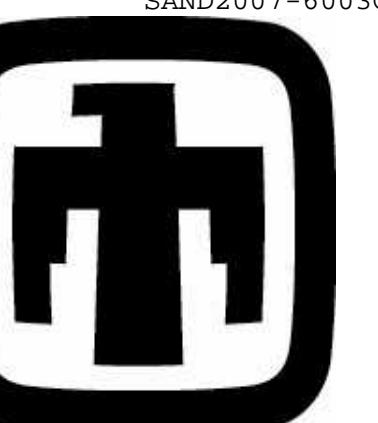


On-Chip Biological Sample Preparation System using Acoustic Lysis

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Introduction

- At present biological sensors and systems lack automated front-end handling to prepare samples prior to detection.
- Consequently, samples must be manually prepared requiring additional time, effort, and equipment, often reducing the effectiveness of microsystem solution.
- The lack of efficient front-end sample handling technology impacts a broad range of biosensor systems, ultimately limiting their portability, reducing sample throughput, and causing detection variability.

Approach

- Acoustic methods are a powerful approach to manipulate biological samples in high throughput applications.
- Using Bulk Acoustic Waves (BAWs) and fluid coupled Surface Acoustic Waves (SAWs), cells can be lysed to release their intracellular components such as specific proteins and DNA.
- Two microlysing methods were compared with a commercial instrument (Misonix) on their efficacy to lyse *E. coli* (K-12) cells.
- Microlysing methods were developed as flow-through assays for subsequent analysis using a microchannel to extract DNA.

Theory

BAW: 1-D Transmission Line Model:

$$Z_e = \frac{1}{j\omega C_o} + \frac{h^2}{\omega^2 A} \cdot \frac{2(\cosh(\gamma a) - 1)Z_o + (Z_r + Z_l)\sinh(\gamma a)}{(Z_r Z_l + Z_o^2)\sinh(\gamma a) + Z_o(Z_r + Z_l)\cosh(\gamma a)}$$

$$h = \frac{e_{33}}{\varepsilon_{33}}$$

$$\alpha = \alpha_o \left(\frac{f}{f_o} \right)^n$$

$$\gamma = \alpha_o \left(\frac{f}{f_o} \right)^n + \frac{j\omega}{v_f}$$

$$Z(\omega) = \frac{j\omega\rho}{\gamma}$$

Z_e : Electrical Impedance of Transducer

h : stress piezoelectric constant

Z_o : Film Impedance $Z_o(\omega, \rho, \alpha, v_f)$

Z_r : Impedance seen to the left

Z_l : Impedance seen to the right

C_o : clamped electrical capacitance

α : attenuation constant (Nepers/m)

