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## Investigation of Cavitation as a Brain Injury Mechanism in Blast Exposure

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# Blast-Induced Traumatic Brain Injury (TBI) Background

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- **Closed-Head Blast Injuries** are leading cause of traumatic brain injury (TBI) in military personnel returning from combat [1,2]
  - Latest statistics show 267,000 US warfighters sustained TBI
  - 69% as a result of IED blast exposure in Iraq & Afghanistan
- **Sandia Focus:** Primary Blast Injury (caused by direct blast exposure)
  - Investigate early-time wave mechanics leading to localized brain injury
  - Previous work suggests shear stress & deviatoric shear energy correlate with localized brain injury identified in clinical TBI study
  - Separate work suggests intracranial cavitation may also cause brain injury
- **Research Approach:**
  - Develop Equation-of-State (EOS) model to capture cavitation phenomena in water & water-bearing soft tissue
  - Conduct macroscale simulations of blast exposure using Cavitation EOS
    - Identify local hydrodynamic conditions that give rise to intracranial cavitation
    - Identify specific brain regions experiencing cavitation phenomenon
  - Create micromechanical models to investigate details of cavitation-induced damage

[1] Defense & Veterans Brain Injury Center TBI numbers: DoD numbers for traumatic brain injury, 2010.

[2] Fischer, H., 2007, United States Military Casualty Statistics: Operation Iraqi Freedom and Operation Enduring Freedom, Congressional Research Service Report RS22452.

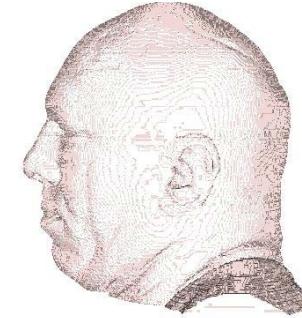
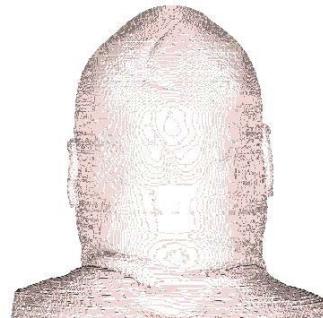


# TBI Macroscale Modeling & Simulation

## Head-Neck Model

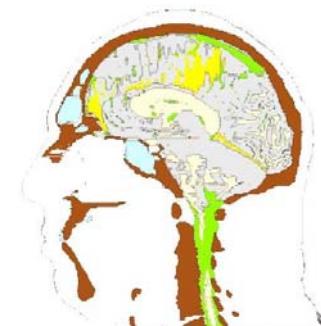
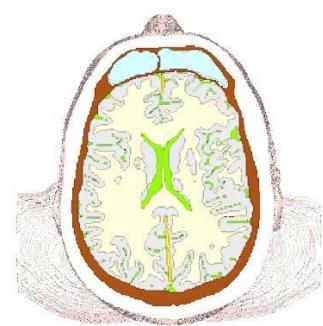
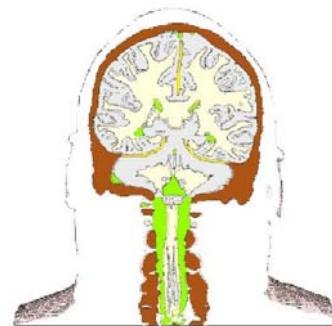
- **Finite volume model** developed from Visible Human Project [3] data
  - Constructed from 256 1mm-thick, axial anatomical slices of human male from the VHP
  - Anatomically correct distributions of white & gray brain matter, cerebral spinal fluid, bone, falx & tentorium membranes, muscle/scalp

Full Model  
 Images:



Model Size:  
 5.9M Cells

Coronal, Axial,  
 & Sagittal Cuts:



[3] National Institutes of Health, 2007, "The Visible Human Project," National Library of Medicine  
[http://www.nlm.nih.gov/research/visible/visible\\_human.html](http://www.nlm.nih.gov/research/visible/visible_human.html)



# TBI Macroscale Modeling & Simulation

## Constitutive Models

- Biological Materials:
  - White & Gray Matter – Mie-Gruneisen EOS, Viscoelastic models [4]
    - M-G EOS being replaced by Tillotson-Brundage Cavitation EOS [5]
  - Bone - Linear Elastic model w/ Fracture [4,6]
  - Falx & Tentorium (membranes) –Elastic models [4]
  - Muscle & Scalp - Elastic models [4,7]
  - Cerebral Spinal Fluid (CSF) – Mie-Gruneisen EOS
    - Being replaced by Tillotson-Brundage Cavitation EOS
  - Sinus Air (and surrounding air) - Non-linear Compressible EOS

- [4] Zhang, L., Yang, K.H., & King, A.I., 2001, "Comparison of Brain Responses between Frontal and Lateral Impacts by Finite Element Modeling," *J. Neurotrauma* **18**(1), pp. 21-30.
- [5] Brundage, A. L., 2013, "Prediction of Shock-Induced Cavitation in Water," Proc. 2013 APS Shock Compression of Condensed Matter, Seattle, WA.
- [6] Carter, D.R., 1985, "Biomechanics of Bone," *Biomechanics of Trauma*, Appleton-Century-Crofts, Norwalk, CT, pp. 135-165.
- [7] Mak, A.F.T. & Zhang, M., 1998, "Skin and Muscle," in *Handbook of Biomaterial Properties*, ed. J. Black & G. Hastings, Chapman & Hall, London, pp. 66-69.



## Modeling & Simulation Methodology & Validation

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- **Simulation Methods**

- Eulerian methods using CTH (w/ finite volume model)
  - Blast, Projectile Penetration
- Lagrangian methods using Presto (w/ finite element model)
  - Blunt Impact, Imposed kinematic conditions (e.g. acceleration)
- Lagrangian-Eulerian coupled methods using Presto/CTH (w/ finite element model)
  - Blast (greater accuracy than Eulerian description)

- **Head/Neck Model Validation**

- Compared Simulation predictions with laboratory data
  - Magnetic Resonance Tagging & Elastography data on the human head (in vivo) courtesy of Prof. Philip Bayly research team, Washington University at St. Louis, MO USA [8,9]

[8] Sabet A.A., Christoforou E., Zatlin B., Genin, G.M., Bayly, P.V., 2008, "Deformation of the Human Brain by Mild Angular Head Acceleration," *J. Biomech.*, **41**, pp. 307-315.

