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Title: Ultra-sensitive Magnetic Microscopy with an Atomic Magnetometer

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Ultra-sensitive Magnetic Microscopy with an Atomic Magnetometer

Young Jin Kim

Los Alamos National Laboratory

Aug. 19, 2015
Postdoc Summer Seminar

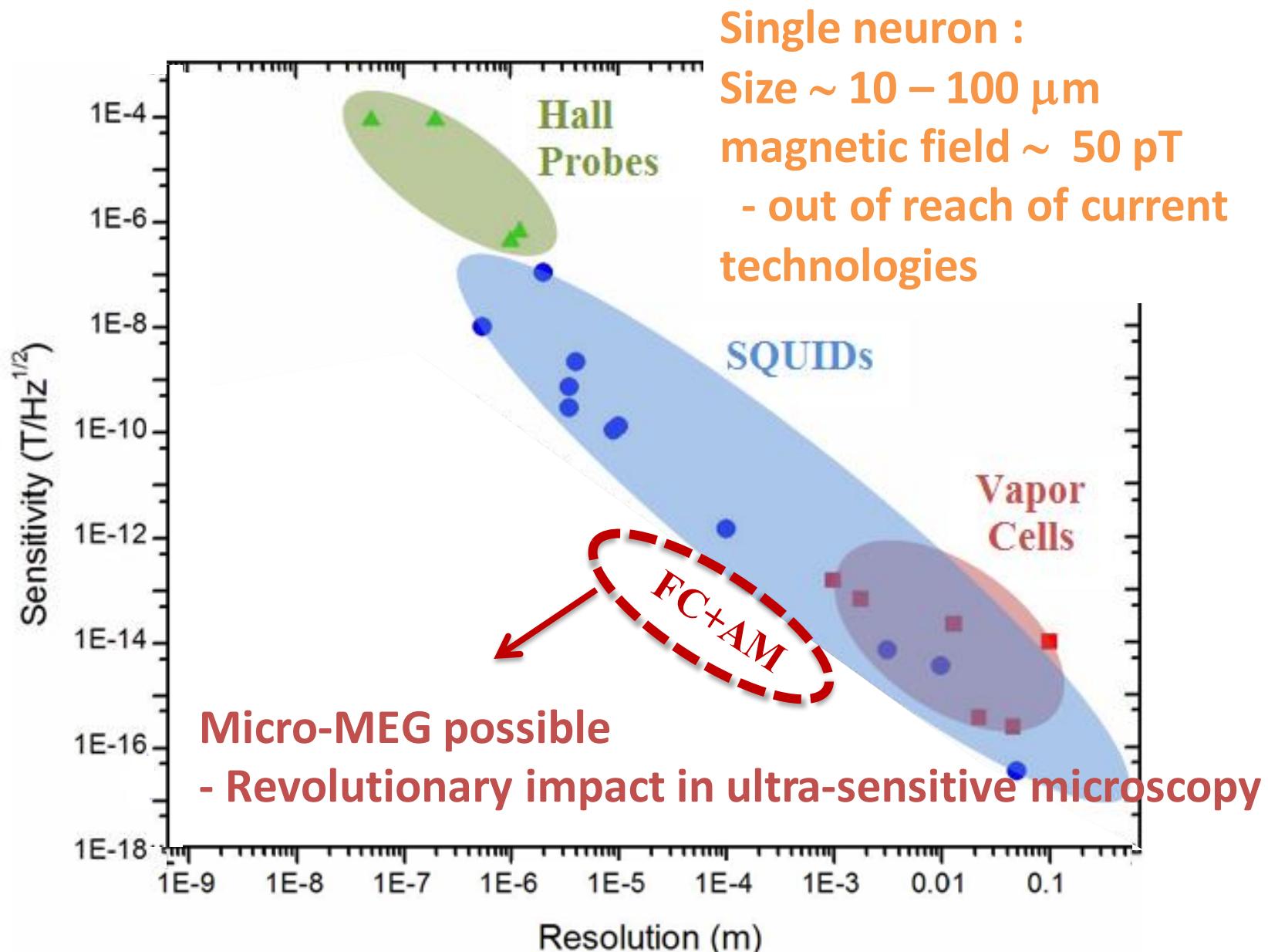
Research goals

- Many applications in neuroscience and other fields require a high-resolution, high-sensitivity magnetic microscope.
- Magnetoencephalography (MEG): a diagnostic technique for studying the brain through measurements of magnetic fields produced by neural currents.



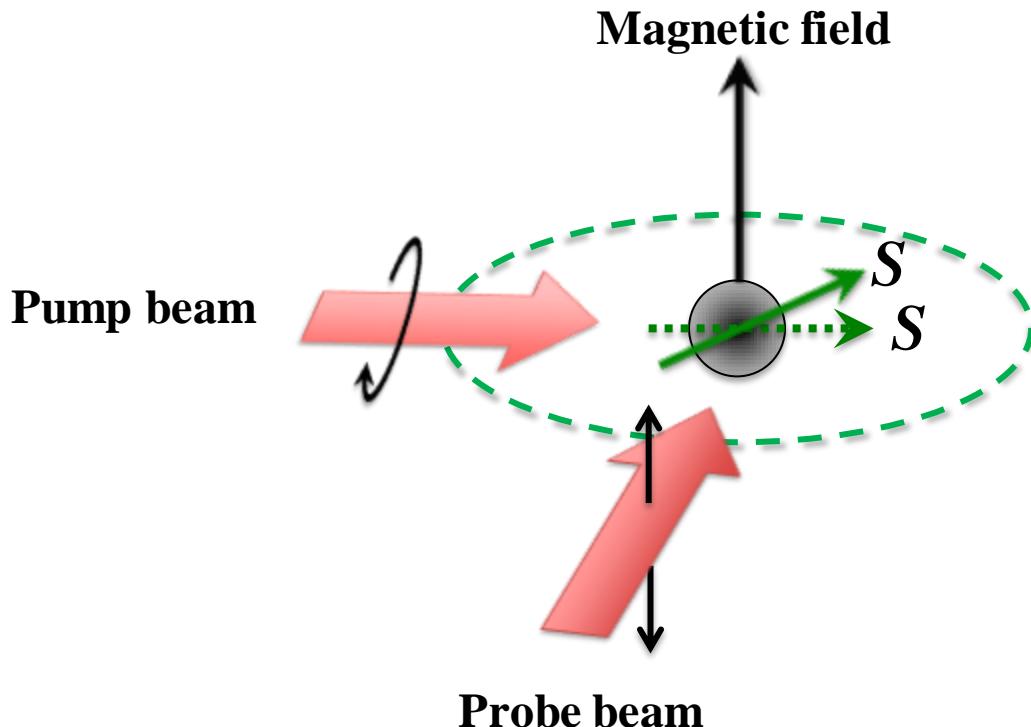
- Current MEG can only measure averages over large numbers of neurons (10^4 to 10^5)
- High-resolution magnetometry, capable of detecting a few neurons;
 - Full understanding of brain function
 - Direct imaging of the structure and composition of proteins and molecules

Research goals



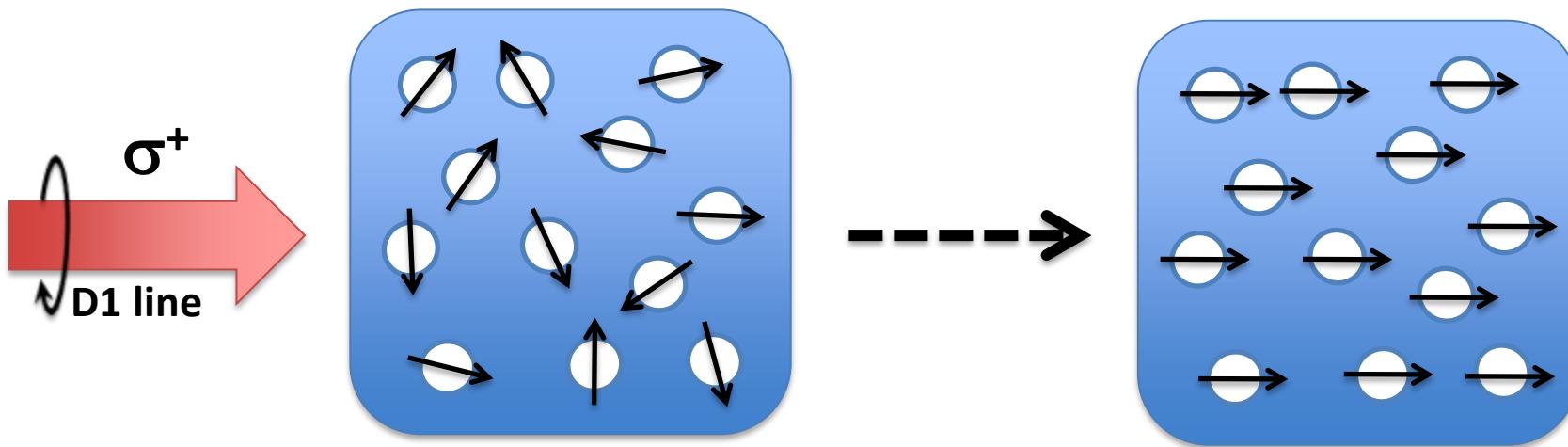
Atomic Magnetometer

- Atomic magnetometer:
 - based on lasers and alkali-metal (Cs, Rb, K) vapor cells
 - the most sensitive non-cryogenic magnetic-field sensor.
- Alkali-metal: a single unpaired electron in the outer energy shell that can be easily manipulated.



Principle of atomic magnetometer

1. Optical pumping



$$n \sim 10^{13} / \text{cm}^3 \text{ at } 150^\circ \text{C}$$

Comparison to thermal polarization (P_T) :

$$P_T = \tanh\left(\frac{0.5g_s\mu_B B}{k_B T}\right)$$

$g_s \approx 2$: Dirac g – factor, μ_B = Bohr magneton
 k_B = Boltzmann constant

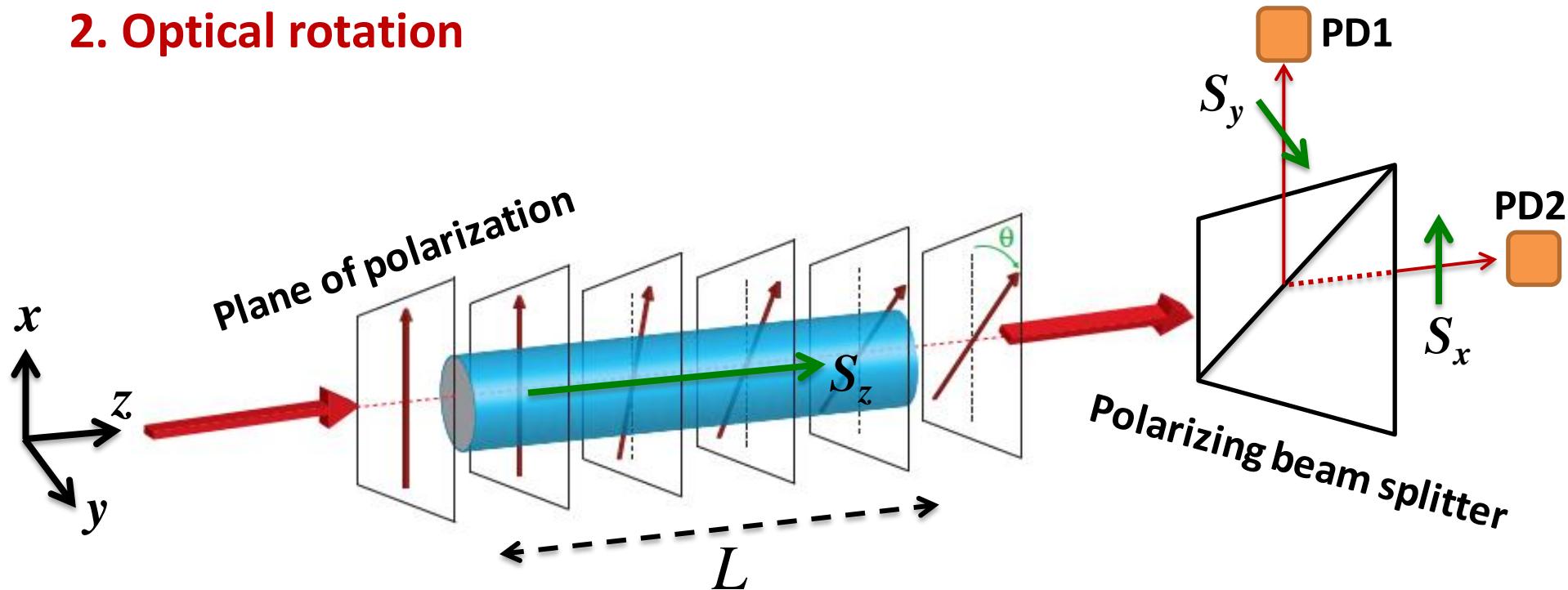
$$P_T = 10^{-7} \text{ with } 0.5 \text{ G, } P_T = 0.02 \text{ with } 10 \text{ T}$$

$P \approx 1$ by optical pumping

(1 W \rightarrow 10^{18} photons/cc, 1 mW is enough for pumping

Principle of atomic magnetometer

2. Optical rotation



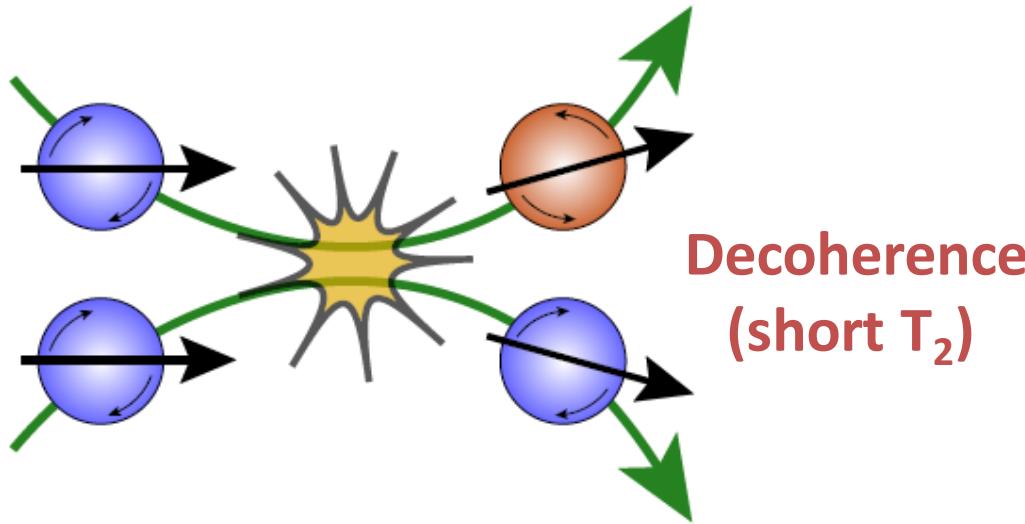
$$\theta \sim L n S_z$$

Optical rotation angle is proportional to the polarization component along the direction of probe beam propagation.

