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Ultra-sensitive Magnetic Microscopy with an Atomic Magnetometer

Young Jin Kim

Los Alamos National Laboratory

Aug. 19, 2015
Postdoc Summer Seminar

Research goals

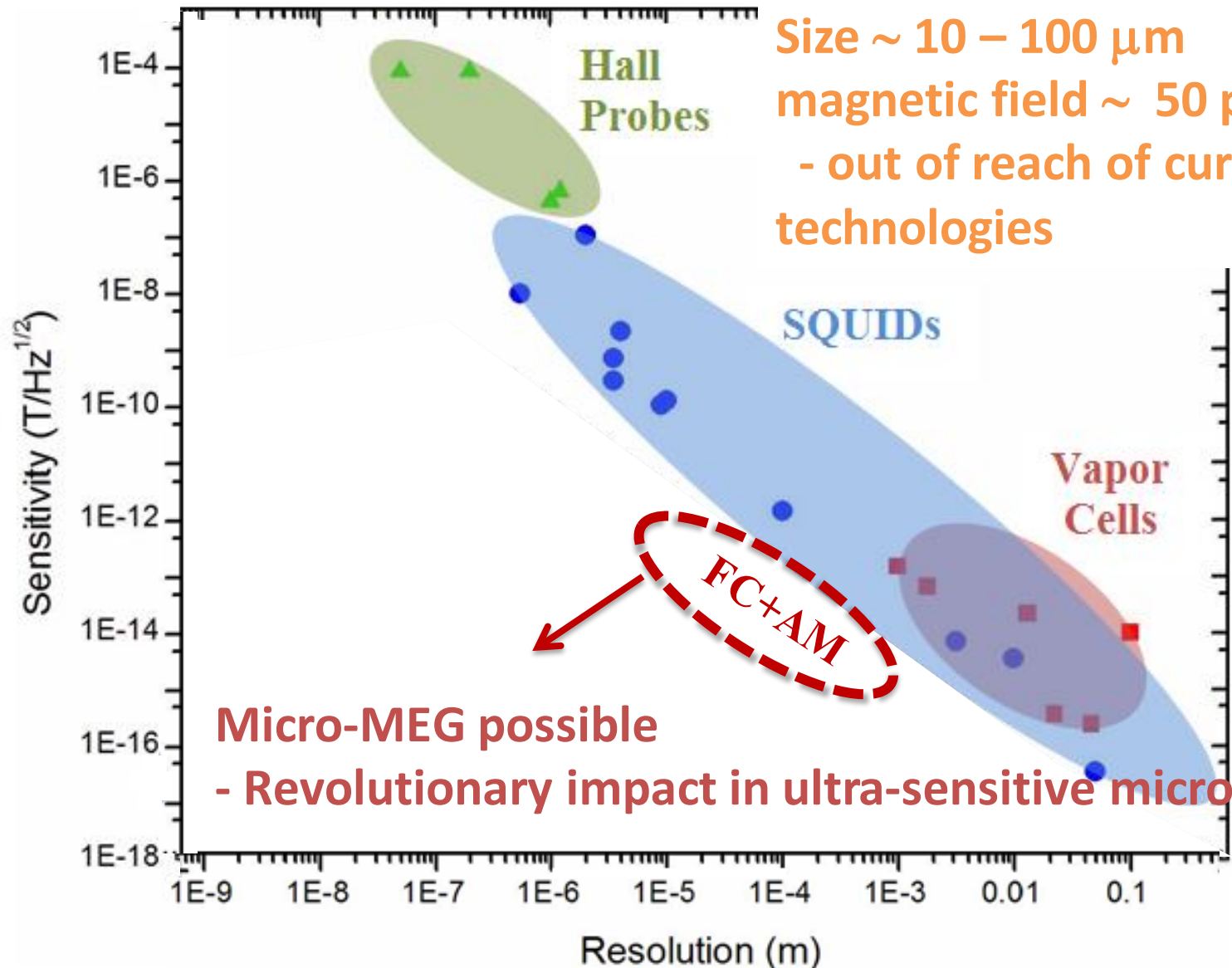
- Many applications in neuroscience and other fields require a high-resolution, high-sensitivity magnetic microscope.
- **Magnetoencephalography (MEG):** a diagnostic technique for studying the brain through measurements of magnetic fields produced by neural currents.



- **Current MEG can only measure averages over large numbers of neurons (10^4 to 10^5)**
- **High-resolution magnetometry, capable of detecting a few neurons;**
 - **Full understanding of brain function**
 - **Direct imaging of the structure and composition of proteins and molecules**

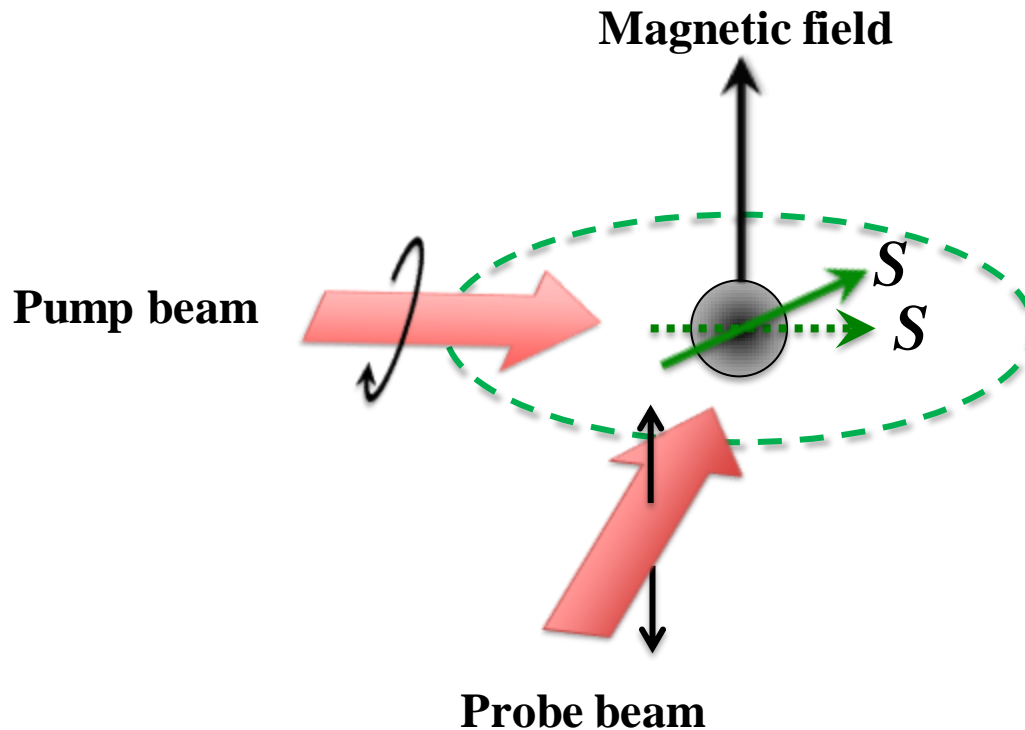
Research goals

Single neuron :
Size $\sim 10 - 100 \mu\text{m}$
magnetic field $\sim 50 \text{ pT}$
- out of reach of current technologies



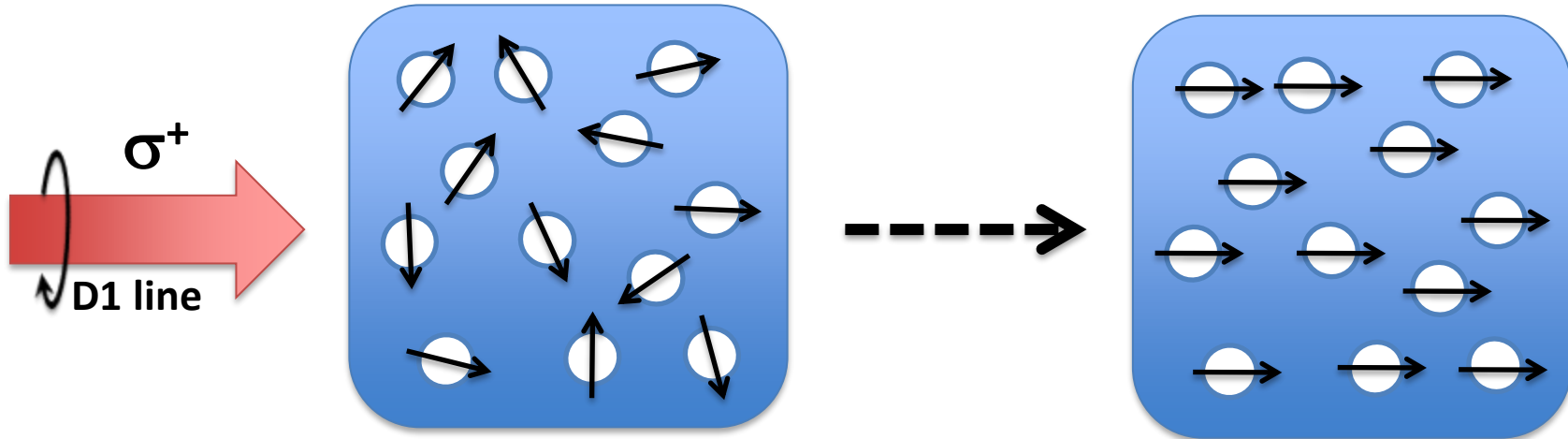
Atomic Magnetometer

- **Atomic magnetometer:**
 - based on lasers and alkali-metal (Cs, Rb, K) vapor cells
 - the most sensitive non-cryogenic magnetic-field sensor.
- **Alkali-metal:** a single unpaired electron in the outer energy shell that can be easily manipulated.



Principle of atomic magnetometer

1. Optical pumping



$n \sim 10^{13} / \text{cm}^3$ at 150°C

Comparison to thermal polarization (P_T) :

$$P_T = \tanh\left(\frac{0.5 g_s \mu_B B}{k_B T}\right)$$

$g_s \approx 2$: Dirac g – factor, μ_B = Bohr magneton
 k_B = Boltzmann constant

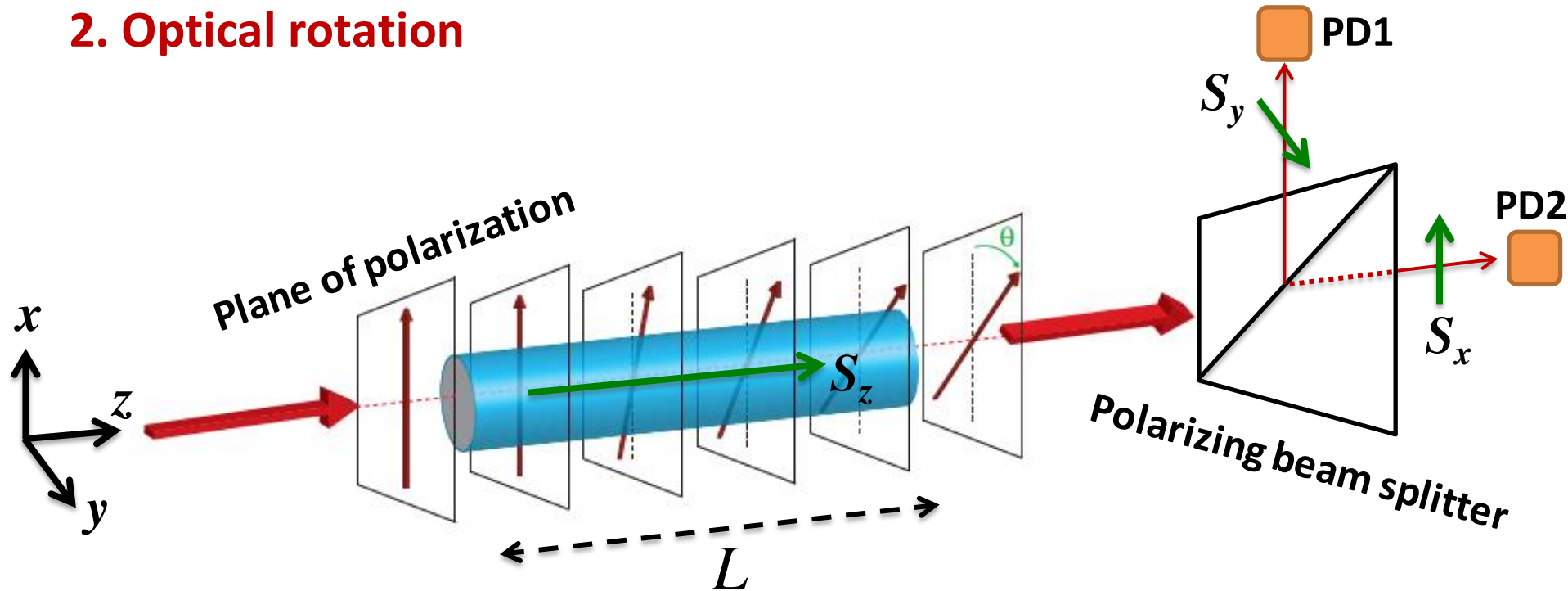
$$P_T = 10^{-7} \text{ with } 0.5 \text{ G}, P_T = 0.02 \text{ with } 10 \text{ T}$$

$P \approx 1$ by optical pumping

(1 W $\rightarrow 10^{18}$ photons/cc, 1 mW is enough for pumping

Principle of atomic magnetometer

2. Optical rotation



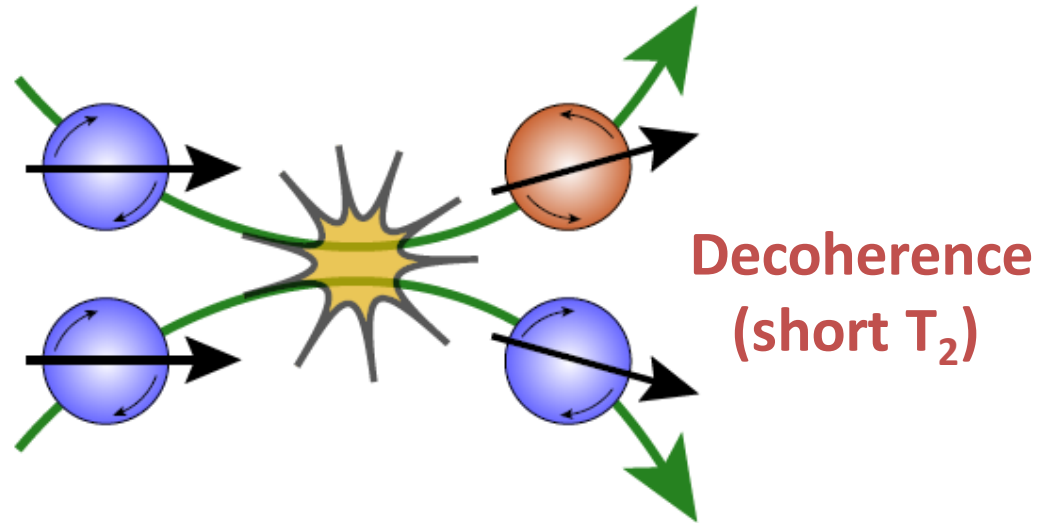
$$\theta \sim L n S_z$$

Optical rotation angle is proportional to the polarization component along the direction of probe beam propagation.