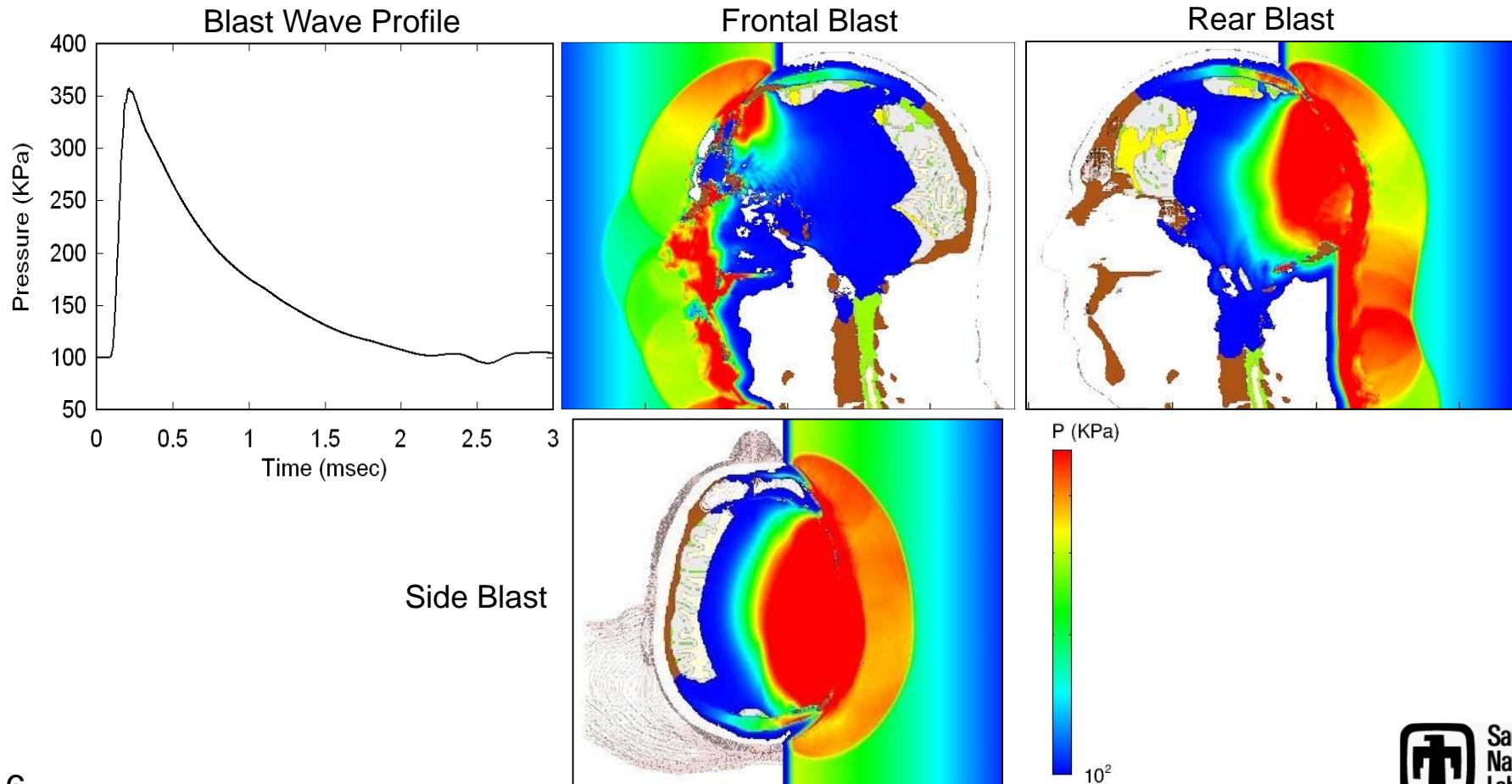
[9] Feng Y., Abney T.M., Okamoto R.J., Pless R.B., Genin G.M., Bayly P.V., 2010, "Relative Brain Displacement and Deformation during Constrained Mild Frontal Head Impact," *J. Roy. Soc. Interface*, **7**(53), pp. 1677-1688.



# TBI Modeling & Simulation

Example: 3.6 bar (360 KPa) Blast

Snap-Shot Images of Blast-Induced Pressure Wave Propagating through Head  
 Time ~ 130  $\mu$ s after blast wave encounters head