Probe signal at PD : $I_1 = I_0 \sin^2 \theta, I_2 = I_0 \cos^2 \theta$

SERF magnetometer

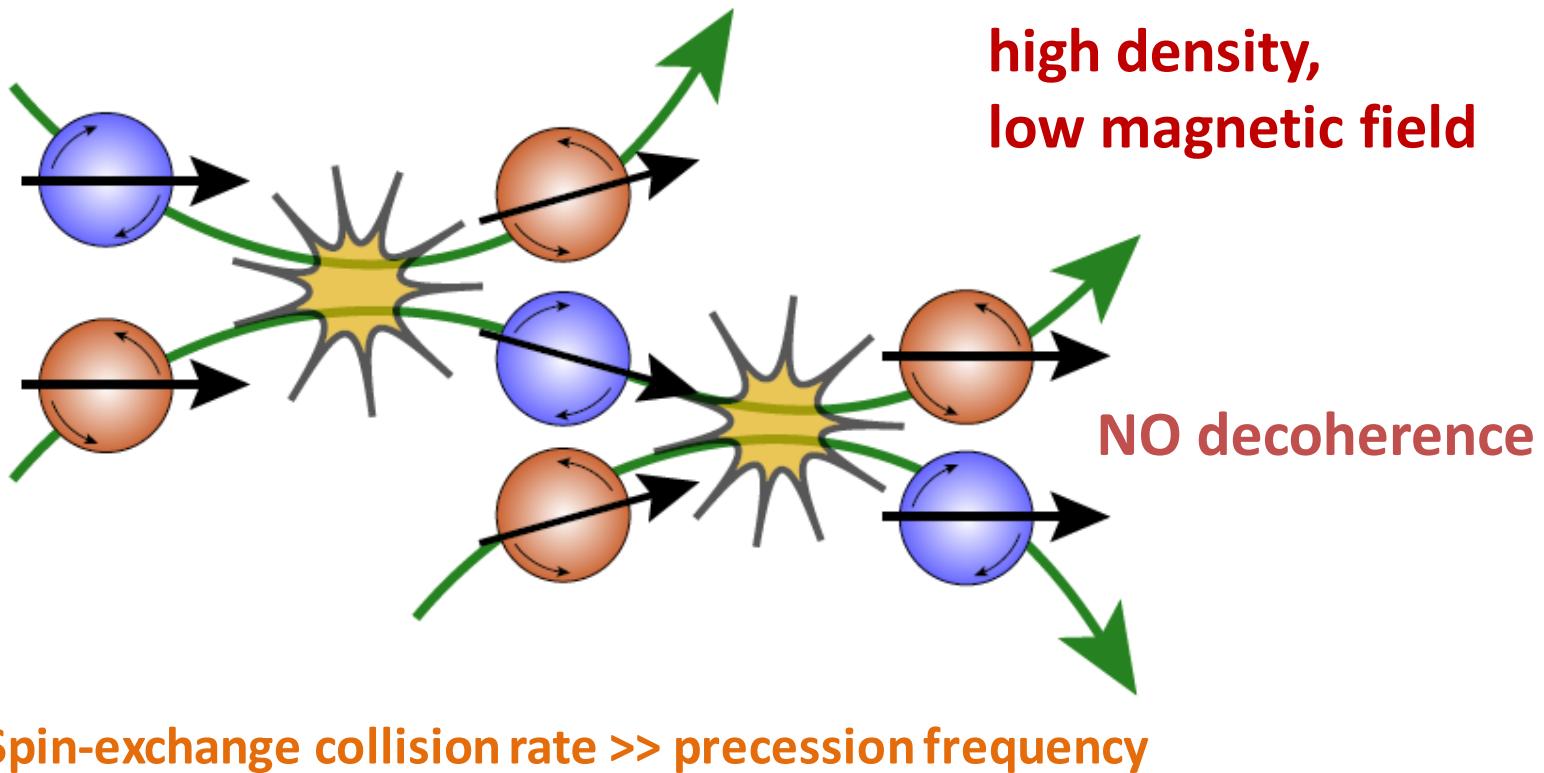
Fundamental Limitation of AM: Spin-exchange collisions.



Breakthrough: Spin-Exchange Relaxation-Free (SERF) magnetometer

- In the regime of high density (strong spin-exchange, strong signal) and low magnetic field, spin-exchange collisions do not depolarize the spins.
- Only SERF magnetometer can achieve subfemtotesla sensitivity in low frequency

SERF magnetometer



SERF magnetometer eliminates spin-exchange relaxation !

First demonstrations of the SERF magnetometer (PRL V. 89, p.130801, 2002):

1. Pump and probe beams were orthogonal (most optimal configuration)
2. Sensitivity $\sim 10 \text{ fT/Hz}^{1/2}$
3. Less convenient for miniaturization and cost reduction

SERF Magnetometer Response

Bloch equation describes the response of the SERF magnetometer to magnetic fields:

$$\frac{d\vec{S}}{dt} = \gamma \vec{S} \times \vec{B} + R(S_0 \hat{z} - \vec{S}) - \frac{\vec{S}}{T_2}$$

S : electron spin polarization vector,
R: optical pumping rate
S₀: equilibrium electron spin polarization
 $\gamma = 2\pi \times 7 \text{ GHz/T}$

Steady state solution, dS/dt =0 :

$$S_x = S_0 \frac{-\beta_y + \beta_x \beta_z}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)},$$

$$S_z = S_0 \frac{1 + \beta_z^2}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)},$$

$$S_y = S_0 \frac{\beta_x + \beta_y \beta_z}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)},$$

$$\vec{\beta} = \frac{\gamma \vec{B}}{R + T_2^{-1}}$$

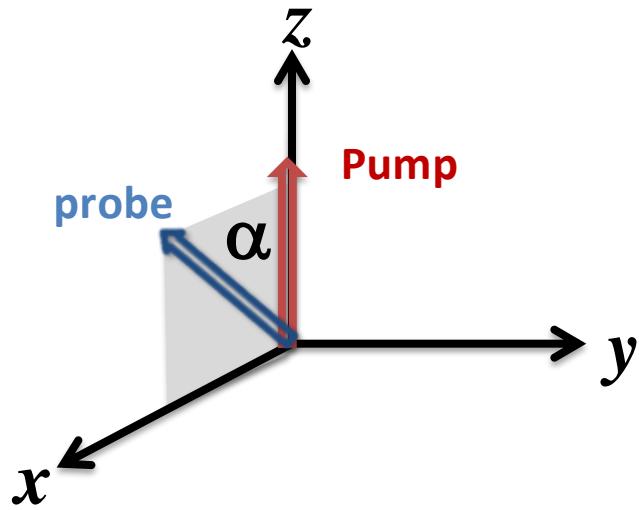
dimensionless magnetic field components

SERF Magnetometer Response

Magnetometer signal proportional to the component of the electron spin in the probe propagation direction:

$$S_{\text{probe}} = S_x \sin \alpha + S_z \cos \alpha$$

$$= S_0 \left[\frac{(-\beta_y + \beta_x \beta_z) \sin \alpha + (1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right]$$



First case: α is not small

$$S_{\text{probe}} \approx S_0 \left[\frac{(-\beta_y + \beta_x \beta_z) \sin \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right]$$

Maximum value when α is $\pi/2$

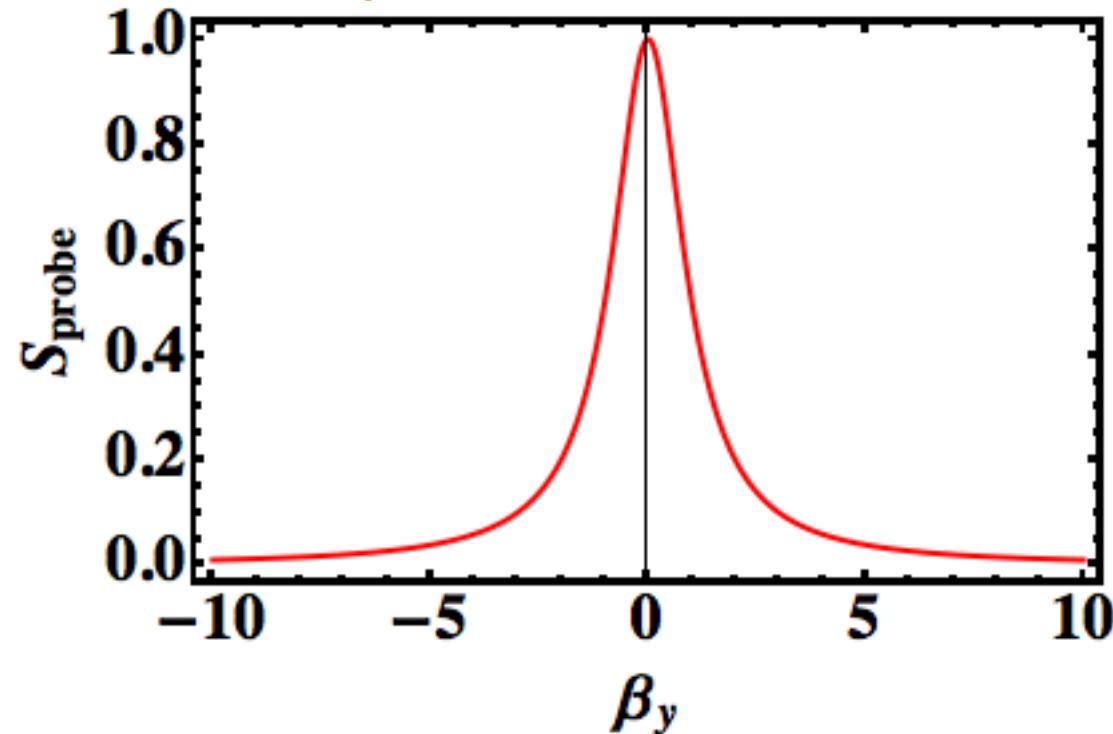
This case is the traditional perpendicular probe-pump orientation, but we are interested in almost parallel beam probe-pump orientation

SERF Magnetometer Response

Second case: α is very small (nearly parallel beams configuration)

$$S_{\text{probe}} \approx S_0 \left[\frac{(1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right] \approx S_0 \left[\frac{1}{1 + (\beta_x^2 + \beta_y^2)/(1 + \beta_z^2)} \right]$$

Example:



For maximum response to a oscillating field:

$$\frac{\partial S_{\text{probe}}}{\partial \beta_y} = \max$$

SERF Magnetometer Response

Second case: α is very small

$$S_{\text{probe}} \approx S_0 \left[\frac{(1 + \beta_z^2) \cos \alpha}{1 + (\beta_x^2 + \beta_y^2 + \beta_z^2)} \right] \approx S_0 \left[\frac{1}{1 + (\beta_x^2 + \beta_y^2)/(1 + \beta_z^2)} \right]$$

- Maximum response to a oscillating field in y direction:

$$\frac{\partial S_{\text{probe}}}{\partial \beta_y} = 0.65 S_0 \quad \text{at } \boxed{\beta_x = \beta_z = 0, \beta_y = 1/\sqrt{3}}$$

Optimal fields

Decreased by a factor of 1.5 compared to the perpendicular beams

- Maximum response to a oscillating field in z direction:

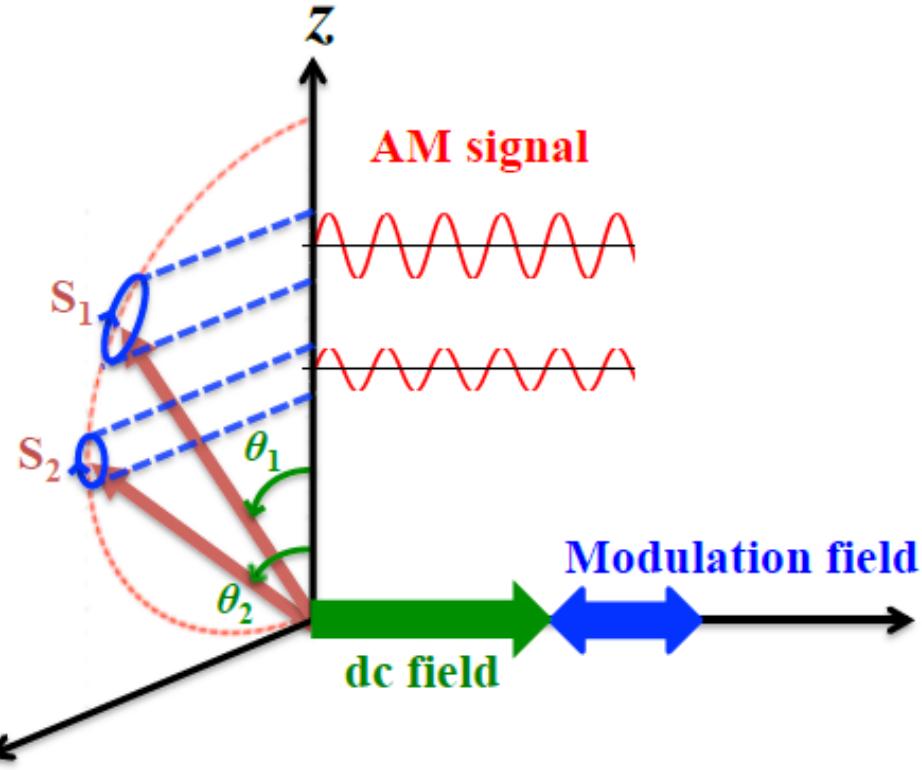
$$\frac{\partial S_{\text{probe}}}{\partial \beta_z} = 0.25 S_0 \quad \text{at } \boxed{\beta_z = 1, \beta_x^2 + \beta_y^2 = 2}$$