Probe signal at PD : $I_1 = I_0 \sin^2 \theta, I_2 = I_0 \cos^2 \theta$

SERF magnetometer

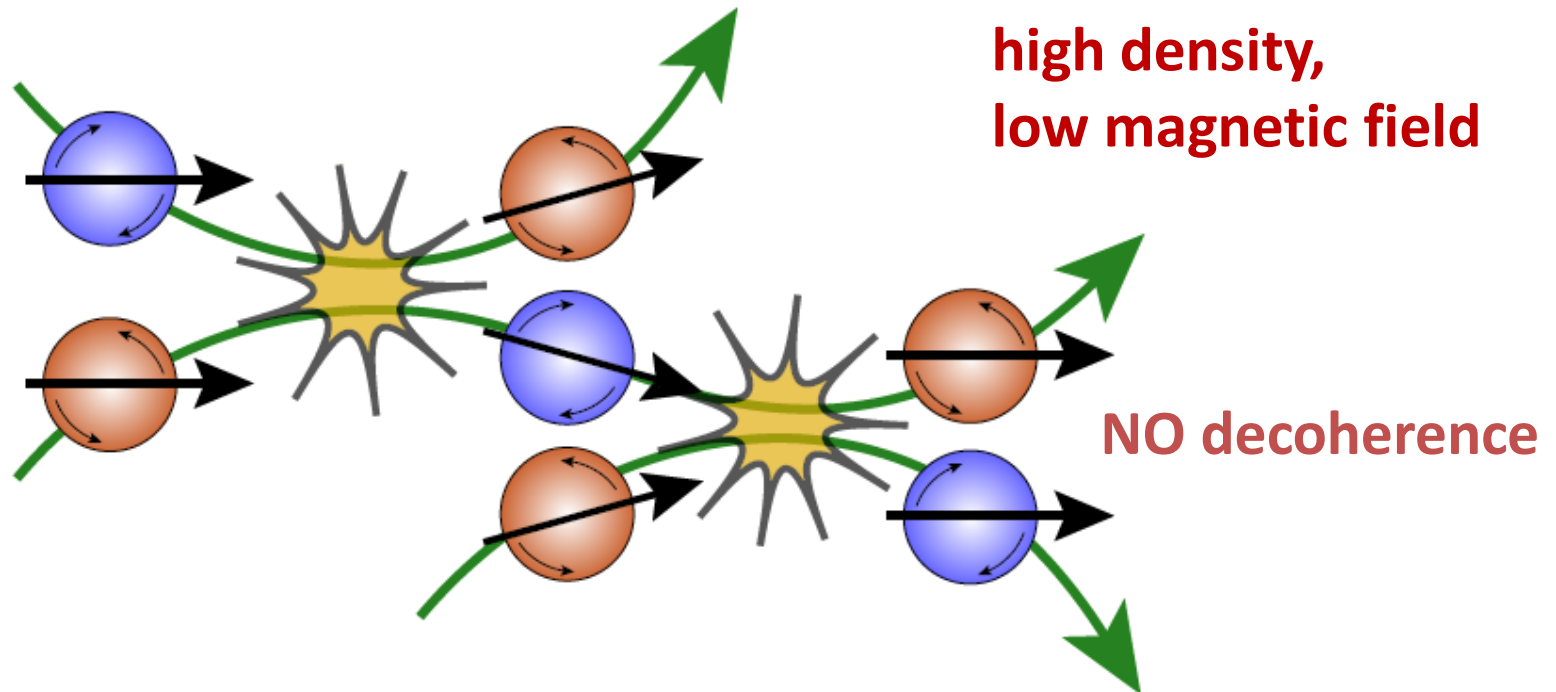
Fundamental Limitation of AM: Spin-exchange collisions.



Breakthrough: Spin-Exchange Relaxation-Free (SERF) magnetometer

- In the regime of high density (strong spin-exchange, strong signal) and low magnetic field, spin-exchange collisions do not depolarize the spins.
- Only SERF magnetometer can achieve subfemtotesla sensitivity in low frequency

SERF magnetometer



Spin-exchange collision rate \gg precession frequency

SERF magnetometer eliminates spin-exchange relaxation !

First demonstrations of the SERF magnetometer (PRL V. 89, p.130801, 2002):

1. Pump and probe beams were orthogonal (most optimal configuration)
2. Sensitivity $\sim 10 \text{ fT/Hz}^{1/2}$
3. Less convenient for miniaturization and cost reduction

SERF Magnetometer Response

Bloch equation describes the response of the SERF magnetometer to magnetic fields:

$$\frac{d\vec{S}}{dt} = \gamma \vec{S} \times \vec{B} + R(S_0 \hat{z} - \vec{S}) - \frac{\vec{S}}{T_2}$$

S : electron spin polarization vector,

R: optical pumping rate

S₀: equilibrium electron spin polarization

$$\gamma = 2\pi \times 7 \text{ GHz/T}$$

Steady state solution, dS/dt = 0 :

$$S_x = S_0 \frac{-\beta_y + \beta_x \beta_z}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)}, \quad S_y = S_0 \frac{\beta_x + \beta_y \beta_z}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)},$$

$$S_z = S_0 \frac{1 + \beta_z^2}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)},$$

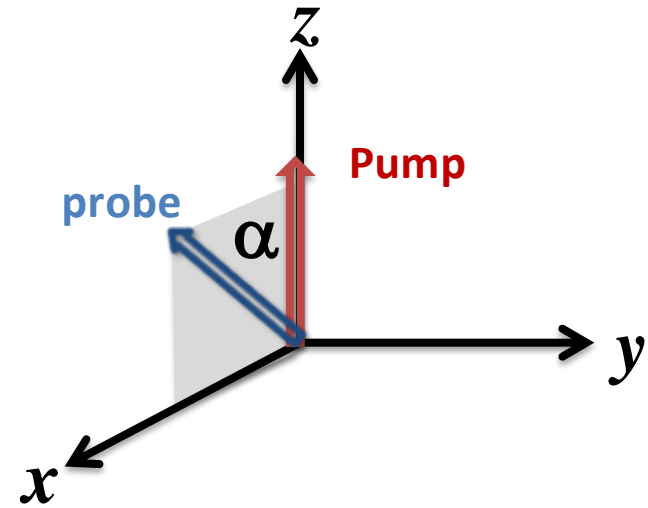
$$\vec{\beta} = \frac{\gamma \vec{B}}{R + T_2^{-1}}$$

**dimensionless magnetic
field components**

SERF Magnetometer Response

Magnetometer signal proportional to the component of the electron spin in the probe propagation direction:

$$S_{probe} = S_x \sin \alpha + S_z \cos \alpha$$
$$= S_0 \left[\frac{(-\beta_y + \beta_x \beta_z) \sin \alpha + (1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right]$$



First case: α is not small

$$S_{probe} \approx S_0 \left[\frac{(-\beta_y + \beta_x \beta_z) \sin \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right]$$

Maximum value when α is $\pi/2$

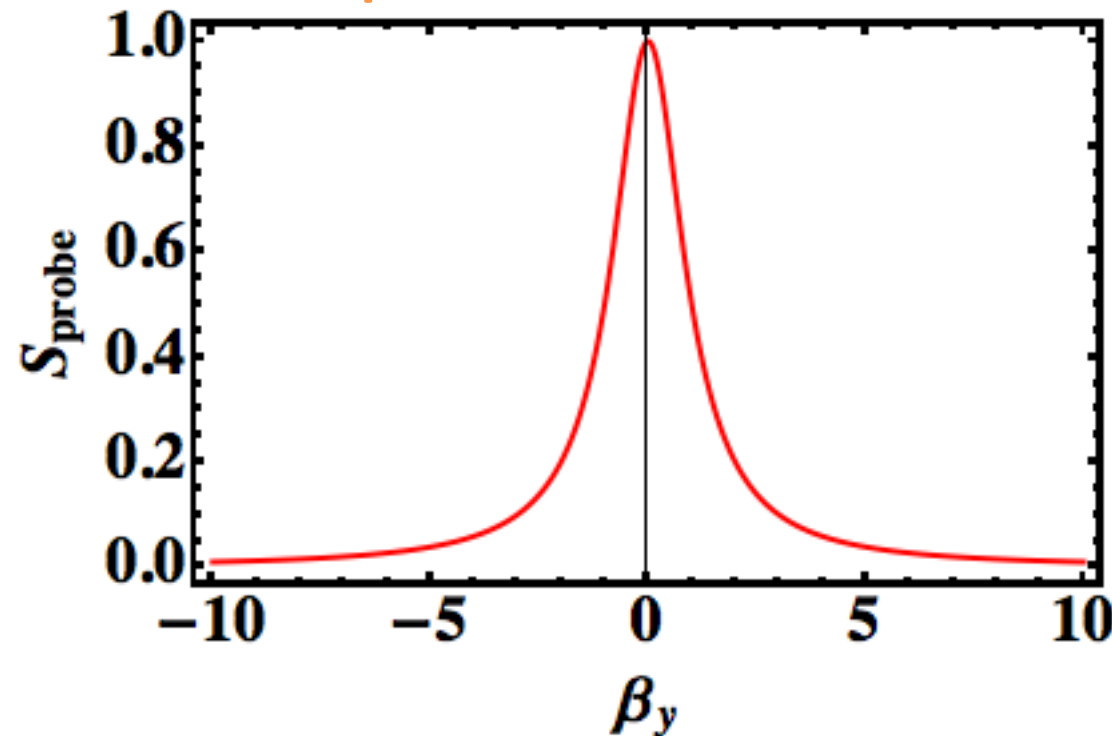
This case is the traditional perpendicular probe-pump orientation, but we are interested in almost parallel beam probe-pump orientation

SERF Magnetometer Response

Second case: α is very small (nearly parallel beams configuration)

$$S_{probe} \approx S_0 \left[\frac{(1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right] \approx S_0 \left[\frac{1}{1 + (\beta_x^2 + \beta_y^2)/(1 + \beta_z^2)} \right]$$

Example:



For maximum response to a oscillating field:

$$\frac{\partial S_{probe}}{\partial \beta_y} = \max$$

SERF Magnetometer Response

Second case: α is very small

$$S_{probe} \approx S_0 \left[\frac{(1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right] \approx S_0 \left[\frac{1}{1 + (\beta_x^2 + \beta_y^2)/(1 + \beta_z^2)} \right]$$

- Maximum response to a oscillating field in y direction:

$$\frac{\partial S_{probe}}{\partial \beta_y} = 0.65 S_0 \quad \text{at } \beta_x = \beta_z = 0, \beta_y = 1/\sqrt{3}$$

Optimal fields

Decreased by a factor of 1.5 compared to the perpendicular beams

- Maximum response to a oscillating field in z direction:

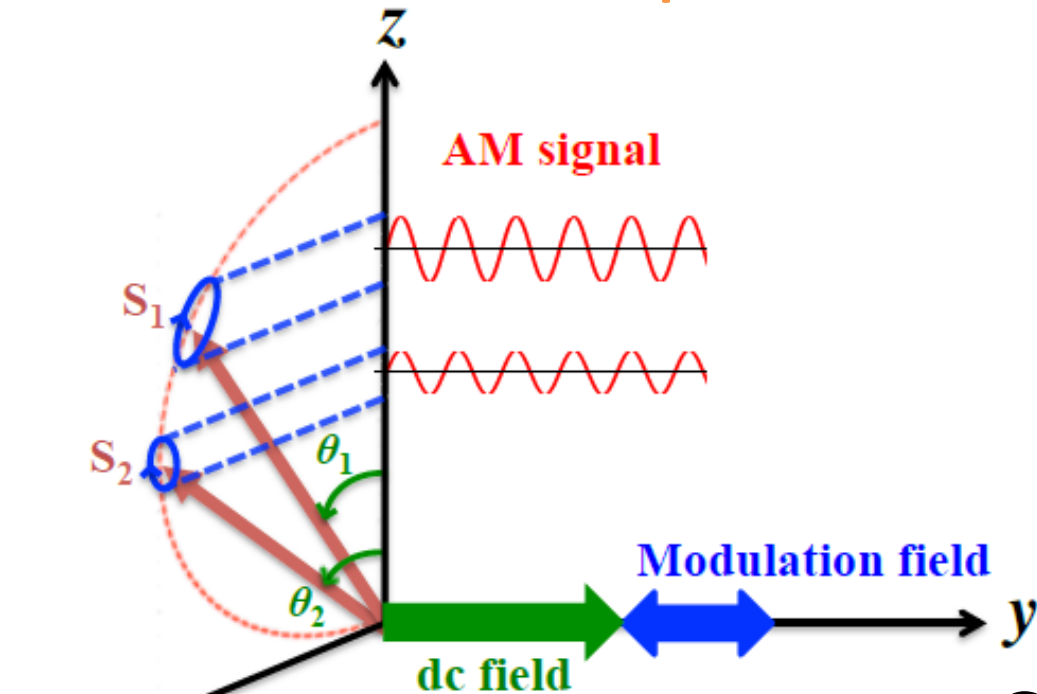
$$\frac{\partial S_{probe}}{\partial \beta_z} = 0.25 S_0 \quad \text{at } \beta_z = 1, \beta_x^2 + \beta_y^2 = 2$$

