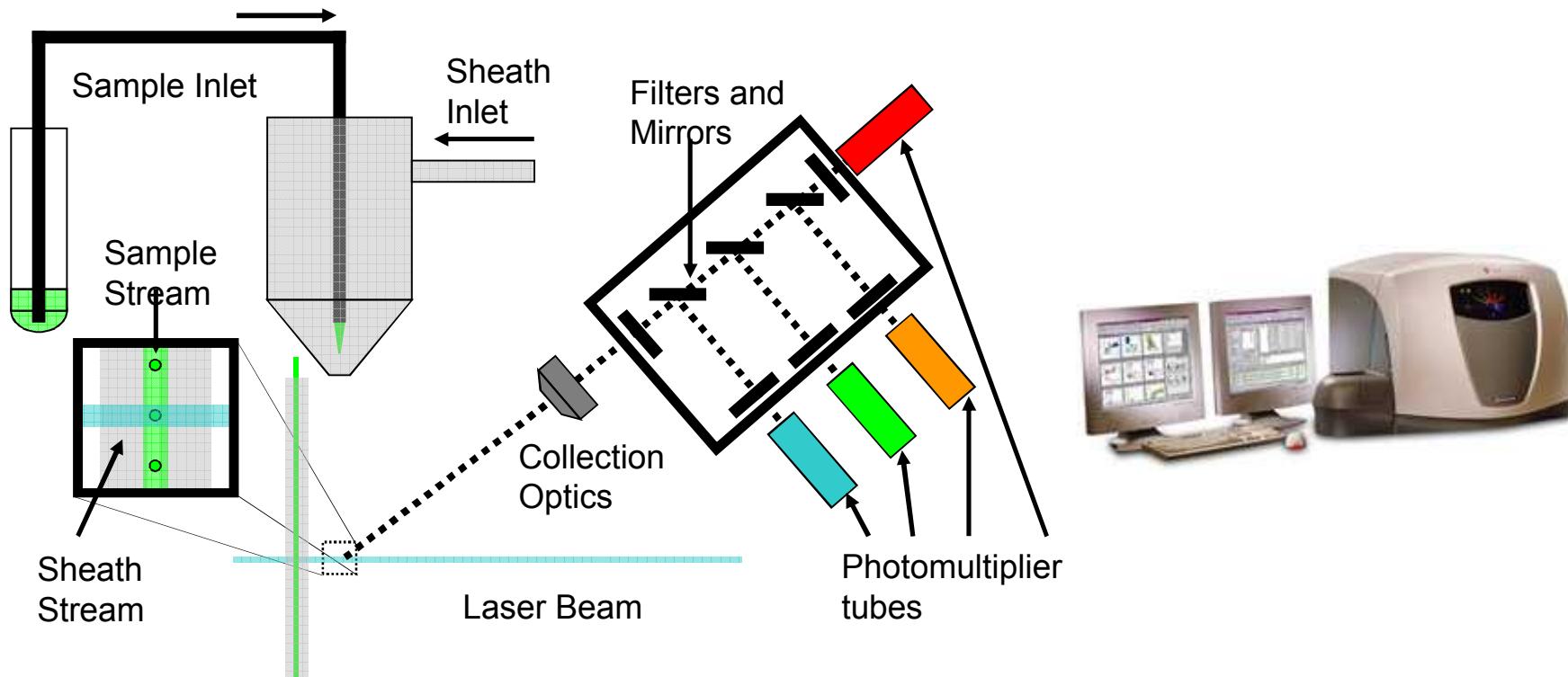


Microfluidics and Microacoustics for Miniature Flow Cytometry

**Surendra K. Ravula, Darren W.
Branch, Jennifer Sigman, Paul G.
Clem, Igal Brener**

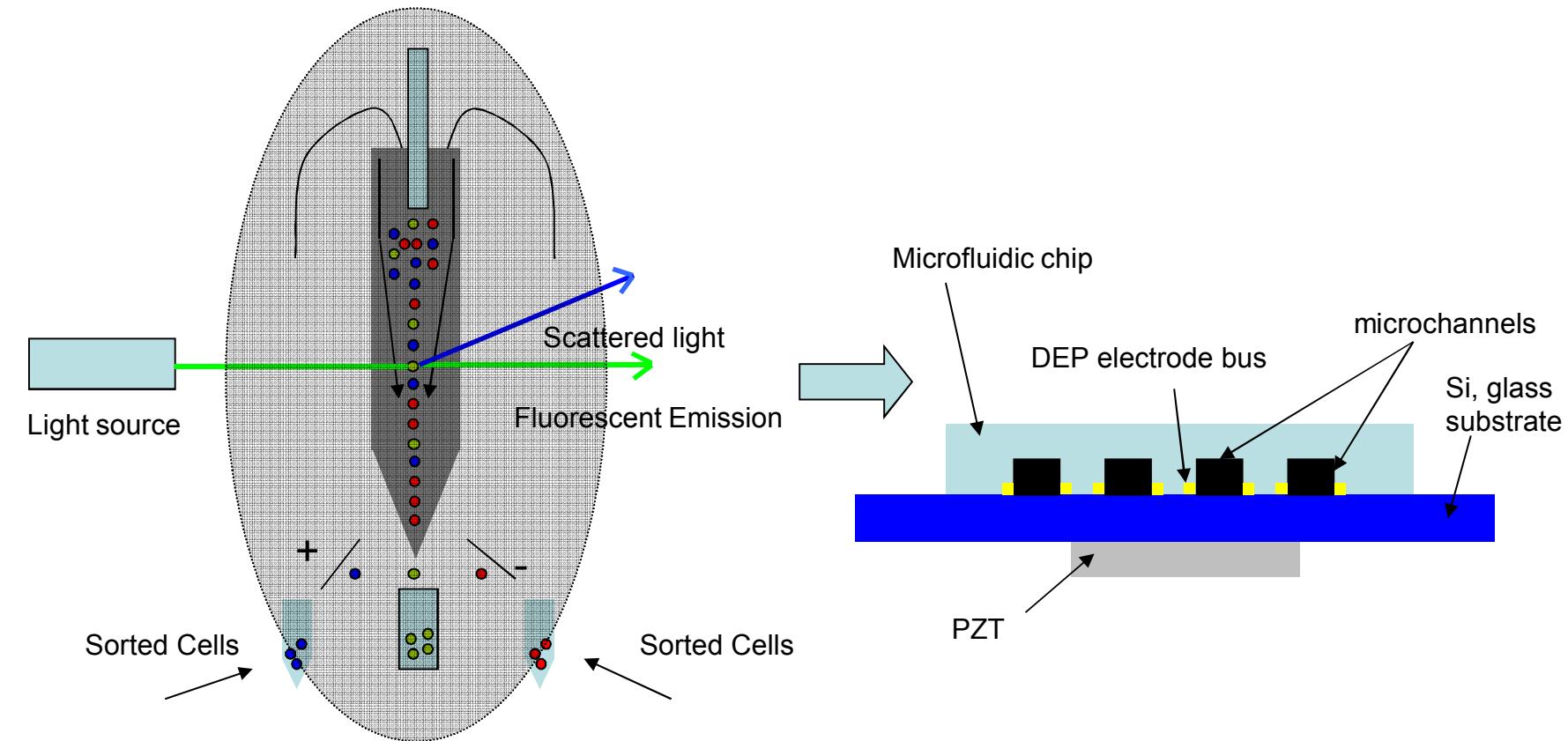
Sandia National Labs, Albuquerque, NM

Introduction to Flow Cytometry

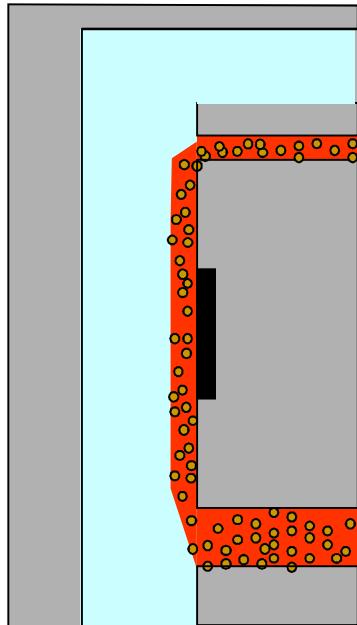


- An analysis tool for understanding chemical and physical properties about biological cells
- A sheath flow focuses cells into a single file line
- A laser through scattering or fluorescence generates a signal that gives a signature of the cell.