Optimal fields

Decreased by a factor of 2 compared to the perpendicular beams

SERF Magnetometer Response

Visualization of the optimization to the y component:



$$\vec{\beta} = \frac{\gamma \vec{B}}{R + T_2^{-1}}, R + T_2^{-1} = 1$$

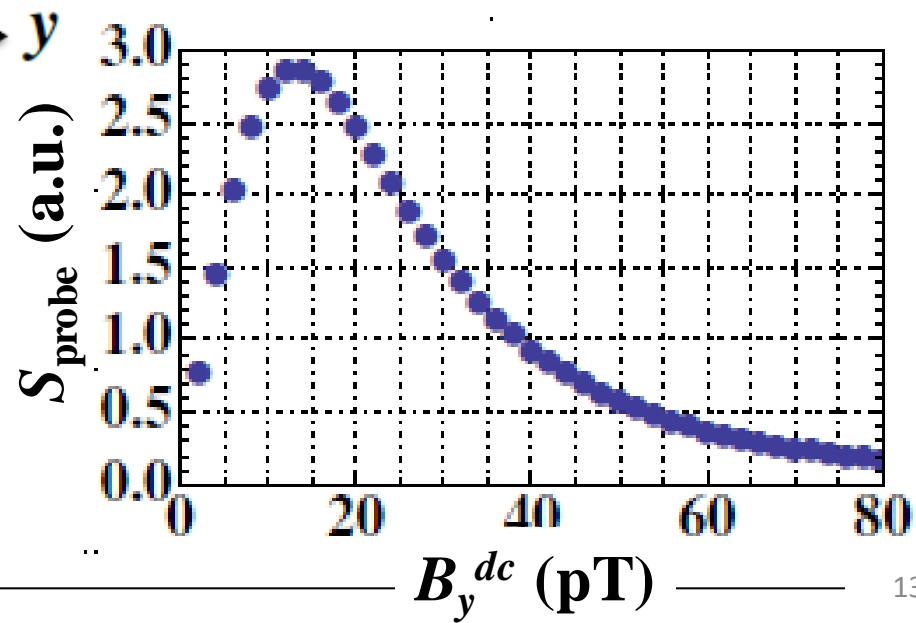
$$B_y^{dc} = (\beta_y = 1/\sqrt{3})/\gamma = 13 \text{ pT}$$

$$\theta = \tan^{-1}(S_x / S_z) = \tan^{-1} \beta_y^{dc}$$

$$\begin{aligned} \text{Magnitude} &= \sqrt{S_x^2 + S_y^2 + S_z^2} \\ &= S_0 / \sqrt{1 + (\tan \theta)^2} \end{aligned}$$

Optimal angle:

$$\theta = \tan^{-1}(1/\sqrt{3}) = 30^\circ$$



Resolution of SERF magnetometer

The fundamental sensitivity limit is due to shot-noise:

$$\delta B = \frac{1}{\gamma \sqrt{NT_2Vt}}$$

N = the number of active atoms
 V = the cell volume,
 t = the measurement time

Higher sensitivity \rightarrow lower resolution

Example: 1 fT/Hz^{1/2} \rightarrow cm-scale resolution

(Nature V. 422, p.596, 2003)

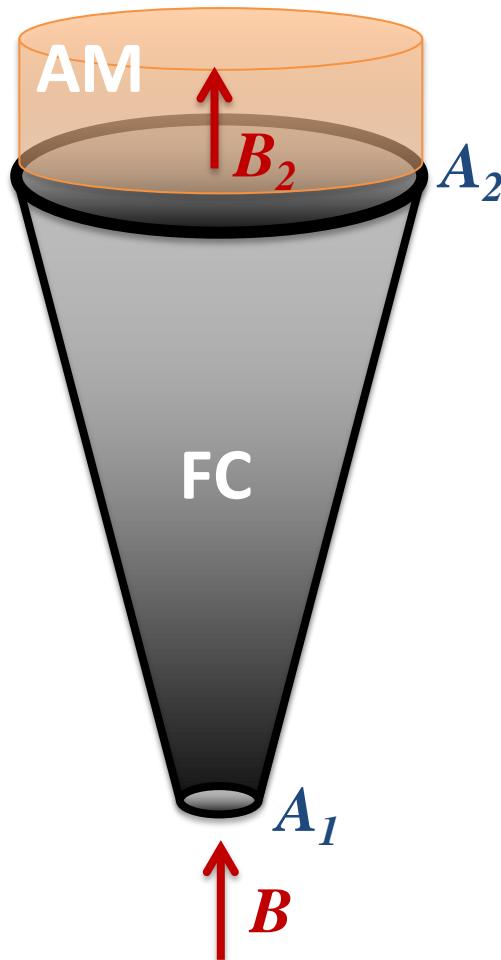
70 fT/Hz^{1/2} \rightarrow mm-scale resolution

(Nat. Photonics V. 1, p.649, 2007)

How to reach high resolution, high sensitivity?

➤ Instead of reducing cell dimensions to micron size, a flux concentrator expands the microscopic magnetic distribution to match the dimensions of AM operating with high sensitivity.

FC + AM system



AM measured B_2 :

$$B_2 = B \frac{A_1}{A_2}$$

Sensitivity of a FC+AM system composed of an AM with 1 fT sensitivity and 5 mm channel and an FC with 100 μm resolution:

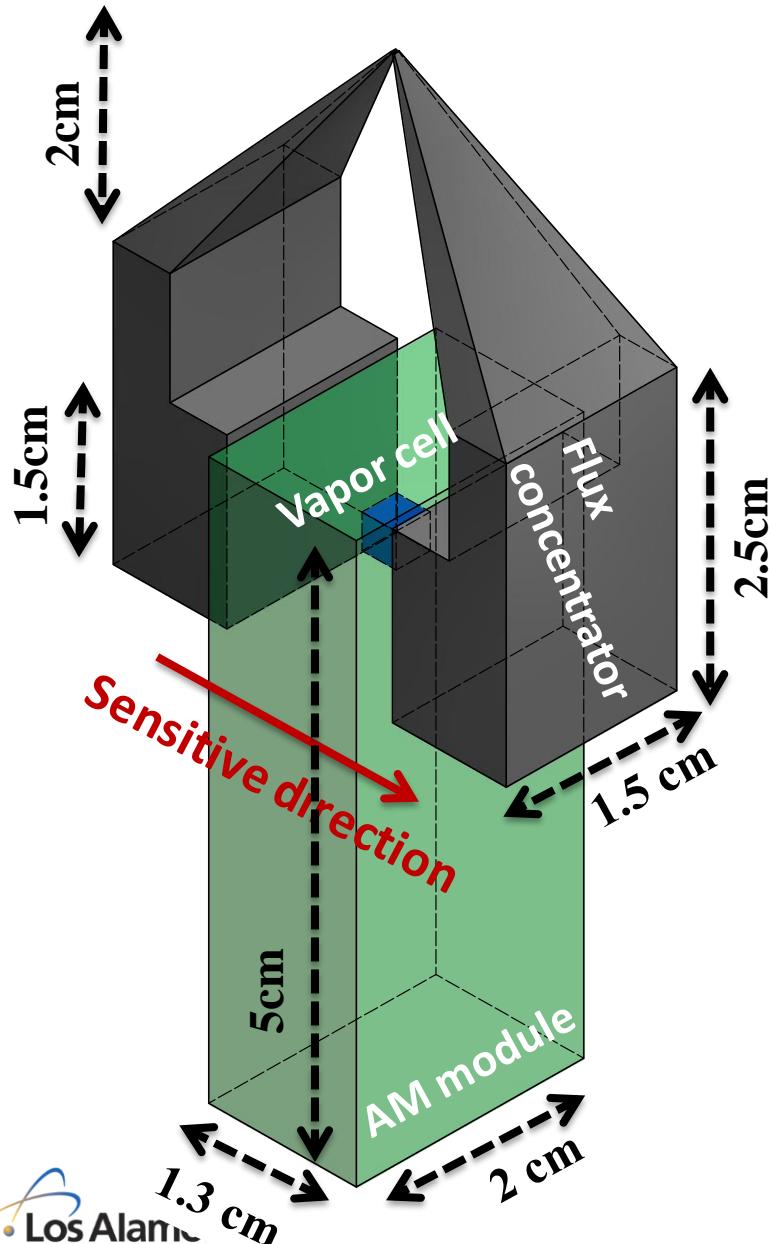
$$B = B_2 \frac{A_2}{A_1} = 1 \text{ fT} \frac{\pi \left(\frac{5 \text{ mm}}{2} \right)^2}{\pi \left(\frac{100 \mu\text{m}}{2} \right)^2} = 2.5 \text{ pT}$$

Magnetic field of interest



Suitable for detecting a single neuron

Design of a single channel FC+AM system



Flux concentrator:

- Constructed from non-conductive MnZn ferrites to avoid large Johnson noise.
- Noise from MnZn ferrite \sim fT level
- $\mu \sim 6500$

Atomic magnetometer:

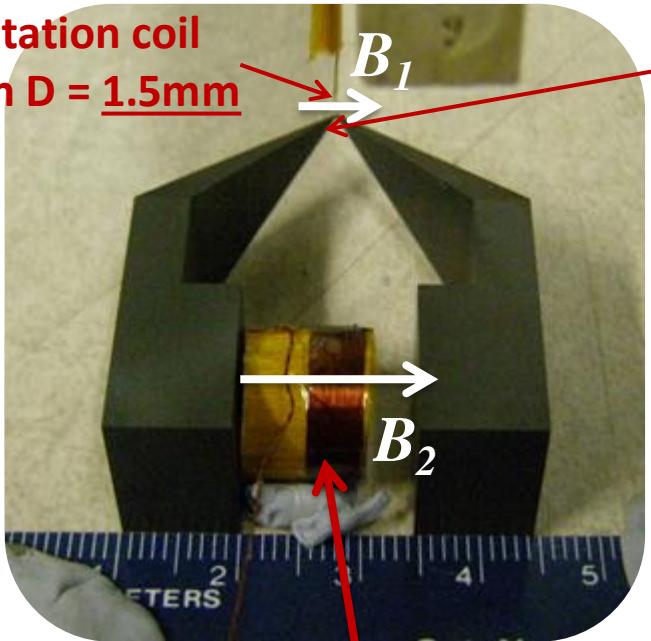
- Commercial integrated AM
- Vapor cell size: 3mm \times 3mm \times 3mm
- Sensitivity \sim 10 fT level (it can be improved to \sim 1 fT level).

Test of field transfer on FC

Excitation coil
with $D = 1.5\text{ mm}$

B_1

Gap between ferrite tips = 2 mm



Sensing coil with $D = 11.6\text{ mm}$, 20 turns

Field at the excitation coil, $B_1 = \frac{\mu_0 I}{D}$

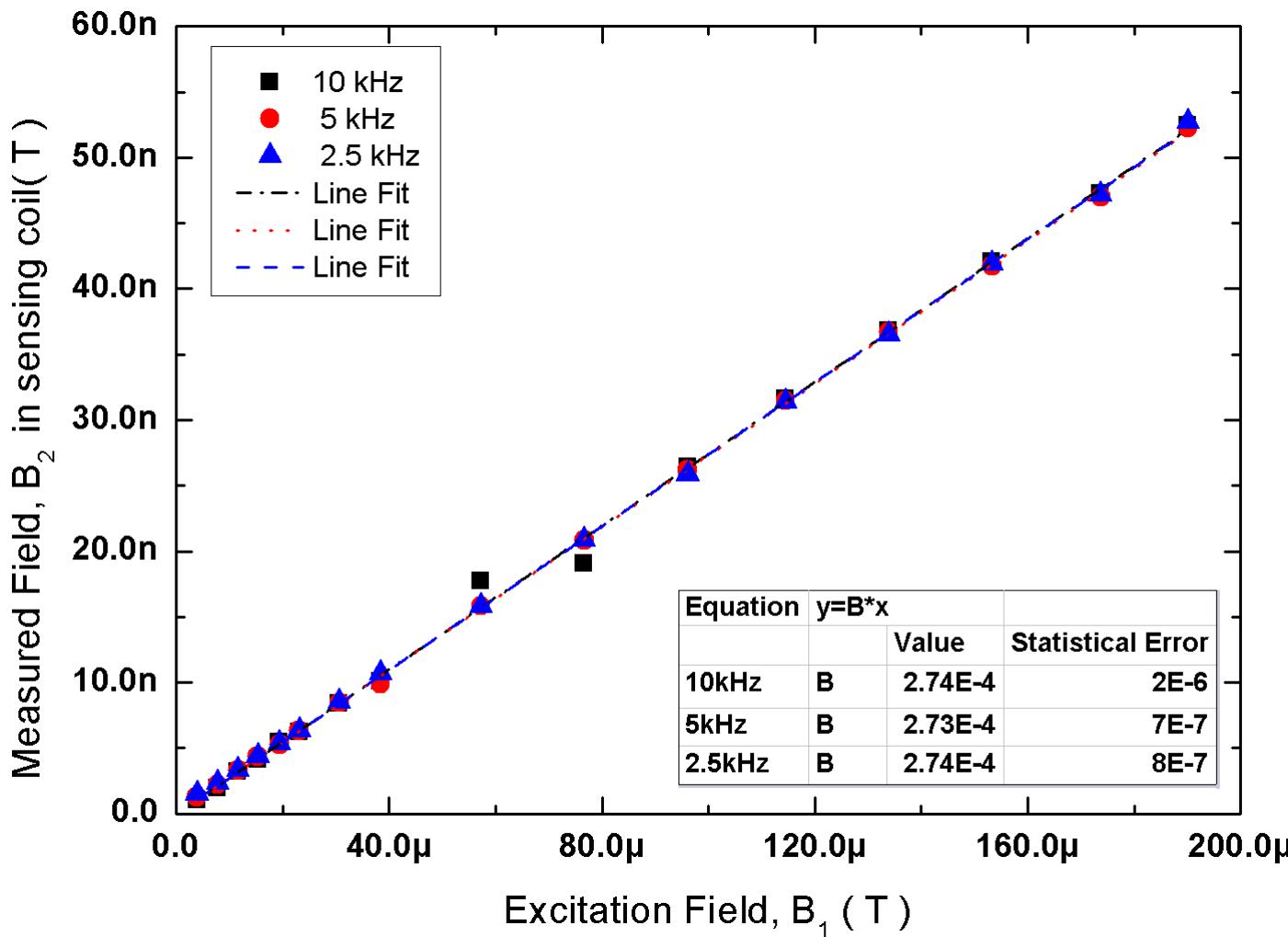
Field at the sensing coil, $B_2 = \frac{V}{NA\omega}$