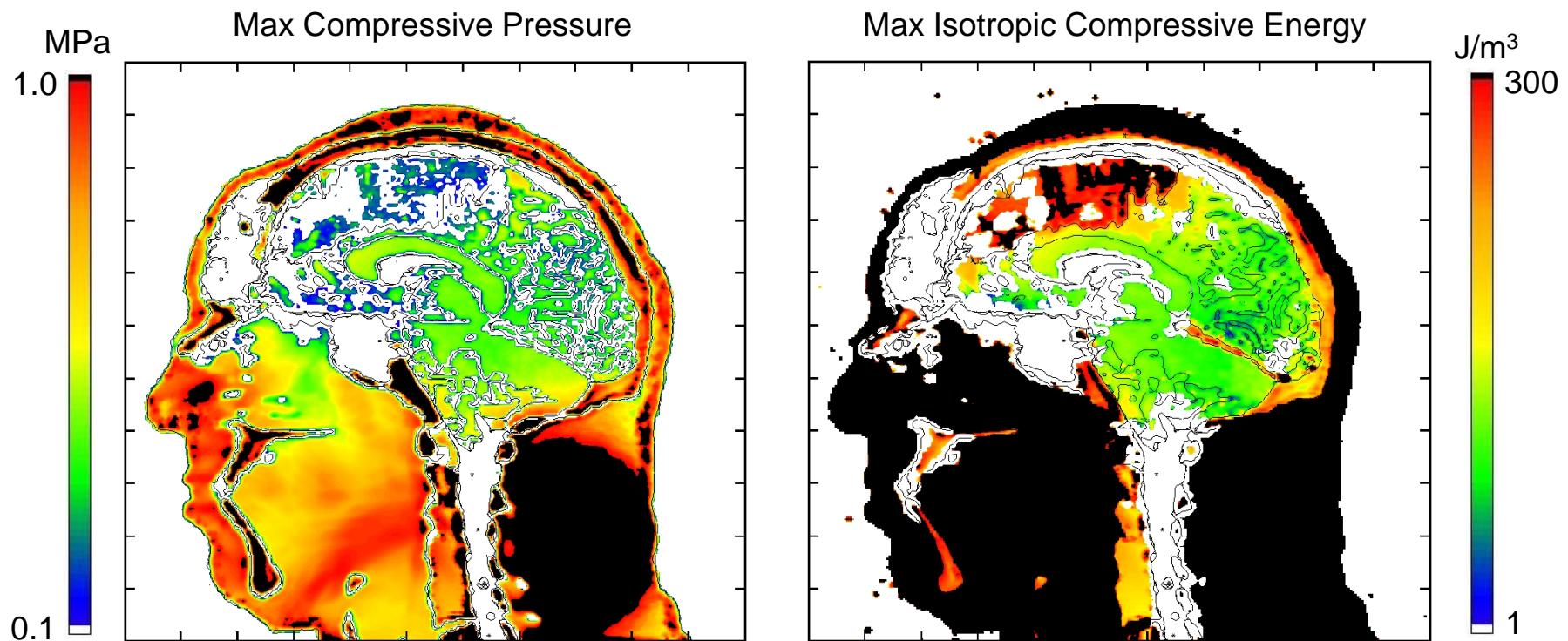
# TBI Modeling & Simulation

## 3.6 bar Frontal Blast Exposure: Compressive Pressure & Energy

**Max Pressure & Isotropic Compressive Energy (ICE) associated with Crush**

- No known correlation with local tissue injury

$$ICE = Pos \left[ \int P \frac{d\rho}{\rho} \right]$$





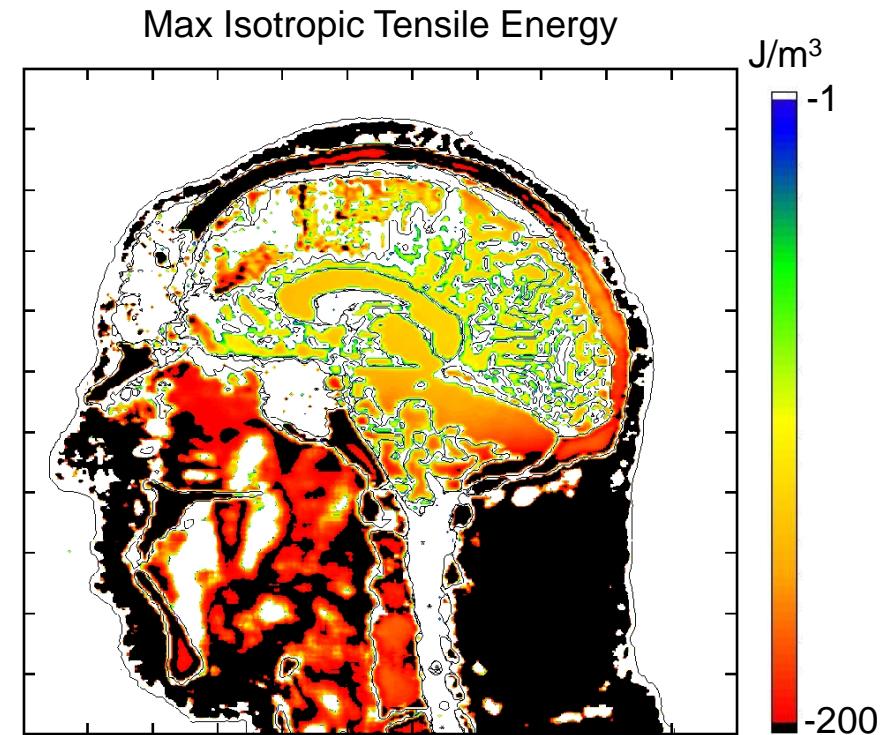
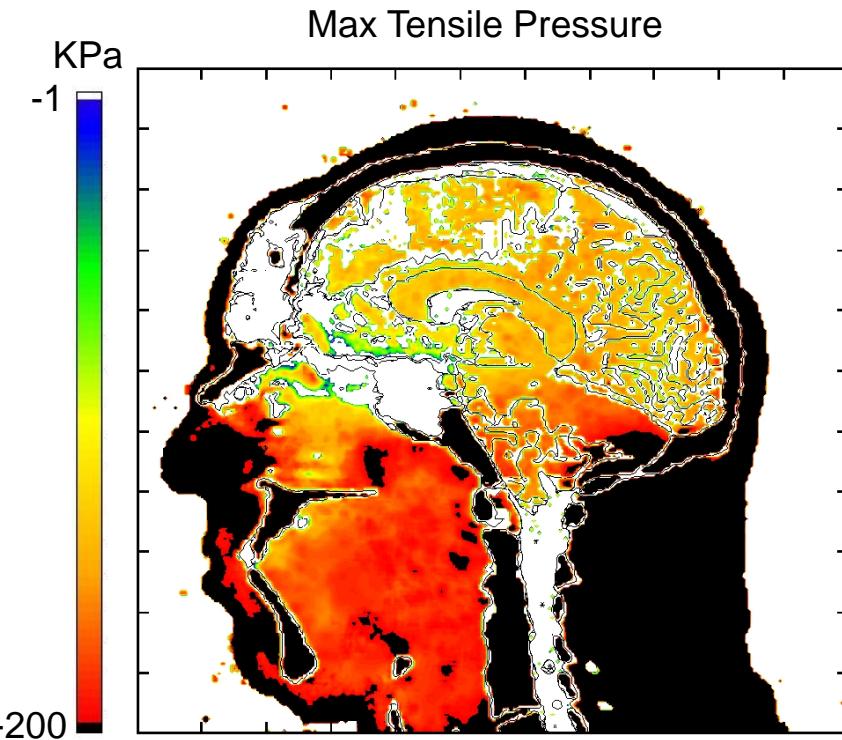
## TBI Modeling & Simulation

### 3.6 bar Frontal Blast Exposure: Tensile Pressure & Energy

Max Tensile Pressure & Isotropic Tensile Energy (ITE) associated with volumetric Dilatation & possibly Cavitation

- Suspected tissue injury mechanism

$$ITE = Neg[\int P \frac{d\rho}{\rho}]$$





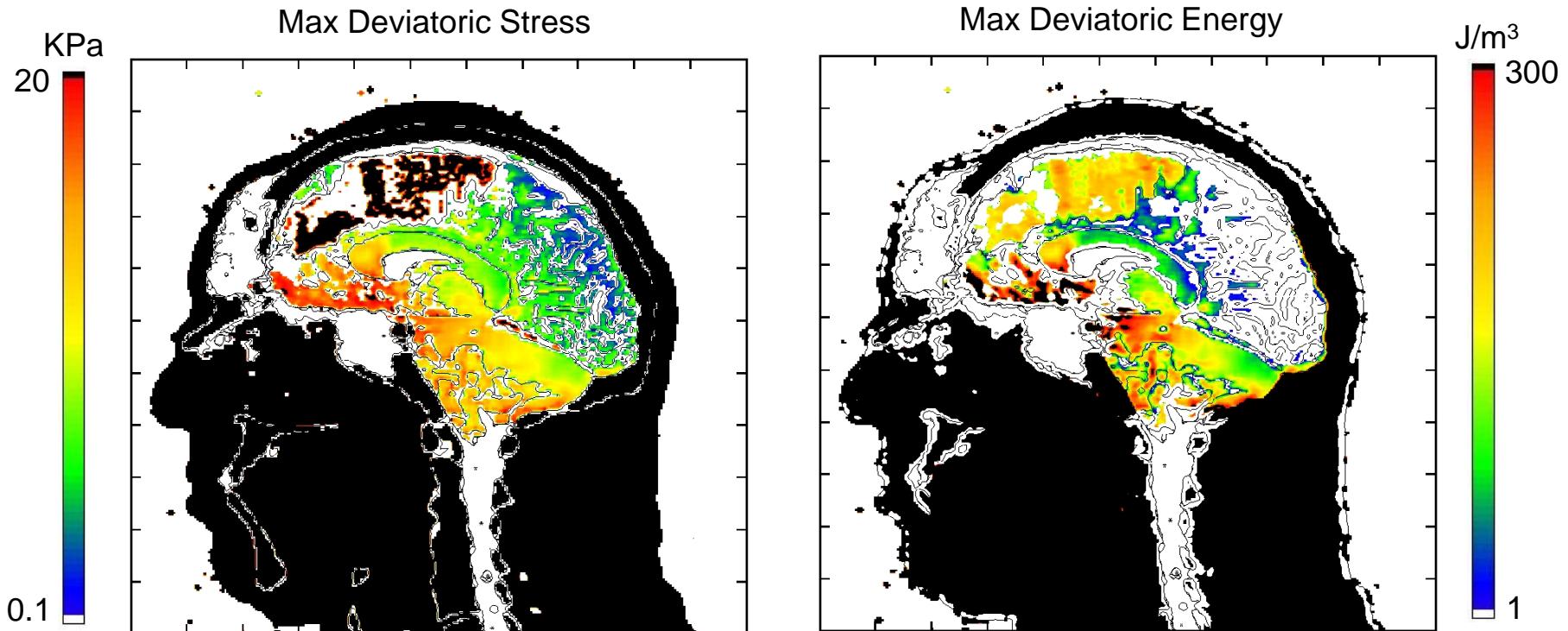
## TBI Modeling & Simulation

### 3.6 bar Frontal Blast Exposure: Deviatoric (Shear) Stress & Energy

**Max Deviatoric Stress & Energy (DSE) associated with Shear & Tearing**

- Suspected tissue injury mechanism
  - Cytoskeleton disruption & membrane rupture

$$DSE = \int \text{tr}(\mathbf{Sd})dt$$





## Blast-Induced TBI Research Summary

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- **Completed Work:**

- Combined simulation & clinical study of TBI blast subjects suggest possible correlation [10]
  - Between maximum deviatoric (shear) stress & energy with local regions of brain hypoactivity in TBI subjects
  - Simulation predictions also show localized regions in brain experiencing elevated levels of tensile pressure and energy
    - Possible Cavitation
  - Cavitation hypothesized to cause local injury leading to TBI [11-13]
    - Collapse of bubbles formed in fluid cause local shock wavelets that could damage surrounding tissue
  - **Need exists to model intracranial cavitation in simulations**

[10] Taylor P.A., Ludwigsen J.S., Vakhtin A.A., Ford C.C., 2013, "Simulation and Clinical Assessment of Blast-Induced Traumatic Brain Injury," *Neurotrauma Letter*, submitted.