Optimal fields

Decreased by a factor of 2 compared to the perpendicular beams

SERF Magnetometer Response

Visualization of the optimization to the y component:



$$\theta = \tan^{-1}(S_x / S_z) = \tan^{-1} \beta_y^{dc}$$

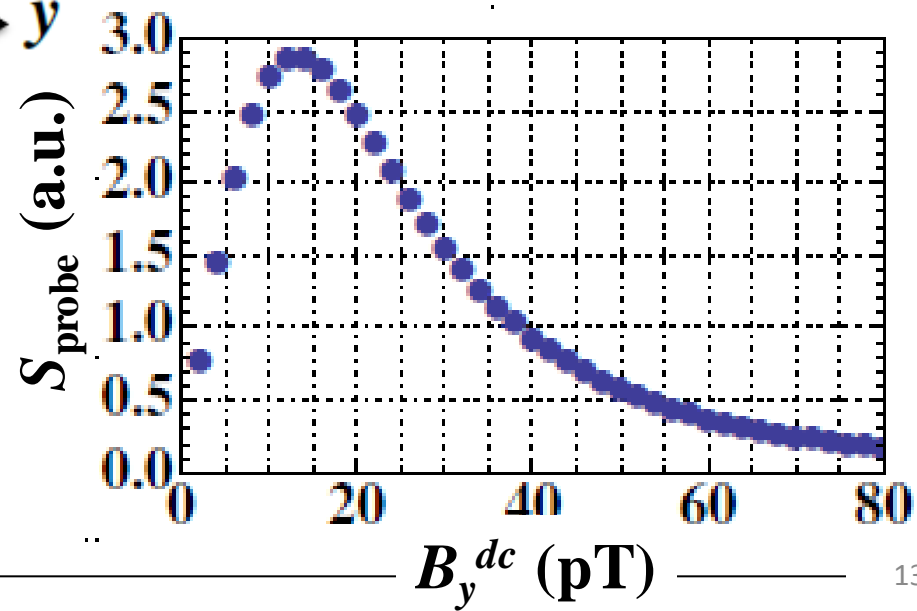
$$\begin{aligned} \text{Magnitude} &= \sqrt{S_x^2 + S_y^2 + S_z^2} \\ &= S_0 / \sqrt{1 + (\tan \theta)^2} \end{aligned}$$

Optimal angle:

$$\theta = \tan^{-1}(1 / \sqrt{3}) = 30^\circ$$

$$\vec{\beta} = \frac{\gamma \vec{B}}{R + T_2^{-1}}, R + T_2^{-1} = 1$$

$$B_y^{dc} = (\beta_y = 1 / \sqrt{3}) / \gamma = 13 \text{ pT}$$



Resolution of SERF magnetometer

The fundamental sensitivity limit is due to shot-noise:

$$\delta B = \frac{1}{\gamma \sqrt{NT_2 V t}}$$

N = the number of active atoms
 V = the cell volume,
 t = the measurement time

Higher sensitivity → lower resolution

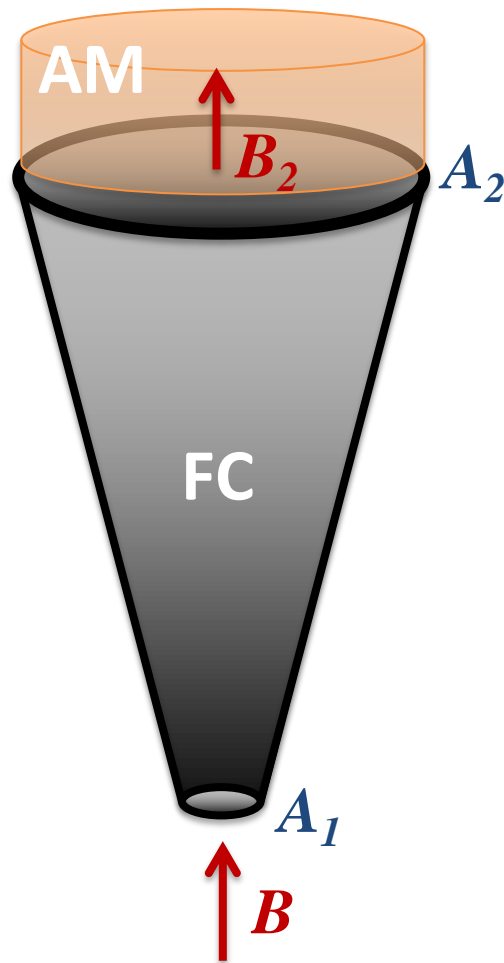
Example: 1 fT/Hz^{1/2} → cm-scale resolution
(Nature V. 422, p.596, 2003)

70 fT/Hz^{1/2} → mm-scale resolution
(Nat. Photonics V. 1, p.649, 2007)

How to reach high resolution, high sensitivity?

- Instead of reducing cell dimensions to micron size, a flux concentrator expands the microscopic magnetic distribution to match the dimensions of AM operating with high sensitivity.

FC + AM system



AM measured B_2 :

$$B_2 = B \frac{A_1}{A_2}$$

Sensitivity of a FC+AM system composed of an AM with 1 fT sensitivity and 5 mm channel and an FC with 100 μm resolution:

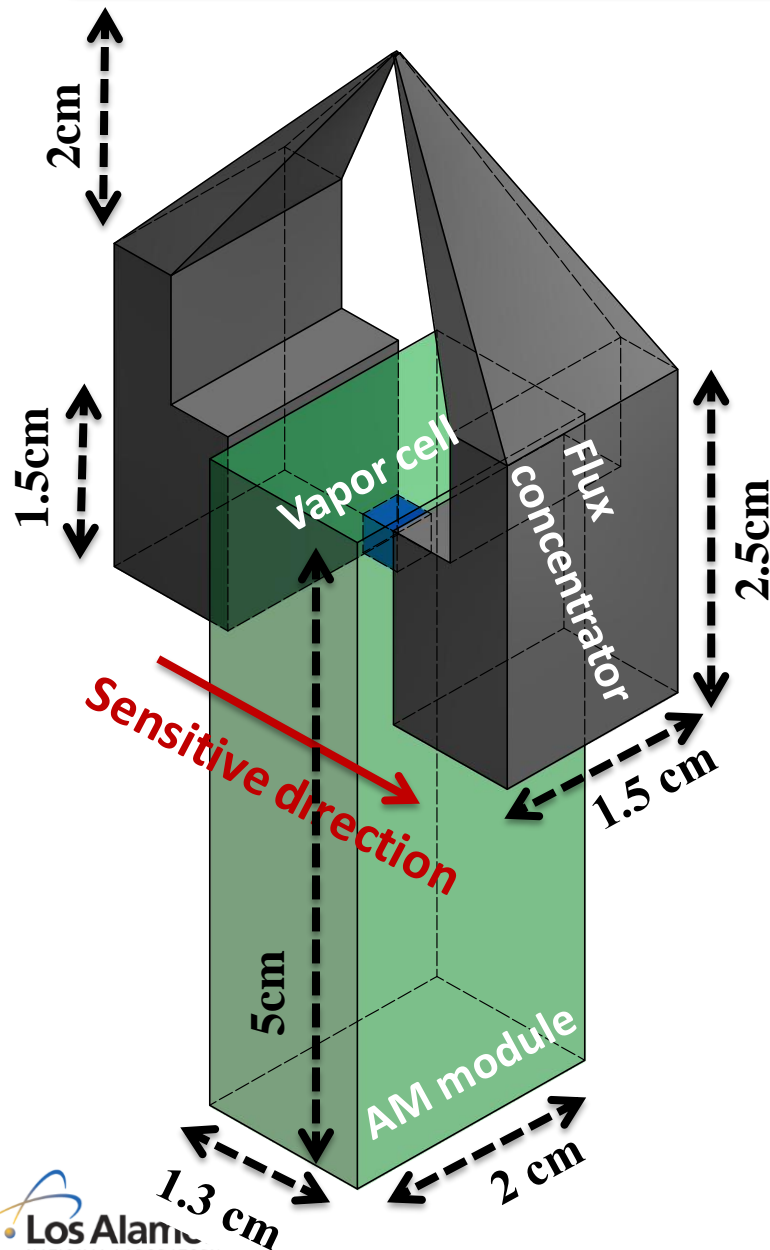
$$B = B_2 \frac{A_2}{A_1} = 1 \text{ fT} \frac{\pi \left(\frac{5 \text{ mm}}{2} \right)^2}{\pi \left(\frac{100 \mu\text{m}}{2} \right)^2} = 2.5 \text{ pT}$$

Magnetic field of interest



Suitable for detecting a single neuron

Design of a single channel FC+AM system



Flux concentrator:

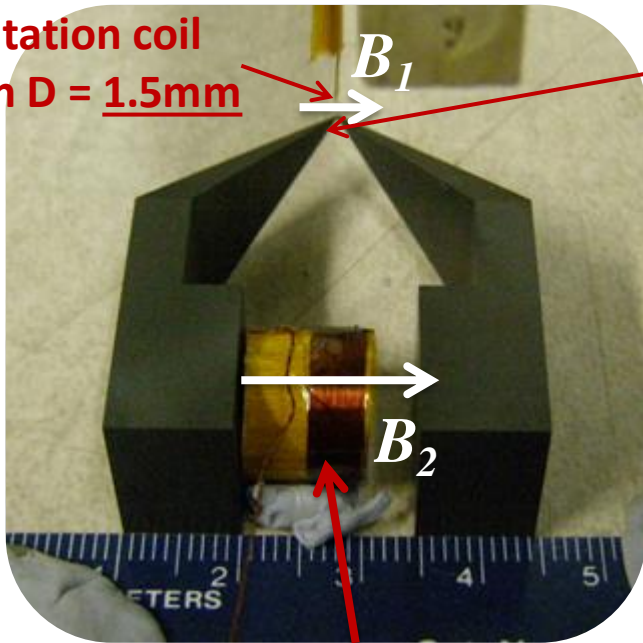
- Constructed from non-conductive MnZn ferrites to avoid large Johnson noise.
- Noise from MnZn ferrite \sim fT level
- $\mu \sim 6500$

Atomic magnetometer:

- Commercial integrated AM
- Vapor cell size: 3mm \times 3mm \times 3mm
- Sensitivity \sim 10 fT level (it can be improved to \sim 1 fT level).

Test of field transfer on FC

Excitation coil
with $D = 1.5\text{mm}$



Gap between ferrite tips = 2 mm

Field at the excitation coil, $B_1 = \frac{\mu_0 I}{D}$

Field at the sensing coil, $B_2 = \frac{V}{NA\omega}$

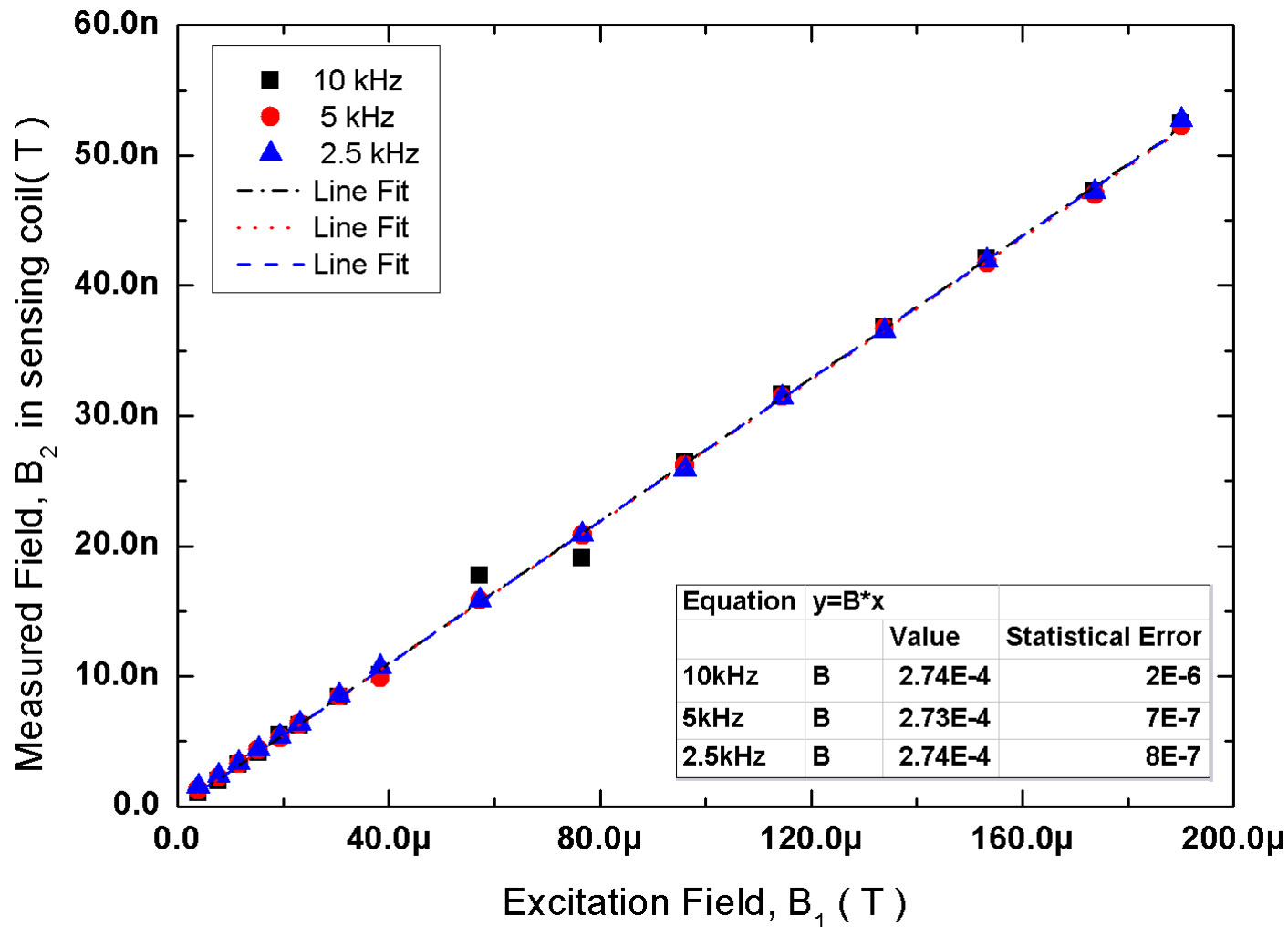
Field transfer coefficient : $k = \frac{B_2}{B_1}$

Sensing coil with $D = 11.6\text{ mm}$, 20 turns

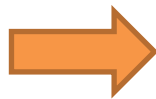
Sensitivity of FC + AM system
 $= (\text{Sensitivity of AM})/k$