Field transfer coefficient : $k = \frac{B_2}{B_1}$

Sensitivity of FC + AM system
= (Sensitivity of AM)/k

Ideal $k = 9.4 \times 10^{-3}$

Test of field transfer on FC

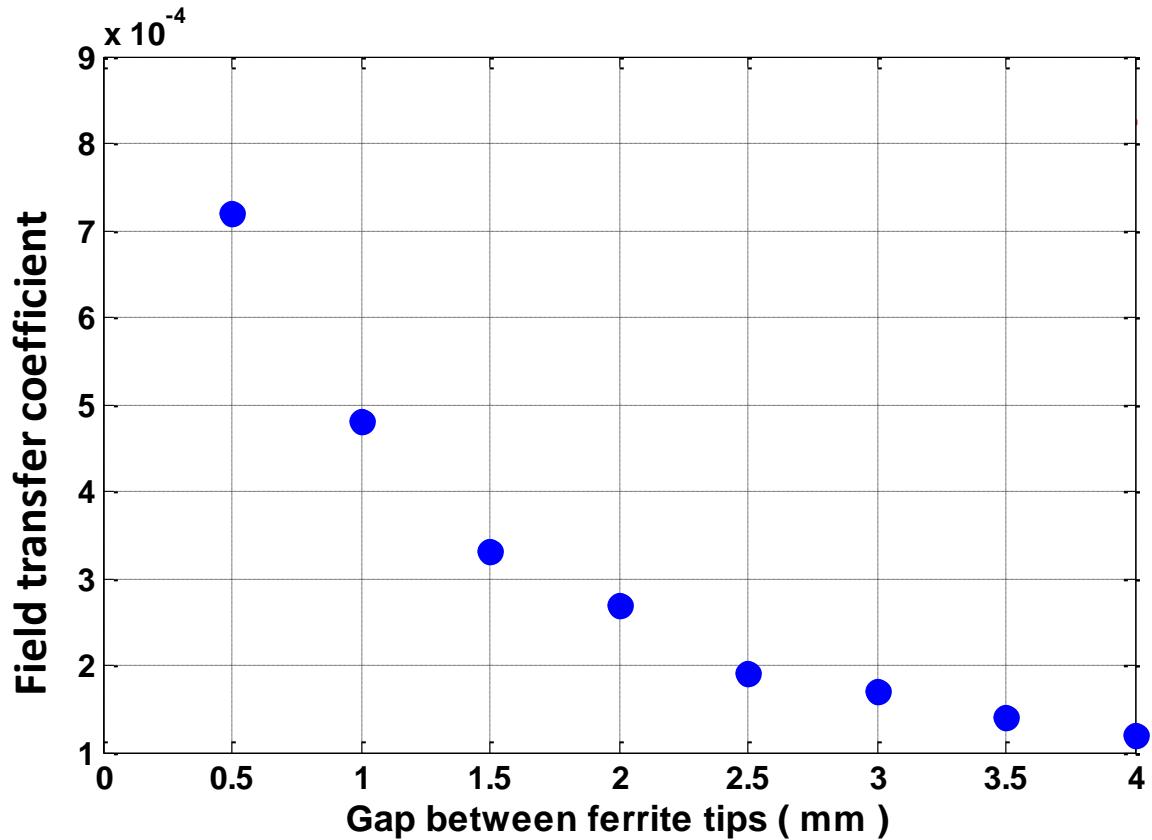
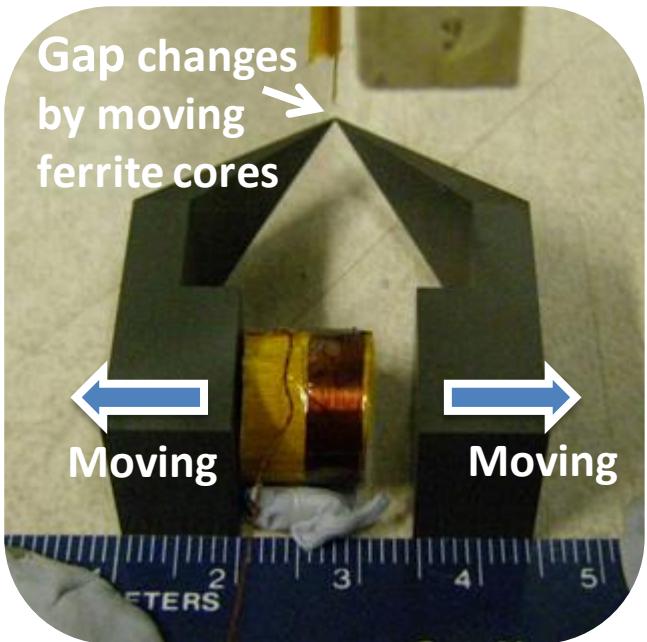


$$k = 2.74 \times 10^{-4}$$



Sensitivity of FC + AM system
 $= 1 \text{ fT}/k = 3.6 \text{ pT}$

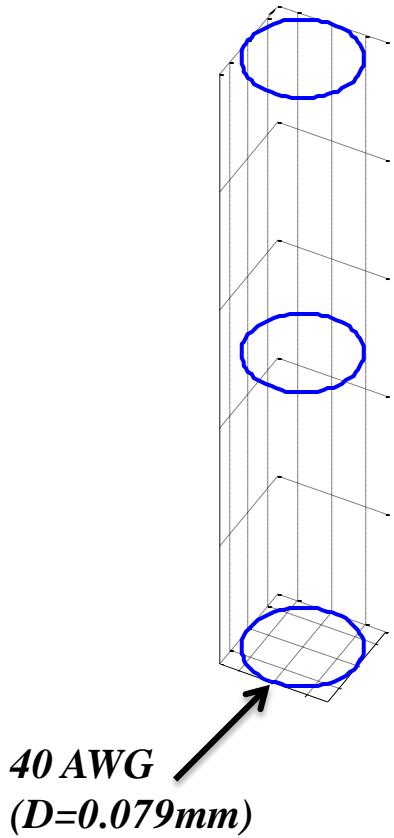
Test of field transfer on FC



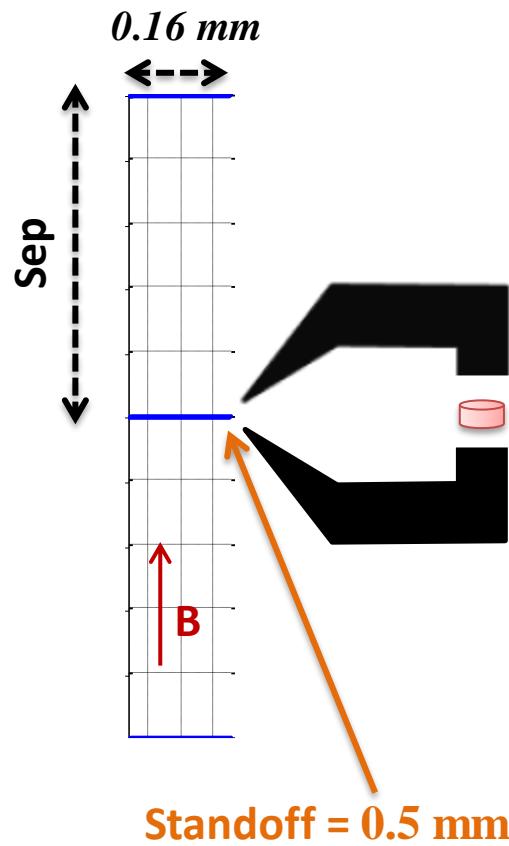
Field transfer improves with smaller gap between ferrite tips
- more flux is collected by ferrite

Test of resolution

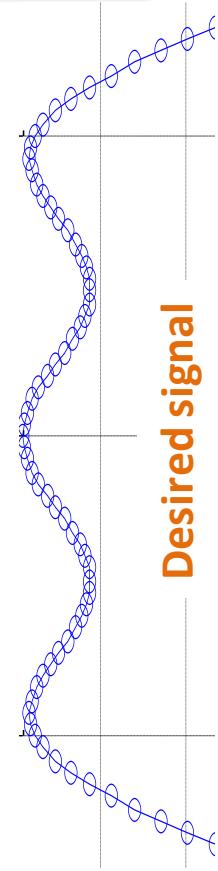
Coil array



Side view



Scanning field through this way

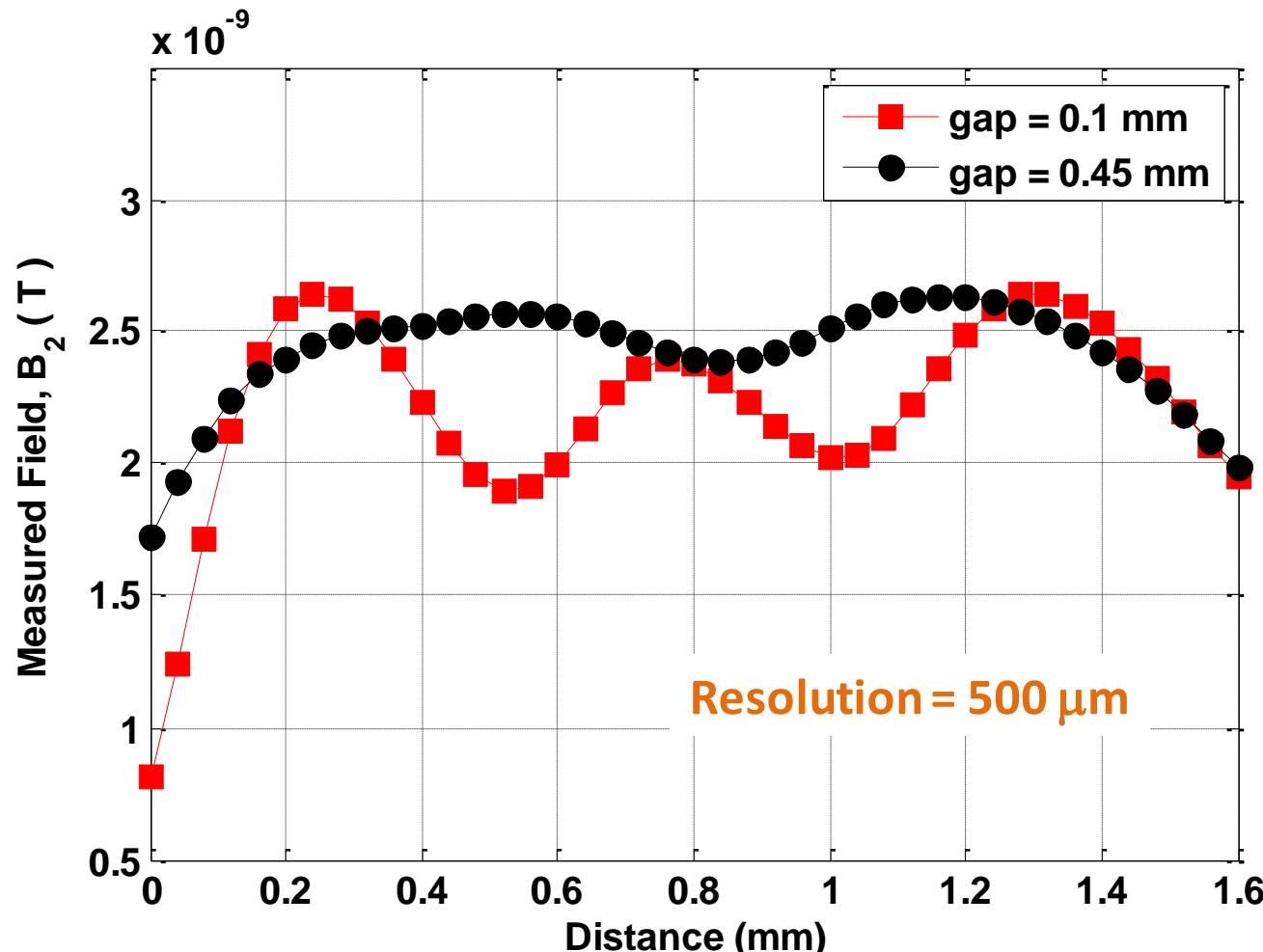


- Change the distance between the coils for resolution tests
- Flux concentrator can see three peaks of the field?

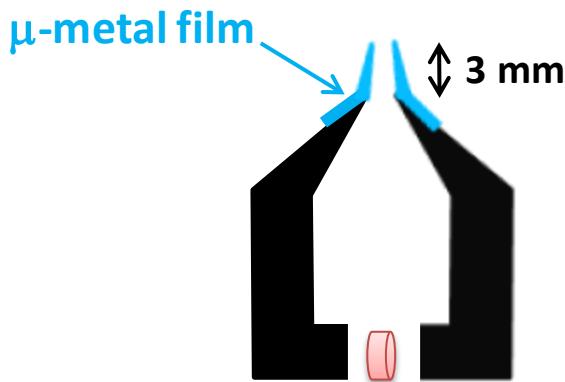


Test of resolution

- Gap between ferrite tips changed
- Measuring three peaks means the resolution of 500 μm .