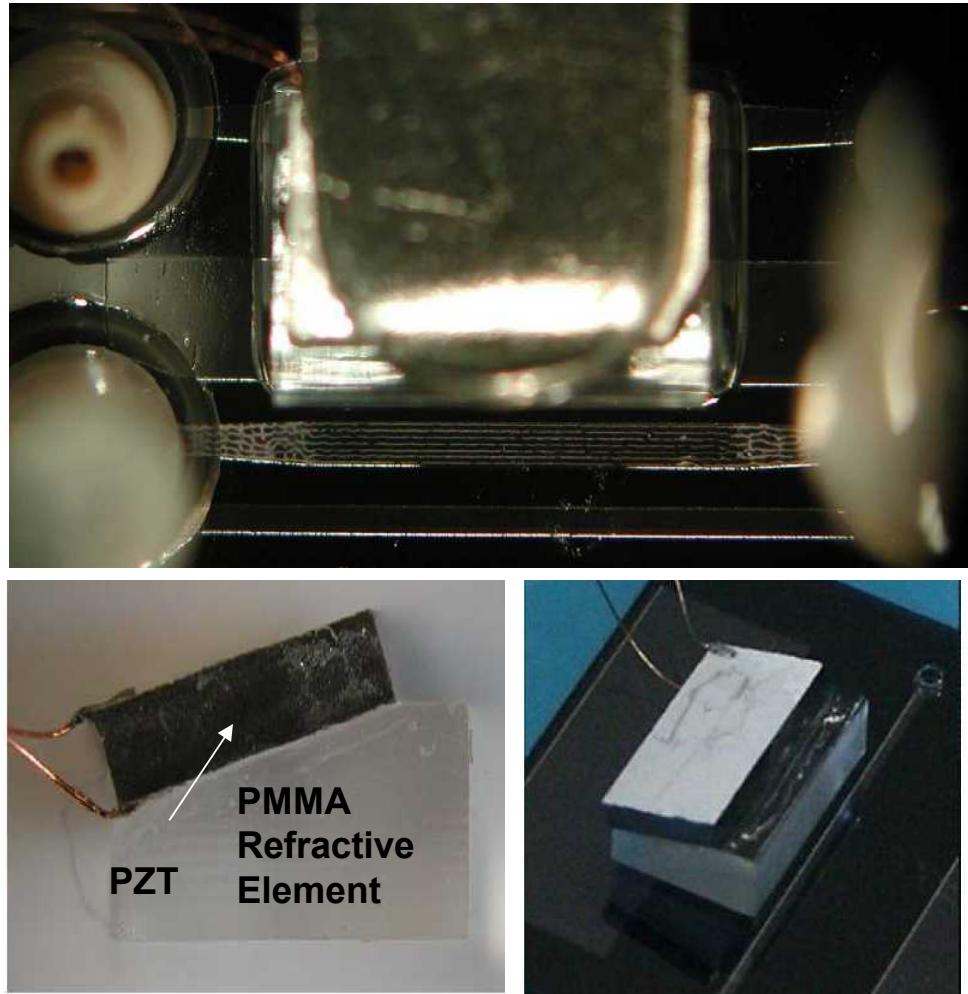
Concept



Background

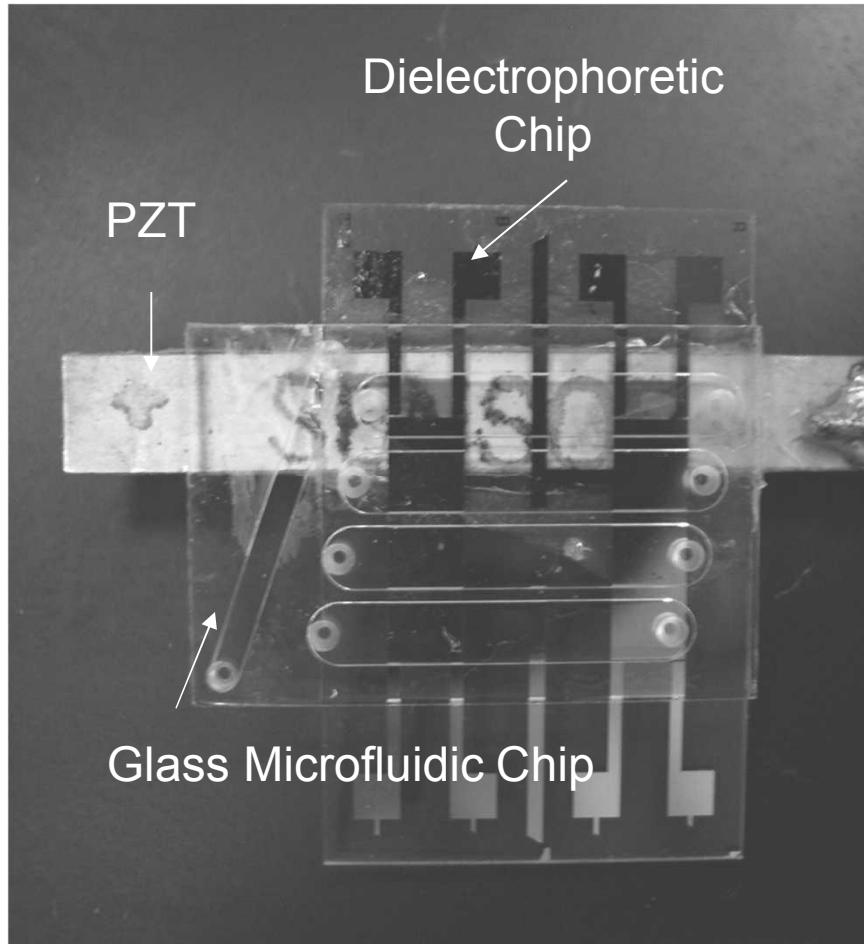


Hawkes et al. Lab Chip. 2004

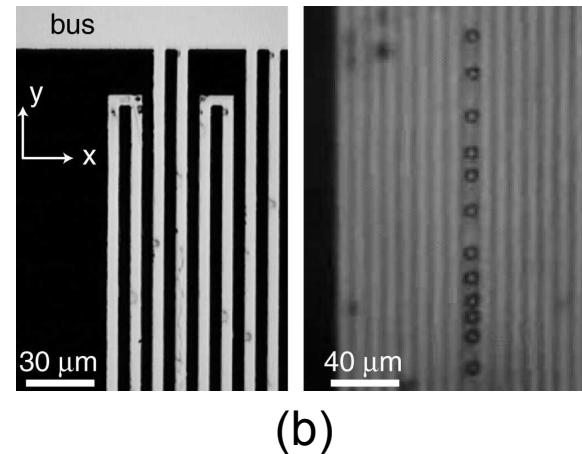


Wiklund, Lab Chip 2006

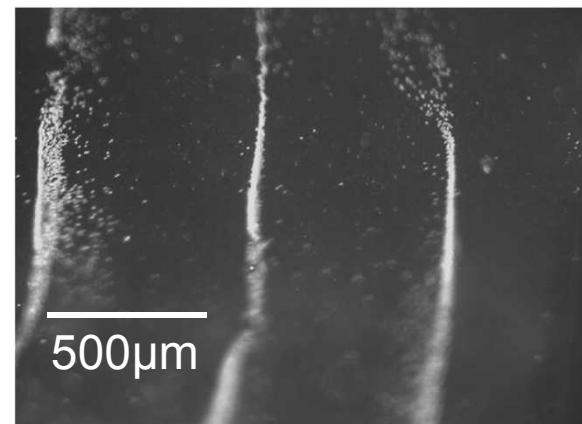
Fabricated Systems



(a)



(b)



(c)

Modeling Paradigm

- 1-D Transmission Line model based on Dion et. al., 1997 in *IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control*

$$Z_e = \frac{1}{j\omega C_0} + \frac{h_{33}^2}{\omega^2 A} \left(\frac{2[\cosh(\gamma a) - 1]Z_f + (Z_L + Z_R) \sinh(\gamma a)}{(Z_L Z_R + Z_f^2) \sinh(\gamma a) + Z_f (Z_L + Z_R) \cosh(\gamma a)} \right)$$

Where C_o is the clamped electrical capacitance, h_{33} is the piezoelectric stress constant, A is the surface area of the transducer, γ is the propagation function, Z_L is the impedance seen to the left, Z_R is the impedance seen to the right, Z_f is the transducer impedance, and a is the transducer thickness.