Ideal $k = 9.4 \times 10^{-3}$

Test of field transfer on FC

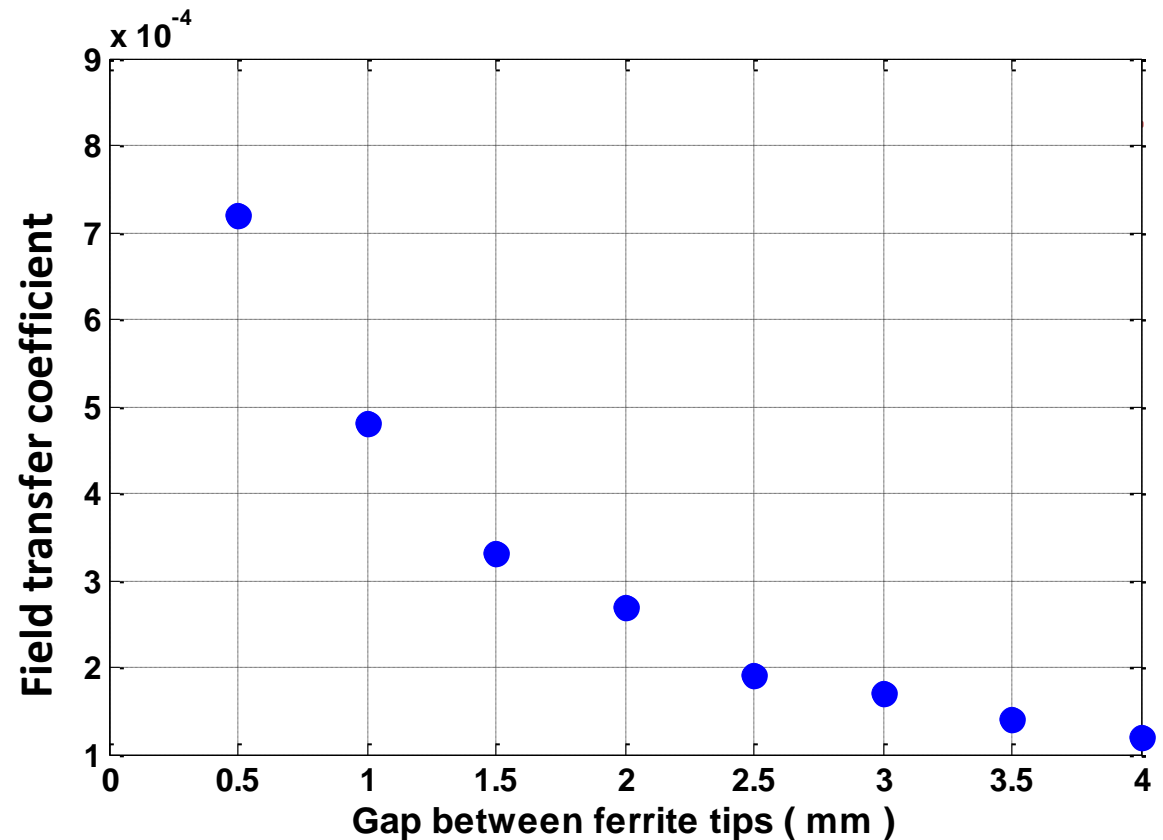
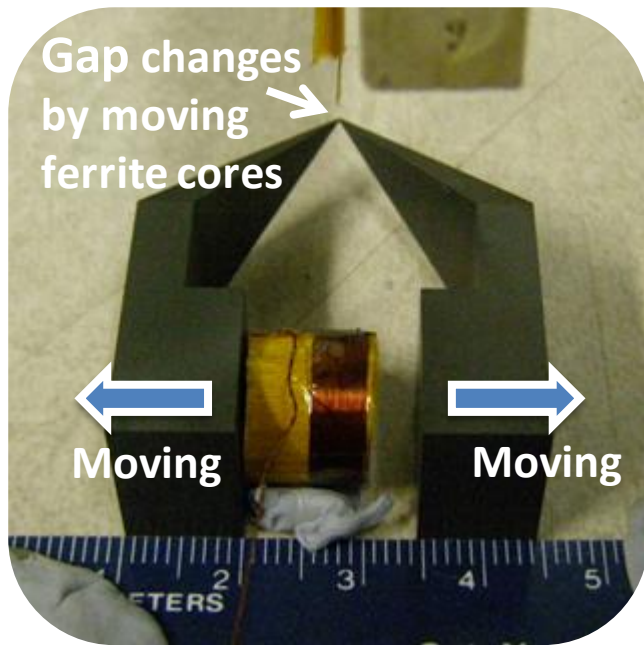


$$k = 2.74 \times 10^{-4}$$



Sensitivity of FC + AM system
 $= 1 \text{ fT}/k = 3.6 \text{ pT}$

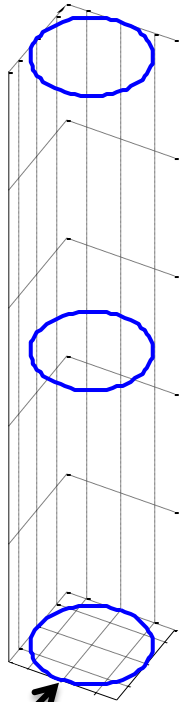
Test of field transfer on FC



Field transfer improves with smaller gap between ferrite tips
- more flux is collected by ferrite

Test of resolution

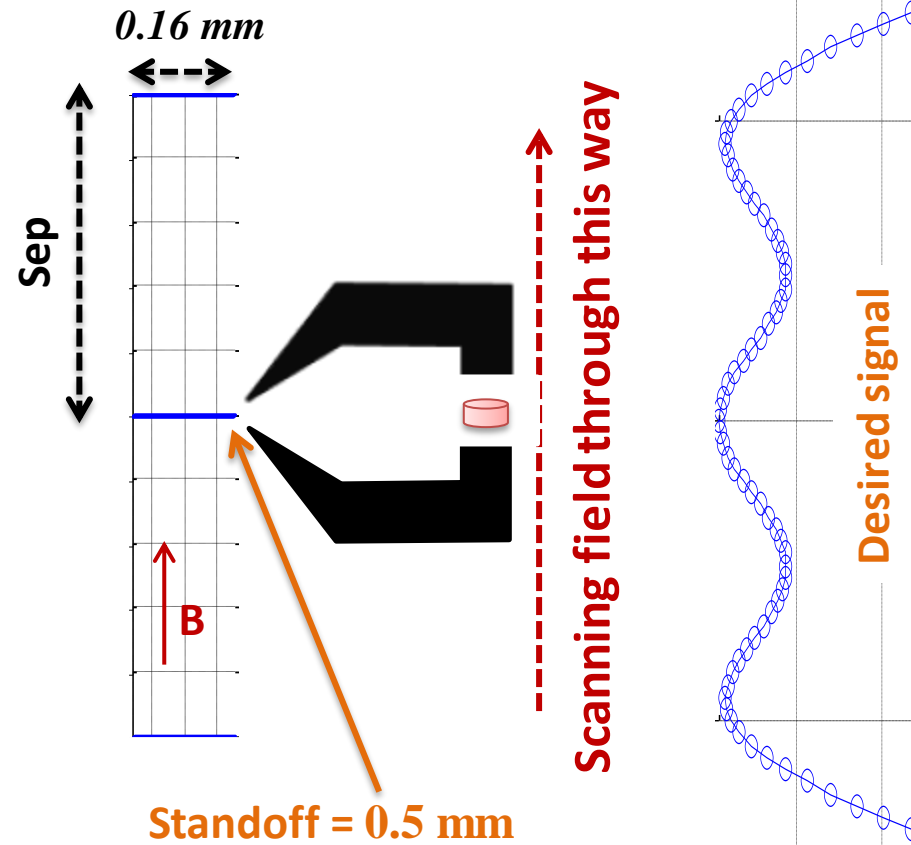
Coil array



40 AWG
($D=0.079\text{mm}$)



Side view

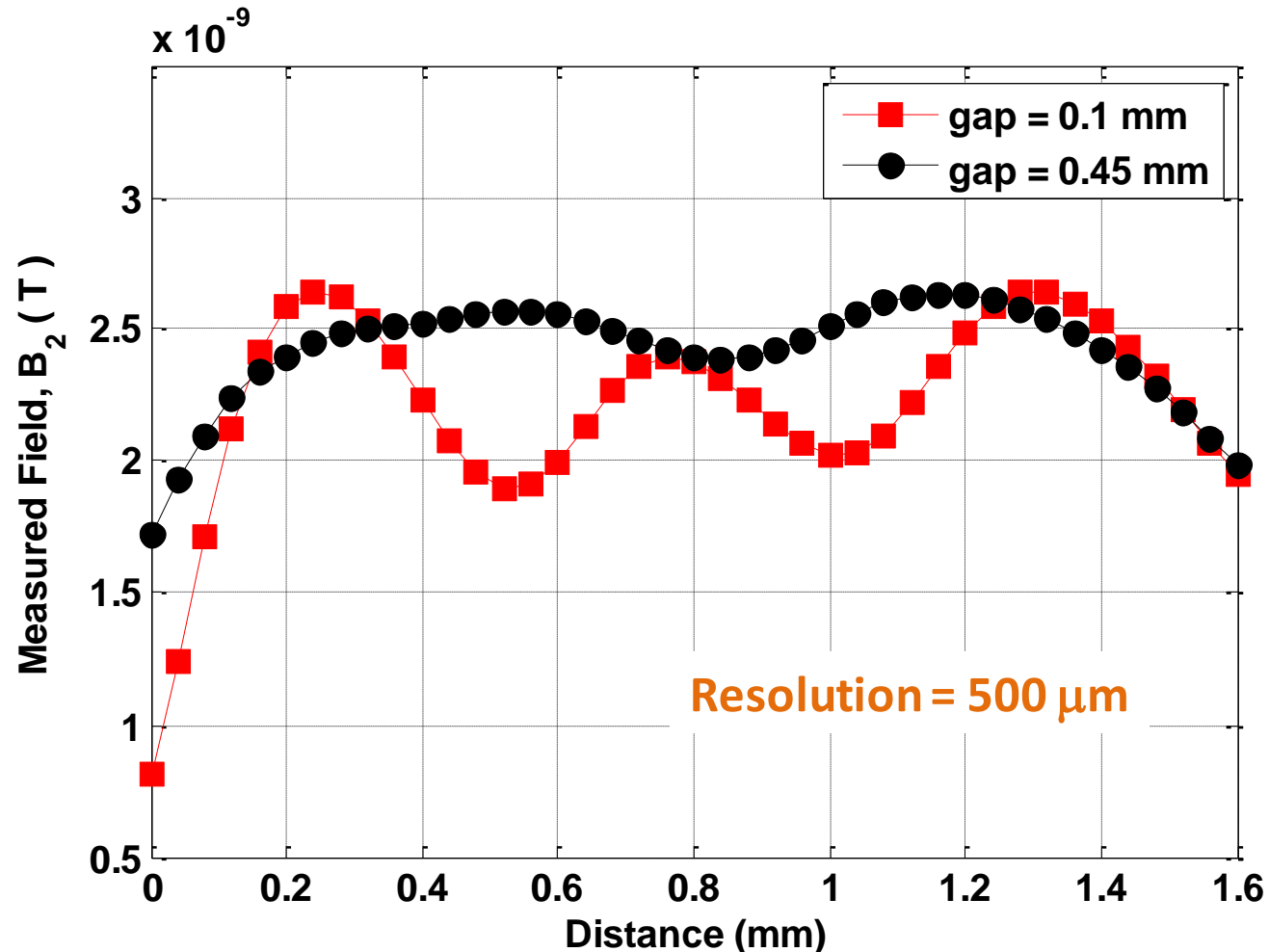


- Change the distance between the coils for resolution tests
- Flux concentrator can see three peaks of the field?

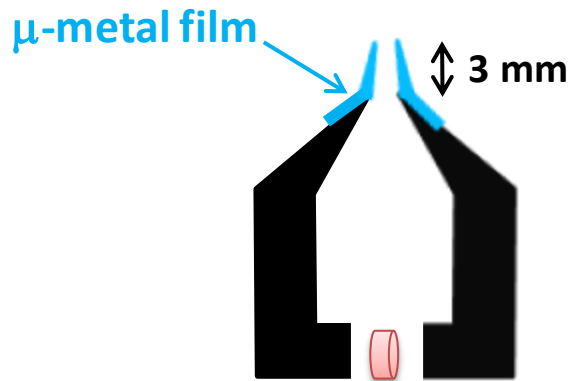


Test of resolution

- Gap between ferrite tips changed
- Measuring three peaks means the resolution of $500\text{ }\mu\text{m}$.