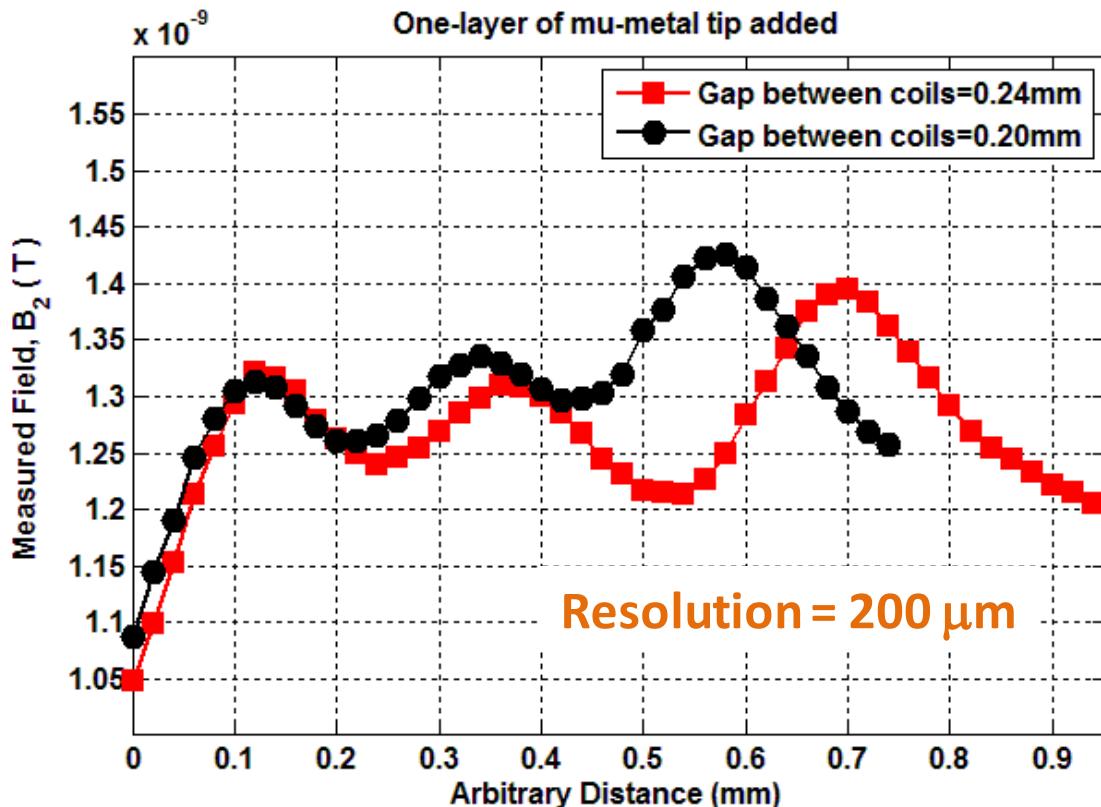


Test of resolution



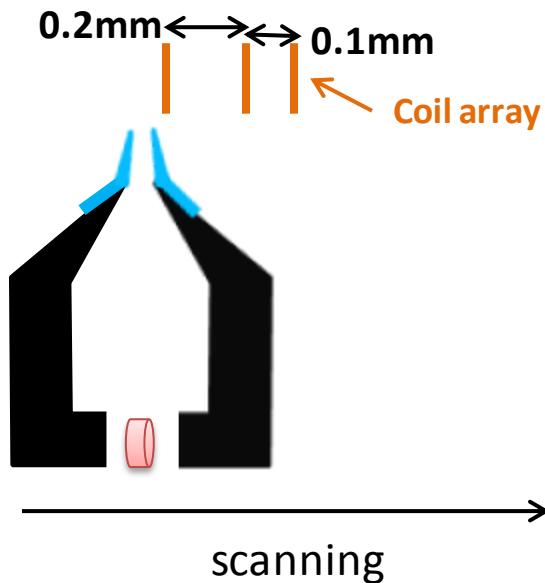
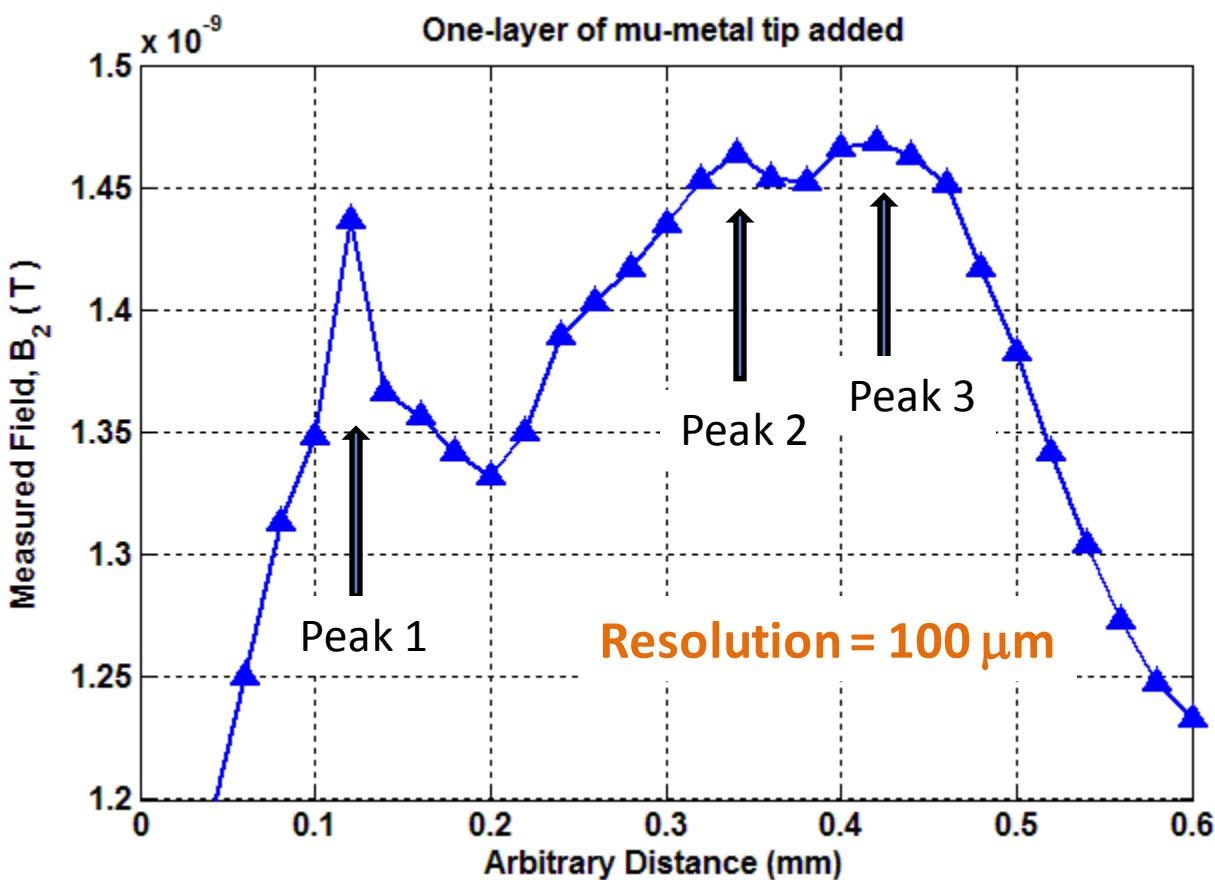
- The distance between excitation coils is ~ 0.2 mm and 0.3 mm.

- For higher resolution, a sharp μ -metal film (one layer) is attached on the ferrite tips
- Gap of the ferrite tips $\sim 0.1\text{mm}$

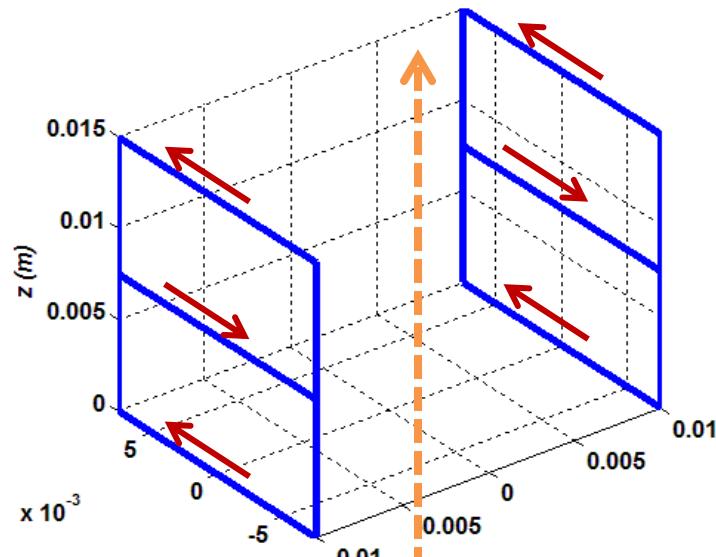


Test of resolution

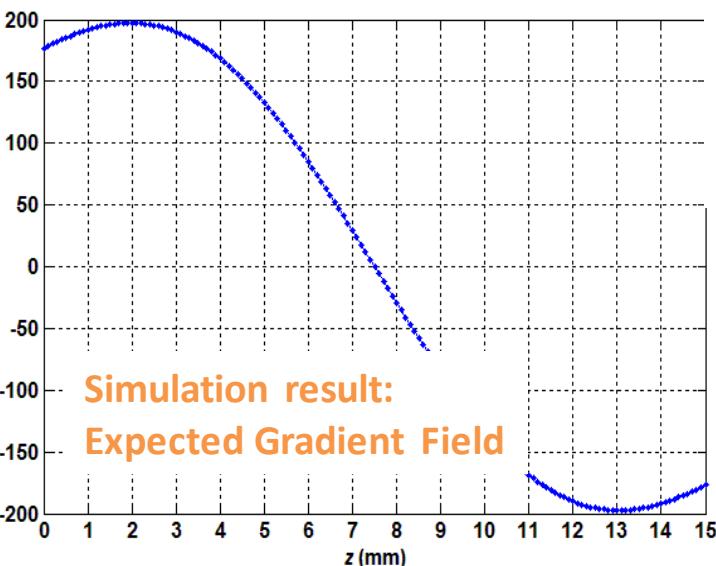
- The distance between excitation coils is $\sim 0.2 \text{ mm}$ and $\sim 0.1 \text{ mm}$.
- Gap of the mu-metal tips $\sim 0.1 \text{ mm}$



Gradient cancellation

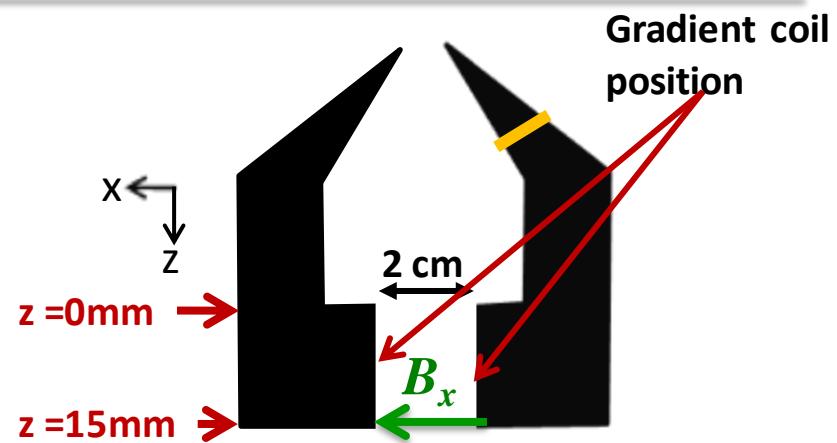
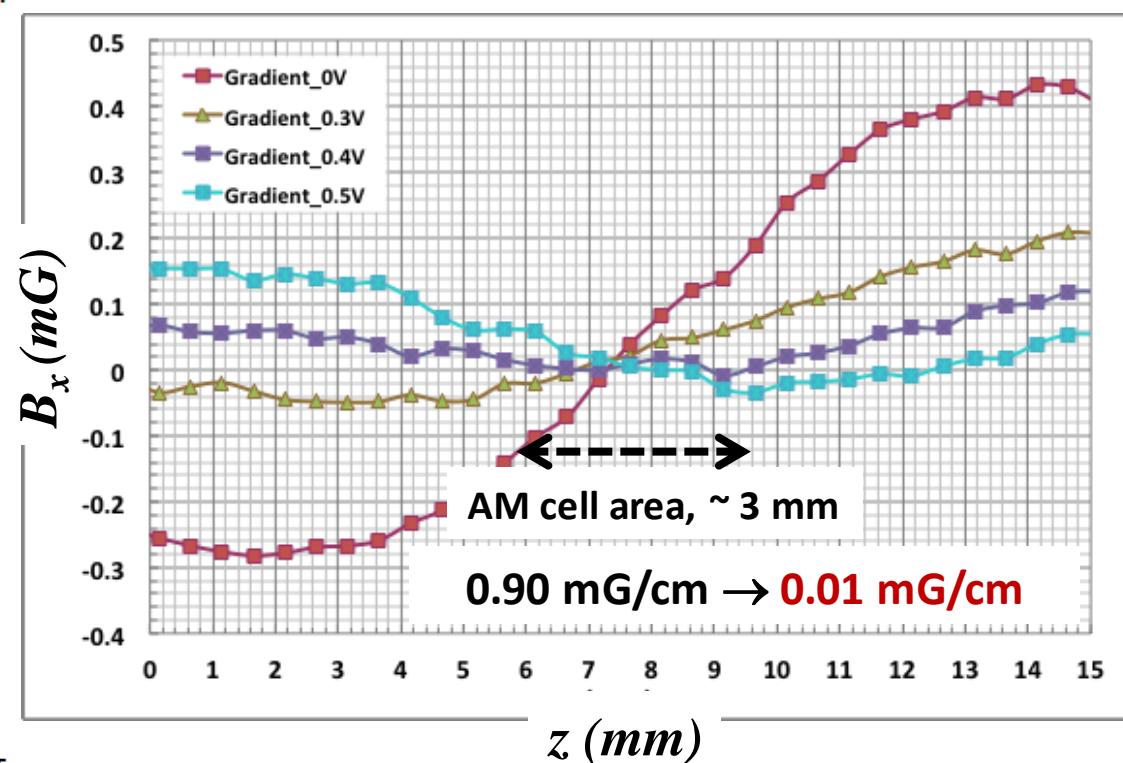


Direction of scanning B_x



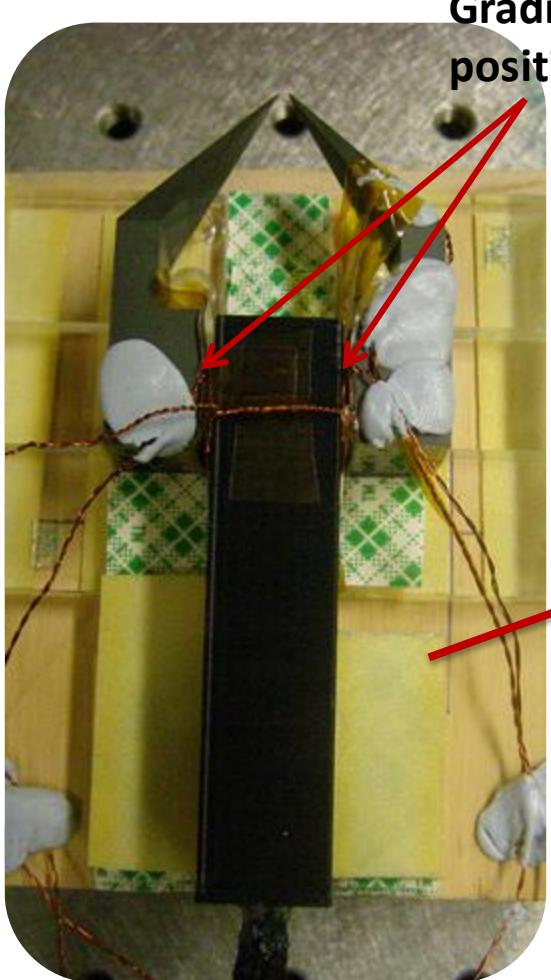
Simulation result:

Expected Gradient Field



Gradient coil position

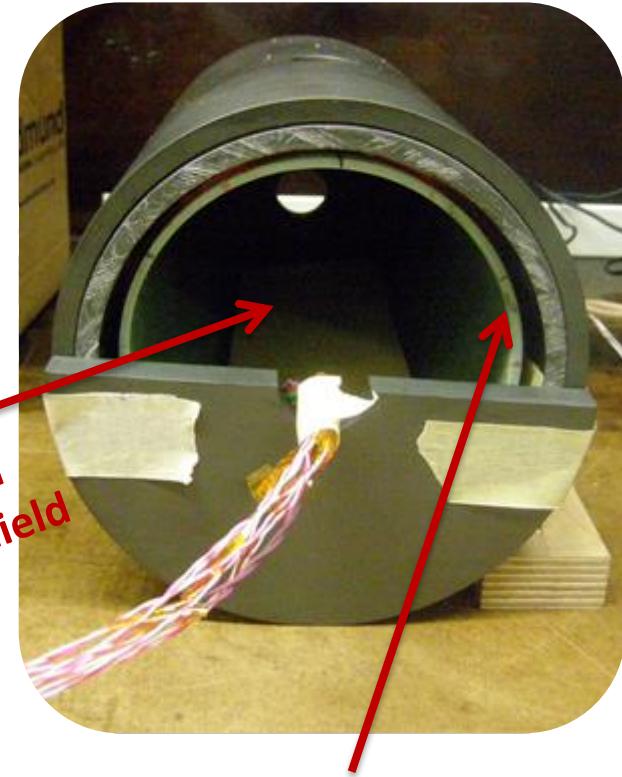
Test of AM performance



FC +AM system

Gradient coil position

One layer of mu-metal shied is not shown

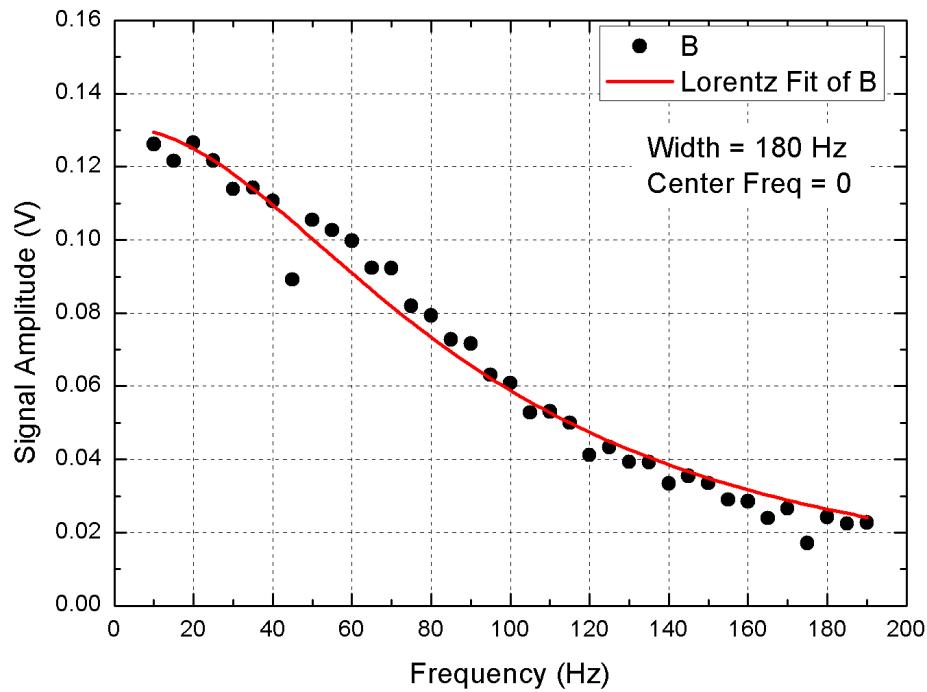


There are 3 axes compensation coil and 5 gradient compensation coil

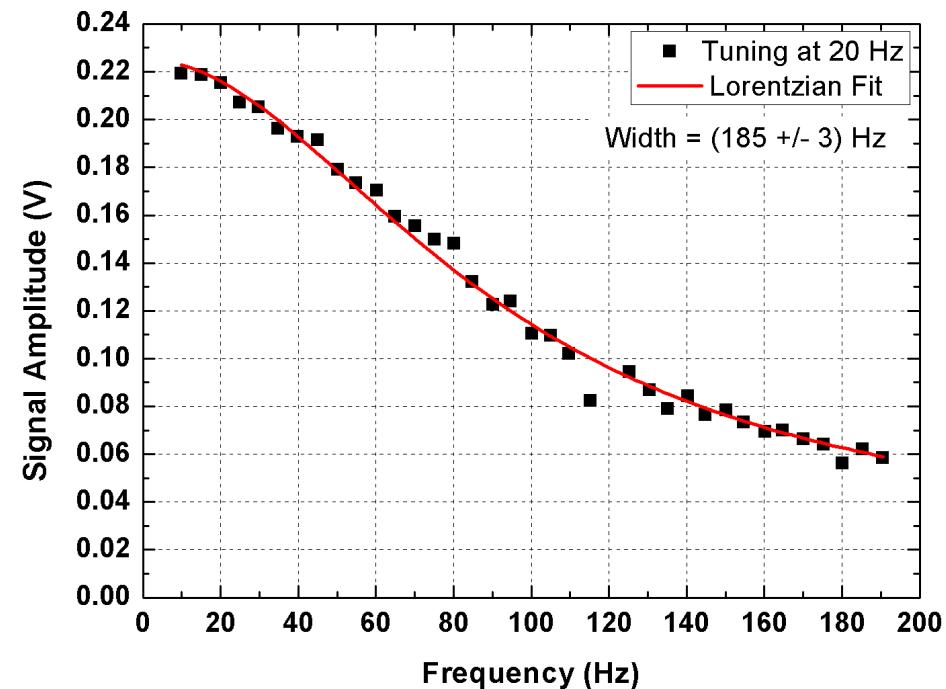
Note: these coils cannot compensate the gradient on FC!

Test of AM performance

Ideal case with shielding

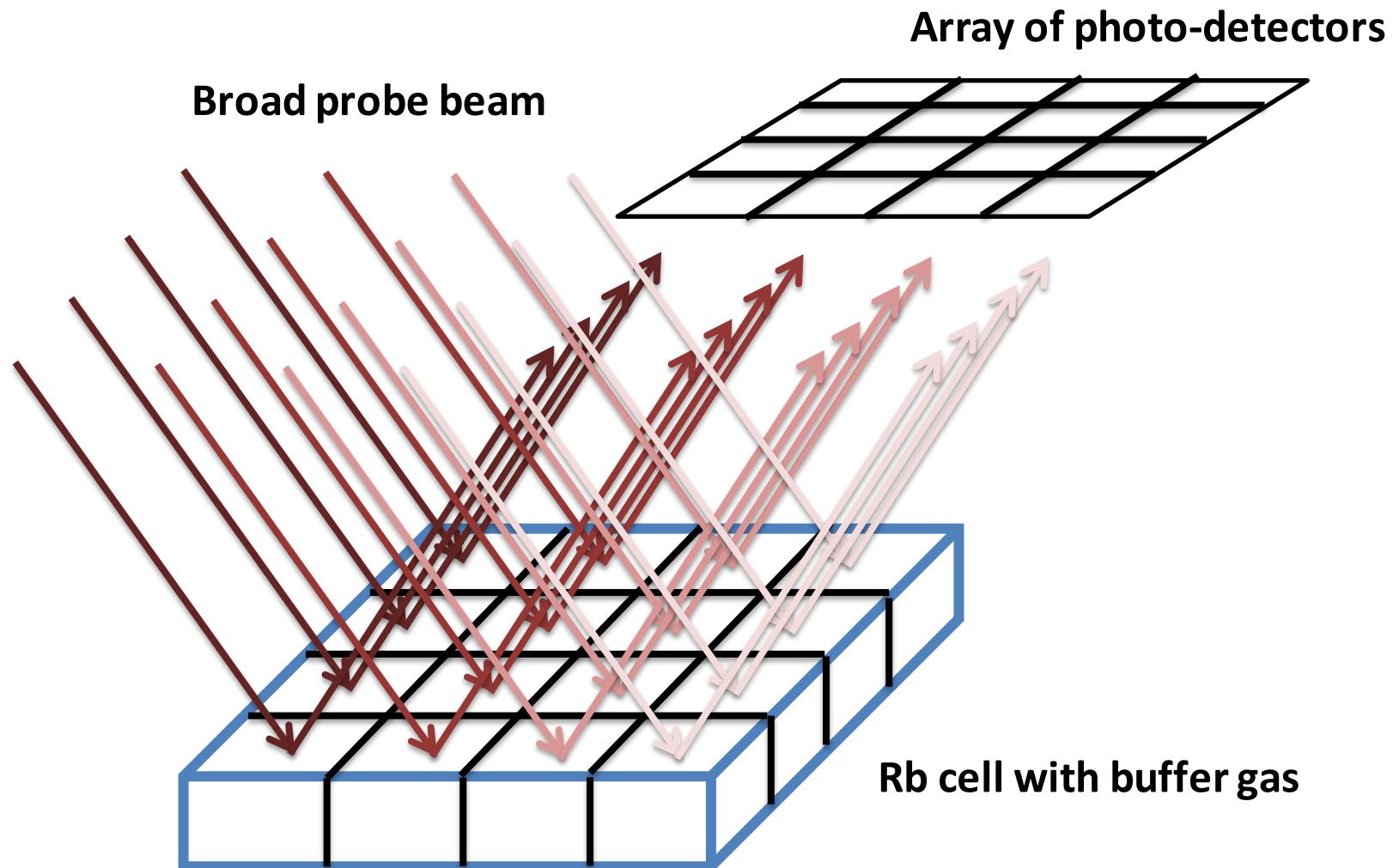


WITH FC in shielding



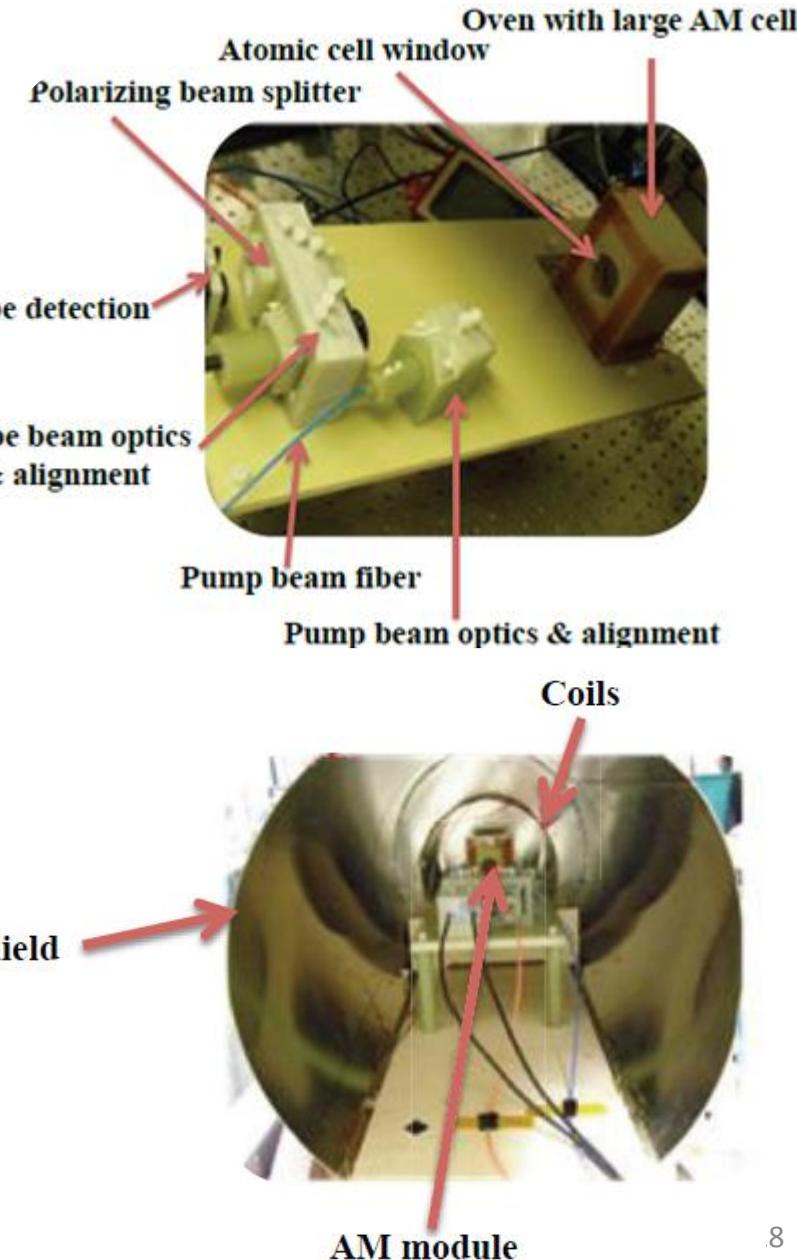
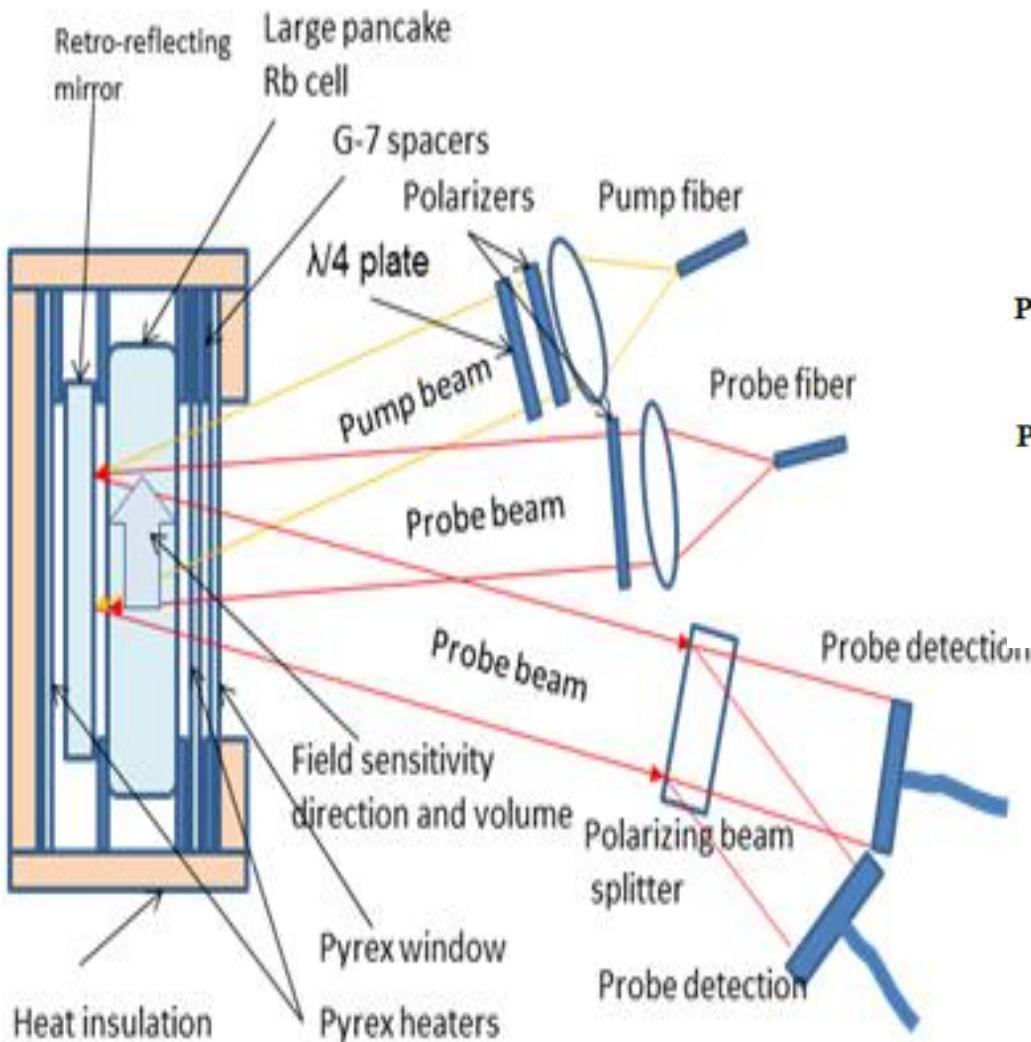
- Flux concentrator doesn't deteriorate AM's performance.
- The gradient compensation coil on the flux concentrator is important to get best AM's performance.