[11] Lubock P., Goldsmith W., 1980, "Experimental Cavitation Studies in a Model Head-Neck System, *J. Biomech.* **13**, pp. 1041-1052.

[12] Brennen C.E., 2003, "Cavitation in Biological and Bioengineering Contexts," *Proc. 5<sup>th</sup> Int. Symp. Cavitation*, Osaka, Japan.

[13] Nakagawa A., Fujimura M., Kato K., Okuyama H., Hashimoto T., Takayama K., Tominaga T., 2008, "Shock Wave-Induced Brain Injury in Rat: Novel Traumatic Brain Injury Animal Model, *Acta Neurochir. Supp.* **102**, pp.421-424.

## Tillotson-Brundage Cavitation EOS Model Cavitation Description



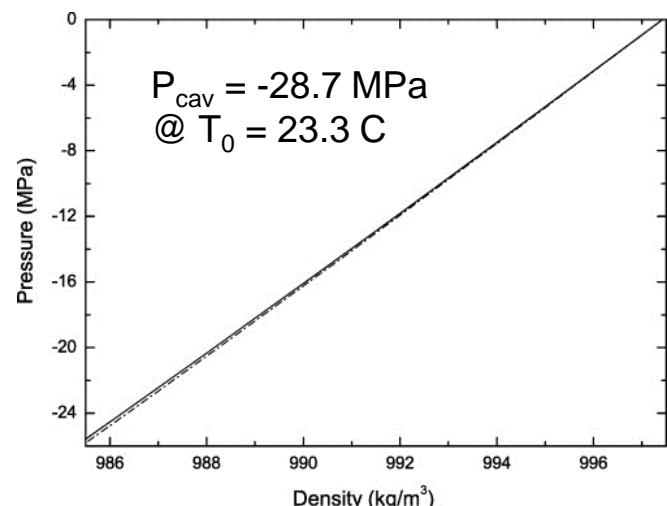
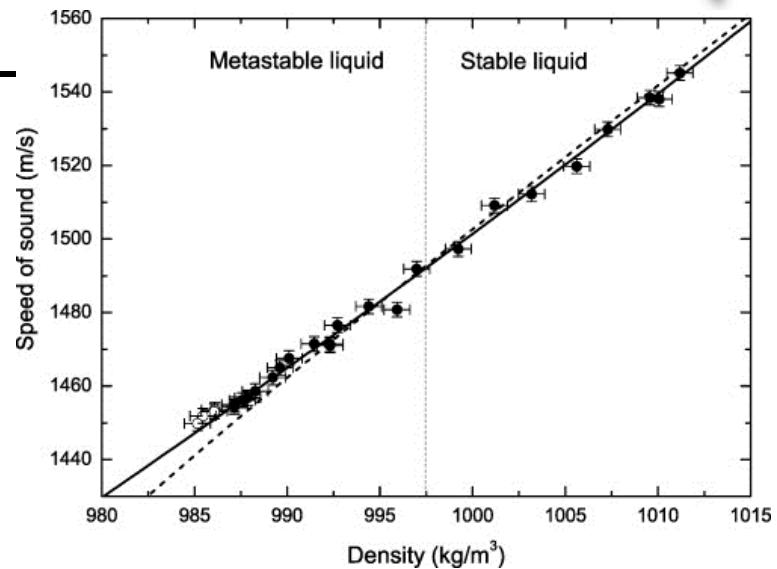
- Manifests as individual vapor bubbles or large (steady or unsteady) cavities that contain air or water vapor; both can quickly cause damage (and noise) upon collapse
- Occurs locally from release to pressures near vapor pressure of liquid (boiling at ambient T)
- Represents a two-phase flow comprising of the liquid and its vapor (or other dissolved gasses)





## Understanding Water “Stretch”<sup>a</sup>

- *Stable* pressure state in fluids is positive
- If the local pressure drops below vapor pressure, fluid *cavitates*
- Experimental research demonstrates that water can “stretch” in a *metastable* state and sustain negative pressures *before* cavitation
- New EOS permits fluid to stretch to metastable states (negative pressures)  $P < P_{\text{cav}}$ ; then fluid returns to stable (positive) vapor pressure
- Modeling approach consistent with experimental evidence of vapor bubbles appearing once  $P < P_{\text{cav}}$



<sup>a</sup>Davitt *et al.*, J. Chem. Phys. 133, 174507 (2010)



## Tillotson-Brundage EOS Development<sup>a,b,c,d,e</sup>

<sup>a</sup>Tillotson, General Atomic Report GA-3216, (1962)

<sup>b</sup>Anderson et al., Int. J. Imp. Engrg. 9, (1990)

<sup>c</sup>Ahrens & O'Keefe, Int. J. Imp. Engng. 5, (1987)

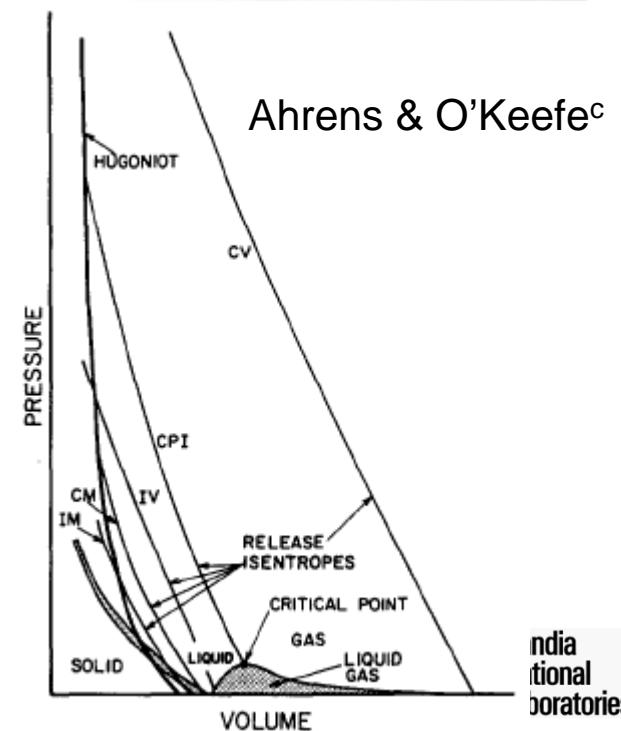
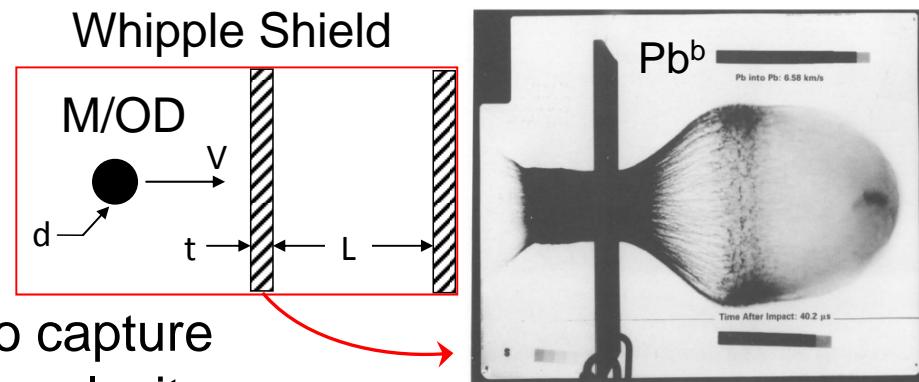
<sup>d</sup>Ahrens & O'Keefe, Imp. and Explosion Cratering (1977)