v_f : Propagation velocity

γ : propagation function $\gamma(\omega, \alpha, v_f) = \alpha + j\beta$

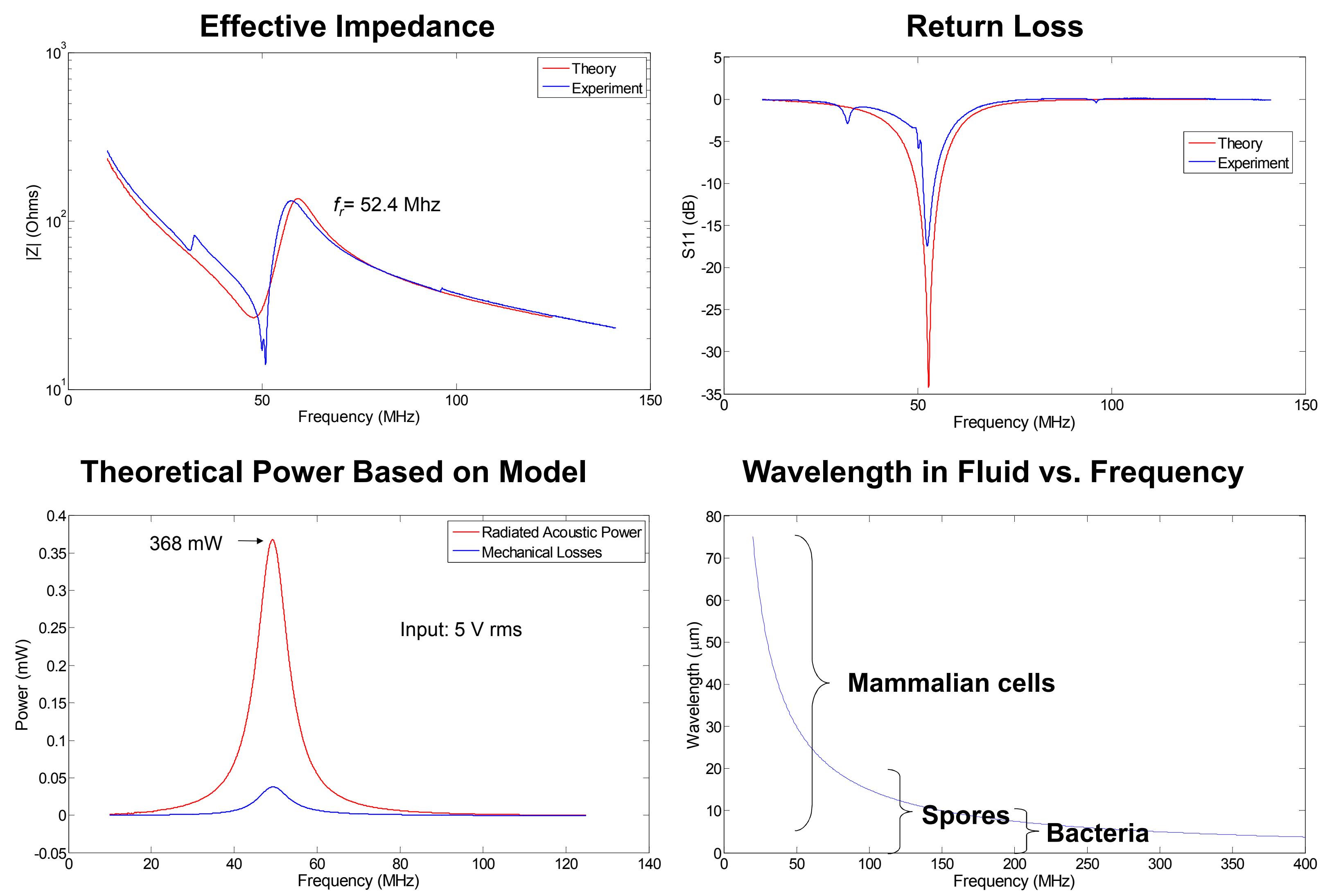
β : ωv_f

a : film thickness

Additional Layers (Z_r, Z_l):

load
intermediate
 $Z^+ = Z_o \frac{Z_L + Z_o \tanh(\gamma a)}{Z_o + Z_L \tanh(\gamma a)}$

2) 54 MHz LNO BAW Transducer:



Theory

54 MHz Lithium Niobate (LNO) BAW Transducer:

$$d = 3 \text{ mm} \Rightarrow A = 7.1 \cdot 10^{-6} \text{ m}^2$$

$$C_o = 46 \text{ pF}$$

$$\epsilon_{33} = 5.3 \text{ F/m}$$

$$h_{33} = 1.57 \cdot 10^{10} \text{ N/C}$$

$$k_f^2 = 0.33$$

$$V_f = 7340 \text{ m/s}$$

$$Z_o = 34 \cdot 10^7 \text{ Rayls}$$

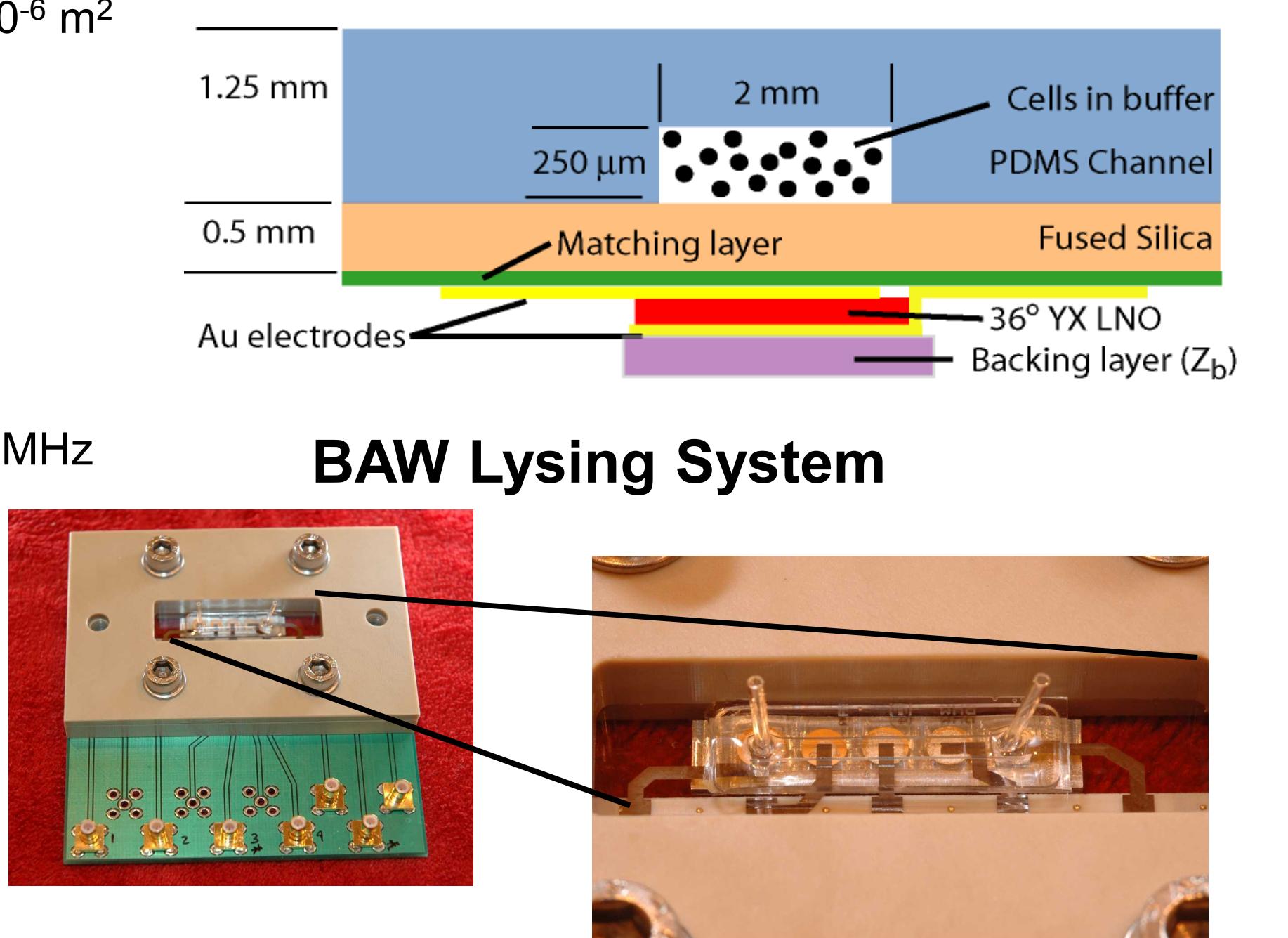
$$\rho_f = 4650 \text{ kg/m}^3$$

$$\alpha_o = 1.3 \text{ Np/m at } f_o = 1.5 \text{ MHz}$$

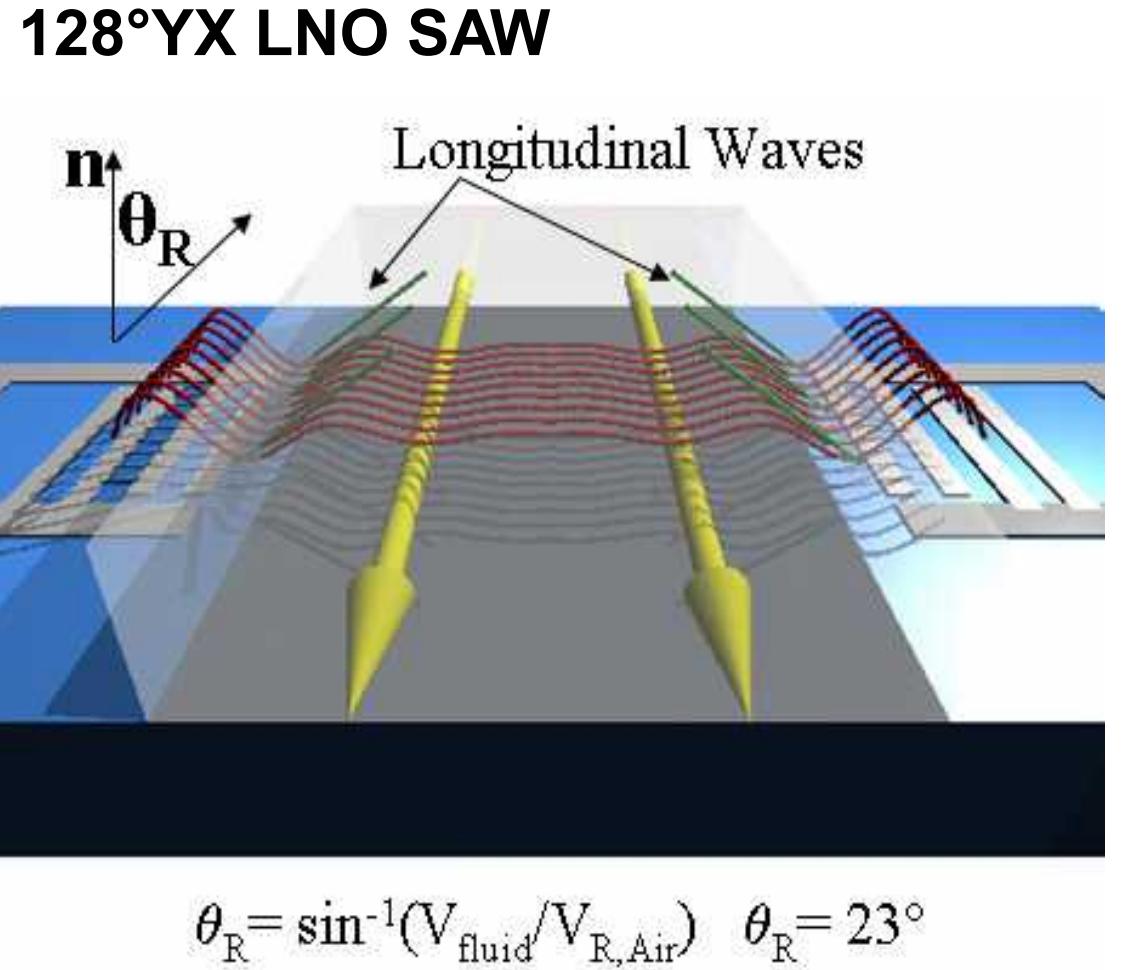
$$t = 15 \mu\text{m}$$

$$\epsilon = 38\epsilon_0$$

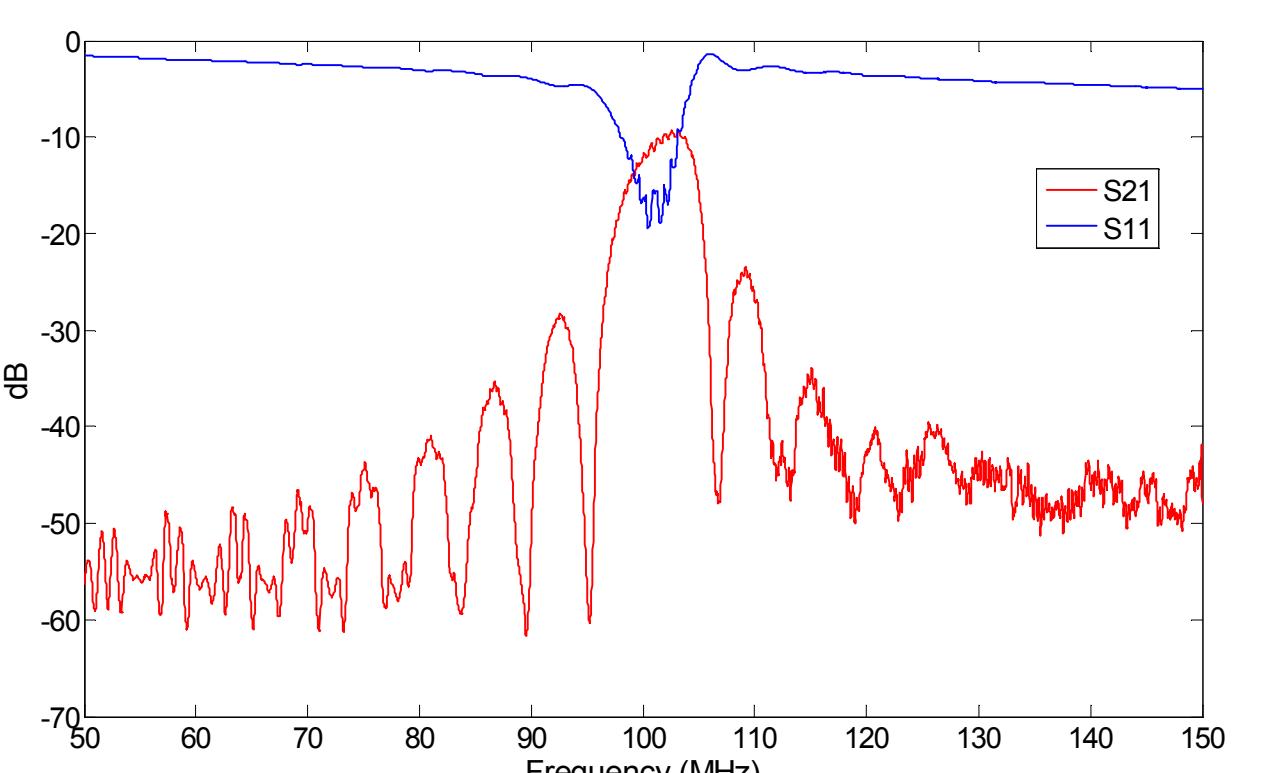
$$n = 1.5$$



98 MHz LNO SAW Transducer:

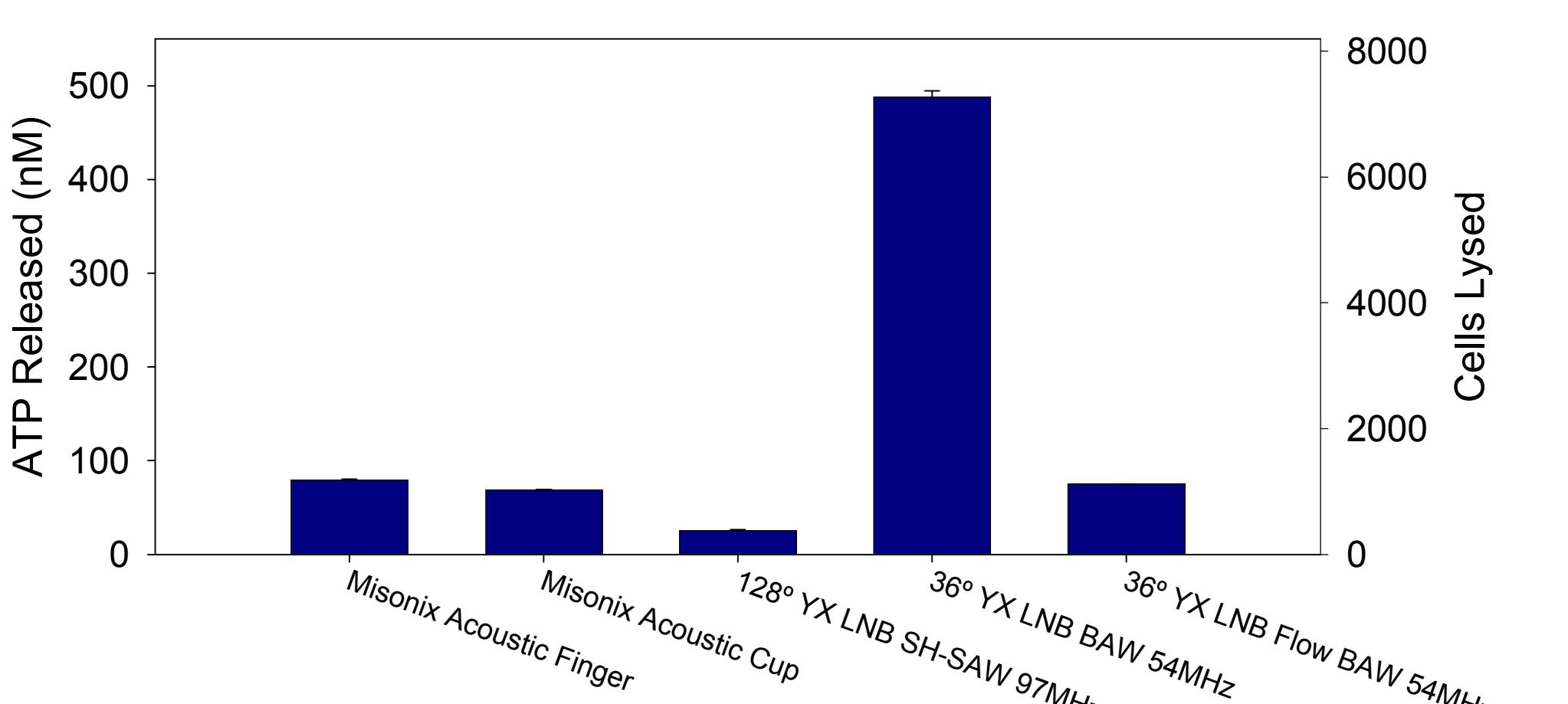


Results

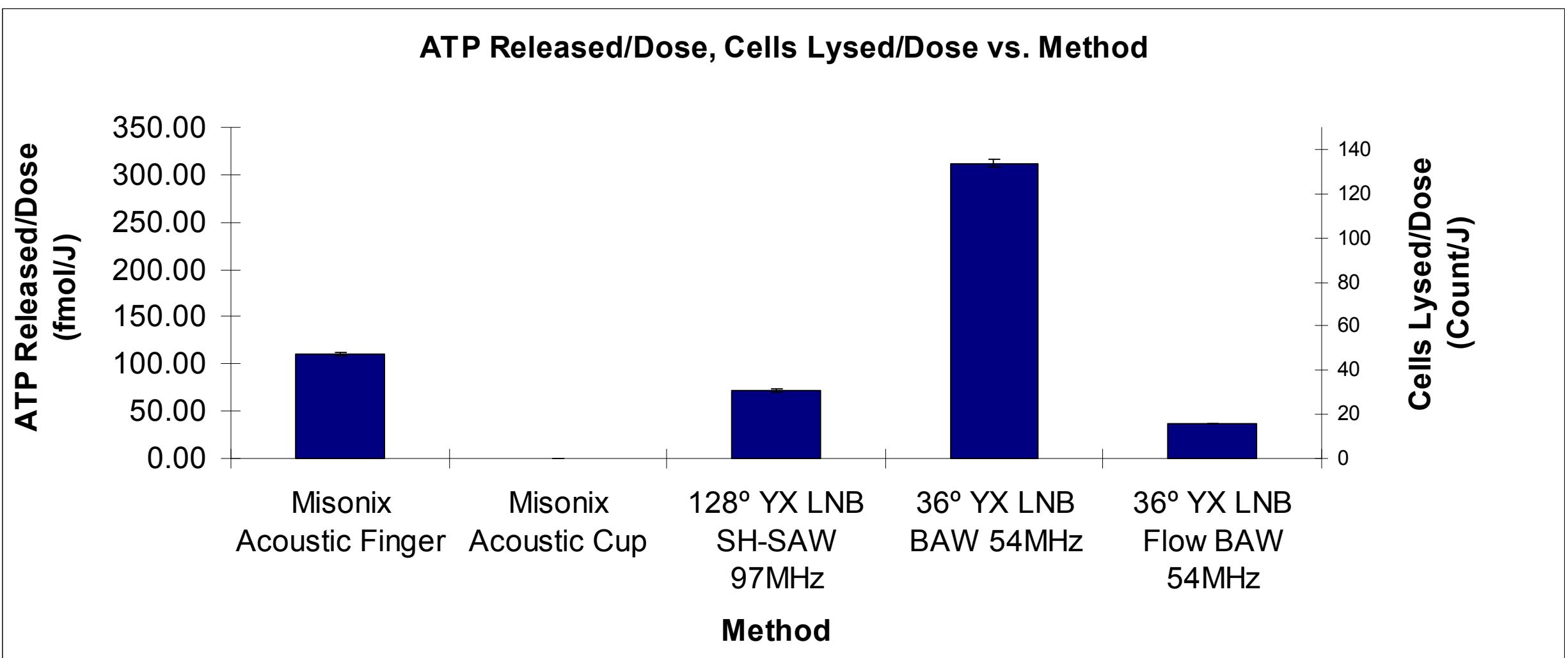


Comparison of Cell Lysing Methods: Benchtop vs. Microlysing System

ATP Released, Cells Lysed vs. Method

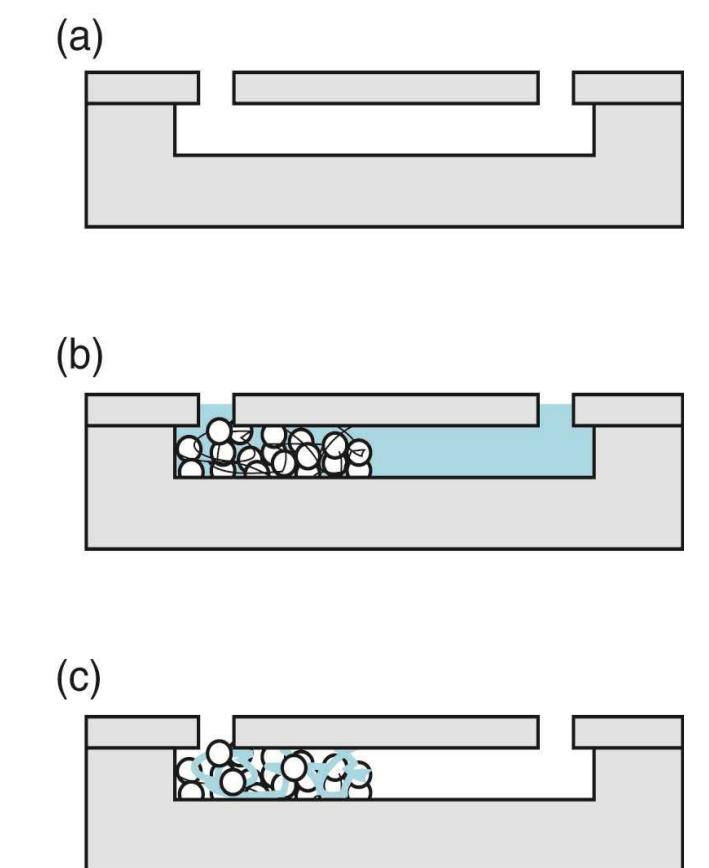


ATP Released/Dose, Cells Lysed/Dose vs. Method

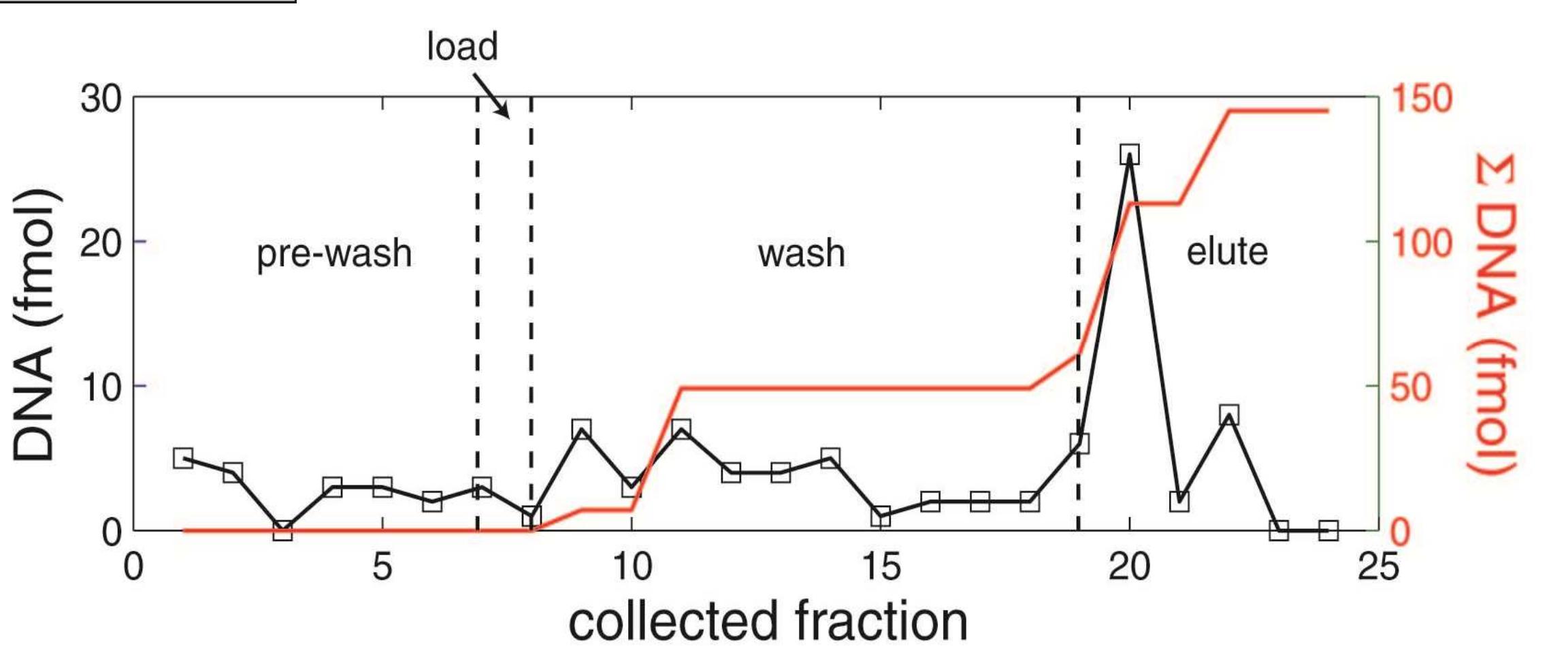