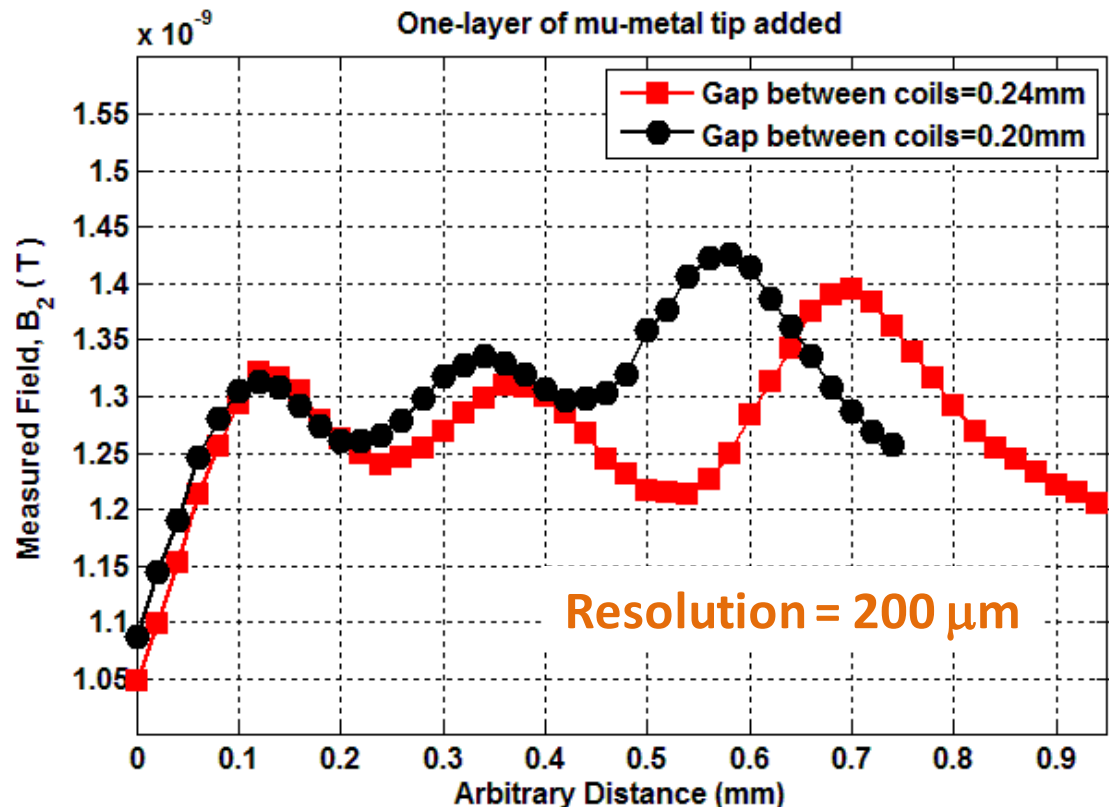


Test of resolution



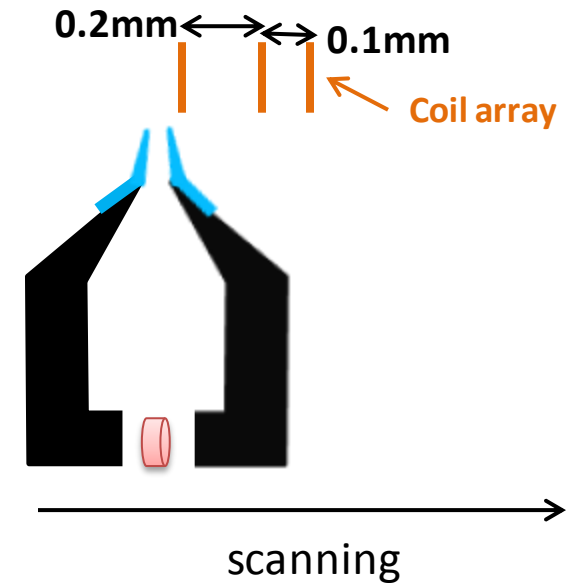
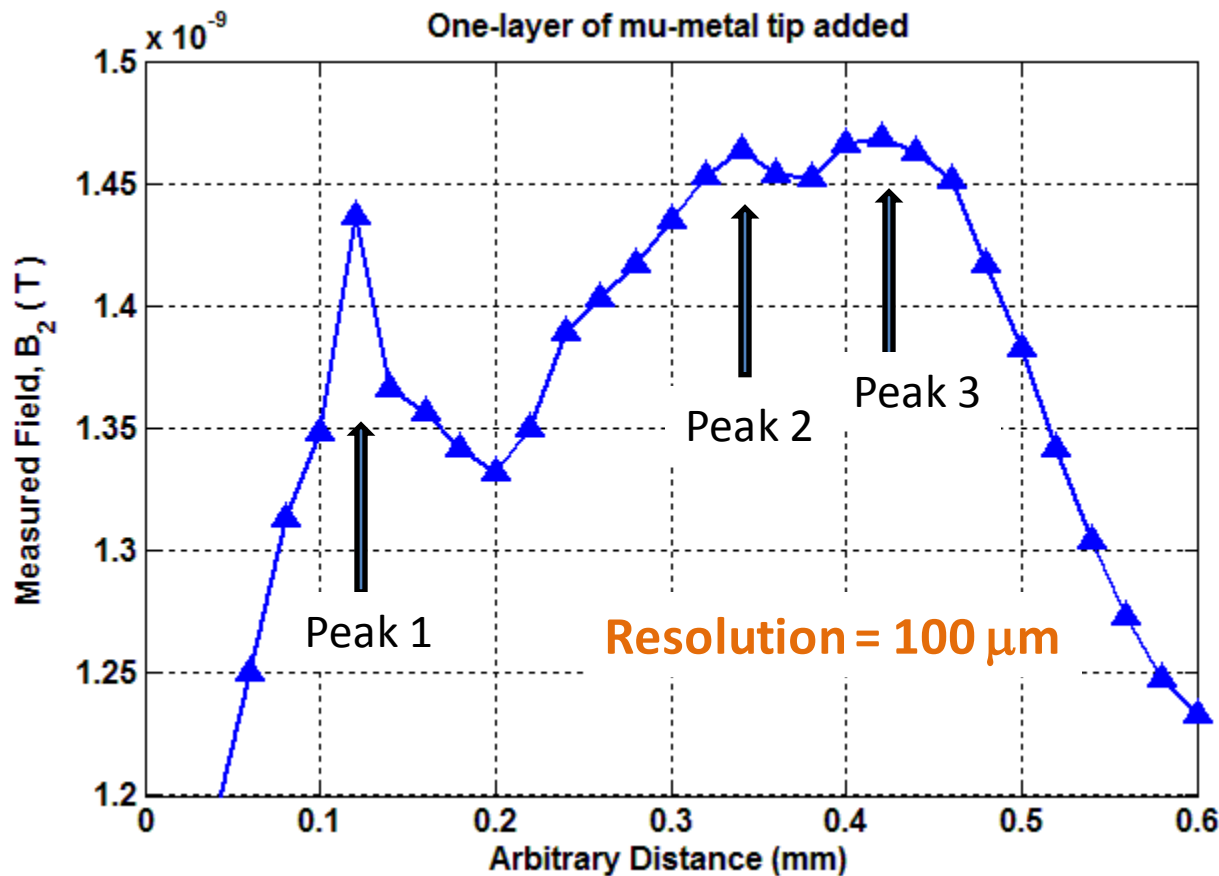
- For higher resolution, a sharp μ -metal film (one layer) is attached on the ferrite tips
- Gap of the ferrite tips ~ 0.1 mm

- The distance between excitation coils is \sim 0.2 mm and 0.3 mm.

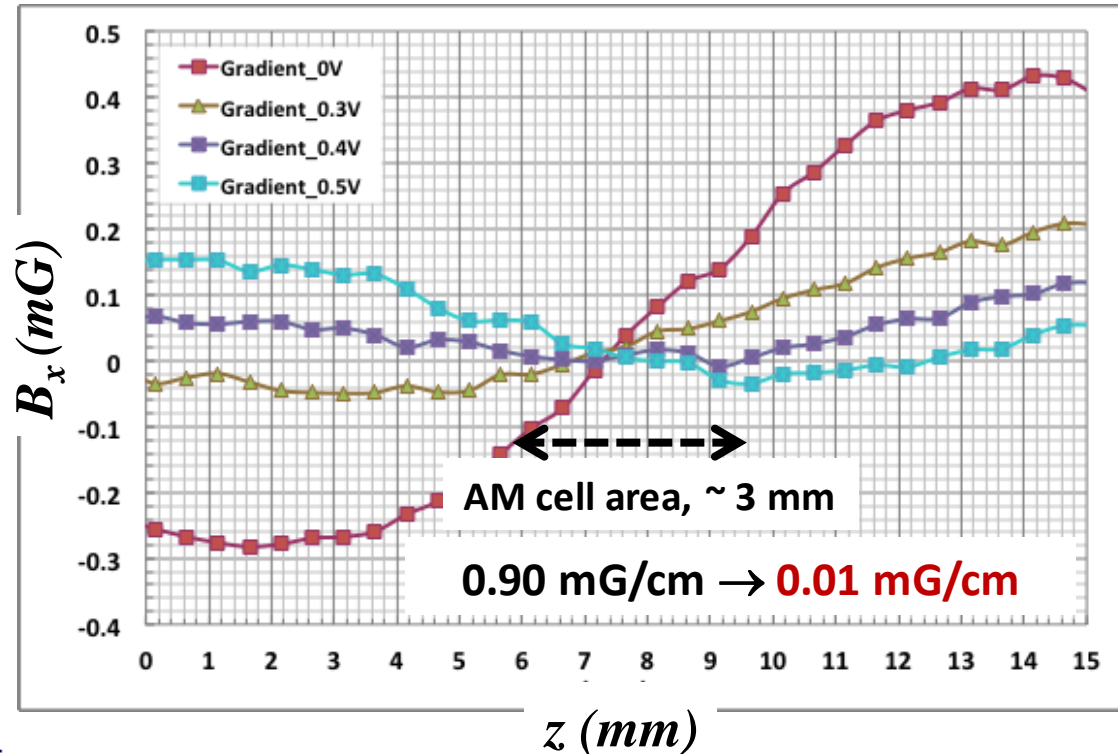
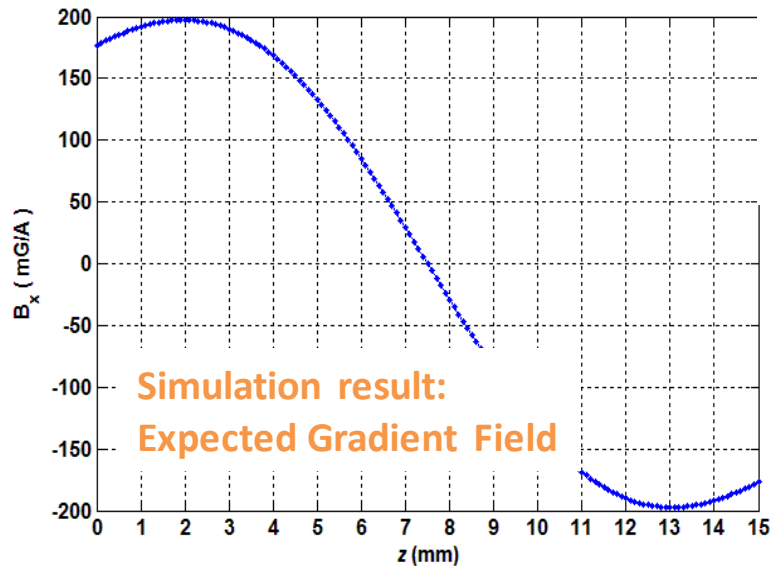
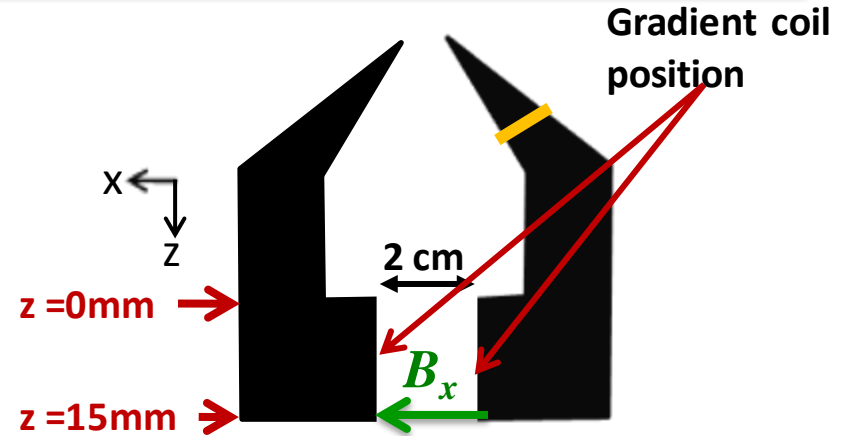
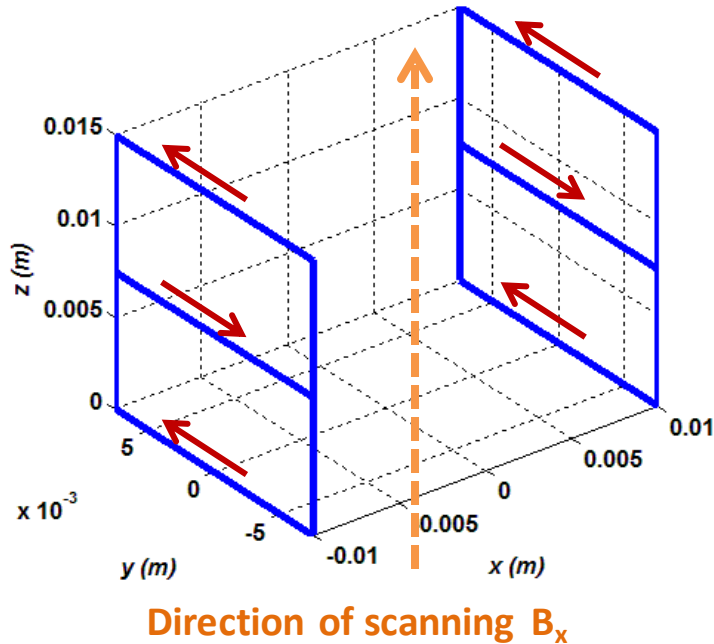


Test of resolution

- The distance between excitation coils is ~ 0.2 mm and ~ 0.1 mm.
- Gap of the mu-metal tips ~ 0.1 mm