<sup>e</sup>Brundage, Procedia Engng (2012)

- Two-phase, Tillotson EOS meant to capture vaporization upon release for hypervelocity impacts<sup>a</sup> of metals
- Single equation for compression ( $\rho \geq \rho_0$ ) and different one for expansion ( $\rho < \rho_0$ )
- No polymorphic phase transformations

### Key Model Revisions by Brundage

- Filled gaps in  $\rho$  -  $E$  space
  - Added new *tensile* regions
  - Significant updates to expansion region<sup>e</sup>
- Cavitation model added for liquids<sup>e</sup>

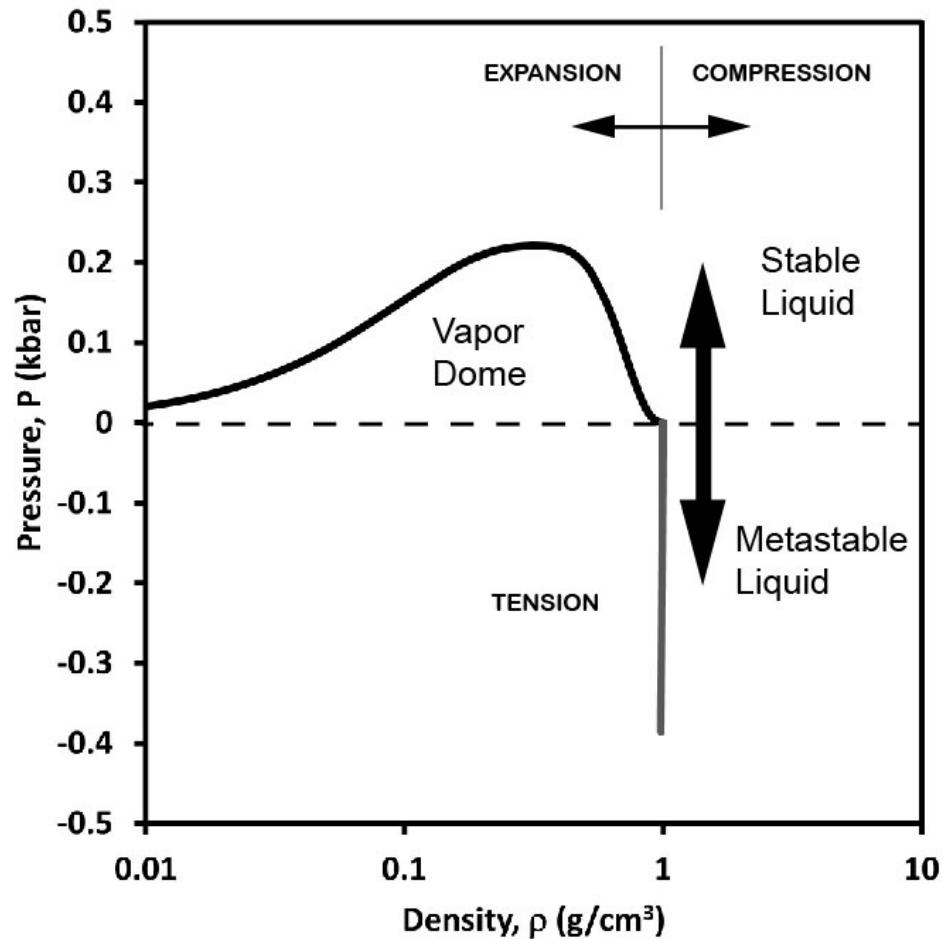




## New EOS for Shock-loaded Metastable Fluids

- Extend Tillotson EOS to capture tension and cavitation in fluids
- EOS fit to general form in compression, expansion, and tension

$$P(\rho, E) = \left[ a + \frac{b}{\frac{E/E_0}{(\rho/\rho_0)^2} + 1} \right] \rho E + f(\rho)$$





## Shock Hugoniot Results

- Compare shock end states to available data
- Modified Tillotson, MGR, and SESAME EOS

EOS surface in compression

$$P(\rho, E) = \left[ a + \frac{b}{\left( E / (E_0 \eta^2) + 1 \right)} \right] \rho E + A\mu + B\mu^2 \quad (\rho \geq \rho_0, E \geq 0)$$

Assume end states in thermodynamic equilibrium:  $E = E_H$ ,  $P = P_H$

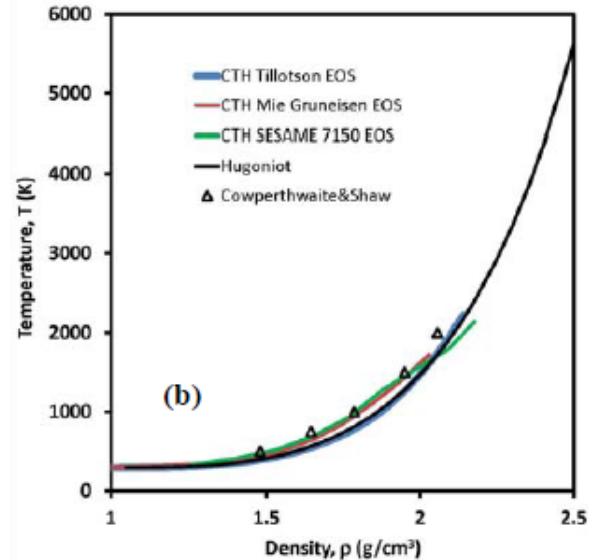
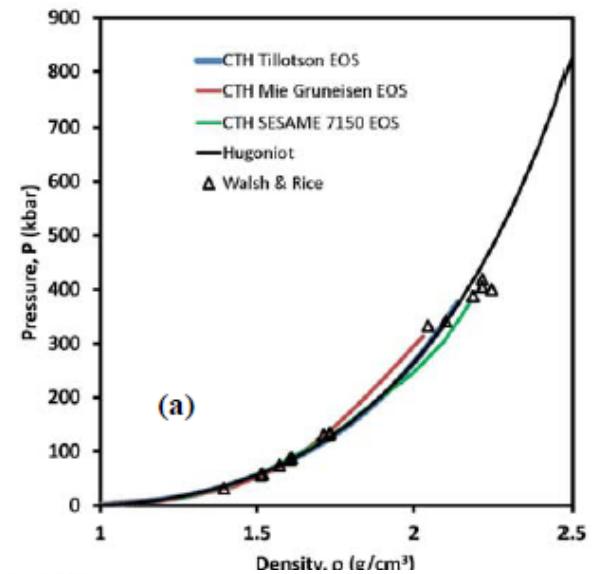
$$E_H(\rho) = \frac{1}{2} P_H(\rho) \left[ \frac{1}{\rho_0} - \frac{1}{\rho} \right]$$

$a, b, E_0, A, B$  adjusted for best fit to data

Solve for  $P_H$ ,  $T_H$

$$P_H(\rho) = \frac{-b_H + \sqrt{(b_H^2 + 4a_H c_H)}}{2a_H} \quad T_H(\rho) = T_0 + \frac{E_H(\rho) - E_C(\rho)}{C_V} \quad (\rho \geq \rho_0)$$