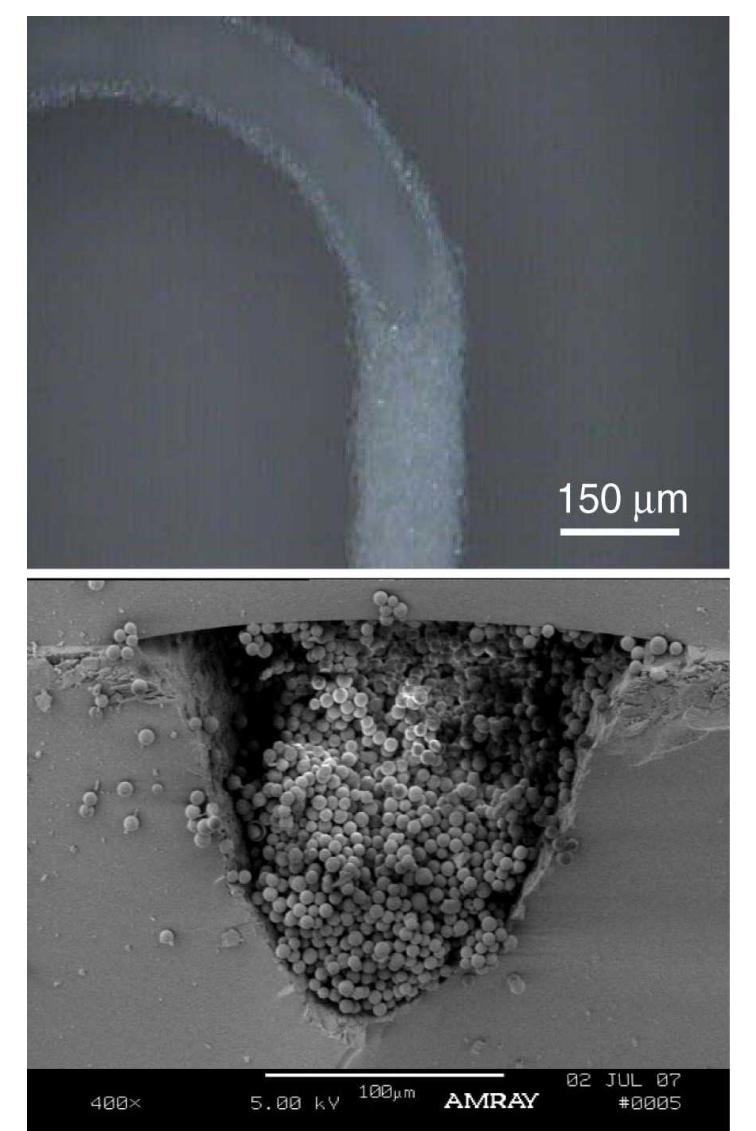


DNA Extraction:

- Fabricate encapsulated glass microfluidic device
- Inject sol-gel-silica bead slurry
- Dry sol-gel with heat (100 °C for 3 hours)



End of the packed bed section of sol-gel immobilized silica beads (5 μm) in a channel (top). SEM of the cross-section of a packed bed section of a channel (bottom).



Extraction profile (black) and cumulative extraction (red) of DNA from a packed bed device as a function of collected fraction. Total DNA injected = 250 fmol, yielding an extraction efficiency of 100/250 = 40% (the 50 fmol eluted during the wash is not included in the efficiency calculation). Minimum detected concentration ~10 fmol.

Future Work

- Determine lysing efficacy for additional flow rates and conditions.
- Optimize DNA microchannel for handling a wide range of sample types.
- Determine lysing conditions for other biological samples.
- Integrate lysing with the DNA extraction microchannel.