Idea of Multi-channel AM



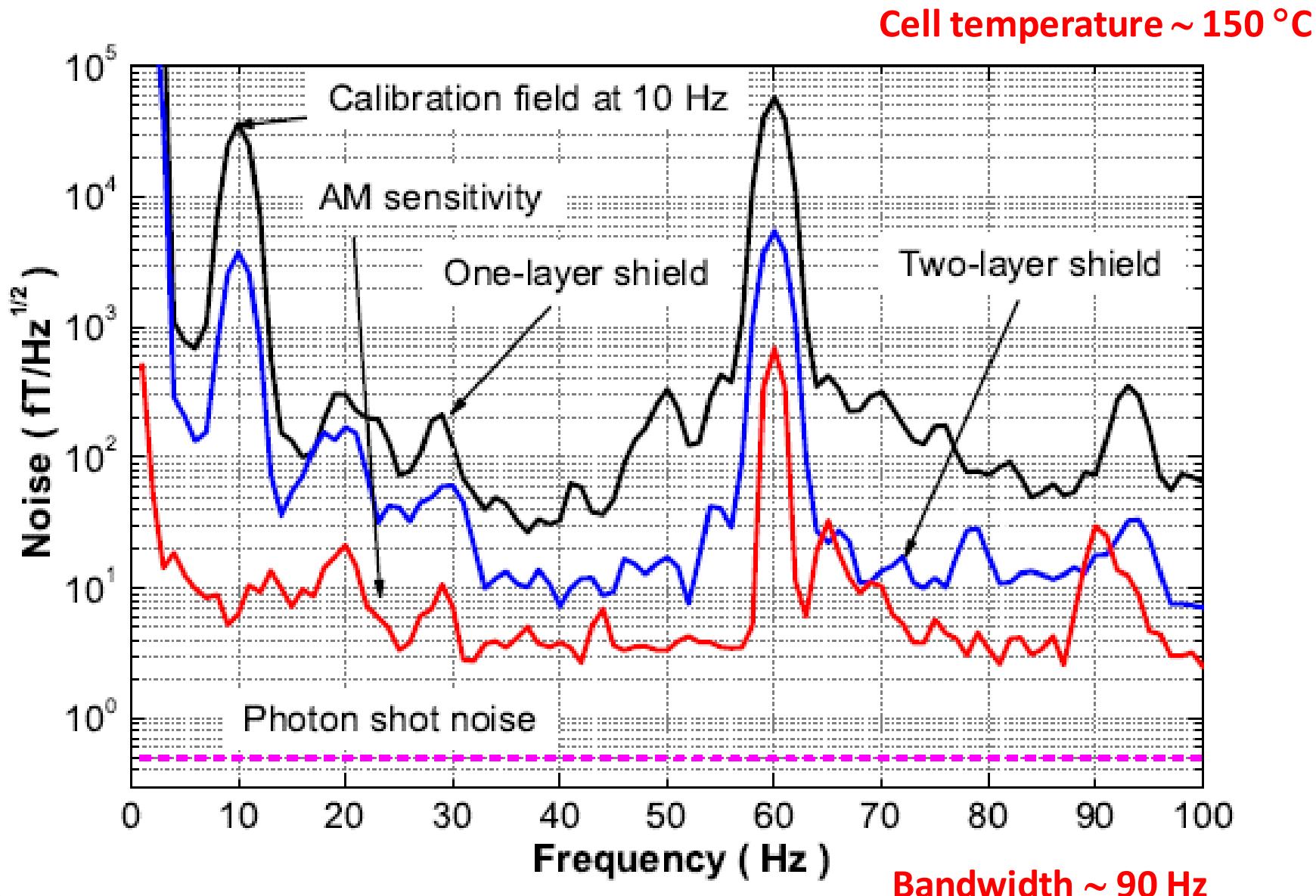
2D multi-channel is possible with Large Rb cell with a buffer gas and broad beams instead of 16 individual cells and beams.

Prototype multi-channel AM

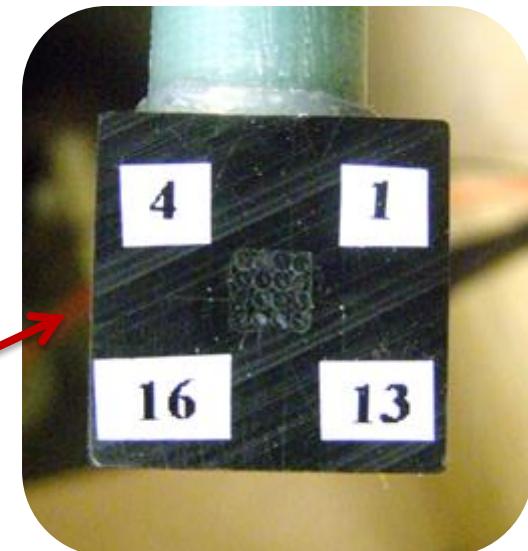
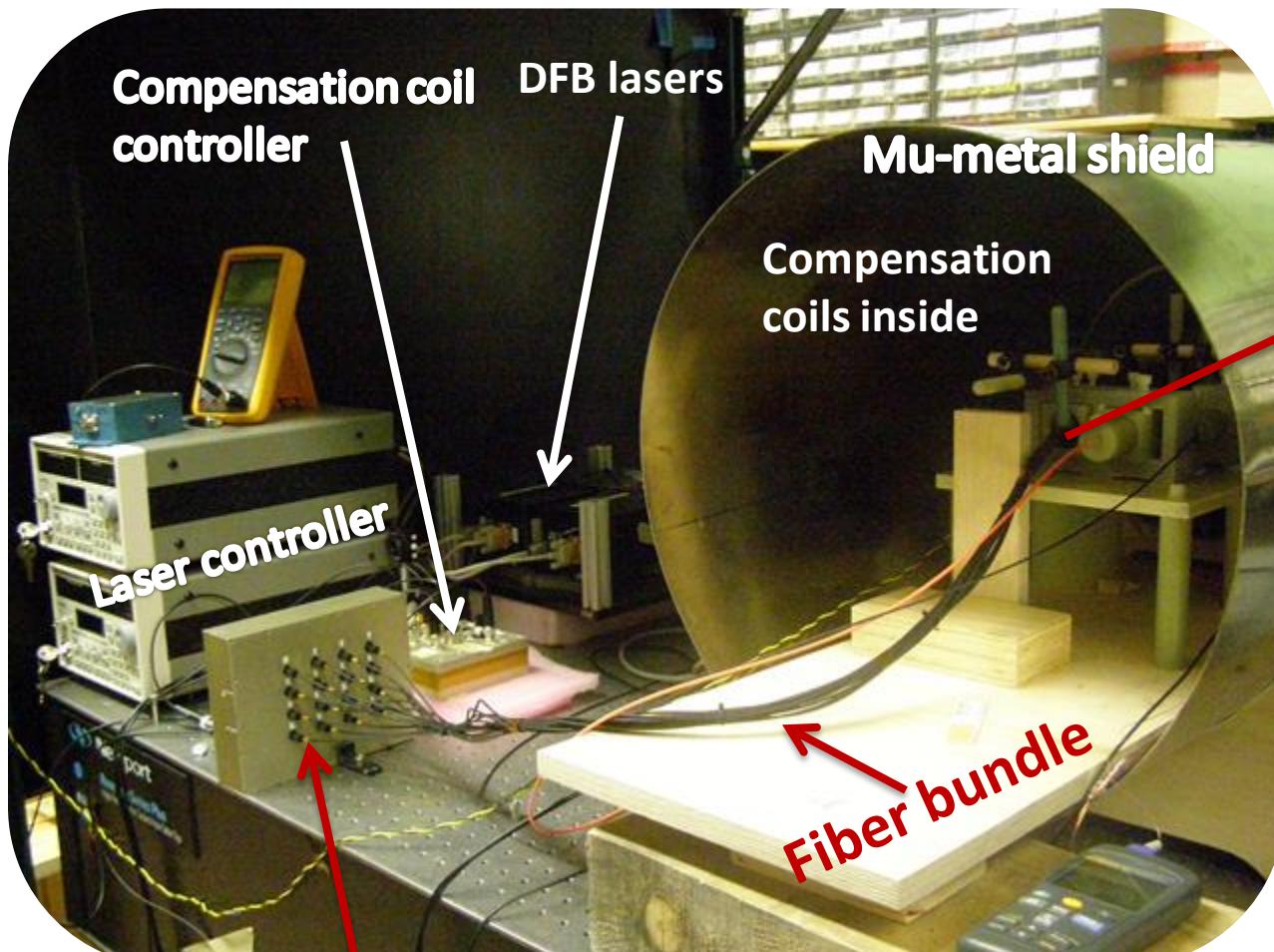


Advantage of using fibers: Flexible AM design

Feasibility proof in single channel



Configuration of multi-channel AM system

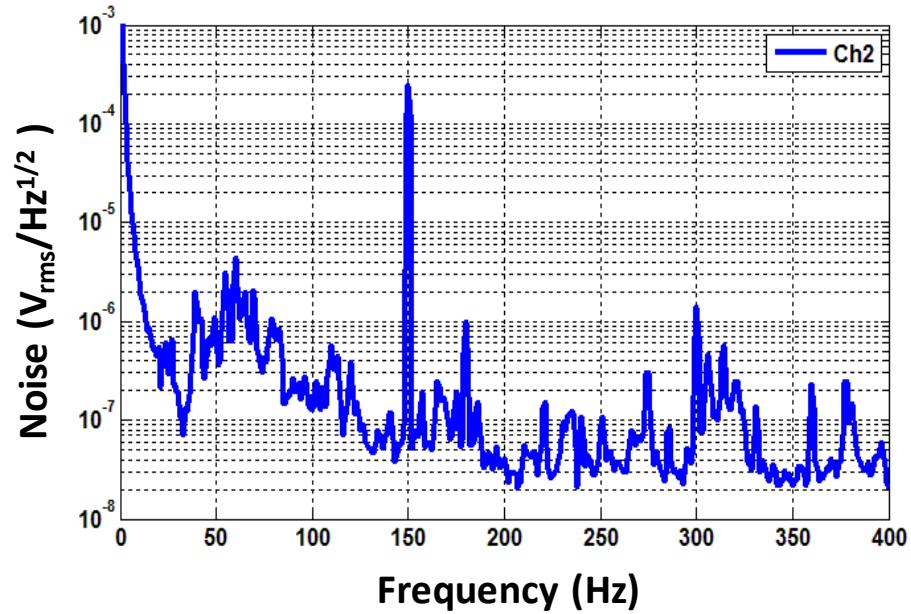
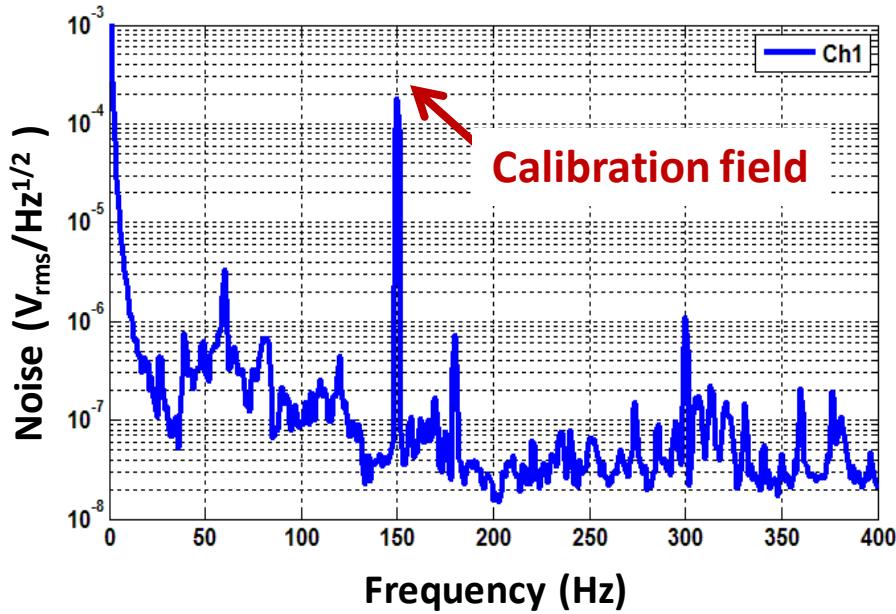