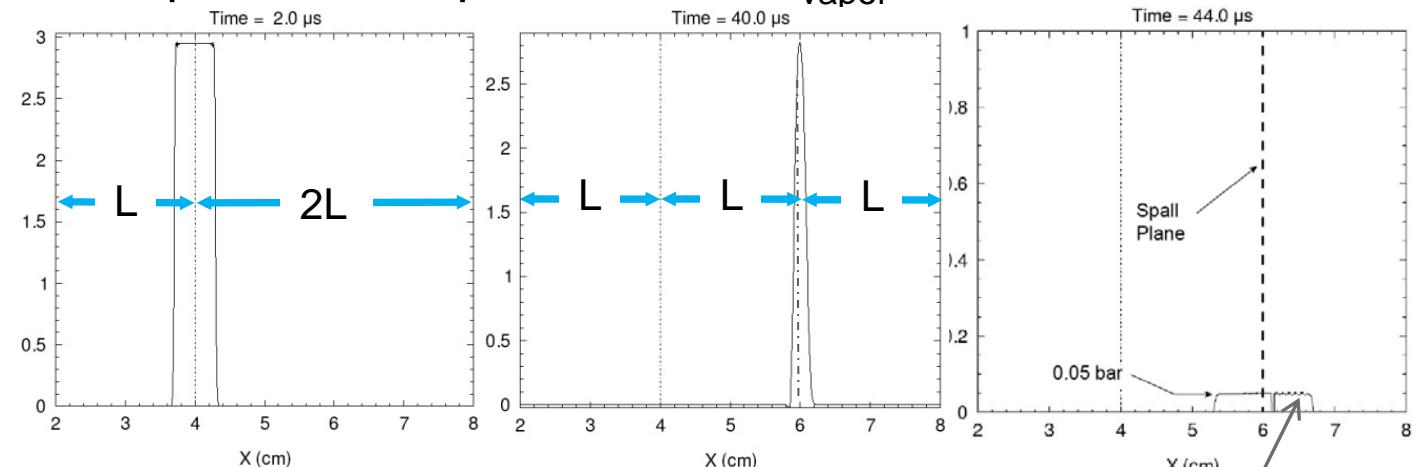
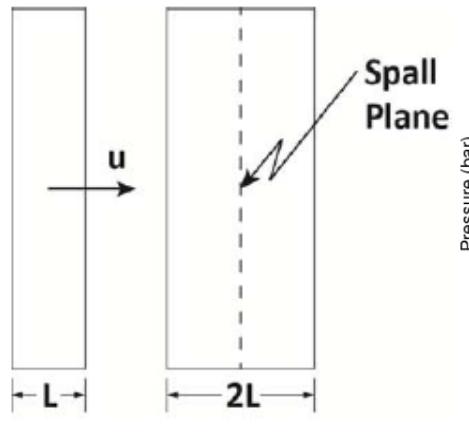
$$\frac{dE_C}{d\rho} = \frac{P(\rho, E_C)}{\rho^2} \quad (\text{at } \rho = \rho_0, E_C = 0)$$





# Cavitation Model Testing

- Cavitation process is ‘liquid spall’ where water in metastable tensile state ruptures
- Evaluate w/1D computational spall experiment
- At spall plane, model produces vapor at stable  $P_{vapor}$



## Key Parameters

$$u = 40 \text{ cm/s}$$

$$L = 2 \text{ cm}$$

$$P = 2.95 \text{ bar (calc)}$$

$$P_{\text{vap}} = 0.05 \text{ bar}$$

## Impact Plane

# Spall Plane

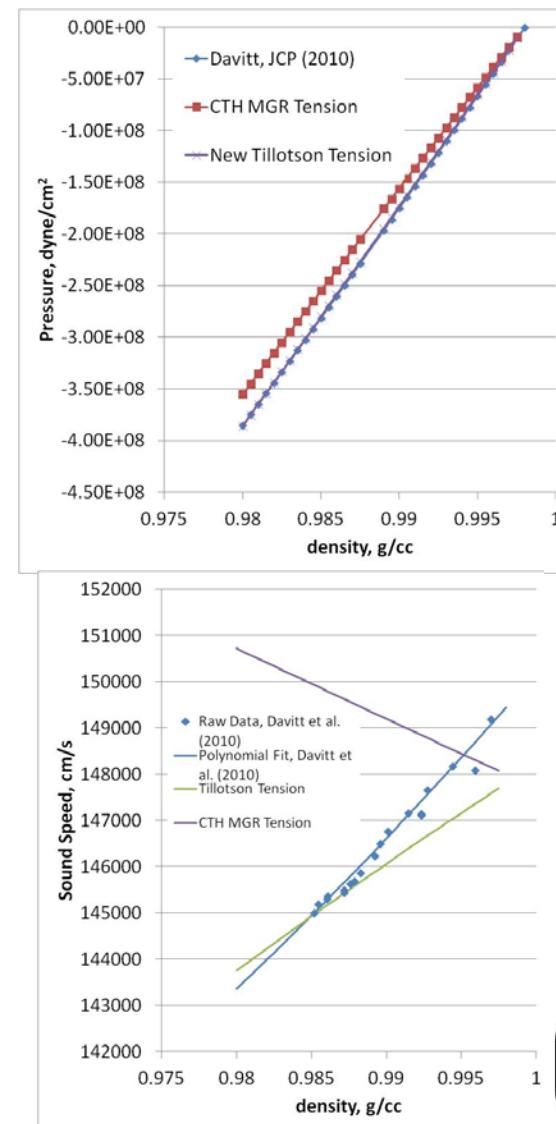
# Cavitation

## Tillotson-Brundage EOS Results



## Evaluate new EOS surface for tension with water data

- *Mie-Gruneisen (MGR) EOS* in CTH, previously used to model biological materials
- In tension, MGR EOS underpredicts tensile stress state in water and has wrong trend in sound speed
- New model for all materials fits pressure data for water but underpredicts sound speed, although gets correct trend





## Tillotson-Brundage Cavitation EOS Development Summary

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- New EOS for water captures realistic physics of metastable stretching before cavitating at stable vapor state
- Revised EOS development required adding tensile region for water (or water-like material)
- Generalize EOS in tension for fluidized soft tissue in human body
- Improvement in prediction of tensile states
- Models are being implemented in Sandia Shockwave Physics codes
  - CTH (Eulerian description)
  - Coupled CTH-PRESTO (Eulerian-Lagrangian description)



## Blast-Induced TBI Research Summary

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- **Current Work:**

- Conduct macroscale simulations of blast scenarios leading to TBI
  - Employ Brundage-Tillotson EOS to model cavitation in brain & CSF
- Identify intracranial regions experiencing cavitation
  - Parameterize local hydrodynamic conditions associated with cavitation

- **Future Work:**

- Develop micromechanical models of those regions in brain that experience cavitation
- Investigate details of brain tissue damage on microscale using hydrodynamic conditions defined from macroscale simulations

Questions?