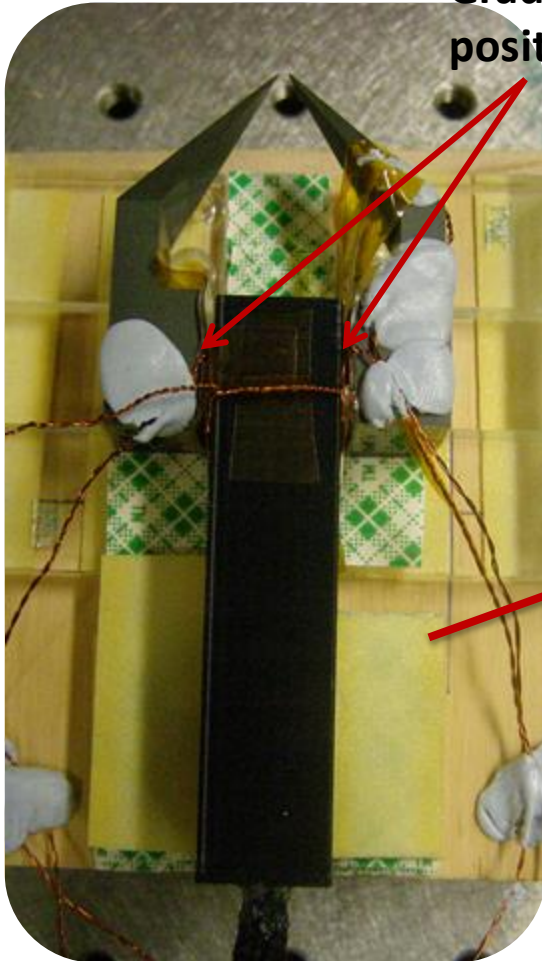


Gradient cancellation

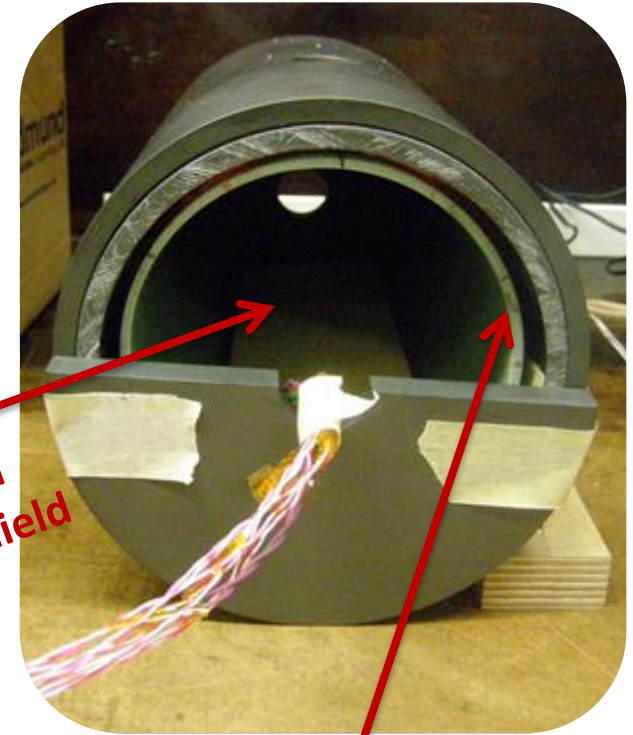


Test of AM performance

Gradient coil
position



One layer of mu-metal shield is not shown



*The assembly placed
inside the ferrite shield*

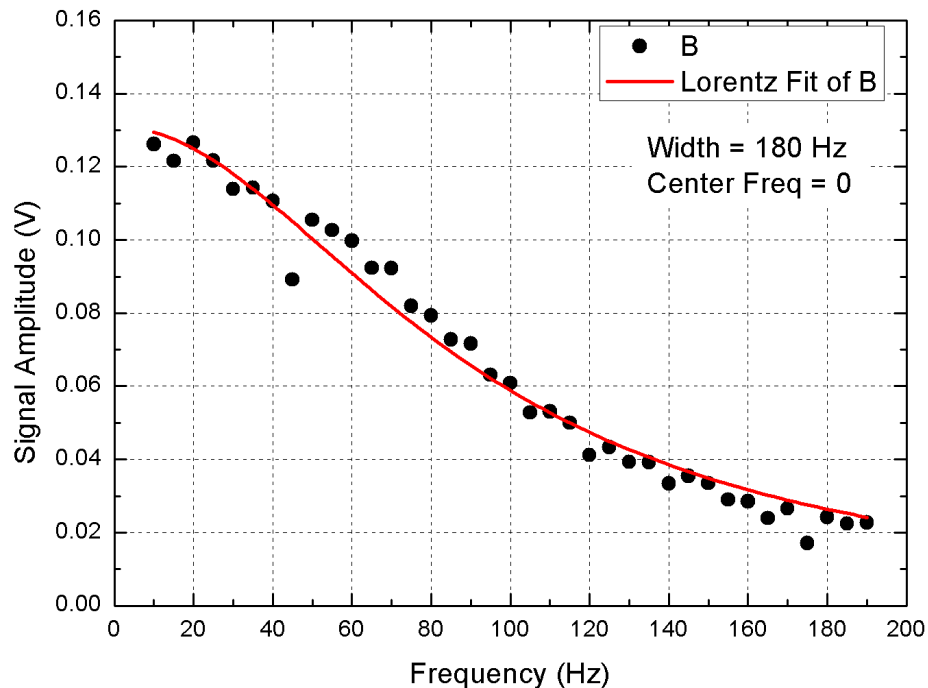
There are 3 axes compensation coil
and 5 gradient compensation coil

FC +AM system

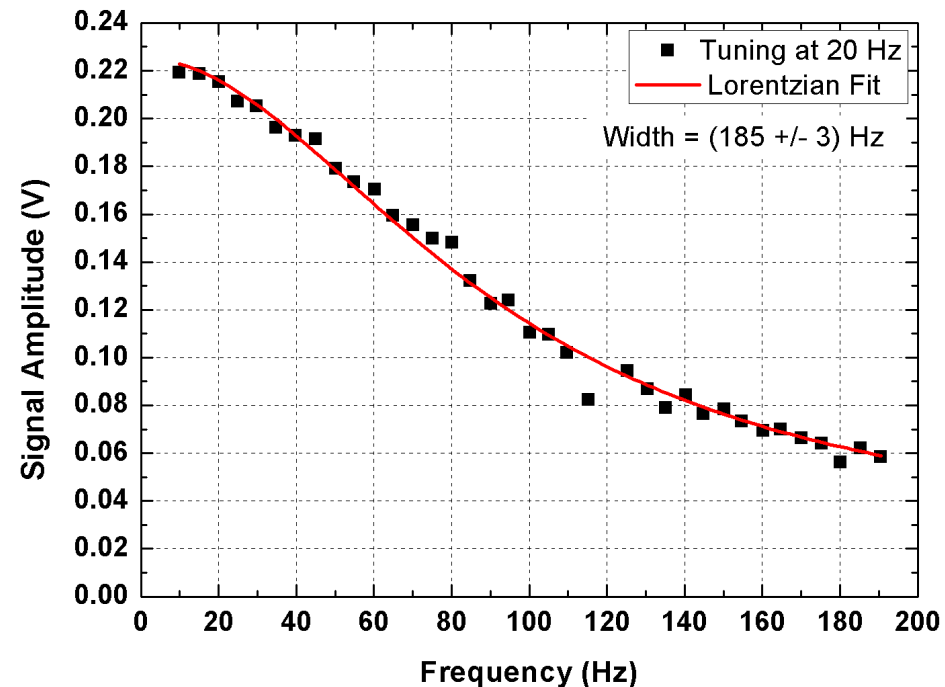
**Note: these coils cannot
compensate the gradient on FC!**

Test of AM performance

Ideal case with shielding

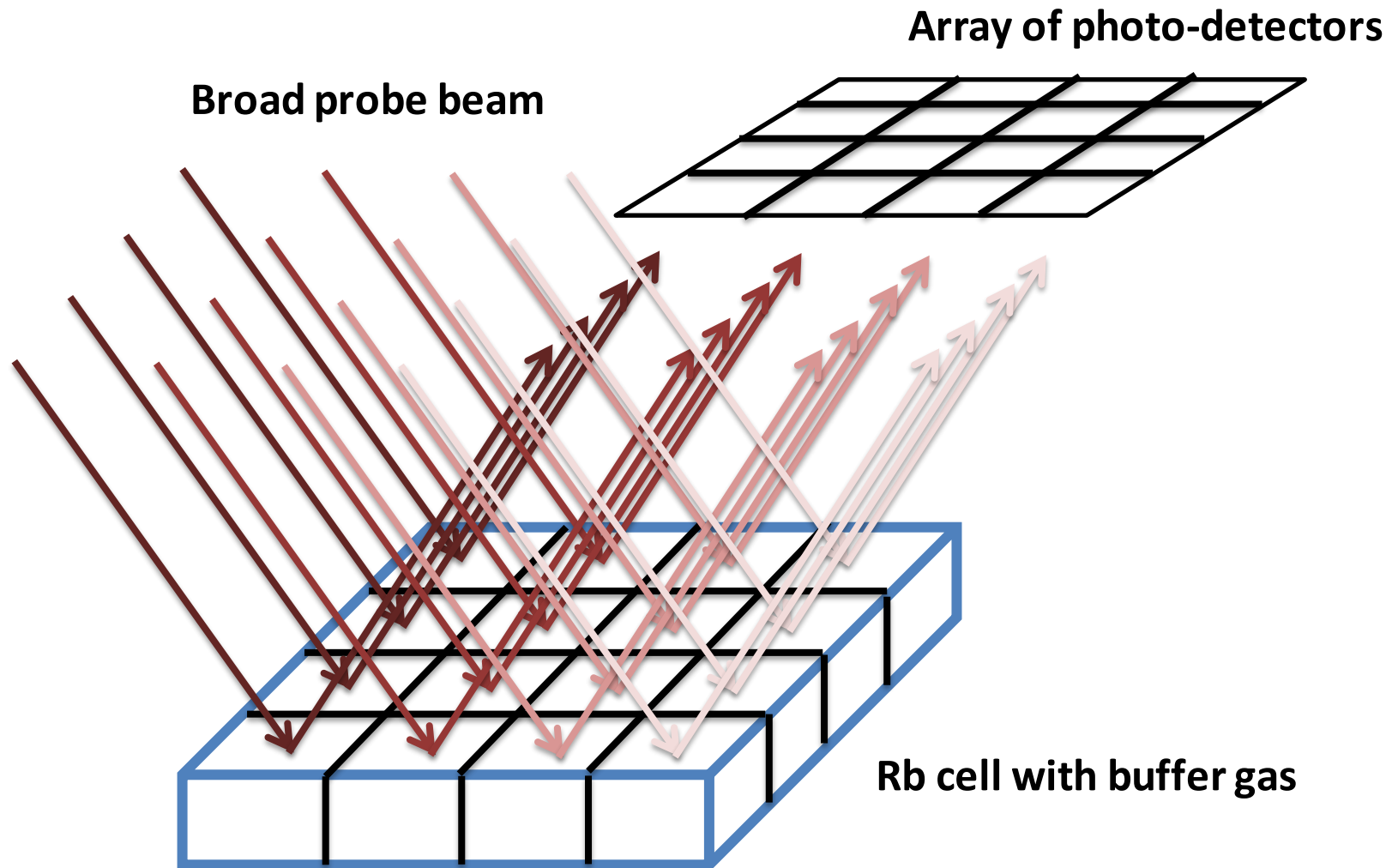


WITH FC in shielding



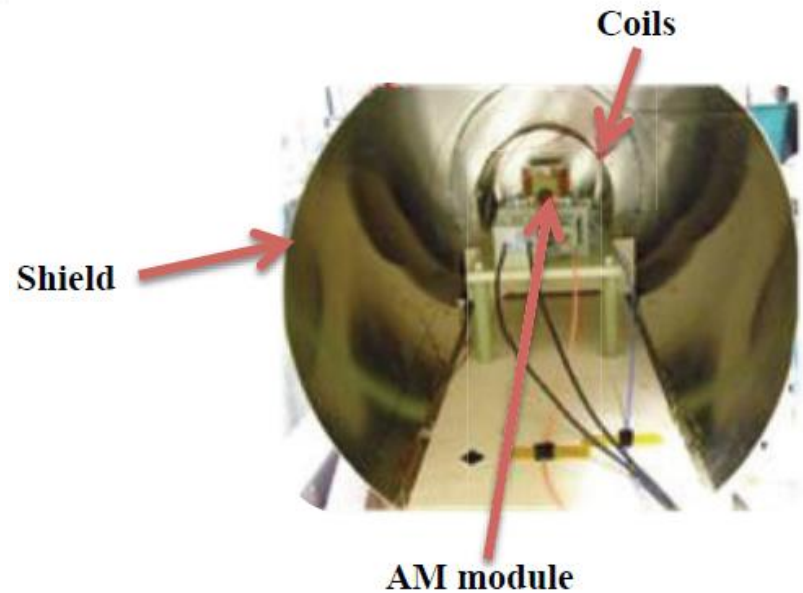
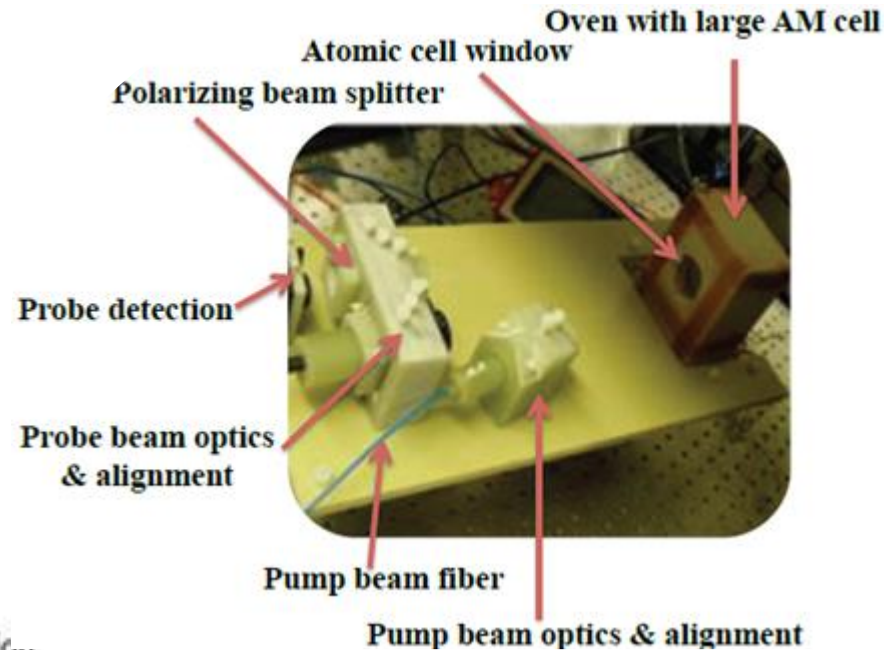
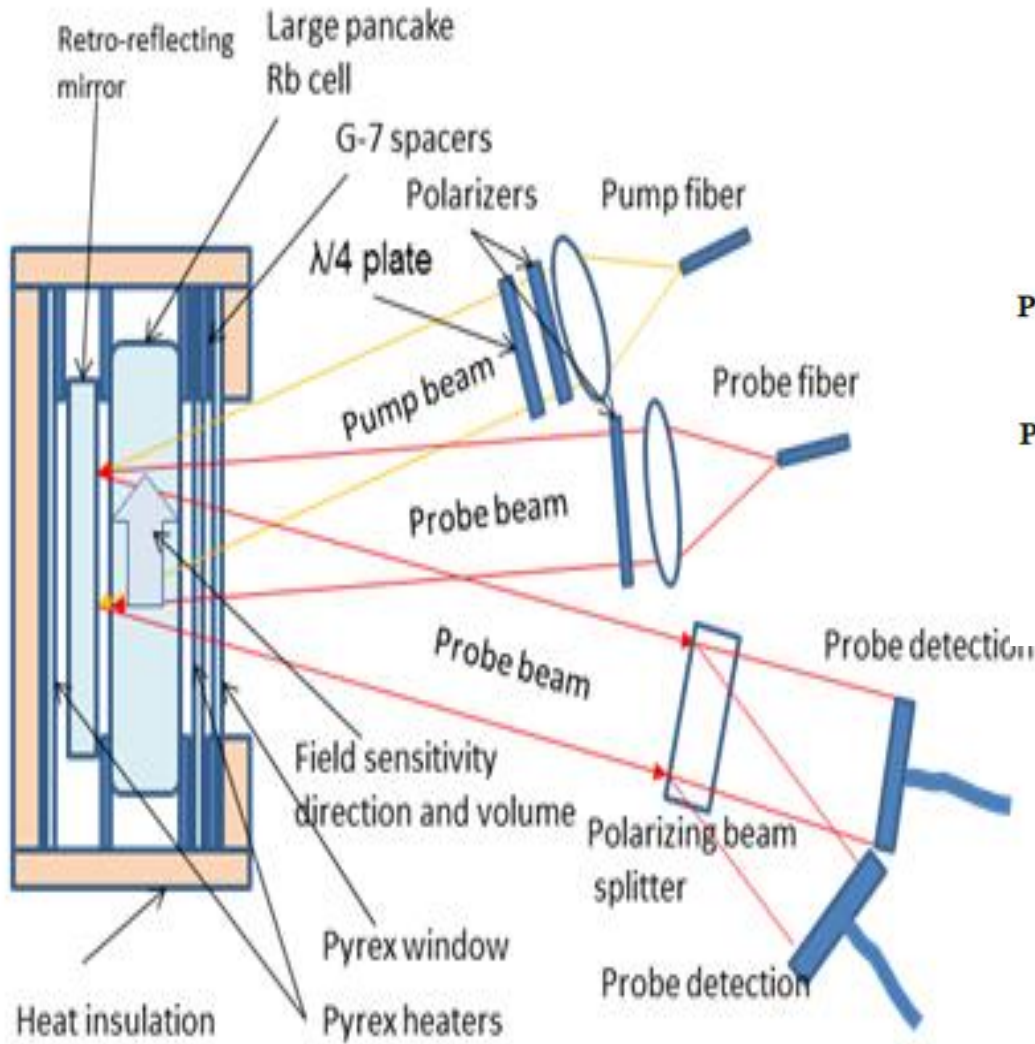
- Flux concentrator doesn't deteriorate AM's performance.
- The gradient compensation coil on the flux concentrator is important to get best AM's performance.