- Use the impedance addition rule to add impedances seen to the left or right for a film stack

$$Z^*(\omega, x) = Z_i^*(\omega) \frac{Z_{LD}^*(\omega) \cosh[\gamma(L-x)] + Z_i^*(\omega) \sinh[\gamma(L-x)]}{Z_i^*(\omega) \cosh[\gamma(L-x)] + Z_{LD}^*(\omega) \sinh[\gamma(L-x)]}$$

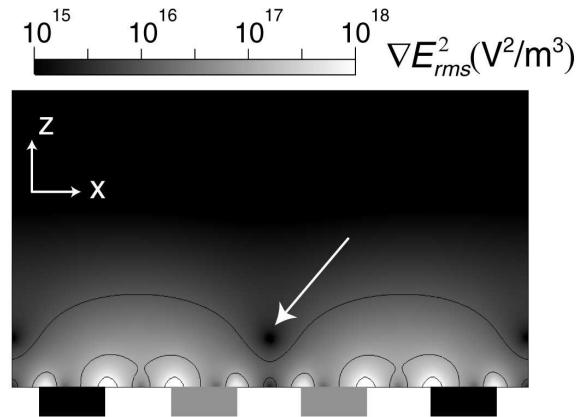
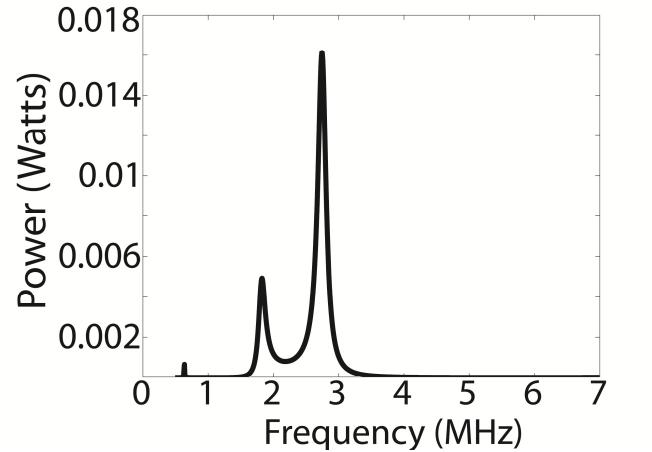
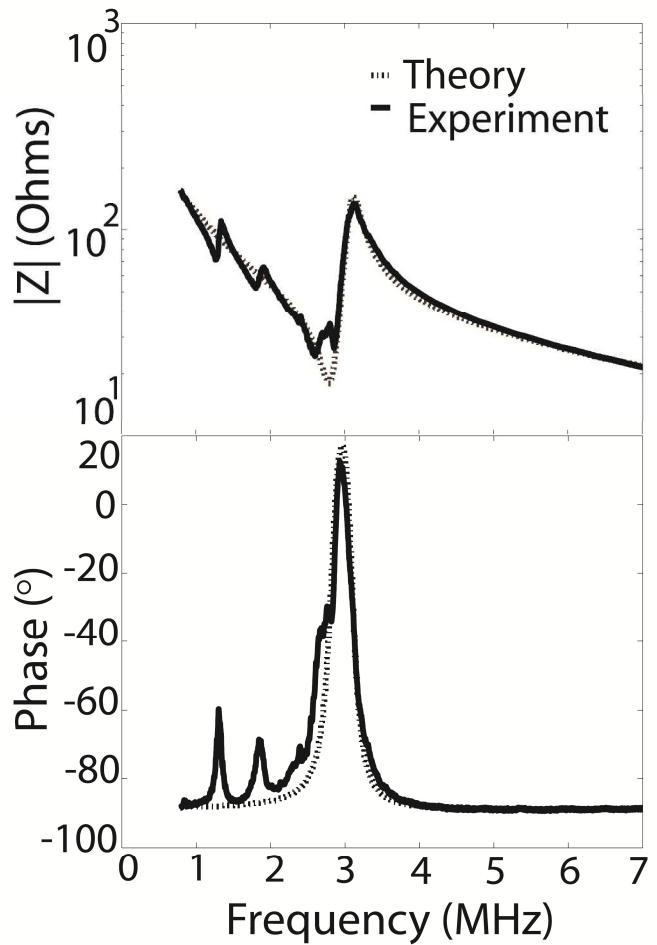
Z_i is the intermediate layer impedance, Z_{LD} is the impedance of the load, and L is the thickness of the intermediate layer