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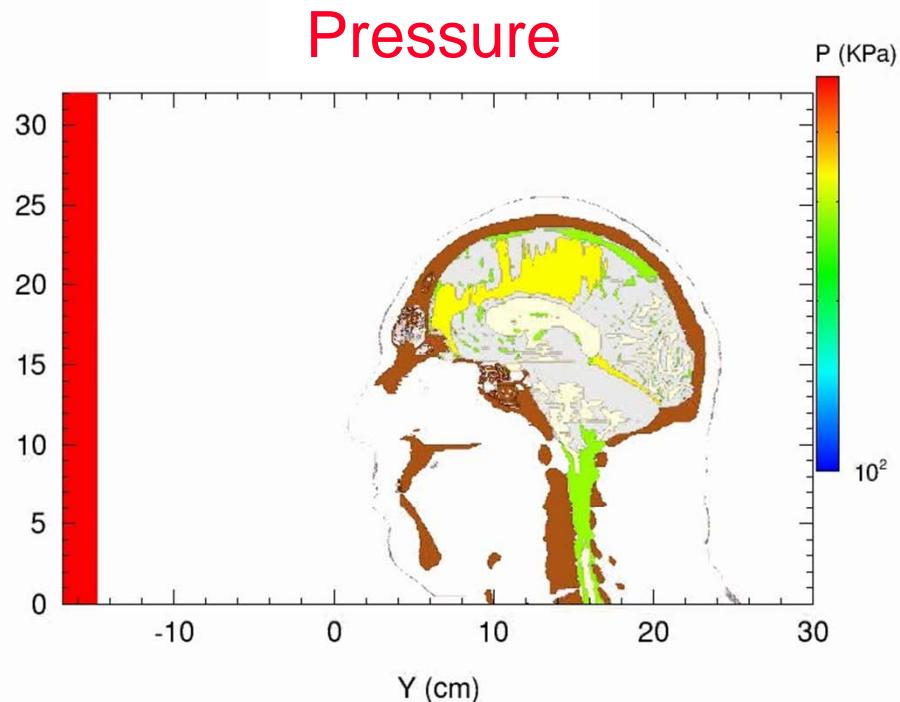
## Supplemental Slides