Idea of Multi-channel AM



2D multi-channel is possible with Large Rb cell with a buffer gas and broad beams instead of 16 individual cells and beams.

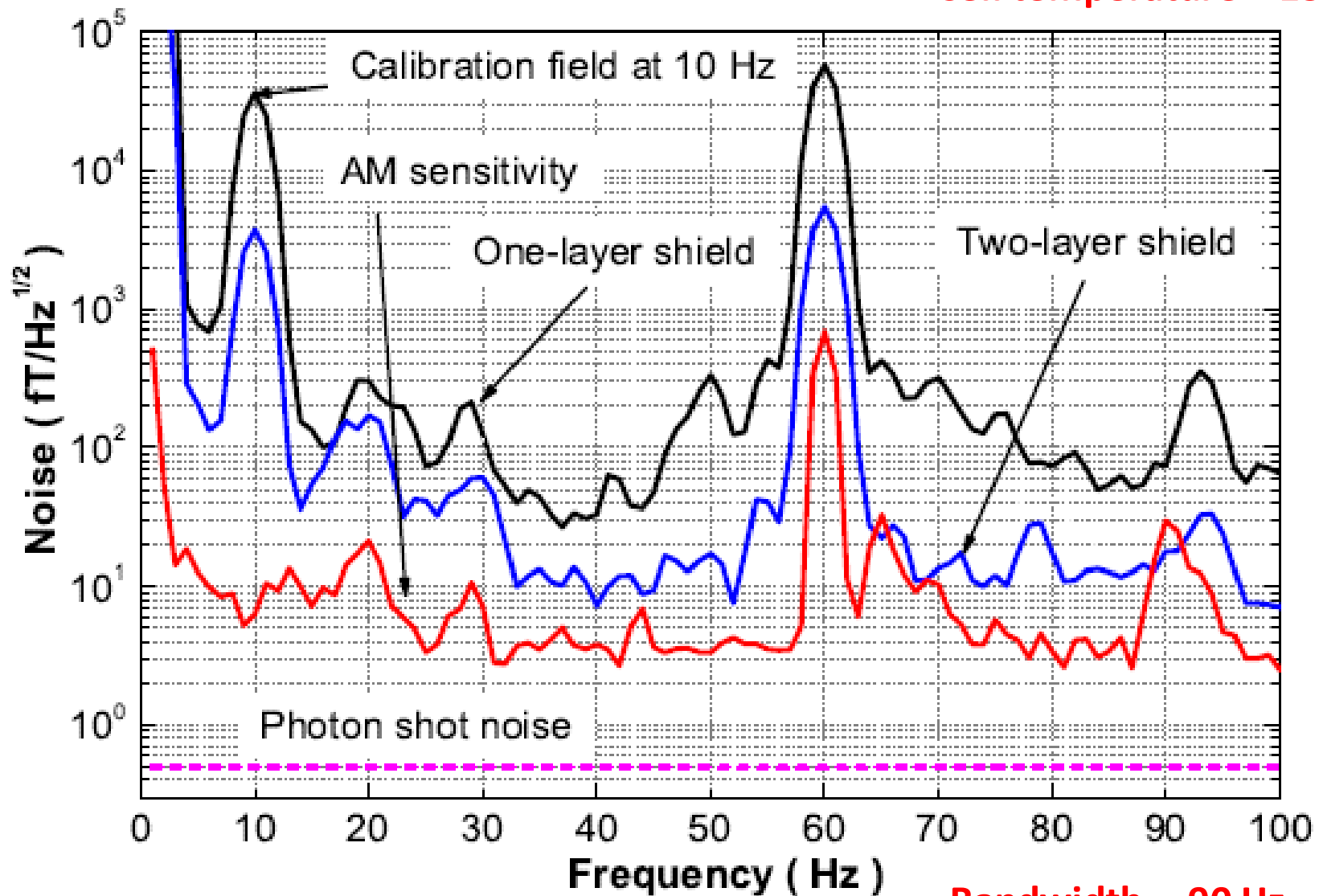
Prototype multi-channel AM



Advantage of using fibers: Flexible AM design

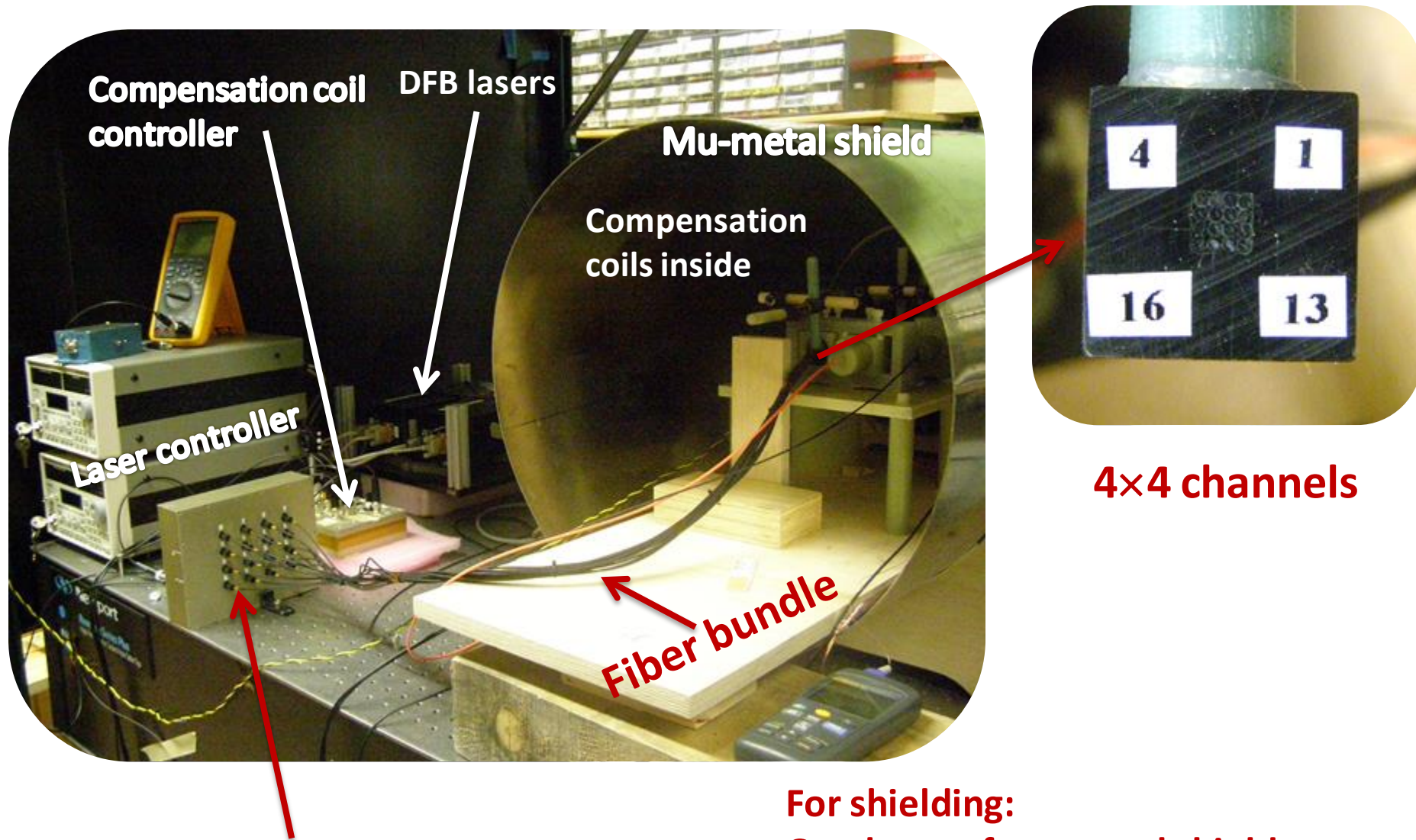
Feasibility proof in single channel

Cell temperature $\sim 150^\circ\text{C}$



Bandwidth $\sim 90 \text{ Hz}$

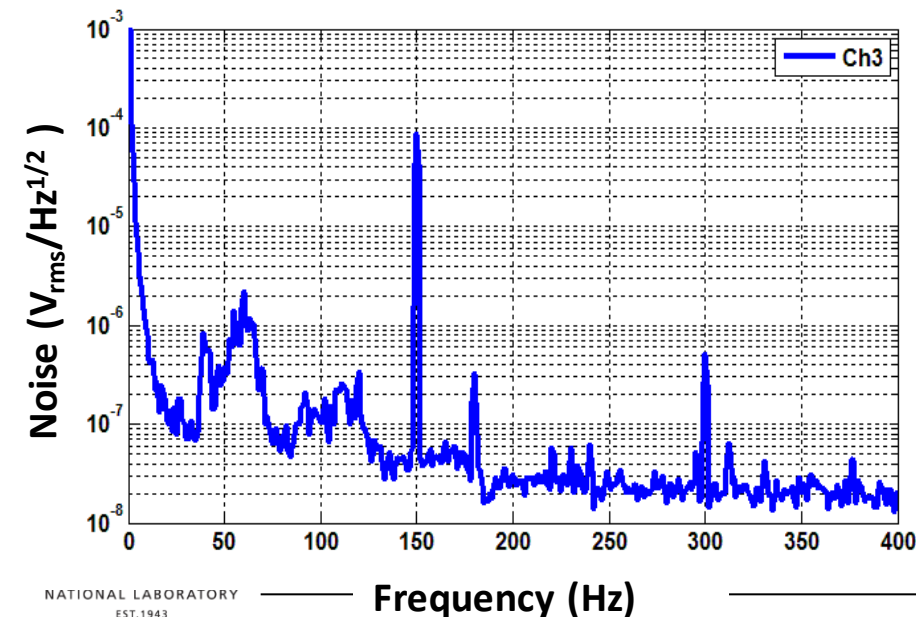
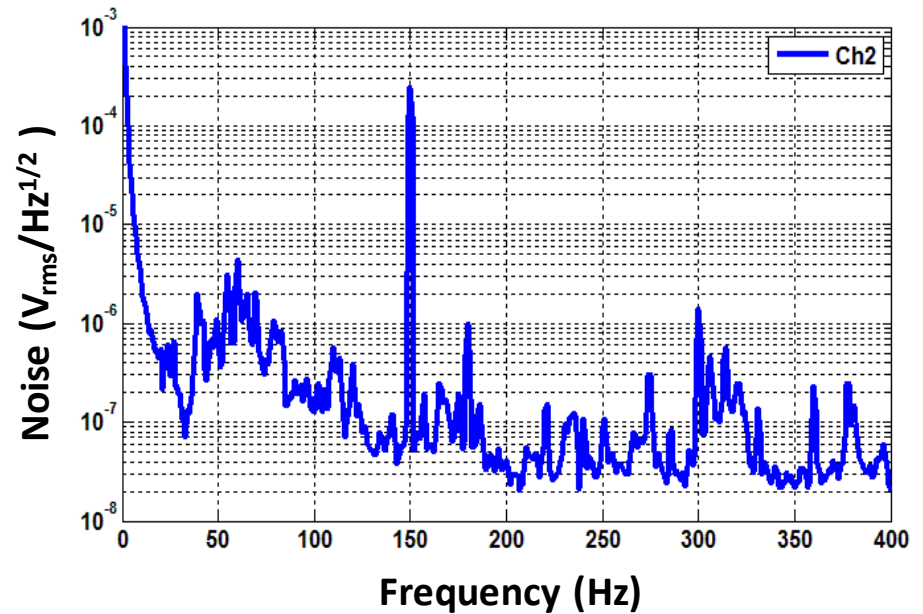
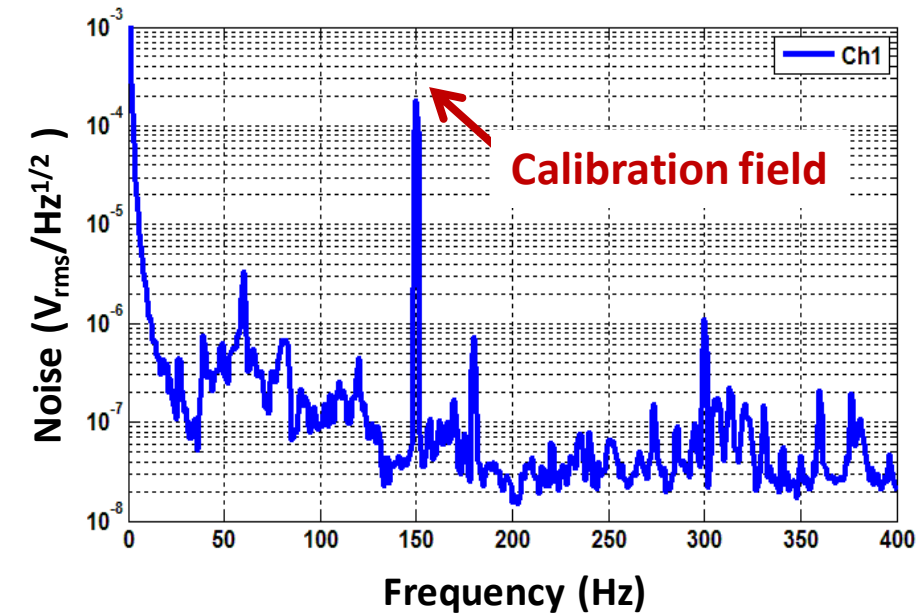
Configuration of multi-channel AM system