Slide 6

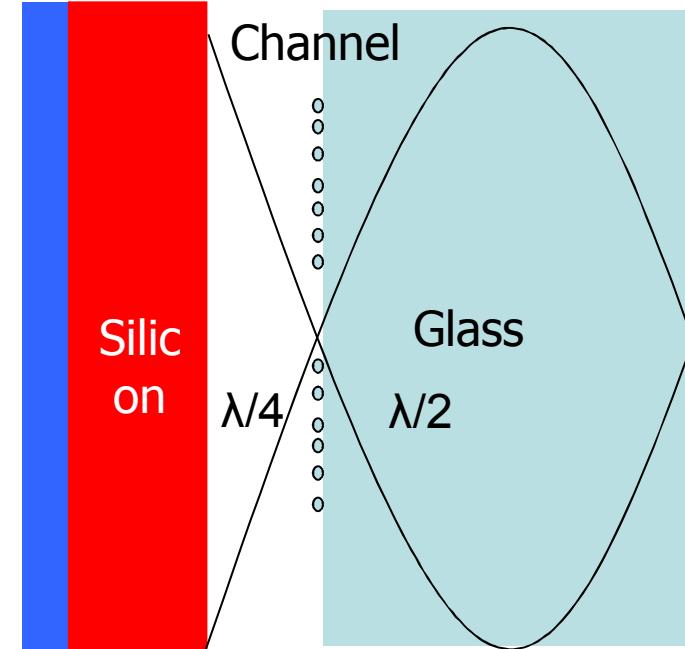
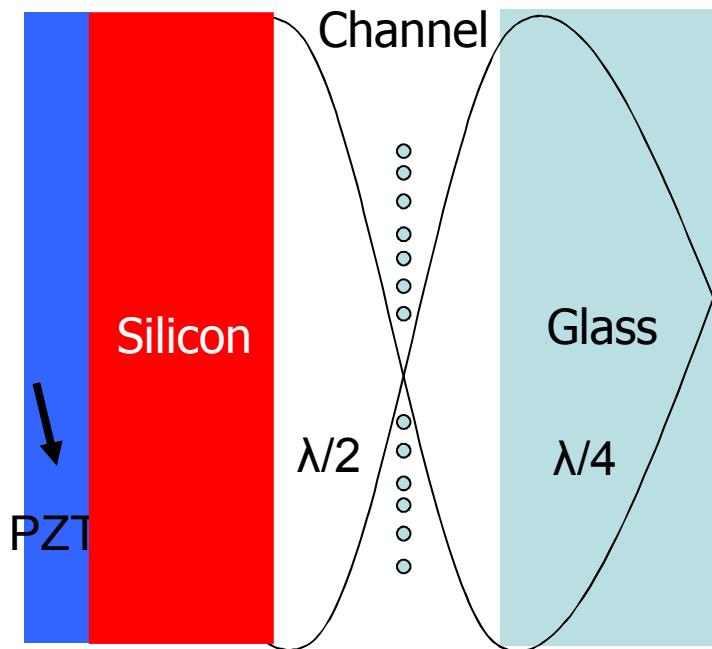
SKVR1 transducer mispelled

Surendra Ravula, 3/2/2007

Modeling of the System



Positioning of streams within the channel



Focusing Characteristics ($\lambda/2$ cavity, $\lambda/4$ roof)

Bead focusing characteristics during PZT actuation (n=4)

Cavity height is 240 μ m.

Frequency of Operation (MHz)	Amplitude of Applied Voltage (V) (peak-to-peak)	Number of Streams	Average Stream Width (μ m)	Average Levitation Height (μ m)
1	6.17	1	26 \pm 2	99 \pm 3
1.59	8.24	2	15 \pm 3	110 \pm 2
2.13	9.32	3	6 \pm 1	119 \pm 7

Values are mean \pm standard error of measurement.

Cell positioning characteristics during DEP actuation (n=4)

Frequency of Operation (MHz)	Average “Pearl chain” Width (μ m)	Number of “Pearl chains”	Average Levitation Height (μ m)
1	11 \pm 2	8 \pm 3	5 \pm 3
1.3	10 \pm 1	14 \pm 3	8 \pm 2
2.1	15 \pm 3	4 \pm 1	12 \pm 7

Values are mean \pm standard error of measurement.

Focusing Characteristics ($\lambda/4$ cavity, $\lambda/2$ roof)

Bead focusing characteristics during PZT actuation (n=4)

Cavity height is 240 μ m.

Frequency of Operation (MHz)	Amplitude of Applied Voltage (V) (peak-to-peak)	Number of Streams	Average Stream Width (μ m)	Average Levitation Height (μ m)
1	9.2	1	15 \pm 3	234 \pm 3
2.54	12.87	2	30 \pm 3	229 \pm 3
3.12	14.92	3	6 \pm 1	219 \pm 7