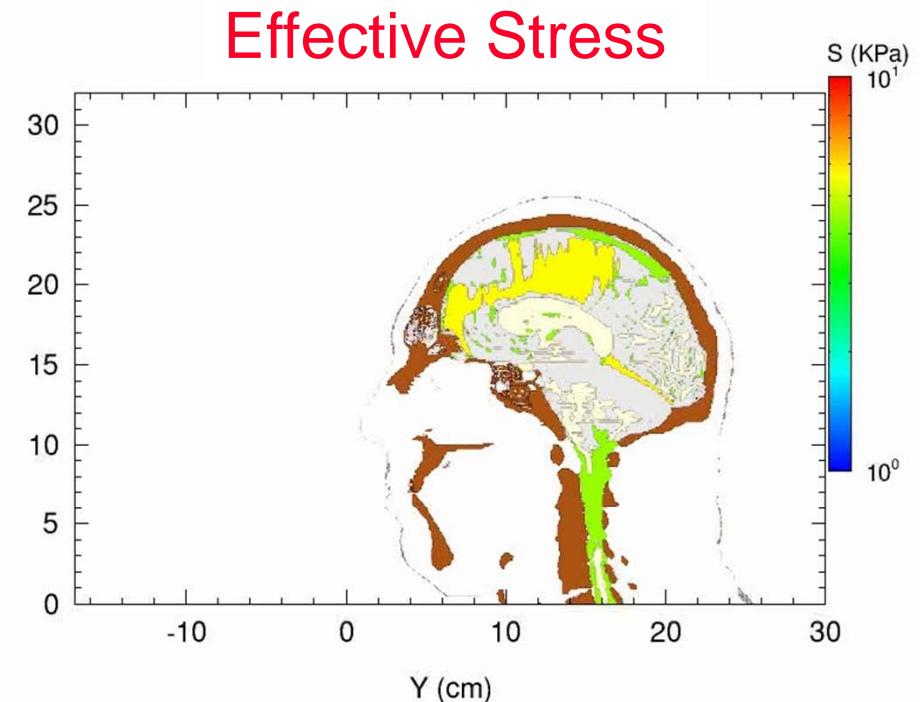
# TBI Modeling & Simulation

## 3.6 bar Frontal Blast Exposure: mid-Sagittal Plane

Pressure at 0.00e+00 sec



Eff. Stress at 0.00e+00 sec



Note: Run Videos Simultaneously

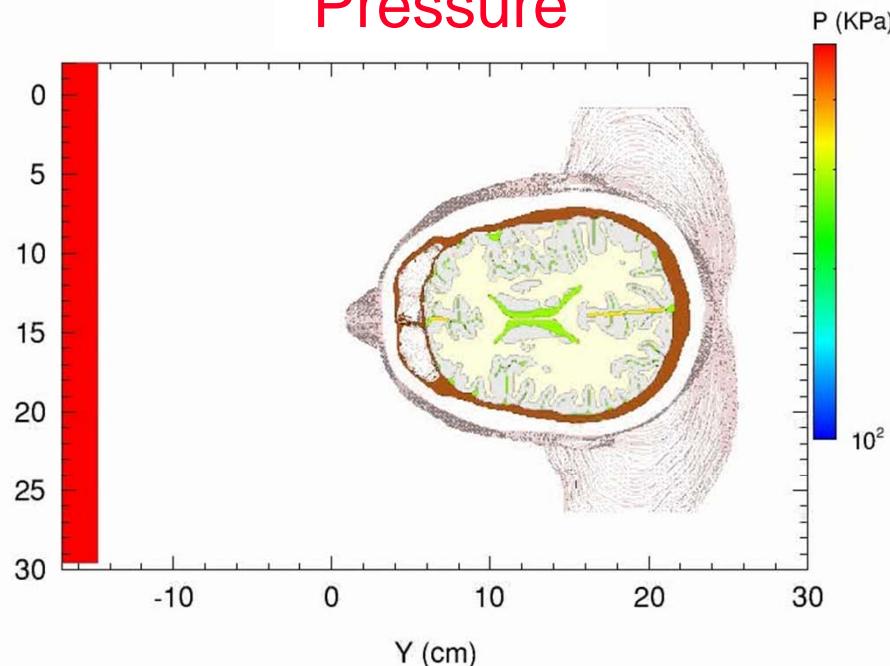


## TBI Modeling & Simulation

### 3.6 bar Frontal Blast Exposure: Axial Plane above Eyes

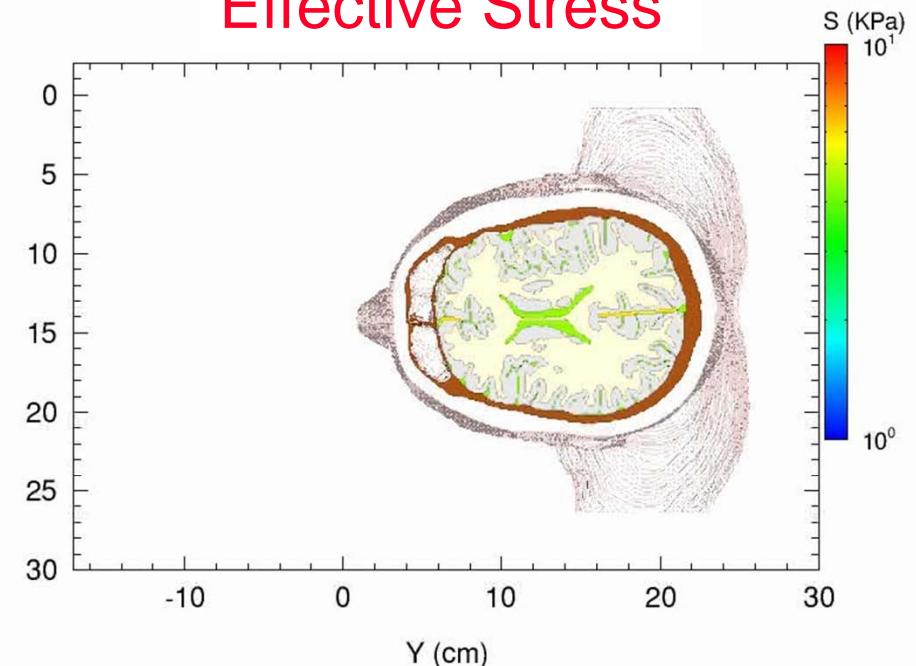
Pressure at 0.00e+00 sec

Pressure



Effective Stress at 0.00e+00 sec

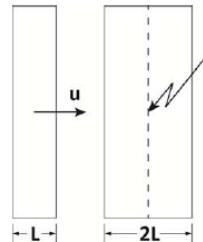
Effective Stress



Note: Run Videos Simultaneously



## Current SESAME EOS inadequate



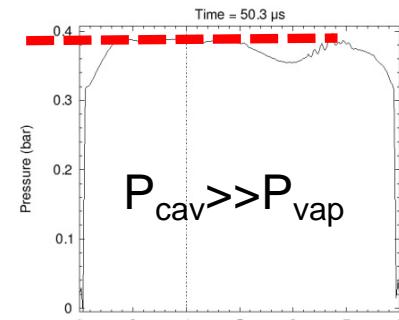
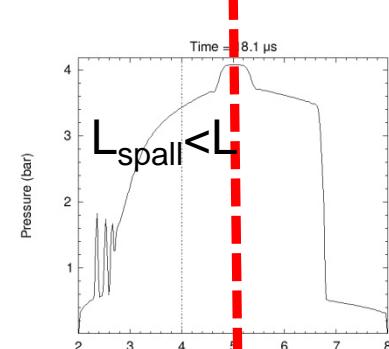
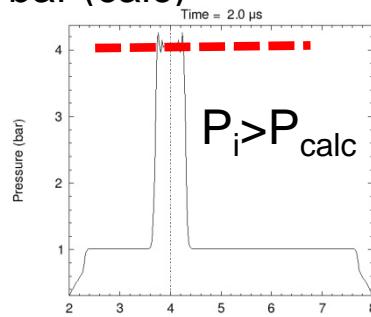
### Impact Conditions

$u = 40 \text{ cm/s}$

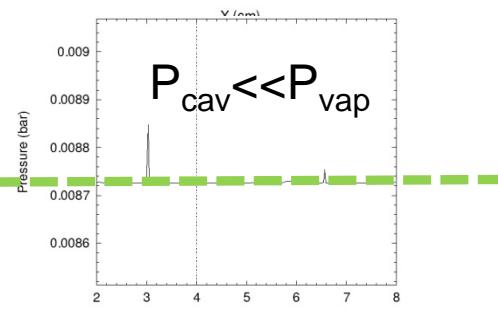
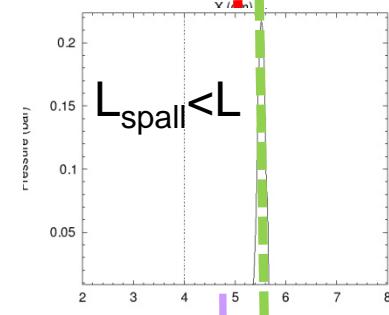
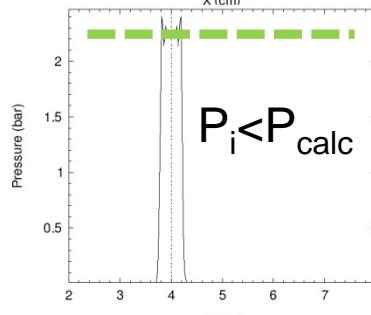
$L = 2 \text{ cm}$

$P = 2.95 \text{ bar (calc)}$

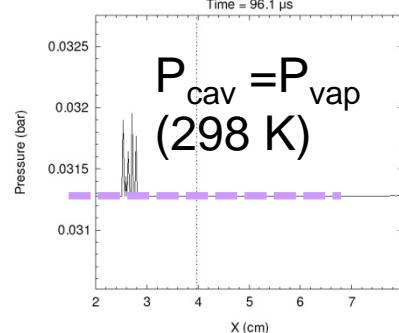
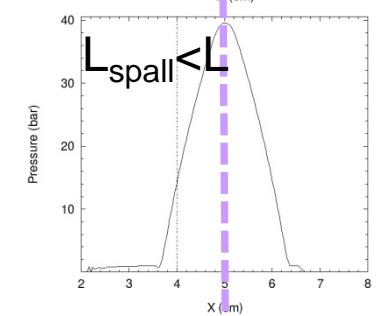
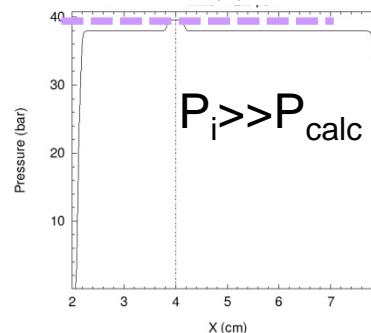
**SESAME  
7150  
(water)**



**SESAME  
7153 (water  
with vapor  
dome)**



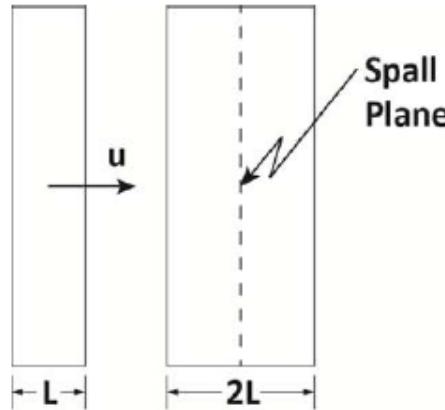
**Harvard (5  
phase EOS)**



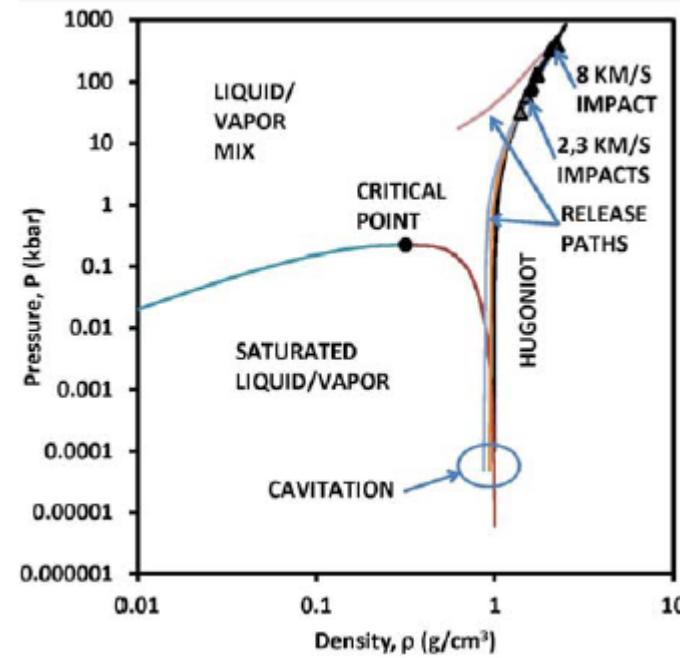


## Cavitation Processes on Phase Diagram

- At spall plane, release to vapor pressure at lower velocities
- Prompt vaporization at hypervelocity impacts



Key Parameters  
 $u = 2, 3, 8 \text{ km/s}$   
 $L = 2 \text{ cm}$   
 $P_{\text{vapor}} = 0.05 \text{ bar}$



Water Phase Diagram