16 channels photodiodes array

**For shielding:
One layer of mu-metal shield
One ferrite box**

Preliminary sensitivity test

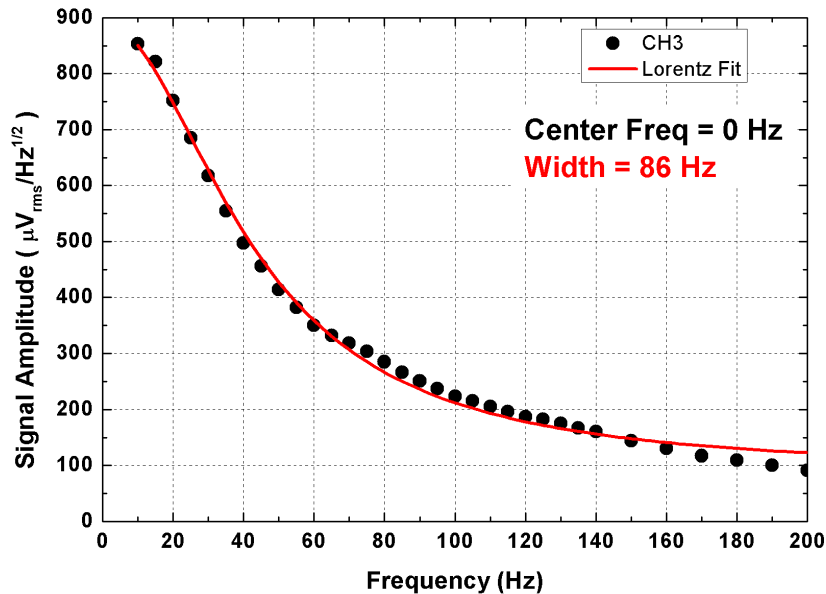
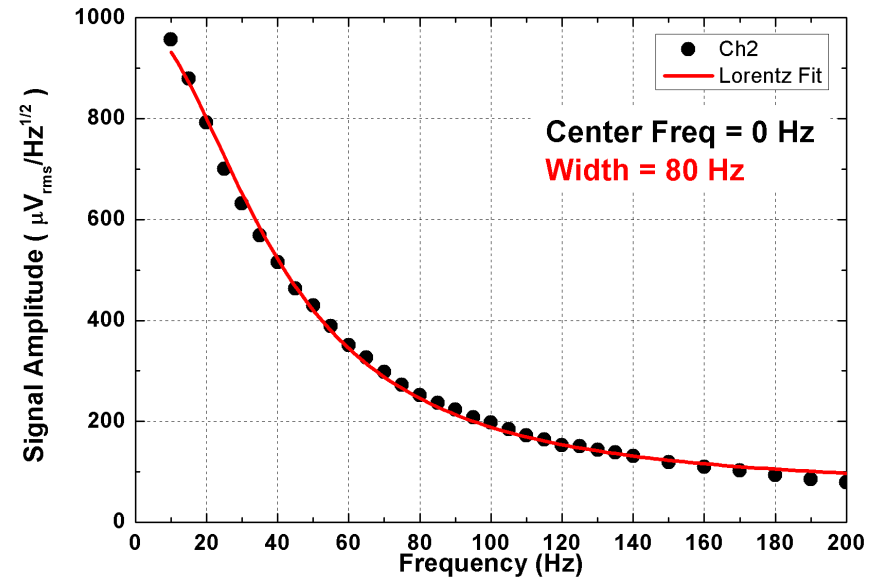
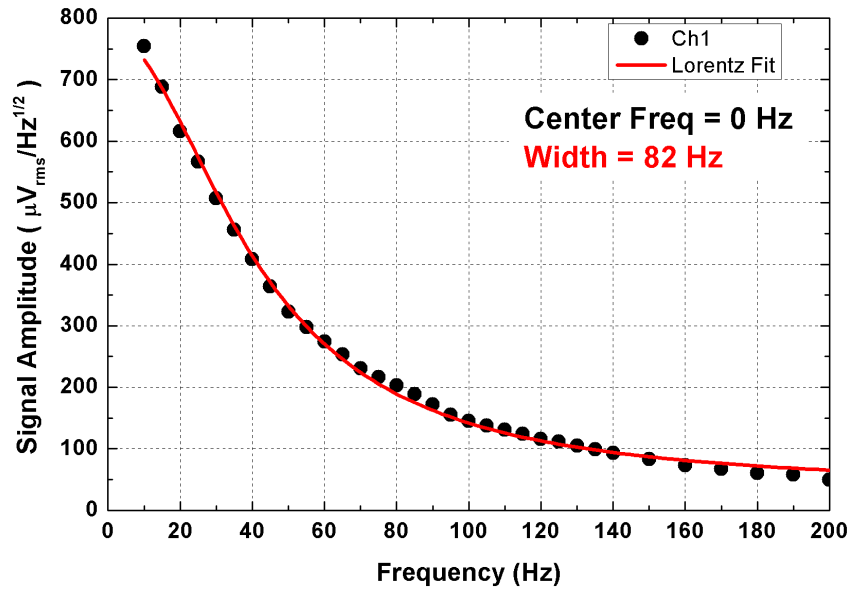


SNR of each channel : 4000 to 100

**Field sensitivity of each channel:
50 $ft/Hz^{1/2}$ to 2000 $ft/Hz^{1/2}$**

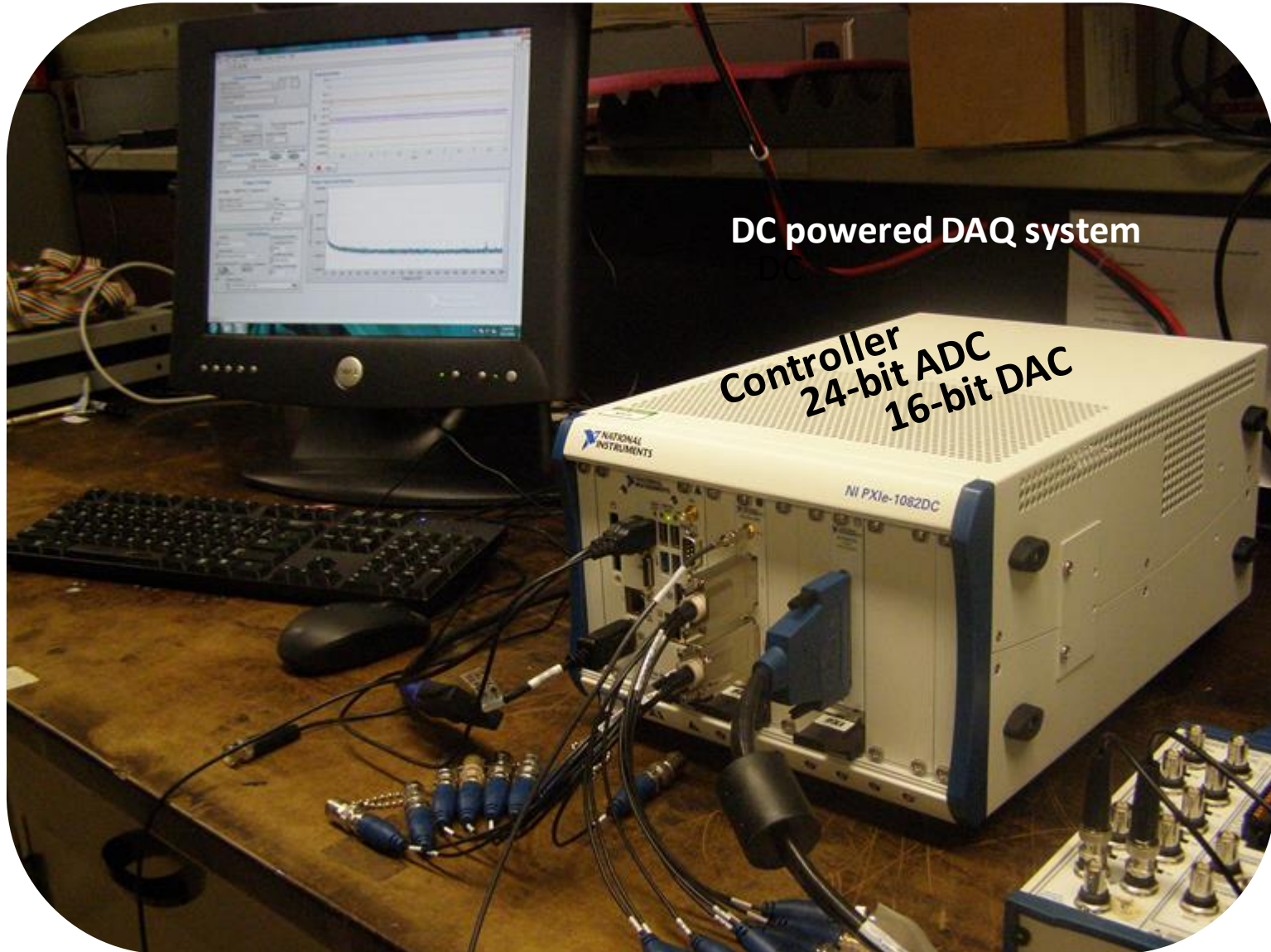
The beam is not uniform?
Intensity attenuation in fiber?

Bandwidth of each channel

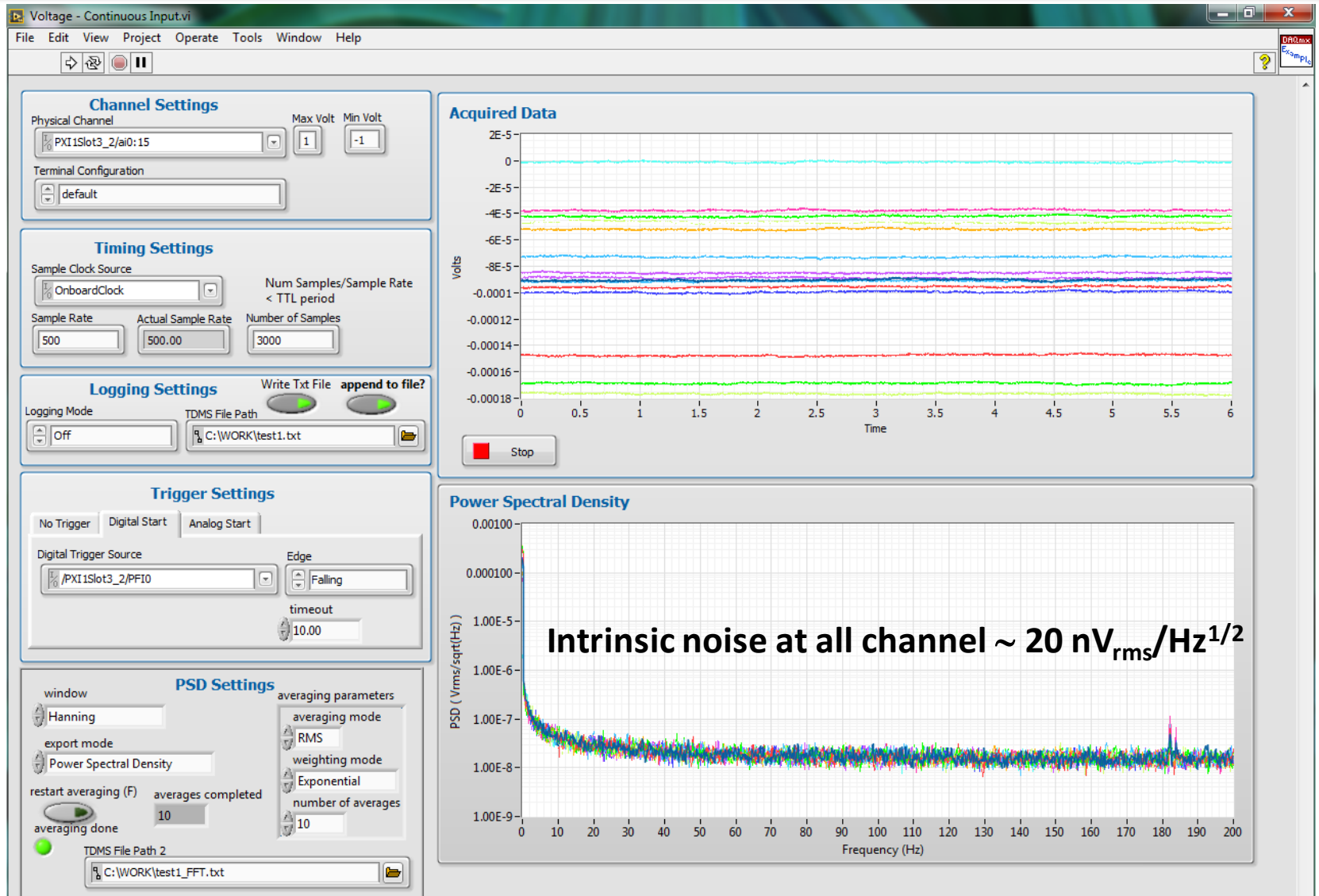


The bandwidth of each channel is good, around 80 Hz

16 channels DAQ system



16 channels DAQ system



Labview program will collect data from 16 channels at same time

future work

- **Application of the FC+AM system to detection of magnetic nanoparticles which in turn are very important for detection of target molecules in national security, medical diagnostics, and other application areas.**
 - **Better AM will be delivered in a week**
- **Improvement of the multi-channel AM system and keep checking its performance**
 - **Place a small coil on the vapor cell and measure the field distribution with 16 channels at same time.**
 - **Check the performance of a 4×4 photodiode array**