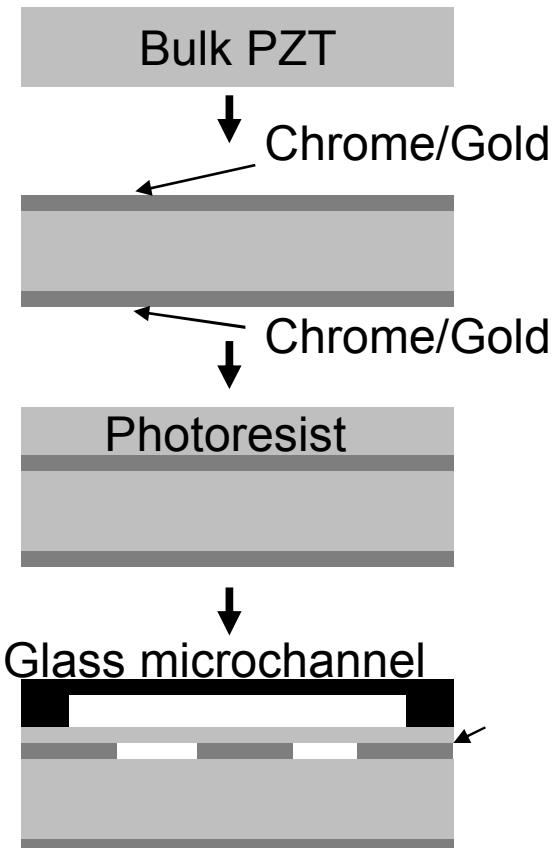
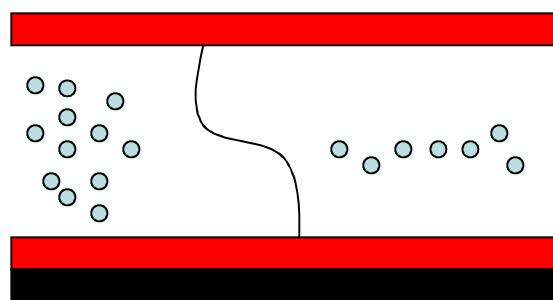
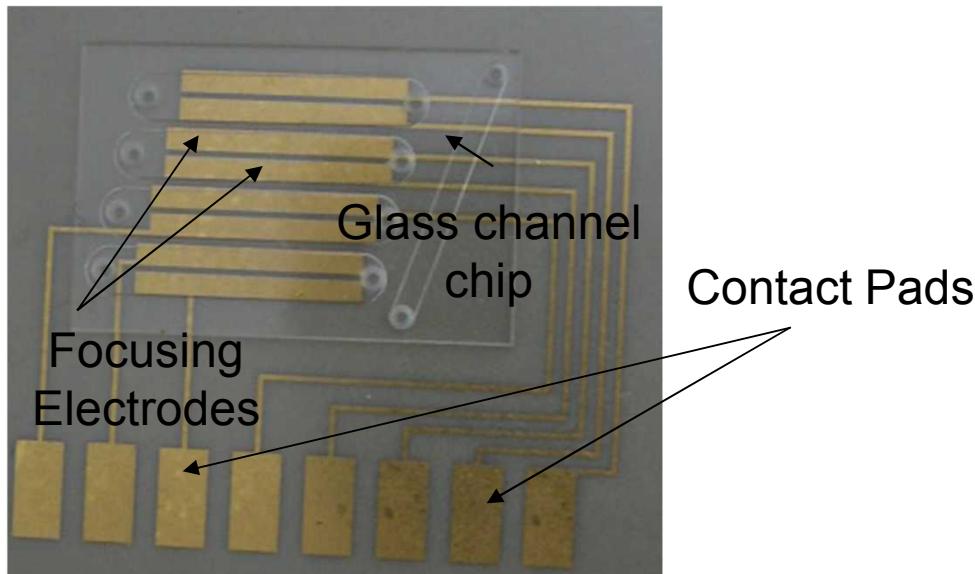
Values are mean \pm standard error of measurement.

Cell positioning characteristics during DEP actuation (n=4)

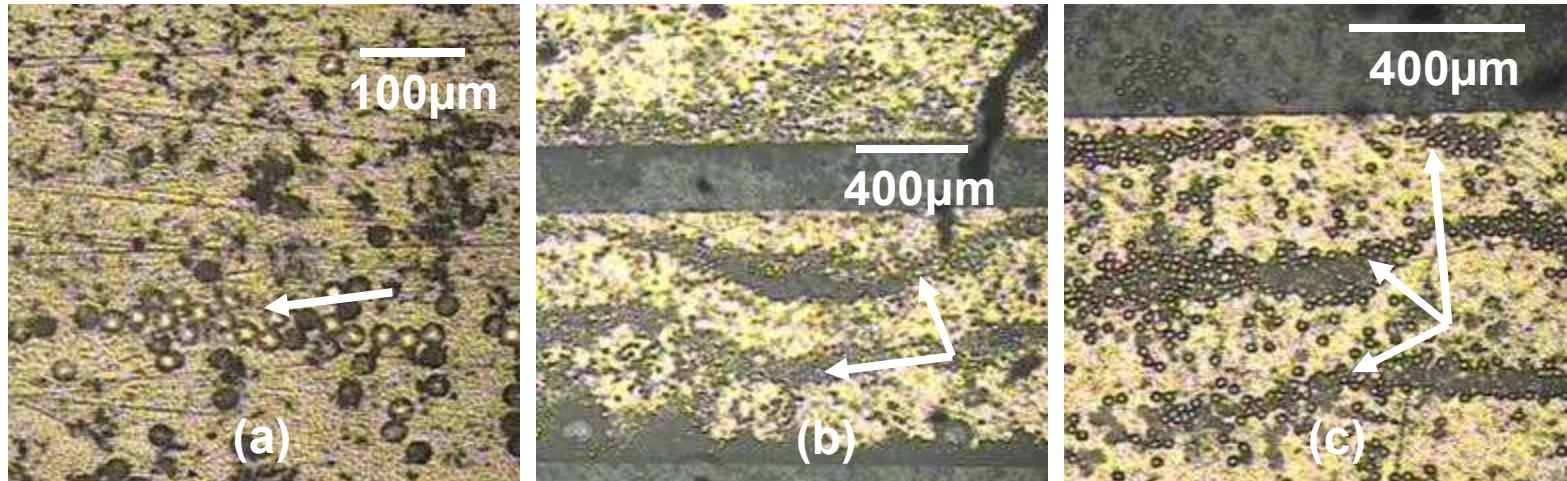
Frequency of Operation (MHz)	Average “Pearl chain” Width (μ m)	Number of “Pearl chains”	Average Levitation Height (μ m)
1	11 \pm 2	8 \pm 3	5 \pm 3
1.3	10 \pm 1	14 \pm 3	8 \pm 2
2.1	15 \pm 3	4 \pm 1	12 \pm 7

Values are mean \pm standard error of measurement.