4x4 channels

16 channels photodiodes array

For shielding:
One layer of mu-metal shield
One ferrite box

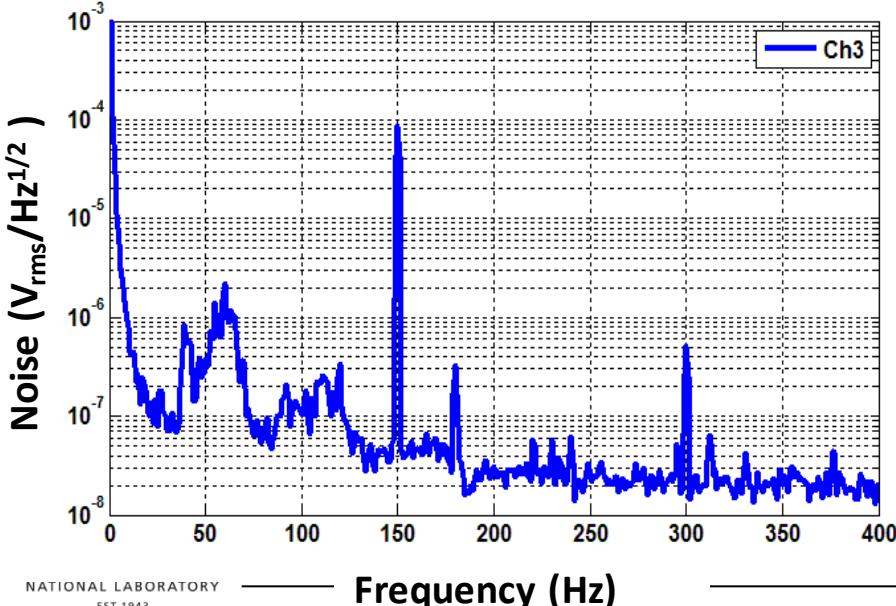
Preliminary sensitivity test



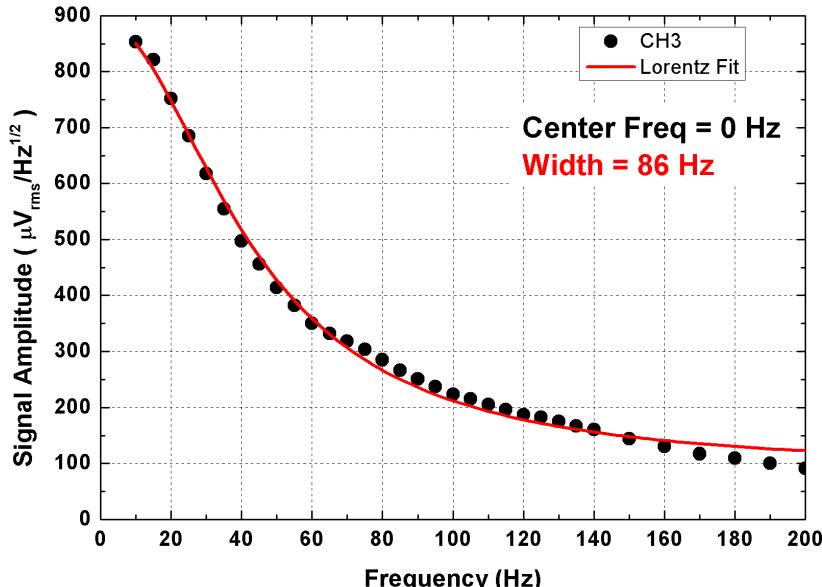
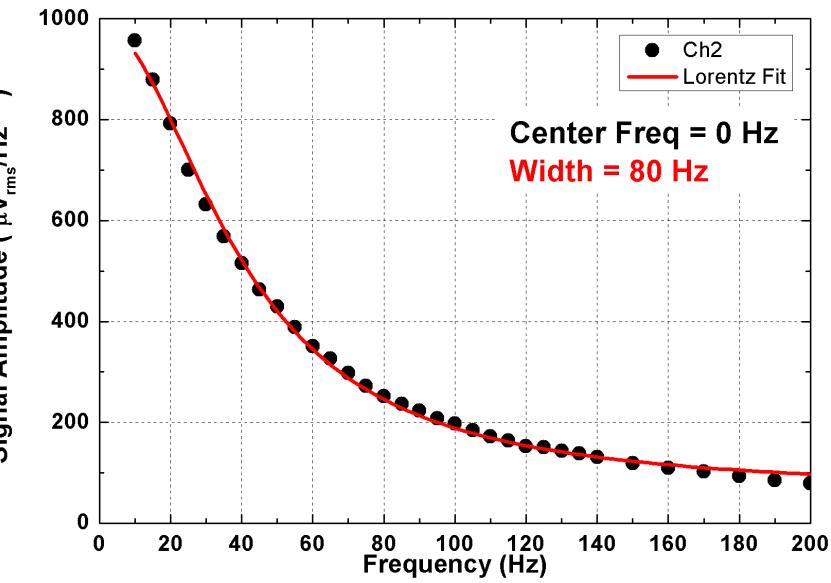
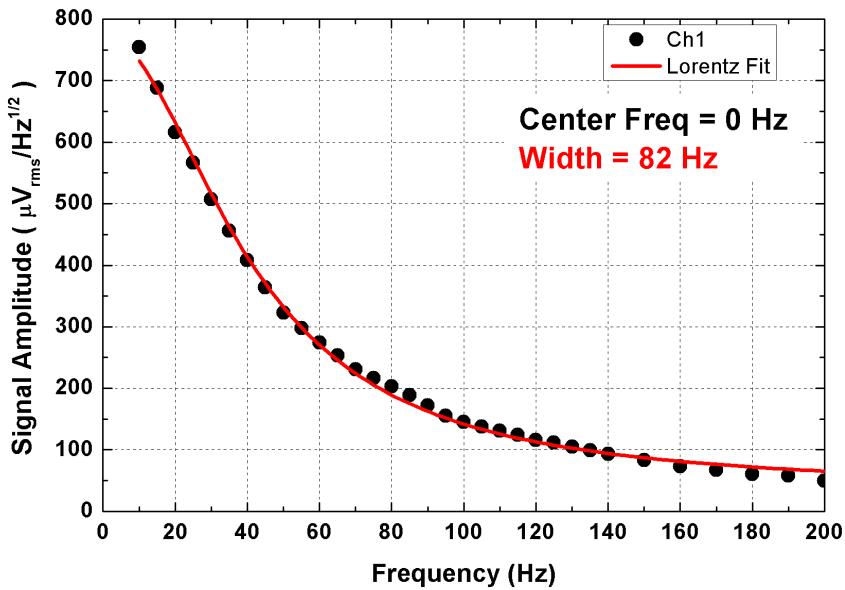
SNR of each channel : 4000 to 100

**Field sensitivity of each channel:
50 fT/Hz^{1/2} to 2000 fT/Hz^{1/2}**

**The beam is not uniform?
Intensity attenuation in fiber?**

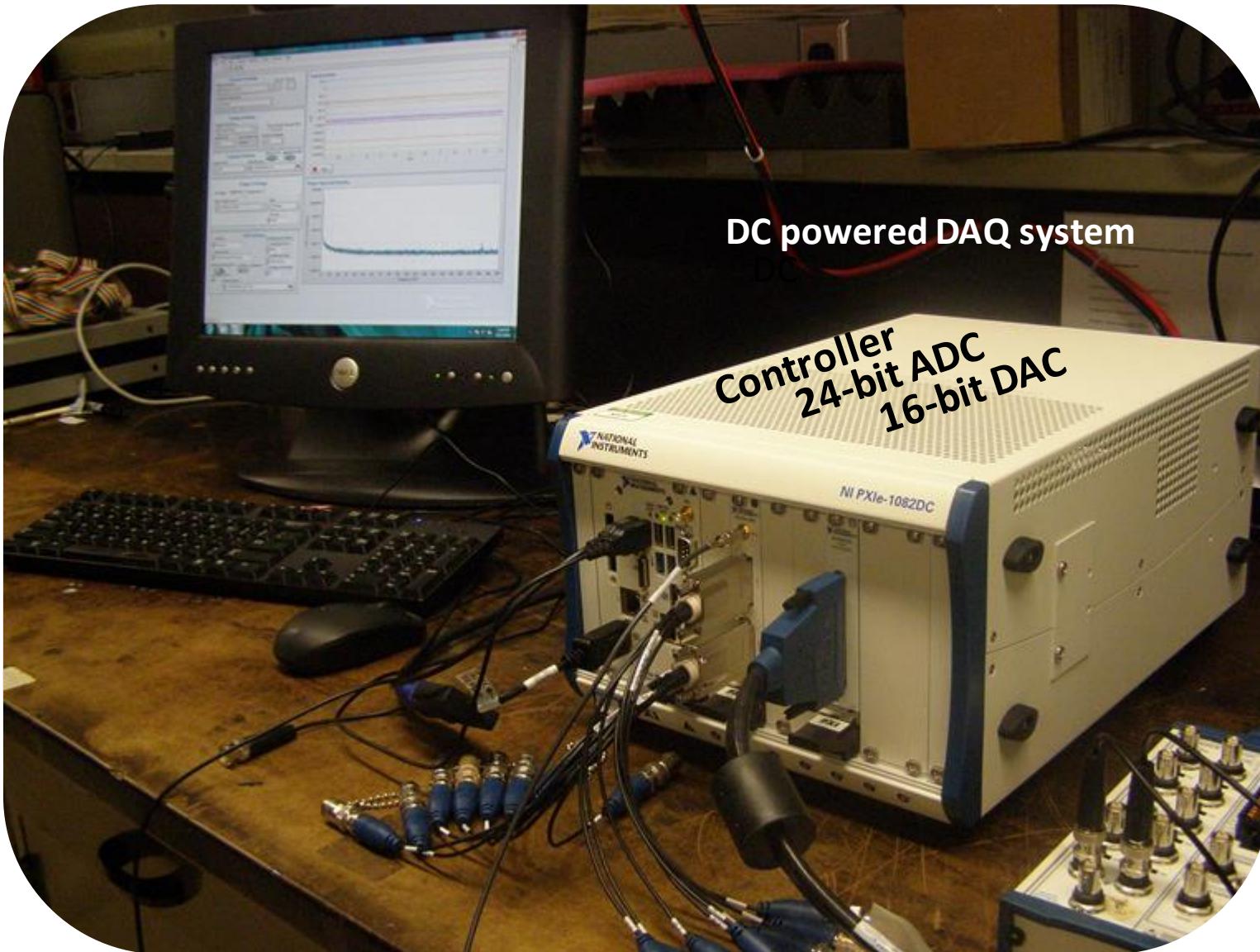


Bandwidth of each channel

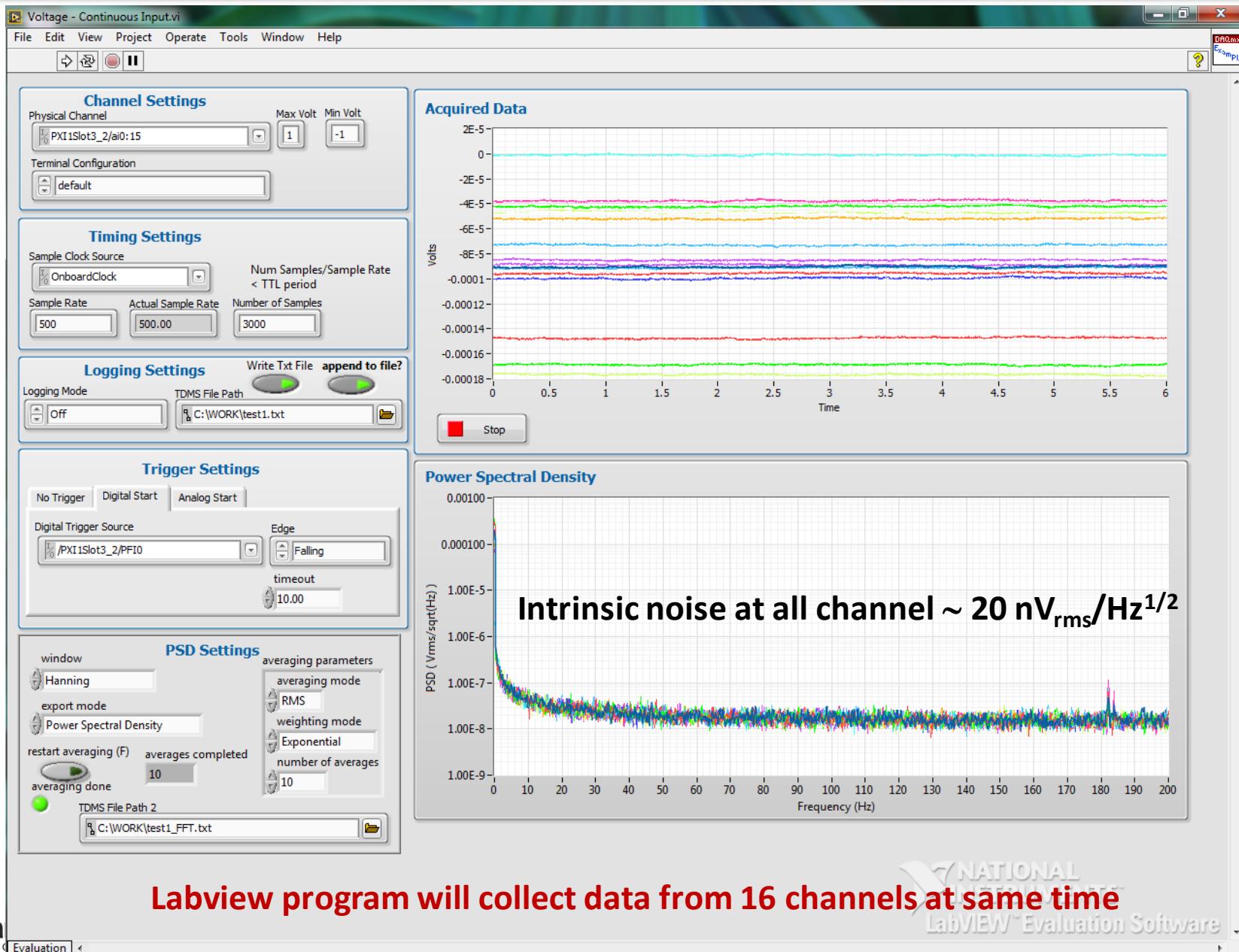


The bandwidth of each channel is good, around 80 Hz

16 channels DAQ system



16 channels DAQ system



future work

- Application of the FC+AM system to detection of magnetic nanoparticles which in turn are very important for detection of target molecules in national security, medical diagnostics, and other application areas.
 - Better AM will be delivered in a week
- Improvement of the multi-channel AM system and keep checking its performance
 - Place a small coil on the vapor cell and measure the field distribution with 16 channels at same time.
 - Check the performance of a 4×4 photodiode array