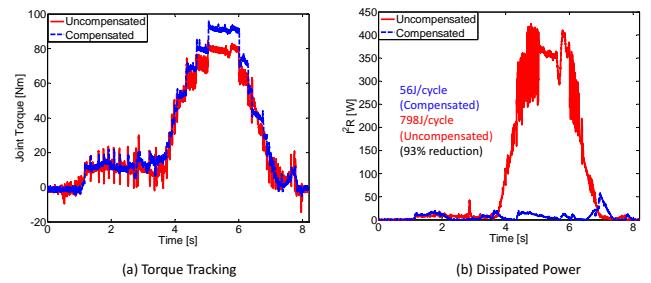


Fig. 13. Experimental data showing torque (a) and dissipated power (b) with and without a hip roll spring.

B. Human-like Robot Gait: Ankle Pitch

To account for limitations in the torque motor, the ankle pitch trajectory was scaled down by 25 percent. In addition, due to space constraints, only one of the two springs was used, resulting in a stiffness of 200Nm/rad . Finally, this system did not include selective engagement. Therefore the compensated stance and swing phases were performed separately and their

data reassembled together in post-processing. The results in Fig. 14 show that even a single spring provides considerable reductions in dissipated power.

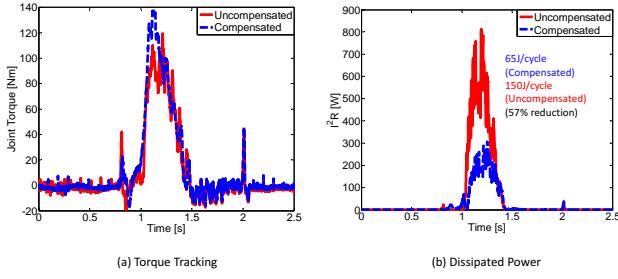


Fig. 14. Experimental data showing torque (a) and dissipated power (b) with and without an ankle pitch spring.

XI. JOINT SPECIFIC MECHANISM DESIGN

With the effectiveness of the full scale spring designs confirmed for hip roll and ankle pitch, the final step is two design “kits” that allow them to mount onto the existing STEPPR design.

A. Hip Roll

The hip roll design is relatively straightforward because it does not require selective engagement. A rendering of the design is provided in Fig. 15-a. As the left leg rolls inward (negative roll angle), the green holder and the red tab come into contact with the spring. However, for motions in the positive roll direction, the spring provides zero torque. Adjustment for different gaits can be achieved by replacing the red engagement tab with longer or shorter pieces. This design has been fabricated and will be tested during real walking soon. A photograph of the prototype design attached to the back of STEPPR is shown in Fig. 15-b.

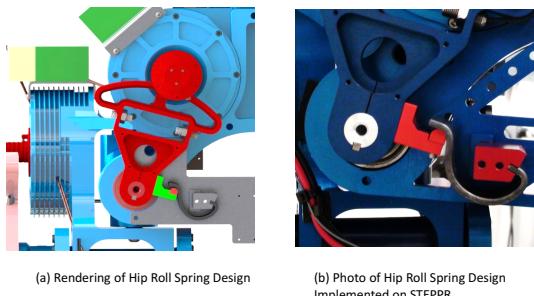


Fig. 15. A rendering (a) and photo (b) of the hip roll spring design.

B. Ankle Pitch

The ankle pitch design is considerably more challenging. This is due to the need for stance only engagement. While many approaches can be used for stance only engagement, we chose to use the force in the shank to activate the spring. Simulation data shows that the force in the shank is quite large during stance ($\sim 700\text{N}$) but is near zero during swing.

Therefore, we add a small amount of compliance to the shank and use this to activate an engagement mechanism for the springs. In the absence of a large shank force, the springs remain disengaged.

A scale prototype of this design is shown in Fig. 16-a. In this design, a pneumatic heel pad is used to push a pair of pins into and out of contact with the spring engagement tab. This mechanism was validated on a scaled down dynamometer (1.4 percent torque, 50 percent speed). The results from this scaled test are shown in Fig. 17. The slow speed of the test allowed a subject to disengage the spring remotely by removing pressure from the pneumatic pad. Therefore in this test, the entire cycle (stance and swing) was performed at one time.

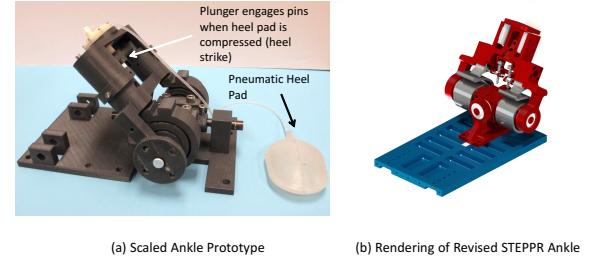


Fig. 16. A photograph (a) and rendering (b) of proposed ankle engagement designs.

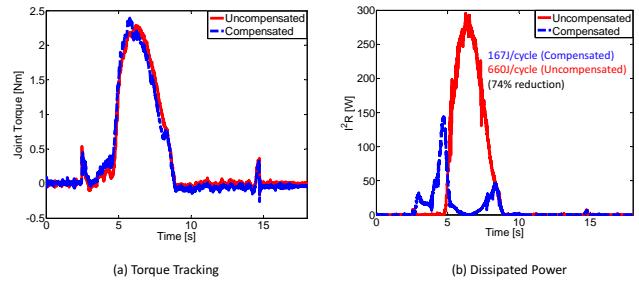


Fig. 17. Experimental data from the scaled down ankle prototype.

These promising results were used to design a new ankle for STEPPR. This is intended as a drop in replacement for the existing ankle. A rendering of this design is shown in Fig. 16-b. Similar to the hip spring design, the spring zero position can be adjusted by swapping out engagement pawls.

XII. CONCLUSIONS

In this paper we have introduced a new bipedal robot designed for disaster response and with the specific goal of improving cost of transport. This robot, titled STEPPR, uses powerful DC motors and efficient rope transmissions to achieve smooth, quiet, and highly backdriveable motions. We use three gait types to illustrate how parallel elastic elements can further improve the efficiency of the design. Specifically, a hip roll spring and an ankle pitch spring provide considerable benefits across the three very different gait types. Full scale springs to handle the large torques and stiffness were designed and validated experimentally. Finally, mechanisms were presented which allow these springs to be seamlessly

incorporated into the existing STEPPR design. As we achieve walking with STEPPR, we envision these designs providing significant improvements in walking performance.

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