Planar Acoustic Transducers

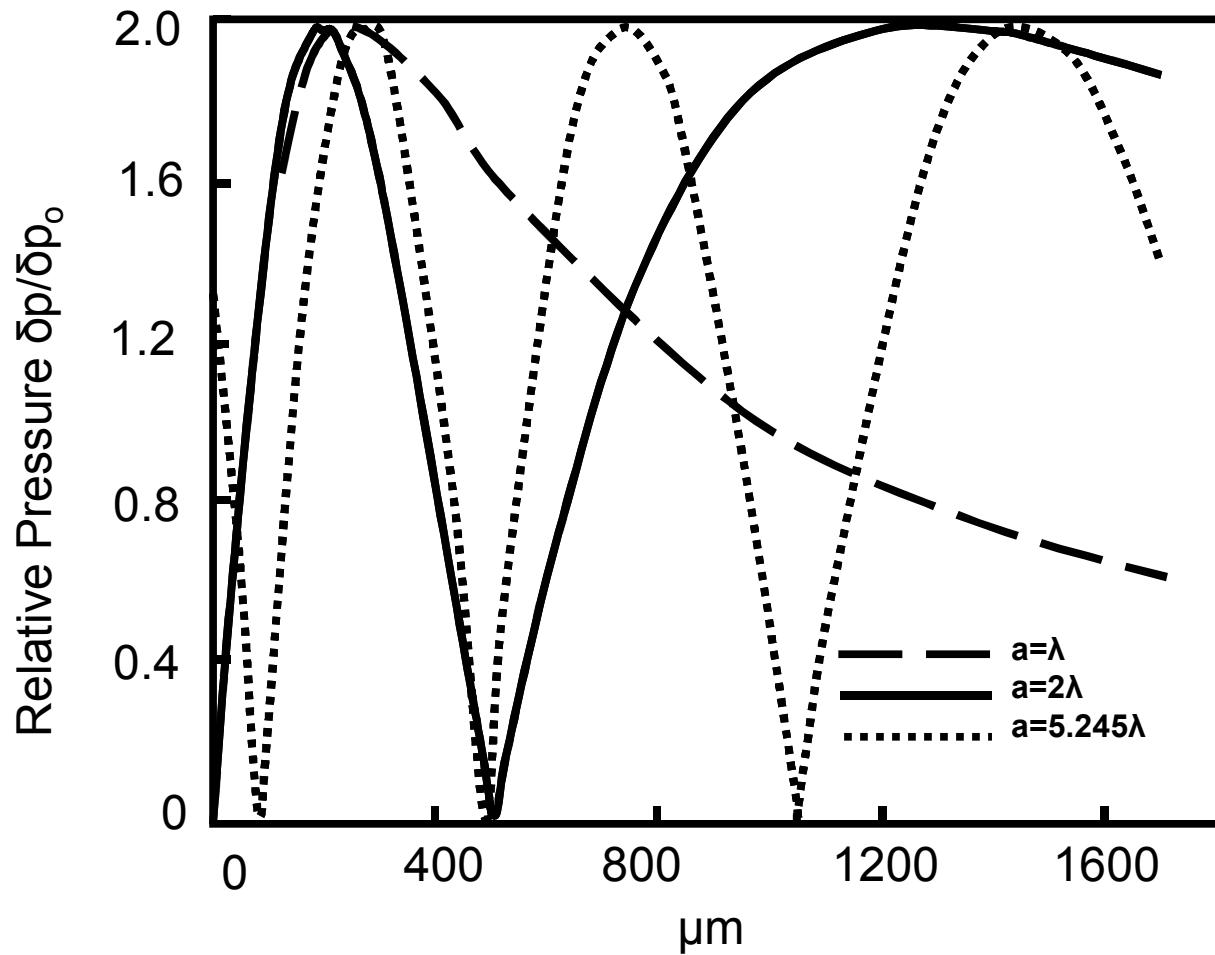


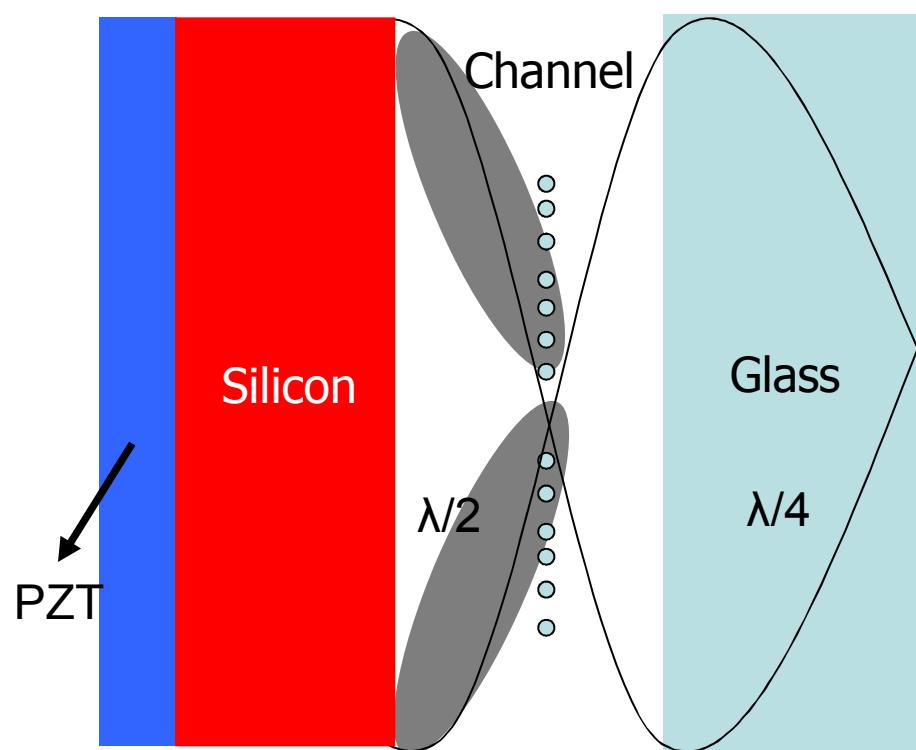
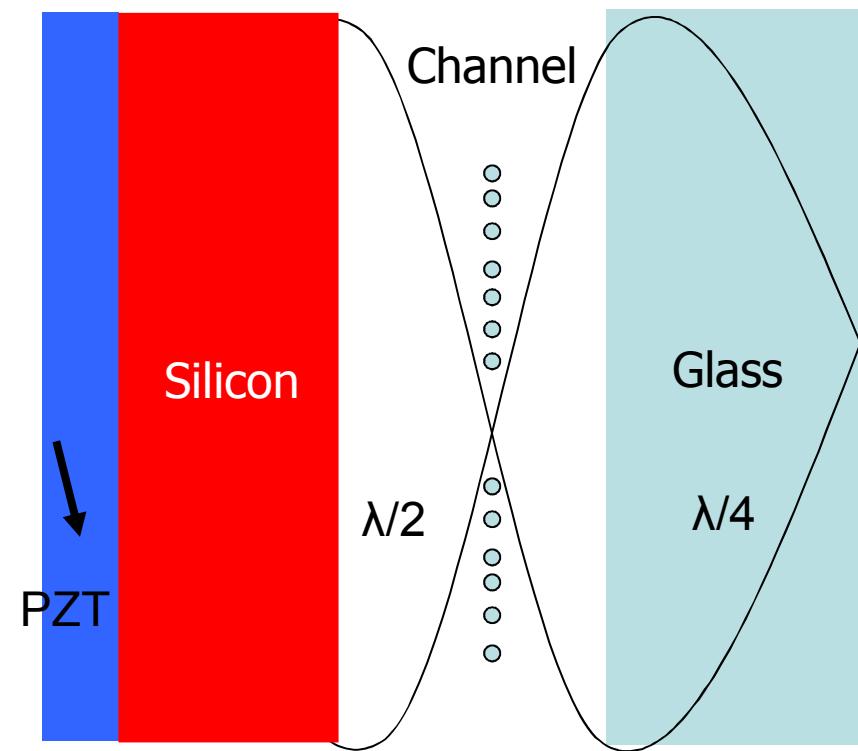
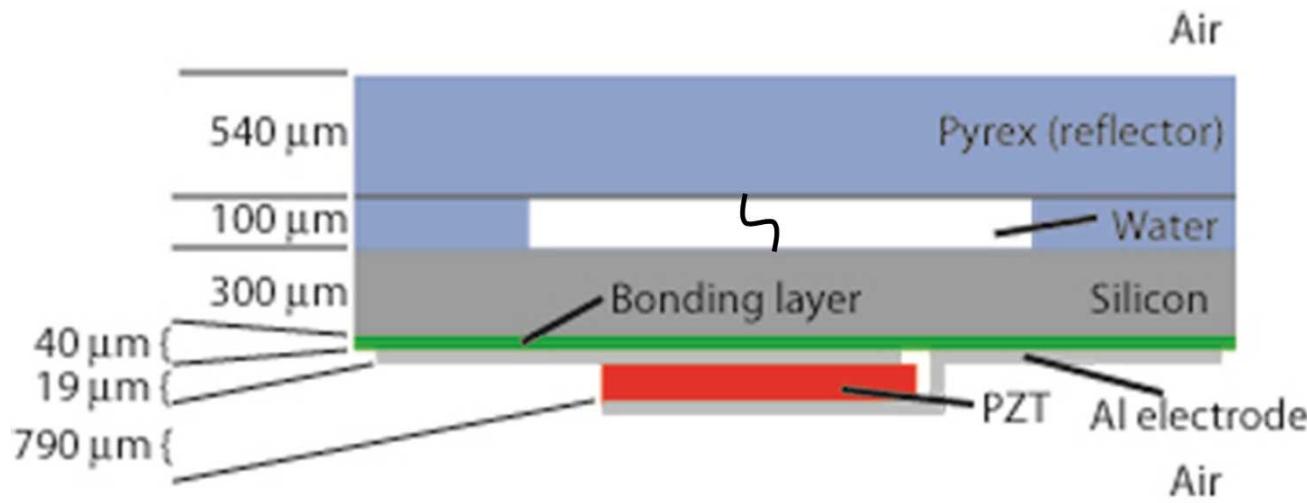
Focusing of Beads in Channels



Acoustic streams (arrows) of beads due to lateral focusing in a microchannel. The PZT transducer was driven with a 10Vp-p sinusoidal signal. The frequency of actuation was 3.1MHz for (a), 3.7MHz for (b), and 4.2MHz for (c).

Near-Field Radiation Pressure





Summary

- Integrated acoustic electrodes in a microfluidic system
- Detailed model allows for device design and analysis
- Experimental results show that beads can be manipulated in microfluidic channels when frequency is tuned and when the geometry of the system is changed